

# Accepted Manuscript

Title: Continuous Theta Burst Stimulation Over the Dorsolateral Prefrontal Cortex and the Pre-SMA Alter Drift Rate and Response Thresholds Respectively during Perceptual Decision-Making

Author: Dejan Georgiev, Lorenzo Rocchi, Pierluigi Tocco, Maarten Speekenbrink, John C. Rothwell, Marjan Jahanshahi

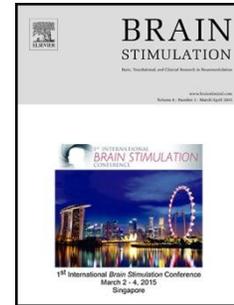
PII: S1935-861X(16)30054-7  
DOI: <http://dx.doi.org/doi: 10.1016/j.brs.2016.04.004>  
Reference: BRS 884

To appear in: *Brain Stimulation*

Received date: 24-7-2015  
Revised date: 6-4-2016  
Accepted date: 8-4-2016

Please cite this article as: Dejan Georgiev, Lorenzo Rocchi, Pierluigi Tocco, Maarten Speekenbrink, John C. Rothwell, Marjan Jahanshahi, Continuous Theta Burst Stimulation Over the Dorsolateral Prefrontal Cortex and the Pre-SMA Alter Drift Rate and Response Thresholds Respectively during Perceptual Decision-Making, *Brain Stimulation* (2016), <http://dx.doi.org/doi: 10.1016/j.brs.2016.04.004>.

This is a PDF file of an unedited manuscript that has been accepted for publication. As a service to our customers we are providing this early version of the manuscript. The manuscript will undergo copyediting, typesetting, and review of the resulting proof before it is published in its final form. Please note that during the production process errors may be discovered which could affect the content, and all legal disclaimers that apply to the journal pertain.



1 **Continuous theta burst stimulation over the dorsolateral prefrontal cortex and the**  
2 **pre-SMA alter drift rate and response thresholds respectively during perceptual**  
3 **decision-making**

4  
5 Dejan Georgiev<sup>1,2,3</sup>, Lorenzo Rocchi<sup>2,4</sup>, Pierluigi Tocco<sup>2</sup>,  
6 Maarten Speekenbrink<sup>5</sup>, John C. Rothwell<sup>2</sup>, Marjan Jahanshahi<sup>1,2</sup>

7  
8 <sup>1</sup> Cognitive Motor Neuroscience Group

9 <sup>2</sup>Sobell Department of Motor Neuroscience & Movement Disorders  
10 UCL Institute of Neurology

11 <sup>3</sup>Department of Neurology, University of Ljubljana

12 <sup>4</sup>Department of Neurology and Psychiatry, Università di Roma “Sapienza”

13 <sup>5</sup>UCL Cognitive, Perceptual and Brain Sciences, Division of Psychology and Language  
14 Sciences, London, UK

15  
16  
17 *Dejan Georgiev, MD, PhD*

18 Sobell Department of Motor Neuroscience and Movement Disorders, Institute of  
19 Neurology, University College London, 33 Queen Square, London WC1N 3BG &

20 Department of Neurology, University of Ljubljana, Zaloška cesta 2, 1000 Ljubljana,

21 Slovenia. E-mail: [dejan.georgiev@kclj.si](mailto:dejan.georgiev@kclj.si) ; [dgeorgiev@ucl.ac.uk](mailto:dgeorgiev@ucl.ac.uk) ;

22 [georgievdejan@gmail.com](mailto:georgievdejan@gmail.com) ; Phone: +44 7719 798 853; Contributions: Designed

23 research, Performed research, Analyzed data, Wrote the paper.

24 *Lorenzo Rocchi, MD*

25 Sobell Department of Motor Neuroscience and Movement Disorders, Institute of  
26 Neurology, University College London, 33 Queen Square, London WC1N 3BG &  
27 Department of Neurology and Psychiatry, Università di Roma “Sapienza”, Viale  
28 dell’Università 30, 00185 Rome, Italy. E-mail: [rocchi.lor@gmail.com](mailto:rocchi.lor@gmail.com) ;  
29 Phone: +39 339 3840403; Contributions: Designed research, Performed research,  
30 Reviewed the paper before submission.

31

32 *Pierluigi Tocco, MD<sup>33</sup>*

33 Sobell Department of Motor Neuroscience and Movement Disorders, Institute of  
34 Neurology, University College London, 33 Queen Square, London WC1N 3BG. E-mail:  
35 [pietocco@hotmail.com](mailto:pietocco@hotmail.com) ; Phone: +39 0458124291; Contributions: Designed research,  
36 Performed research, Reviewed the paper before submission.

37

38 *Maarten Speekenbrink, PhD*

39 UCL Cognitive, Perceptual and Brain Sciences, Division of Psychology and Language  
40 Sciences, London WC1E 6BT. E-mail: [m.speekenbrink@ucl.ac.uk](mailto:m.speekenbrink@ucl.ac.uk) ; Phone: +44 7679  
41 8548; Contributions: Designed research, Analyzed data.

42

43 *Prof John C. Rotwell*

44 Sobell Department of Motor Neuroscience and Movement Disorders, Institute of  
45 Neurology, University College London, 33 Queen Square, London WC1N 3BG. E-mail:

46 [j.rothwell@ucl.ac.uk](mailto:j.rothwell@ucl.ac.uk) ; Phone: +44 20 7829 8725; Contributions: Designed research,  
47 Reviewed the paper before submission.

48

49 Address for correspondence: *Prof Marjan Jahanshahi*, UCL Institute of Neurology, The  
50 National Hospital for Neurology and Neurosurgery, 33 Queen Square, London WC1N

51 3BG, UK, E-mail: [m.jahanshahi@ucl.ac.uk](mailto:m.jahanshahi@ucl.ac.uk) ; Phone: + 44 20 7837 3611; Contributions:  
52 Designed research, Participated in paper writing, Reviewed the paper before submission.

53

### Highlights

54

- 55 • What is the contribution of DLPFC and pre-SMA to perceptual decision-  
56 making?
- 57 • Two versions of the moving dots task were used
- 58 • cTBS over the right DLPFC, pre-SMA and sham stimulation was applied
- 59 • Right DLPFC cTBS modulates drift rate as a function of task difficulty
- 60 • pre-SMA cTBS modifies boundary separation when accuracy is emphasized

61

62

63

### Abstract

64 Background: The speed-accuracy trade-off (SAT) refers to the balancing of speed  
65 versus accuracy during decision-making. SAT is very commonly investigated with  
66 perceptual decision-making tasks such as the moving dots task (MDT). The dorsolateral  
67 prefrontal cortex (DLPFC) and the pre-supplementary motor area (pre-SMA) are two  
68 brain regions considered to be involved in the control of SAT.

