

# Comparison Between Smartwatch-Derived and CPET-Measured VO<sub>2</sub>max

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## Abstract

*This study aimed to determine the accuracy of smartwatch-derived maximal oxygen consumption (VO<sub>2</sub>max) and the percentage of predicted VO<sub>2</sub>max (%pVO<sub>2</sub>max), two standard measures of cardiorespiratory fitness with established clinical predictive value. 215 adults (44 (21%) male; median [interquartile range; IQR] 55 [32, 62] years old) performed a maximal exercise test (CPET) on a semi-recumbent ergometer and wore a Garmin Vivoactive 4s (GV4) smartwatch for 60 days. The first and last VO<sub>2</sub>max estimates provided by GV4 were compared to CPET measured VO<sub>2</sub>max and %pVO<sub>2</sub>max (Wasserman and Whipp's anthropometric-based equation). Agreement was assessed using Bland-Altman analysis (bias and limits of agreement [LoA]), absolute percentage error (APE), reported as median [interquartile range], and Pearson's correlation coefficient (cc). VO<sub>2</sub>max and %pVO<sub>2</sub>max measured during CPET was 22.4 [17.5, 27.4] ml/kg/min and 90.9% [78.1%, 101.3%], respectively. VO<sub>2</sub>max estimates from GV4 were moderately correlated with CPET measures (cc≤0.66) and showed a large positive bias ~14 ml/kg/min with LoA from 0 – 27 ml/kg/min. Correlation between VO<sub>2</sub>max from GV4 and anthropometric-based prediction of VO<sub>2</sub>max was high (cc>0.90). Agreement between %pVO<sub>2</sub>max from GV4 and CPET was poor (cc~0.15, bias ~52%, LoA 7-98%). GV4 provides estimates of VO<sub>2</sub>max that overestimate but moderately correlate with CPET measured VO<sub>2</sub>max. The agreement for %pVO<sub>2</sub>max is poor.*

## 1. Introduction

Cardiorespiratory fitness (CRF) has been linked to several health-related outcomes, with low fitness being associated with increased risk of cardiovascular disease [1, 2], metabolic syndrome [3], cognitive function [4] and severe COVID-19 [5].

Maximal cardiopulmonary exercise testing (CPET) is considered the gold standard assessment of CRF. It is a dynamic symptom-limited test that is incremental in nature

with a continual increase in workload until the individual cannot exercise anymore (self-reported exhaustion) [6]. The CPET allows for breath-by-breath analysis of gas exchange: oxygen consumption (VO<sub>2</sub>) and carbon dioxide production (VCO<sub>2</sub>) to derive the primary outcome measure of maximal oxygen consumption (VO<sub>2</sub>max). Direct measurement of VO<sub>2</sub>max requires expensive monitoring equipment, experienced personnel and is not without risk. Therefore, the application of maximal CPET is limited in the context of the unselected general population or large epidemiological studies. Furthermore, high levels of motivation and physical effort are required by the individual to achieve a maximal test, which may not be feasible in the presence of chronic conditions such as pain or fatigue.

Predicted VO<sub>2</sub>max is typically estimated using anthropometric-based equations which are population specific, based on both active and sedentary individuals, men and women and individuals with and without cardiac conditions [7, 8]. The percentage of predicted VO<sub>2</sub>max (%pVO<sub>2</sub>max) is calculated as the ratio between measured or estimated VO<sub>2</sub>max and predicted VO<sub>2</sub>max. %pVO<sub>2</sub>max has both prognostic value in assessing CRF and predicting clinical outcomes [9].

Novel wrist-worn wearable technologies (hereafter *smartwatches*) use tri-axial accelerometers, and photoplethysmography (PPG) sensors to measure physiological parameters such as heart rate (HR), distance and step count. Smartwatch estimates of VO<sub>2</sub>max are derived using the PPG signal measured HR while adjusting for factors such as age, sex, height, weight and exercise type using proprietary algorithms [10, 11]. In the context of healthcare, these devices provide an opportunity to estimate CRF parameters outside of the clinical environment, at scale.

Molina-Garcia and colleagues (2022) performed a systematic review with meta-analysis of 14 studies (n=403) that assessed the validity of smartwatch estimation of VO<sub>2</sub>max in both resting and exercise test conditions [12]. In the context of resting conditions, the authors observed an overestimation of VO<sub>2</sub>max (Bias [Limits of

Agreement; LoA] = 2.17 [-13.07, 17.41] ml/kg/min;  $p=0.020$ ) compared to the reference CPET. In contrast, a bias close to nil but wide LoA (Bias [LoA] = -0.09 [-16.79, 16.61] ml/kg/min;  $p=0.910$ ) was observed when exercise test conditions were utilized.

Yet, there are very few studies assessing the agreement between CPET (reference standard) assessment of CRF and smartwatch estimation of  $\text{VO}_{2\text{max}}$  from remote community-based data capture. The aim of this study was to determine smartwatch device accuracy in estimating  $\text{VO}_{2\text{max}}$  and %p $\text{VO}_{2\text{max}}$  using data from CPET as a reference.