69 Objectives/Hypotheses: The study tested whether the DLPFC and the pre-SMA  
70 play an essential role in the control of SAT. We hypothesized that continuous theta burst  
71 stimulation (cTBS) over the right DLPFC would primarily alter the rate of accumulation  
72 of evidence, whereas stimulation of the pre-SMA would influence the threshold for  
73 reaching a decision.

74 Methods: Fifteen (5 females; mean age=30,  $SD=5.40$ ) healthy volunteers  
75 participated in the study. We used two versions of the MDT and cTBS over the right  
76 DLPFC, pre-SMA and sham stimulation. The drift diffusion model was fit to the  
77 behavioural data (reaction time and error rate) in order to calculate the drift rate,  
78 boundary separation (threshold) and non-decision time.

79 Results: cTBS over the right DLPFC decreased the rate of accumulation of  
80 evidence (i.e. the drift rate from the diffusion model) in high (0.35 and 0.5) but not in low  
81 coherence trials. cTBS over the pre-SMA changed the boundary separation/threshold  
82 required to reach a decision on accuracy, but not on speed trials.

83 Conclusions: The results suggest for the first time that both the DLPFC and the  
84 pre-SMA make essential but distinct contributions to the modulation of SAT.

85

86 **Keywords:** speed-accuracy trade off, perceptual decision-making, continuous  
87 theta burst stimulation, DLPFC, pre-SMA.

88

89 **Abbreviations:** DLPFC=dorsolateral prefrontal cortex, pre-SMA=pre-  
90 supplementary motor area, cTBS=continuous theta burst stimulation

91

92

**Introduction**

93           Perceptual decision-making is widely held to involve the process of making a  
94 choice from a set of alternative options based on accumulation of information from the  
95 sensory systems [1]. It is proposed that sensory information accumulates from a starting  
96 point until a threshold is reached favouring one option over another [2]. Making an  
97 accurate decision requires spending a longer time to collect the relevant information,  
98 making the decision processes slow; whereas making a fast decision entails spending less  
99 time in accumulating evidence, with the potential cost of lower accuracy. This so-called  
100 speed-accuracy trade off (SAT) [3] has been most commonly investigated in perceptual  
101 decision-making tasks, such as the ‘moving dots’ task (MDT) [4].

102           One outstanding question is in relation to the brain areas involved in the  
103 modulation of SAT [3, 5]. In imaging studies a number of prefrontal areas including the  
104 DLPFC [6-11] and the pre-SMA [12, 13], as well as the striatum and the subthalamic  
105 nucleus (STN), have been reported to be engaged during performance of tasks that  
106 involve modulation of SAT [14]. While evidence from theoretical and imaging studies  
107 suggest that the DLPFC and pre-SMA are involved in the modulation of SAT, because of  
108 the correlational nature of imaging data, the specific contributions of these regions to  
109 SAT regulation is not clear and differs between studies. For example, while both Ivanoff  
110 et al. (2008)[6], and Vallesi et al. (2012)[11] found that the right and left DLPFC are  
111 respectively involved in the regulation of the amount of information necessary to reach a  
112 decision, the results from other studies suggest involvement of the DLPFC in regulation  
113 of the speed/rate of data collection [7-9].

114 Thus, the primary aim of our study was to use the MDT and continuous theta  
115 burst stimulation (cTBS) (that has inhibitory effects [15]) over the DLPFC and the pre-  
116 SMA to *first* establish whether these brain areas make an essential contribution to  
117 modulation of SAT and *second* to identify the nature of their respective contributions to  
118 the modulation of SAT. Based on theoretical models [3, 5] and imaging data [7-10] we  
119 predicted that cTBS over the right DLPFC would primarily change the rate of  
120 accumulation of evidence (i.e. the drift rate), whereas stimulation of pre-SMA would  
121 influence the amount of information needed in order to make a decision (i.e. the boundary  
122 separation/threshold) during MDT performance [5, 12]. Furthermore, based on the  
123 findings from recent studies [11, 16] as a part of the post-hoc analysis, we also analysed  
124 the role of the right DLPFC and pre-SMA in the regulation of switching between speed  
125 and accuracy strategies.

126

127

## Materials and Methods

### 128 Participants

129 Fifteen (5 females; 13 right handed, 2 ambidextrous; mean age =30,  $SD=5.40$ )  
130 healthy volunteers participated in the study. All participants had normal or corrected-to-  
131 normal vision. None of the participants had a history of neurological, psychiatric or  
132 physical illness, head injury or drug or alcohol abuse. Handedness was assessed by the  
133 Briggs and Nebbs handedness inventory [17].

134

### 135 Design and procedure

136 A repeated measures design was used. Continuous theta-burst stimulation (cTBS)  
137 over the right DLPFC, pre-SMA and left S1 leg area (sham stimulation) was administered  
138 in three different sessions in a randomized fashion. During each session all participants  
139 performed two versions of the moving dots task (see below). The minimal interval  
140 between two consecutive sessions was 5 days (range: 5-16 days).

141 The joint ethics committee of the UCL Institute of Neurology and the National  
142 Hospital for Neurology and Neurosurgery approved the study. Informed consent was  
143 obtained from all participants.

144

#### 145 **The moving dots task**

146 The speed-accuracy version of the MDT manipulated the speed-accuracy  
147 instructions (Figure 1A). Participants were required to decide whether a cloud of dots,  
148 with a fixed coherence level of 0.5 across trials, moved to the left or the right of the  
149 screen. Each dot consisted of three pixels; the diameter of the entire cloud of dots was  
150 250 pixels. At the beginning of each trial, a written cue, either FAST or ACCURATE,  
151 was presented pseudorandomly, instructing participants to adopt different levels of  
152 cautiousness. The participants decided on the direction of the moving dots by pressing  
153 one of two buttons with either their left (for dots moving left) or right (for dots moving  
154 right) index finger. Two blocks (100 trials each), with a short break between blocks, were  
155 completed by every participant. At the end of each trial, participants received feedback:  
156 on speed trials, whenever participants exceeded the reaction time criterion of 400 ms, a  
157 TOO SLOW feedback was presented, otherwise they received an IN TIME message. The  
158 criterion of 400 ms for the TOO SLOW feedback was adopted from previous studies

159 [12]. In the accuracy trials, participants were presented with an INCORRECT or  
160 CORRECT feedback. If participants exceeded a time criterion of 1500 ms, a NO  
161 RESPONSE feedback was presented on the screen. The negative feedbacks were  
162 presented in red, while the positive feedbacks appeared in green.

163 In the coherence version of the task (Figure 1B) the participants were instructed to  
164 perform the task as fast and as accurately as possible; no cues for speed or accuracy were  
165 used in this task. However, the coherence ('difficulty') level of the moving dots changed  
166 between trials. Six levels of coherence were set at 0.05, 0.10, 0.15, 0.25, 0.35 and 0.50  
167 with 20 trials per coherence level resulting in a block of 120 trials. Participants performed  
168 two blocks of the task. The coherence level was manipulated to make it harder (0.05) or  
169 easier (0.5) to decide the direction of the moving dots. At the end of each trial,  
170 participants received INCORRECT, CORRECT or NO RESPONSE (if criterion of '1500  
171 ms' was exceeded) feedback depending on their response.

172 The tasks were programmed and presented using PsychoPy software [18] on a 27  
173 inch wide LG monitor (Flatron W2753VC) with a resolution of 1920 × 1080 and a  
174 refresh rate of 60 Hz. Participants sat in a comfortable chair at a distance 100 cm from the  
175 monitor. Before each task participants completed practice trials. The order of the tasks  
176 performed in a single session was randomized. Completion of both tasks required about  
177 35 minutes.

178

179 – insert Figure 1 approximately here –

180

181 **Continuous Theta Burst Stimulation (cTBS)**

182 Magstim (Magstim Company Ltd, Wales, UK) stimulators (Magstim 200 for  
183 single pulse TMS, and Magstim Rapid<sup>2</sup> stimulator for cTBS) were used for stimulation.  
184 Active motor threshold (AMT) for the first dorsal interosseus muscle (FDI) was obtained  
185 by applying monophasic pulses with a 7 cm figure-of-eight-coil placed tangentially over  
186 the participants' right M1 with the handle kept 45° backwards and laterally over the  
187 hotspot for the left FDI. AMT for the tibialis anterior (TA) was obtained by using a  
188 double-cone coil (P/N 9902-00; Magstim Co. Ltd) to stimulate M1 for the left leg. AMT  
189 was defined as the stimulator output at which a motor evoked potential (MEP) higher  
190 than 200  $\mu$ V was elicited on five out of ten trials while participants maintained an FDI or  
191 TA contraction of approximately 20% of their maximal force measured by surface EMG  
192 [19].

193 The cTBS protocol, consisting of a series of bursts of three pulses 20 ms apart  
194 repeated every 200 ms for 40 s (600 pulses) [15] was used to stimulate the right DLPFC,  
195 pre-SMA and for sham stimulation. The right DLPFC was stimulated with a power of  
196 80% of the ATM for the left FDI by placing the figure-of-eight-coil at a position F4  
197 according to the 10-20 system as described in Beam et al. [20]. We opted to stimulate the  
198 right DLPFC rather than the left because there is evidence that in addition to the left  
199 DLPFC, already probed in a repetitive TMS study [10], the right DLPFC is also involved  
200 in SAT regulation [6, 7]. The pre-SMA was stimulated with 80% of the AMT for the left  
201 TA at a point located 5 cm anterior to the hotspot for TA over Cz according to the 10-20  
202 system [21, 22] by using a double-cone coil. The 7 cm-figure-of-eight coil tilted 90° to  
203 the surface of the head at 20% of the AMT for FDI was used for sham stimulation over

204 the S1 area for the left leg, defined as 2 cm posterior to the FDI hot spot in the central  
205 midline area [23].

206

### 207 **Diffusion model analysis**

208 Diffusion model analysis was performed by the use of *fast-dm* [24]. This program  
209 estimates the parameters of Ratcliff's [2] drift diffusion model (DDM). The model can be  
210 applied in cognitive tasks with binary decisions, such as the MDT [25]. The basic  
211 assumption of this model is that during a binary decisions information accumulates  
212 continuously from a certain predefined starting point until it reaches a threshold, when a  
213 decision is made. One of the advantages of the DDM model is that the parameters allow  
214 for a high degree of information utilisation [26]. Thus, instead of relying solely on the  
215 behavioural measures of performance – the mean reaction time (RT) and mean error rate  
216 (ER) – the so called problem of common metrics –, performance can be presented by  
217 DDM parameters that take into account the distribution of both correct and incorrect RTs  
218 [25], which avoids the reliance on different measures. Indeed, by analysing the RT and  
219 ER separately the probability of Type I error increases [25]. In addition, whenever  
220 differences in performance spread over the two metrics, a reduction of statistical power  
221 might occur possibly producing non-significant effects for both RT and ER [25]. Thus,  
222 DDM provides a powerful tool for a more detailed analysis of the processes underlying  
223 the behavioural measures [26].

224 Several parameters are calculated from applying the diffusion model [27]. The  
225 boundary separation ( $a$ ) represents the difference between baseline activity and the  
226 response threshold to reach a decision - the larger the distance between the starting point

227 and decision threshold, the longer it takes to make a decision, hence the longer the RT  
228 and the less likely errors are. Drift rate ( $v$ ) refers to the speed with which evidence for the  
229 correct response accumulates; a high drift rate results in more accurate and faster  
230 responses. The non-decision time ( $t_0$ ) captures the time needed for other processes such  
231 as stimulus encoding and motor execution. The starting point ( $z$ ) reflects possible *a priori*  
232 biases in the decision threshold.

233         One of the important steps when applying DDMs is to decide which of the above  
234 mentioned parameters ( $a$ ,  $v$ ,  $t_0$ ,  $z$ ) are to be fixed and which are to be allowed to vary  
235 across conditions. In general, models should be defined as parsimoniously as possible, as  
236 numerous free parameters might lead to overfitting and make the results unreliable  
237 especially in cases of low trial numbers [28], which calls for a careful selection of free  
238 parameters for the models depending on the task [25]. For example, because changing the  
239 characteristics of the sensory information changes the speed of information accumulation,  
240 the drift rate should be left to vary freely in tasks with trials with variable sensory content  
241 [27]. Therefore, in the coherence task separate drift rates were calculated for each  
242 coherence level for the three brain regions – right DLPFC, pre-SMA and sham; the  
243 values for the boundary separation and the non-decision time were allowed to vary  
244 relative to brain region only.