## 2. Methods

### 2.1. Study participants

215 adults (44 (21%) male; median [interquartile range; IQR] 56 [32, 62] years old) were recruited from two population-based cohorts the Avon Longitudinal Study of Parents and Children (ALSPAC; REC: 21/SC/0030) [13, 14] and TwinsUK (REC: 19/NW/0187). Clinic investigations were conducted at the UCL Bloomsbury Centre for Clinical Phenotyping, London. All participants gave written informed consent.

Participant age and sex were collected by questionnaire. Height was measured using a stadiometer (Seca217, Seca, Germany) to the closest centimetre and weight was measured in kilograms using digital bio-impedance scales (BC-418 or MC-780MA, Tanita, USA) to calculate BMI.

### 2.2. Cardiopulmonary exercise test

All exercise tests were conducted according to the ATS/ACCP (2003) guidelines for CPET [15]. CPET was performed using a semi-recumbent cycle ergometer (Ergoline 900, Hamburg, Germany) and metabolic cart (Quark Cosmed, Rome, Italy). Following 1 minute of rest and 2 minutes of warm-up cycling at 5 Watts, the work rate was incrementally increased using a ramp protocol in an individualized manner by either 15, 20, 25 or 30 Watts each minute based on the Wasserman weight algorithm [16]. The test was terminated if the participant (i) reached their age-predicted (220-age) maximum HR (ii) experienced limiting symptoms or (iii) developed arrhythmia, hypotension (systolic blood pressure (BP) drop of >10mmHg despite increasing workload) or (iv) an excessive blood pressure rise during the test (>250 systolic mmHg). Expired gases were analyzed breath-by-breath, and HR measured using a continuous 6-lead ECG (Quark CPET, Cosmed, Italy). Key CPET outcome measures derived included highest achieved  $\text{VO}_2$  ( $\text{VO}_{2\text{max}}$ ) and peak HR. %p $\text{VO}_{2\text{max}}$  was estimated as the ratio between measured or estimated  $\text{VO}_{2\text{max}}$  and predicted  $\text{VO}_{2\text{max}}$  using sex-specific equations from Wasserman and Whipp

[8]. 145 participants wore the GV4 during CPET.

### 2.3. Smartwatch $\text{VO}_{2\text{max}}$ estimate

Participants were fitted with a Garmin Vivoactive 4s (GV4) smartwatch. An app enabled the transfer of physiological data from the watch to servers at UCL for research purposes [17]. Garmin reports that  $\text{VO}_{2\text{max}}$  estimates can be generated from all-day passive HR data collection, activity recordings or both and can take up to 30 days to populate.

### 2.4. Data processing & statistical analysis

First and last  $\text{VO}_{2\text{max}}$  estimates provided by GV4 along with the number and duration of activity recordings in the 60 days following CPET were used. %p $\text{VO}_{2\text{max}}$  was measured using predicted  $\text{VO}_{2\text{max}}$  from Wasserman and Whipp's anthropometric-based equations [16]. Statistical analyses were performed using MATLAB 2022a. Sample characteristics and outcome parameters are described using median [interquartile range; IQR] for continuous variables and frequency (percentage) for categorical variables. Agreement was assessed using Bland-Altman analysis [18] presented as mean bias [Limits of agreement; LoA], absolute percentage error (APE), reported as median [IQR] and Pearson's correlation coefficient (cc). LoAs were measured as  $m_E \pm 1.96*SD_E$ , where  $m_E$  and  $SD_E$  represent the mean and standard deviation of the estimation error.

## 3. Results

A summary of study participant characteristics and study parameters is presented in Table 1. The peak HR and peak  $\text{VO}_2$  measured during CPET were 145 [129, 159] beats per minute (bpm) and 22.4 [17.5, 27.4] ml/kg/min, respectively.

**Table 1.** Study participant characteristics and outcome parameters presented as median [IQR; interquartile range] or n (%). BMI (body mass index), HR (heart rate), bpm (beats per minute), CPET (cardiopulmonary exercise test), GV4 (Garmin Vivoactive 4s),  $\text{VO}_2$  (oxygen consumption), No. (number).

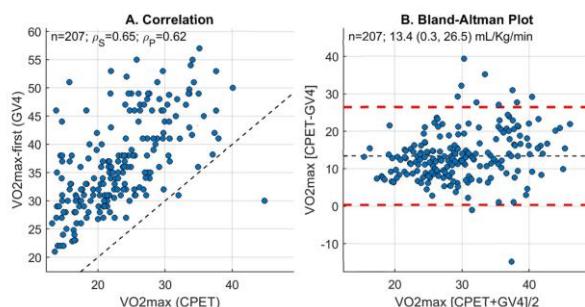
	n	Median [IQR] or n (%)
Age (years)	215	56 [32, 62]
Male Sex	215	44 (21%)
BMI ( $\text{kg}/\text{m}^2$ )	215	25.1 [21.9, 28.5]
Resting HR (bpm)	212	70 [62, 78]
CPET peak HR (bpm)	212	145 [129, 159]
GV4 peak HR (bpm)	145	148 [134, 163]
CPET $\text{VO}_{2\text{max}}$ (ml/kg/min)	207	22.4 [17.5, 27.4]
GV4 $\text{VO}_{2\text{max}}$ [First] (ml/kg/min)	215	35.0 [30.0, 41.9]
GV4 $\text{VO}_{2\text{max}}$ [Last] (ml/kg/min)	215	37.0 [31.3, 43.0]