245         In contrast, based on the classical proposal that under speed instructions there is a  
246 reduction of the distance between the baseline and the threshold, in the speed-accuracy  
247 version of the task both, the boundary separation and the non-decision times were  
248 calculated separately for ‘speed’ and ‘accuracy’ trials relative to the region of  
249 stimulation; whereas the drift rate was allowed to vary freely only for the brain region,

250 but not for the type of instructions (FAST vs. ACCURATE). Indeed, the results from a  
251 recent study have shown that while the effect of the speed-accuracy instructions on  
252 boundary separation is present during multiple sessions of the MDT, a presumed effect of  
253 speed-accuracy instructions on the drift rate could only be traced at the beginning of  
254 training; after training the speed accuracy instructions change solely the boundary  
255 separation [29].

256 The starting point in both tasks was fixed to zero. Optimization criterion based on  
257 the Kolmogorov-Smirnov (KS) statistics was used in both tasks. The KS approach yields  
258 robust results in the presence of relatively smaller number of trials [25]. The assessment  
259 of model fit was performed based on the values of the KS statistics.

260 The DDM and behavioural parameters were subjected to statistical analysis using  
261 SPSS. The Shapiro-Wilk test was used to test for normality. A two-way repeated measure  
262 ANOVA with factors brain region (right DLPFC, pre-SMA and sham) and task  
263 difficulty/coherence level (0.05, 0.10, 0.15 0.25, 0.35 and 0.50) for the coherence task  
264 and brain region (right DLPFC, pre-SMA and sham) and instructions (Speed vs.  
265 Accuracy) for the speed-accuracy task, as well as *t*-tests where appropriate, were used to  
266 analyze the data. As part of the post-hoc analysis, we also tested the effect of the right  
267 DLPFC and pre-SMA on switching between speed and accuracy strategies on the  
268 behavioural and DDM parameters. For this analysis, the RTs and ERs in speed and  
269 accuracy trials were first separated into “switch” and “no-switch” trials, and then the  
270 DDM parameters calculated as explained above. A three-way repeated ANOVA with  
271 factors instructions (Speed vs. Accuracy), brain region (right DLPFC, pre-SMA and  
272 sham) and switching (Switch vs. No-switch Trial) was then used to analyse both the

273 behavioural and DDM parameters. If the assumption of sphericity was violated  
274 (Mauchly's test), a Greenhouse-Geisser correction was used. Probability value of  $p=0.05$   
275 was used as a criterion for statistical significance. A Bonferroni correction was used to  
276 control for multiple comparisons.

277

278

## Results

279

### Behavioural Measures

280

#### Speed-accuracy task - behavioural measures

281

282

283

284

285

286

287

– insert Figure 2 approximately here –

288

289

290

291

292

293

294

295

*Mean RT in speed-accuracy task.* As expected, the RTs for the speed trials were shorter than for the accuracy trials ( $F(1,14)=19.34, p=0.001$ ) (Figure 2 A). Although the mean RT after right pre-SMA stimulation was shorter than the RT after right DLPFC or sham stimulation, the main effect of brain region ( $p=0.254$ ) and the brain region  $\times$  instructions interaction ( $p=0.689$ ) were not significant.

*Mean ER in speed-accuracy task.* Participants made more errors after speed than after accuracy instruction ( $F(1,14)=17.88, p=0.001$ ) (Figure 2 B). The main effect of brain region ( $p=0.883$ ) and the brain region  $\times$  instruction interaction ( $p=0.571$ ) were not significant.

*Post-hoc analysis of the switch vs. non-switch trials.* There was no main effect of switching or brain region or any significant interactions on mean RTs or ER (all  $ps>0.252$ ) on both speed and accuracy trials.

296

297 **Coherence task - behavioural measures**

298 *Mean RT in coherence task.* As expected, the main effect of coherence was  
299 significant ( $F(5,70)=34.48, p<0.0001$ ) (Figure 3A) indicating shorter RTs in higher than  
300 in the lower coherence trials. Neither the main effect of brain region ( $p=0.494$ ) nor the  
301 brain region  $\times$  coherence interaction ( $p=0.440$ ) were significant.

302

303 – insert Figure 3 approximately here –

304

305 *Mean ER in coherence version of the task.* The main effect of coherence was  
306 significant ( $F(5,70)=88.07, p=0.001$ ) with higher ER in low coherence trials (Figure 3B).  
307 The main effect of stimulation target ( $p=0.922$ ) and brain region  $\times$  coherence interaction  
308 ( $p=0.530$ ) were not significant.

309

310 **Drift Diffusion Model (DDM) analysis**

311 The Kolmogorov-Smirnov tests revealed no significant results at the alpha level  
312 of 0.05 for the model fits in both tasks, indicating that the individual models described  
313 the RT distribution well.

314

315 **Speed-accuracy task – DDM results**

316 *Boundary separation in the speed-accuracy task.* As expected, the boundary  
317 separation for the speed trials was lower compared to accuracy trials ( $F(1,14)=11.41,$   
318  $p=0.005$ ) (Figure 4A). The main effect of brain region was significant ( $F(2,28)=4.46,$

319  $p=0.021$ ) indicating a significant decrease of the boundary separation after stimulation of  
320 the pre-SMA compared to the right DLPFC and sham stimulation. The significant brain  
321 region  $\times$  instructions interaction ( $F(2,28)=4.26, p=0.024$ ) indicated a differential effect of  
322 the stimulation over the pre-SMA depending on instructions. Namely, the decrease of the  
323 boundary separation after stimulation of pre-SMA in accuracy trials was significant  
324 compared to both right DLPFC ( $t(14)=2.46, p=0.027$ ) and sham stimulation ( $t(14)=2.33,$   
325  $p=0.035$ ). By contrast, with speed instructions, the decrease of the boundary separation  
326 after pre-SMA stimulation was not significant relative to either the right DLPFC  
327 ( $p=0.067$ ), or sham stimulation ( $p=0.205$ ). There was no significant difference in  
328 boundary separation in either accuracy ( $p=0.382$ ), or speed trials ( $p=0.946$ ) when  
329 stimulation of the right DLPFC was compared to sham stimulation.

330

331 – insert Figure 4 approximately here –

332

333 *Non—decision time in the speed-accuracy task.* The non-decision time was  
334 shorter for speed as compared to accuracy trials ( $F(1,14)=16.40, p=0.001$ ) (Figure 4B).  
335 There was no effect of brain region on the non-decision time ( $p=0.534$ ). The brain region  
336  $\times$  instructions interaction was also not significant ( $p=0.195$ ).

337 *Drift rate in the speed-accuracy task.* As mentioned above, the drift rate was  
338 calculated for the brain region regardless of instruction. There was no effect of brain  
339 region on the drift rate ( $p=0.442$ ) in the speed-accuracy task.

340 *Post-hoc analysis of the switch vs. non-switch trials.* There was no significant  
341 main effect of switching or brain regions or any significant interactions on the boundary

342 separation or non-decision time parameters (all  $p$ s > 0.156) on both the speed and  
343 accuracy trials.

344

### 345 **Coherence task - DDM results**

346 *Drift rate in the coherence task.* As expected, the main effect of coherence level  
347 was significant and the drift rate was lower on trials with lower coherence than higher  
348 coherence ( $F(5,70)=84.86$ ,  $p<0.0001$ ) (Figure 5). The main effect of brain region was not  
349 significant ( $p=0.141$ ). However, the brain region  $\times$  coherence level interaction was  
350 significant ( $F(10,140)=2.03$ ,  $p=0.025$ ), which indicated a differential effect of stimulation  
351 of different cortical regions depending on the coherence level. Namely, there was a  
352 decrease of drift rate at high coherence levels (0.35 and 0.5) after stimulation of the right  
353 DLPFC compared to the stimulation of the right pre-SMA (coherence level 0.35:  $t(14)=-$   
354 2.69,  $p=0.018$ , coherence level 0.5:  $t(14)=-2.07$ ,  $p=0.047$ ) and the sham stimulation  
355 (coherence level 0.35:  $t(14)=-2.77$ ,  $p=0.015$ , coherence level 0.5:  $t(14)=-2.53$ ,  $p=0.024$ ),  
356 but not at coherence levels below 0.25 ( $p=0.485$ ). The drift rates were not significantly  
357 different for stimulation of the right DLPFC and for sham stimulation ( $p=0.230$ ).

358

359 – insert Figure 5 approximately here –

360 *Boundary separation and non-decision time in the coherence task.* The boundary  
361 separation and the non-decision time were calculated for stimulation of the right DLPFC,  
362 right pre-SMA and after sham stimulation regardless of the level of coherence. The effect  
363 of stimulated brain region on boundary separation ( $p=0.260$ ) and non-decision time  
364 ( $p=0.453$ ) was not significant (see Table 1).

365

366

– insert Table 1 approximately here –

367

368

**Discussion**

369

370

371

372

373

374

375

376

377

**Stimulation of the pre-SMA decreases the boundary separation on accuracy trials**

378

379

380

381

382

383

384

385

386

387

Although imaging studies [6, 12-14, 30] clearly showed engagement of the pre-SMA in SAT control, the functional significance of activation of the pre-SMA in relation to SAT control remained unclear. Our results provide the first evidence that inhibition of the pre-SMA with cTBS induces a decrease in the boundary separation when accuracy is emphasized over speed, suggesting a decrease of the amount of information needed to reach threshold before a decision was made under accuracy instructions.

At first glance this finding may seem to be in contradiction to the imaging literature showing greater activation of the pre-SMA under speed instructions [6, 11, 12, 14], because this would lead to the assumption that since there is a greater activation of the pre-SMA when speed is emphasized over accuracy, stimulation of the pre-SMA

388 would affect primarily the responses under speed rather than under accuracy instructions.  
389 However, activation of the pre-SMA by speed instructions is related to the decrease of  
390 the boundary separation [13]; whereas the opposite holds true when accuracy is  
391 emphasized - accuracy instructions increase boundary separation; the latter was also  
392 shown in our study. Boundary separation represents the level of cautiousness, such that  
393 higher boundary separation indicates higher levels of cautiousness as in the case of  
394 accuracy trials [27]. Therefore, because the level of cautiousness and boundary separation  
395 were higher under accuracy than under speed trials, cTBS was able to selectively alter  
396 (decrease) the boundary separation on accuracy trials, and failed to modulate it on speed  
397 trials for which the boundary separation was low even before cTBS was applied over the  
398 pre-SMA.

399

400 **Stimulation of the right DLPFC decreases the drift rate in high coherence ('easy')**  
401 **trials**

402 The second key finding of the present study is that stimulation over the right  
403 DLPFC selectively decreased the drift rate in high coherence ('easy') as compared to low  
404 coherence ('difficult') trials.

405 Our finding that cTBS over the right DLPFC differentially decreased the rate of  
406 accumulation of information as a function of task difficulty is consistent with the fMRI  
407 results of Heekeren and coauthors [8, 9], who found that the DLPFC is more active  
408 during easy decisions than during harder decisions, which is in turn in line with the  
409 theoretical assumptions that areas representing decision variables at a more abstract level  
410 show greater activation on trials when the available sensory evidence required to make a

411 decision is greater, such as on the easier trials. In a recent fMRI study, however, by using  
412 a visual searching task Vallesi et al [31] found higher activation of the right DLPFC on  
413 target-absent and salient trials, when the stimuli should be evaluated to prevent false  
414 alarms; and target-absent and non-salient trials, when the cognitive system should be  
415 engaged more extensively in visual search to check for the absence of the target stimulus,  
416 i.e. on harder trials. Similarly, Fleck et al. [32] reported a greater activation of the right  
417 DLPFC for low (harder to decide) than for high confidence (easier to decide) trials during  
418 episodic retrieval/visual perception tasks. The difference in the results from these studies  
419 and the results from our study and the studies mentioned before [8, 9] might be due to the  
420 difference in tasks used: while Fleck et al. [32] and Vallesi [31] (but see also [33, 34])  
421 used more complex tasks that engage frontal cognitive abilities more extensively, in our  
422 study as well as in the study of Heekeren et al. [9] a MDT task was used to assess  
423 perceptual decision-making, which does not depend as extensively on frontal control  
424 mechanisms. Similar results have also been reported with a facial recognition as a  
425 measure of perceptual decision-making [8, 10].