CPET %pVO <sub>2</sub> max	144	91 [78, 101]
GV4 %pVO <sub>2</sub> max [First]	207	142 [135, 149]
GV4 %pVO <sub>2</sub> max [Last]	207	148 [138, 155]
No. GV4 activities	214	18 [10, 42]
No. GV4 activities $\geq$ 10 mins	214	9 [2, 32]
Activity duration (mins)	214	21 [9, 35]

VO<sub>2</sub>max estimates from GV4 were moderately correlated with CPET measures (cc=0.62 and 0.66 for first and last estimates) and showed a large positive bias  $\sim$ 14 ml/kg/min with LoA from 0 – 27 ml/kg/min. Correlation between VO<sub>2</sub>max from GV4 and anthropometric-based prediction of VO<sub>2</sub>max was high (cc>0.90). Agreement between %pVO<sub>2</sub>max from GV4 and CPET was poor (cc~0.15, bias  $\sim$ 52%, LoA 7-98 %) (Table 2 & Figure 1).

**Table 2.** Level of agreement between Garmin Vivoactive 4s (GV4) derived and cardiopulmonary exercise test (CPET) measured parameters presented as Pearson's correlation coefficients (cc), bias [LoA; Limits of Agreement] and absolute percentage error (APE) median [interquartile range; IQR]. VO<sub>2</sub> (oxygen consumption), Ave. (average), %p (% predicted), HR (heart rate), bpm (beats per minute).

	n	cc	Bias [LoA]	APE [IQR]
VO <sub>2</sub> max [First] (ml/kg/min)	207	0.62	13.4 [0.3, 26.5]	56 [40, 80]
VO <sub>2</sub> max [Last] (ml/kg/min)	207	0.66	14.6 [2.5, 26.6]	60 [45, 88]
%pVO <sub>2</sub> max [First]	207	0.14	52.4 [7.0, 97.8]	56 [40, 80]
%pVO <sub>2</sub> max [Last]	207	0.28	57.4 [15.5, 99.2]	60 [45, 88]
Peak HR (bpm)	144	0.93	3.9 [-11.9, 19.7]	4 [2, 7]



**Figure 1.** Correlation and Bland-Altman plots demonstrating levels of agreement between Garmin Vivoactive 4s (GV4) derived VO<sub>2</sub>max [First] and cardiopulmonary exercise test (CPET) measured VO<sub>2</sub>max.

## 4. Discussion

We sought to establish the accuracy of remote smartwatch estimation of VO<sub>2</sub>max and %pVO<sub>2</sub>max compared to a clinic based CPET. Our primary findings

were 1) a moderate correlation and agreement with large positive bias between GV4 derived and CPET-measured VO<sub>2</sub>max; 2) no improvement in GV4 performance after two months of monitoring; 3) agreement between GV4 derived and CPET measured %pVO<sub>2</sub>max was poor.

Clinical assessment of CRF provides an optimal approach for stratifying patients according to risk [9] and smartwatches provide an opportunity to do so remotely without the requirement for expensive testing equipment, clinical staff and time. We observed moderate agreement with large positive bias between GV4 derived and CPET measured VO<sub>2</sub>max, consistent with Molina-Garcia and colleagues' review findings during resting conditions [12]. HR is the primary parameter utilised by smartwatches for the estimation of VO<sub>2</sub>max. In line with prior work, we observed strong correlation, good agreement and small APE between GV4 derived and CPET measured HR [19]. A limitation of our study is that CPET was performed on a semi-recumbent cycle ergometer which can be associated with a lower achieved VO<sub>2</sub>max when compared to that of treadmill testing [20] or upright cycling [21]. We cannot confirm whether the observed differences between the GV4 derived and CPET measured VO<sub>2</sub>max are due, in part, to testing modality.

We observed poor agreement between GV4 derived and CPET measured %pVO<sub>2</sub>max. This may in part be explained by the strong correlation (cc~0.90) between VO<sub>2</sub>max estimated by GV4 and by anthropometric-based equations. As expected, CPET-measured VO<sub>2</sub>max was lower, but GV4-estimated VO<sub>2</sub>max was higher, than anthropometric-based prediction of VO<sub>2</sub>max. This in turn, resulted in poor agreement between CPET- and GV4-based %pVO<sub>2</sub>max.

Other limitations of our study include that all participants wore the GV4 and therefore our results may not be generalizable to other manufacturers. Participants were not asked to perform strenuous physical activities whilst wearing the GV4, which may have impacted the accuracy of VO<sub>2</sub>max estimation. A comparison between those who did and did not wear the GV4 during CPET was not performed and would be valuable.

## 5. Conclusion

GV4 provided estimates of VO<sub>2</sub>max that overestimates but moderately correlated with CPET measured VO<sub>2</sub>max. The agreement for %pVO<sub>2</sub>max was poor.

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