426 Philiastides et al. [10] applied 1 Hz rTMS over the left DLPFC for 12 minutes and  
427 examined two levels of difficulty on the facial recognition test. 1 Hz rTMS over the left  
428 DLPFC reduced the drift rate, providing evidence for left DLPFC involvement in the  
429 process of evidence accumulation. Our study extends the findings of Philiastides et al.  
430 [10] in two important ways. First, we showed that stimulation of the right DLPFC could  
431 also decrease the drift rate, hence suggesting that there is no specific hemispheric  
432 specialization for the involvement of the DLPFC in relation to accumulation of sensory  
433 information. Second, with our six levels of task difficulty we have shown that that the

434 decrease of drift rate by right DLPFC stimulation is a function of the level of task  
435 difficulty, i.e. the rate of accumulation of sensory evidence was distorted by cTBS on  
436 high coherence (easy) trials (0.35 and 0.5) and was not changed by stimulation on low  
437 coherence (difficult) trials (0.05, 0.1, 0.15 and 0.25). Furthermore, the use of cTBS,  
438 which has longer lasting effects of about 45-60 minutes [15] covered the whole period of  
439 task performance in our study, rather than the first half of the trials only, as in the  
440 Philiastides et al. [10] study. Therefore, our data and the data from Philiastides et al. [10]  
441 provide further evidence that the DLPFC is important in linking sensation to action, as  
442 previously shown in animal studies [35, 36].

443       The effect of switching between speed and accuracy strategies has been recently  
444 addressed in a few studies from the Valessi group [11, 16]. In a fMRI study with healthy  
445 participants, they first showed that switching from a quick to an accurate strategy was  
446 associated with activation of the left middle frontal gyrus [11]. In a later study employing  
447 patients with brain tumors (and after their subsequent surgical removal) located in the left  
448 or right prefrontal cortex, they found that flexibility of selecting an accurate strategy after  
449 adoption of a fast strategy is impaired in patients with left prefrontal tumors [16]. We,  
450 however, failed to find any effect of stimulation of the right DLPFC or pre-SMA on  
451 switching strategies. Campanella et al. [16] compared the effect of brain tumors in  
452 patients with left and right prefrontal lesions and found a failure to flexibly switch from  
453 speed to accuracy instructions in patients with left prefrontal lesion only, but not in  
454 patients with right prefrontal brain tumors, suggesting that the switching between speed-  
455 accuracy strategies might be functionally segregated in the left prefrontal cortex. In  
456 addition, while we used the MDT in our study, they used a color discrimination task,

457 which might also explain the differences in the results obtained in this study and their  
458 studies. However, the effect of stimulation on switching between strategies was not a  
459 primary aim of our study and it was examined as a post-hoc analysis.

460         There are a few limitations of the study. Even though the RT and ER in general  
461 showed similar trends as the parameters derived from the DDM, the differences between  
462 stimulated brain areas failed to reach significance for these measures. However, there  
463 were significant effects when comparing the DDM parameters. As noted in the methods  
464 section, one of the advantages of the DDM model is that the DDM parameters allow for a  
465 high degree of information utilisation relative to the behavioural measures [26], since the  
466 DDM parameters take into account the distribution of both correct and incorrect RT  
467 simultaneously. Thus, instead of solely relying on behavioural measures, the performance  
468 as presented by the DDM parameters allows for more subtle inferences about the  
469 mediating processes [25]. Furthermore, in the speed-accuracy task we used a fixed  
470 criterion of 400 ms such that whenever the reaction time of the participant exceeded the  
471 value of 400 ms a “TOO SLOW” feedback appeared on the screen. However, this  
472 criterion might have been too strict for some and too lenient for other participants.  
473 Adjustment of the feedback criterion more flexibly according to each individual's average  
474 speed may have been more appropriate. We, however, decided to use a fixed criterion of  
475 400 ms based on the previous studies [12], which also makes the results of this study  
476 more directly comparable to the results of these previous studies. We used a double cone  
477 coil for cTBS, which is considered suitable for stimulating deeper brain structures such as  
478 the pre-SMA [37]. However, taking into account the size of the coil and the overall low  
479 spatial resolution of TMS [38], an effect due to stimulation of other more superficial

480 prefrontal areas cannot be completely ruled out. Nevertheless, the difference in the effects  
481 of stimulation of the pre-SMA versus DLPFC on the DDM parameters in both tasks  
482 argues against this possibility. Another factor, which might have limited stimulation  
483 accuracy, is our reliance on craniometric measures to localize target areas instead of a  
484 neuronavigation system. However, the craniometric measurement have been used  
485 successfully many times in TMS research so far [20-22] and have been shown to be able  
486 to reach desired cortex regions reliably [39]. Furthermore, there is a high inter-participant  
487 variability of TBS protocols on neurophysiological outcome measures [40]. Indeed, some  
488 participants respond to the cTBS “as expected” (i.e. inhibition of the cortical activity),  
489 others do not show any response to the protocol, while for other participants cTBS may  
490 produce the opposite effect – a facilitation rather than inhibition of cortical activity [41].  
491 This variability might be due to inter-individual differences in the recruitment of  
492 interneuron networks [41], but can also be accounted for by the different level of  
493 contraction/relaxation of the recording muscle, i.e. it can be abolished by tonic  
494 contraction while cTBS is applied [42], or it can even be reversed to facilitation by phasic  
495 contraction of the muscles [43]. Nevertheless, we were very persistent in our demands to  
496 the participants to relax the muscles as much as possible. In addition, it is known that the  
497 effect of cTBS depends on the stimulation intensity [40]. However, we were very  
498 cautious to apply cTBS at the level 80% of the AMT at FDI for each participant. There is  
499 still a need for more meticulous recruitment of participants in future studies based on  
500 their individual response to cTBS.

501

502 **Conclusions**

503 In conclusion, the selective decrease of boundary separation on accuracy trials  
504 with stimulation over the pre-SMA, and the decrease of the drift rate on high but not low  
505 coherence trials with stimulation over the right-DLPFC, provide evidence that causally  
506 relates pre-SMA and the right-DLPFC to the regulation of SAT. The ‘selective influence’  
507 assumption of the DDM refers to the idea that changes in specific cognitive processes  
508 such as urgency or increased caution selectively influence one parameter of the model  
509 [44], which has been supported by simulated data (e.g. Ratcliff and Frank, 2012 [45]).  
510 Our data provide support for the ‘selective influence’ assumption by showing that cTBS-  
511 induced disruption of the pre-SMA and DLPFC selectively alter boundary separation and  
512 drift rate respectively.

513

#### 514 **Acknowledgements**

515 This work was supported by a grant awarded to Dejan Georgiev (ARRS 30915).

516 The authors declare no competing financial interests.

517

518 **Conflicts of interest:** No conflicts of interest are declared by the authors.

519

520

521

522

523

524

525

526

**References**

- 527 1. Gold JJ, Shadlen MN. The neural basis of decision making. *Annu Rev Neurosci*  
528 2007 30:535-574
- 529 2. Ratcliff R. A theory of memory retrieval. *Psychol Rev* 1978 85:59-108
- 530 3. Bogacz R, Wagenmakers EJ, Forstmann BU, Nieuwenhuis S. The neural basis of  
531 the speed-accuracy tradeoff. *Trends Neurosci* 2010 33:10-16
- 532 4. Britten KH, Shadlen MN, Newsome WT, Movshon JA. The analysis of visual  
533 motion: a comparison of neuronal and psychophysical performance. *J Neurosci*  
534 1992 12:4745-4765
- 535 5. Standage D, Blohm G, Dorris MC. On the neural implementation of the speed-  
536 accuracy trade-off. *Front Neurosci* 2014 8:236
- 537 6. Ivanoff J, Branning P, Marois R. fMRI evidence for a dual process account of the  
538 speed-accuracy tradeoff in decision-making. *PLoS One* 2008 3:e2635
- 539 7. Domenech P, Dreher JC. Decision threshold modulation in the human brain. *J*  
540 *Neurosci* 2010 30:14305-14317
- 541 8. Heekeren HR, Marrett S, Bandettini PA, Ungerleider LG. A general mechanism  
542 for perceptual decision-making in the human brain. *Nature* 2004 431:859-862
- 543 9. Heekeren HR, Marrett S, Ruff DA, Bandettini PA, Ungerleider LG. Involvement  
544 of human left dorsolateral prefrontal cortex in perceptual decision making is  
545 independent of response modality. *Proc Natl Acad Sci U S A* 2006 103:10023–  
546 10028

- 547 10. Philiastides MG, Auzszulewicz R, Heekeren HR, Blankenburg F. Causal role of  
548 dorsolateral prefrontal cortex in human perceptual decision making. *Curr Biol*  
549 2011 21:980-983
- 550 11. Vallesi A, McIntosh AR, Crescentini C, Stuss DT. fMRI investigation of speed-  
551 accuracy strategy switching. *Hum Brain Mapp* 2012 33:1677-1688
- 552 12. Forstmann BU, Dutilh G, Brown S, Neumann J, von Cramon DY, Ridderinkhof  
553 KR, Wagenmakers EJ. Striatum and pre-SMA facilitate decision-making under  
554 time pressure. *Proc Natl Acad Sci U S A* 2008 105:17538-17542
- 555 13. Mansfield EL, Karayanidis F, Jamadar S, Heathcote A, Forstmann BU.  
556 Adjustments of response threshold during task switching: a model-based  
557 functional magnetic resonance imaging study. *J Neurosci* 2011 31:14688-14692
- 558 14. van Veen V, Krug MK, Carter CS. The neural and computational basis of  
559 controlled speed-accuracy tradeoff during task performance. *J Cogn Neurosci*  
560 2008 20:1952-1965
- 561 15. Huang YZ, Edwards MJ, Rounis E, Bhatia KP, Rothwell JC. Theta burst  
562 stimulation of the human motor cortex. *Neuron* 2005 45:201-206
- 563 16. Campanella F, Skrap M, Vallesi A. Speed-accuracy strategy regulations in  
564 prefrontal tumor patients. *Neuropsychologia* 2016 82:1-10
- 565 17. Briggs GG, Nebes RD. Patterns of hand preference in a student population.  
566 *Cortex* 1975 11:230-238
- 567 18. Peirce JW. PsychoPy--Psychophysics software in Python. *J Neurosci Methods*  
568 2007 162:8-13

- 569 19. Rothwell JC, Hallett M, Berardelli A, Eisen A, Rossini P, Paulus W. Magnetic  
570 stimulation: motor evoked potentials. *The International Federation of Clinical*  
571 *Neurophysiology. Electroencephalogr Clin Neurophysiol Suppl* 1999 52:97-103
- 572 20. Beam W, Borckardt JJ, Reeves ST, George MS. An efficient and accurate new  
573 method for locating the F3 position for prefrontal TMS applications. *Brain Stimul*  
574 2009 2:50-54
- 575 21. Cunnington R, Iansek R, Thickbroom GW, Laing BA, Mastaglia FL, Bradshaw  
576 JL, Phillips JG. Effects of magnetic stimulation over supplementary motor area on  
577 movement in Parkinson's disease. *Brain* 1996 119 ( Pt 3):815-822
- 578 22. Rushworth MF, Hadland KA, Paus T, Sipila PK. Role of the human medial  
579 frontal cortex in task switching: a combined fMRI and TMS study. *J*  
580 *Neurophysiol* 2002 87:2577-2592
- 581 23. Moore JW, Ruge D, Wenke D, Rothwell J, Haggard P. Disrupting the experience  
582 of control in the human brain: pre-supplementary motor area contributes to the  
583 sense of agency. *Proc Biol Sci* 2010 277:2503-2509
- 584 24. Voss A, Voss J. Fast-dm: a free program for efficient diffusion model analysis.  
585 *Behav Res Methods* 2007 39:767-775
- 586 25. Voss A, Nagler M, Lerche V. Diffusion models in experimental psychology: a  
587 practical introduction. *Exp Psychol* 2013 60:385-402
- 588 26. Voss A, Rothermund K, Voss J. Interpreting the parameters of the diffusion  
589 model: an empirical validation. *Mem Cognit* 2004 32:1206-1220
- 590 27. Ratcliff R, McKoon G. The diffusion decision model: theory and data for two-  
591 choice decision tasks. *Neural Comput* 2008 20:873-922

- 592 28. Voss A, Voss J, Lerche V. Assessing cognitive processes with diffusion model  
593 analyses: a tutorial based on fast-dm-30. *Front Psychol* 2015 6:336
- 594 29. Zhang J, Rowe JB. Dissociable mechanisms of speed-accuracy tradeoff during  
595 visual perceptual learning are revealed by a hierarchical drift-diffusion model.  
596 *Front Neurosci* 2014 8:69
- 597 30. Forstmann BU, Anwander A, Schafer A, Neumann J, Brown S, Wagenmakers EJ,  
598 Bogacz R, Turner R. Cortico-striatal connections predict control over speed and  
599 accuracy in perceptual decision making. *Proc Natl Acad Sci U S A* 2010  
600 107:15916-15920
- 601 31. Vallesi A. Monitoring mechanisms in visual search: an fMRI study. *Brain Res*  
602 2014 1579:65-73
- 603 32. Fleck MS, Daselaar SM, Dobbins IG, Cabeza R. Role of prefrontal and anterior  
604 cingulate regions in decision-making processes shared by memory and  
605 nonmemory tasks. *Cereb Cortex* 2006 16:1623-1630
- 606 33. Vallesi A, Mussoni A, Mondani M, Budai R, Skrap M, Shallice T. The neural  
607 basis of temporal preparation: Insights from brain tumor patients.  
608 *Neuropsychologia* 2007 45:2755-2763
- 609 34. Vallesi A, Shallice T, Walsh V. Role of the prefrontal cortex in the foreperiod  
610 effect: TMS evidence for dual mechanisms in temporal preparation. *Cereb Cortex*  
611 2007 17:466-474
- 612 35. Kim JN, Shadlen MN. Neural correlates of a decision in the dorsolateral  
613 prefrontal cortex of the macaque. *Nat Neurosci* 1999 2:176-185

- 614 36. Funahashi S, Bruce CJ, Goldman-Rakic PS. Mnemonic coding of visual space in  
615 the monkey's dorsolateral prefrontal cortex. *J Neurophysiol* 1989 61:331-349
- 616 37. Cai W, George JS, Verbruggen F, Chambers CD, Aron AR. The role of the right  
617 presupplementary motor area in stopping action: two studies with event-related  
618 transcranial magnetic stimulation. *J Neurophysiol* 2012 108:380-389
- 619 38. Sandrini M, Umiltà C, Rusconi E. The use of transcranial magnetic stimulation in  
620 cognitive neuroscience: a new synthesis of methodological issues. *Neurosci*  
621 *Biobehav Rev* 2011 35:516-536
- 622 39. Accolla E, Caputo E, Cogiamanian F, Tamma F, Mrakic-Sposta S, Marceglia S,  
623 Egidi M, Rampini P, Locatelli M, Priori A. Gender differences in patients with  
624 Parkinson's disease treated with subthalamic deep brain stimulation. *Mov Disord*  
625 2007 22:1150-1156
- 626 40. Brownjohn PW, Reynolds JN, Matheson N, Fox J, Shemmell JB. The effects of  
627 individualized theta burst stimulation on the excitability of the human motor  
628 system. *Brain Stimul* 2014 7:260-268
- 629 41. Hamada M, Murase N, Hasan A, Balaratnam M, Rothwell JC. The role of  
630 interneuron networks in driving human motor cortical plasticity. *Cereb Cortex*  
631 2013 23:1593-1605
- 632 42. Huang YZ, Rothwell JC, Edwards MJ, Chen RS. Effect of physiological activity  
633 on an NMDA-dependent form of cortical plasticity in human. *Cereb Cortex* 2008  
634 18:563-570

- 635 43. Iezzi E, Conte A, Suppa A, Agostino R, Dinapoli L, Scontrini A, Berardelli A.  
636 Phasic voluntary movements reverse the aftereffects of subsequent theta-burst  
637 stimulation in humans. *J Neurophysiol* 2008 100:2070-2076
- 638 44. Rae B, Heathcote A, Donkin C, Averell L, S. B. The hare and the tortoise:  
639 emphasizing speed can change the evidence used to make decisions. *J Exp*  
640 *Psychol Learn Mem Cogn* 2014 40:1226-1243
- 641 45. Ratcliff R, Frank MJ. Reinforcement-based decision making in corticostriatal  
642 circuits: mutual constraints by neurocomputational and diffusion models. *Neural*  
643 *Comput* 2012 24:1186-1229
- 644
- 645
- 646
- 647
- 648
- 649
- 650
- 651
- 652
- 653
- 654
- 655
- 656
- 657

658 Figure 1. The Moving dots task used in the study; A) Speed-accuracy version of the task;  
659 B) Coherence version of the task, in which the coherence (difficulty) level of the moving  
660 dots was manipulated.

661

662 Figure 2. Mean Reaction Time in milliseconds (*ms*) (A) and Mean Error Rate in the speed  
663 and accuracy trials after stimulation of the right dorsolateral prefrontal cortex (right  
664 DLPFC), right pre-supplementary motor area (pre-SMA) and after sham stimulation.

665

666 Figure 3. Mean Reaction Time in milliseconds (*ms*) (A) and Mean Error Rate for 6  
667 different coherence levels after stimulation of the right dorsolateral prefrontal cortex  
668 (right DLPFC), right pre-supplementary motor area (pre-SMA) and after sham  
669 stimulation.

670

671 Figure 4. Effect of stimulation (right dorsolateral prefrontal cortex – right DLPFC, pre-  
672 supplementary area – pre-SMA and sham) on boundary separation (A) and non-decision  
673 time (B) in speed-accuracy task as a function of instructions (Speed vs. Accuracy). The  
674 significant effects of stimulation are marked with \*.

675

676 Figure 5. Effect of stimulation (right dorsolateral prefrontal cortex – right DLPFC, pre-  
677 supplementary area – pre-SMA and sham) on the drift rate as a function of the coherence  
678 level of the task. The significant effects of stimulation are marked with \*.

679

680

681 Table 1. Mean boundary separation ( $a$ ) and mean non-decision time ( $t_0$ ) before and after  
 682 continuous theta burst stimulation over the right dorsolateral prefrontal cortex (r-  
 683 DLPFC), pre-supplementary area (pre-SMA) and during sham stimulation in the  
 684 coherence version of the moving dots task.

	$a$ before	SD	$a$ after	SD	$t_0$ before	SD	$t_0$ after	SD
r-DLPFC	0.903	0.275	0.914	0.248	0.373	0.076	0.345	0.059
pre-SMA	0.831	0.220	0.811	0.136	0.378	0.058	0.367	0.056
sham	0.952	0.272	0.894	0.237	0.388	0.065	0.364	0.052

685

686

Accepted Manuscript