

1 Decreased cardio-respiratory information transfer is associated
2 with deterioration and a poor prognosis in critically ill patients
3 with sepsis

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27 **Running title:** Physiological network mapping in sepsis

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29 **Conflict of interest:** None

30
31 **Ethics statement:** MIMIC-III is publicly available to researchers under a data use agreement. The data
32 has been deidentified according to HIPAA standards and the project was approved by the Institutional
33 Review Boards of Beth Israel Deaconess Medical Center and MIT (IRB protocol nos. 2001P001699/14
34 and 0403000206). Individual patient consent was waived as the project did not affect clinical care and
35 all protected health information was deidentified. The authors involved in data extraction completed
36 mandatory online ethics training at MIT and were credentialed (ID 10304625).

38 **Abstract**

39 Assessing illness severity in the ICU is crucial for early prediction of deterioration and prognosis.
40 Traditional prognostic scores often treat organ systems separately, overlooking the body's
41 interconnected nature. Network physiology offers a new approach to understanding these complex
42 interactions. This study used the concept of transfer entropy (TE) to measure information flow
43 between heart rate (HR), respiratory rate (RR), and capillary oxygen saturation (SpO₂) in critically ill
44 sepsis patients, hypothesizing that TE between these signals would correlate with disease outcome.
45 The retrospective cohort study utilized the MIMIC III Clinical Database, including patients who met
46 Sepsis-3 criteria on admission and had 30 minutes of continuous HR, RR, and SpO₂ data. TE between
47 the signals was calculated to create physiological network maps. Cox regression assessed the
48 relationship between cardiorespiratory network indices and both deterioration (SOFA score increase
49 of ≥2 points at 48 hours) and 30-day mortality. Among 164 patients, higher information flow from
50 SpO₂ to HR [TE(SpO₂→HR)] and reciprocal flow between HR and RR [TE(RR→HR) and TE(HR→RR)] were
51 linked to reduced mortality, independent of age, mechanical ventilation, SOFA score, and
52 comorbidity. Reductions in TE(HR → RR), TE(RR→HR), TE(SpO₂→RR), and TE(SpO₂→HR) were associated
53 with increased risk of 48-hour deterioration. After adjustment for potential confounders, only TE(HR→
54 RR) and TE(RR→HR) remained statistically significant. The study confirmed that physiological network
55 mapping using routine signals in sepsis patients could indicate illness severity and that higher TE
56 values were generally associated with improved outcomes.

57
58 **New & Noteworthy:** This study adopts an integrative approach through physiological network analysis
59 to investigate sepsis, with the goal of identifying differences in information transfer between
60 physiological signals in sepsis survivors versus non-survivors. We found that greater information flow
61 between heart rate, respiratory rate, and capillary oxygen saturation was associated with reduced
62 mortality, independent of age, disease severity, and comorbidities. Additionally, reduced information
63 transfer was linked to an increased risk of 48-hour deterioration in patients with sepsis.

64
65 **Key words:** Intensive Care, Network physiology, Sepsis, Survival, Transfer Entropy

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67

68 Introduction

69

70 Sepsis is a complex disease that causes life-threatening organ dysfunction due to a dysregulated host
71 response to infection (1). It is one of the most frequent causes of death worldwide, requiring patients
72 to be admitted to intensive care units (ICU) for intensive physiological and clinical monitoring (2). The
73 complexity of its pathophysiology and the heterogeneity of its manifestations make sepsis challenging
74 to detect, monitor, and treat. Quantifying illness severity is a crucial aspect of any ICU admission, as it
75 allows for timely interventions to improve outcomes, aids in decision-making, and helps allocate
76 scarce resources (3). However, despite the existence of severity scores for almost 40 years,
77 predictions remain imperfect, and they are primarily used for hospital-level case-mix adjustment.
78 Novel digital biomarkers for measuring illness severity may therefore be useful to ICU staff.

79

80 The commonest approaches to date have assigned increasing numerical values for progressive
81 dysfunction in each organ system in order to assess their overall association with mortality using
82 regression. Well-known examples include the Sequential Organ Failure Assessment (SOFA) (4), the
83 Simplified Acute Physiology Score II (SAPS II) (3), the Acute Physiology and Chronic Health Evaluation II
84 (APACHE II) score (5), and the UK's Intensive Care National Audit and Research Centre (ICNARC)
85 model (6). However, these scores are usually only calculated at the time of critical care admission, or
86 at most on a daily basis, and they often rely on summary measures such as the worst recorded value.
87 Recent machine learning approaches using more granular data have managed to improve short-term
88 prognostication for specific outcomes (7-11), but by treating organs as independent parts to be
89 combined, even these techniques may be ignoring useful information.

90

91 Network physiology is a new way of viewing the problem, focussing not on individual organs, but on
92 the degree of interaction *between* them (12). Various measurable aspects of physiology, such as heart
93 rate or respiratory rate, can be conceptualised as “nodes”, with an overall network created by
94 functional connections or “edges” between each node pair if they interact. Strong networks are those
95 which have multiple edges between multiple nodes, or high quantitative values for their connections,
96 as measured by a variety of techniques including simple correlation (13-15) and information transfer
97 (16-18). The relevance to illness prediction is that a strong, well-connected network, despite
98 significant individual organ system stress, may represent physiological resilience and predict survival
99 or response to therapy (13,19).

100 According to information theory, the amount of information in a physiological time series (e.g., heart
101 rate or capillary oxygen saturation fluctuations) can be measured by computing the degree of
102 complexity (i.e., entropy) of the signal (20,21). This idea can be extended to quantify the amount of
103 information exchanged between two physiological signals (18,22,23). Transfer entropy (TE) is one
104 measure of information transfer between parallel time-series. It is a non-parametric, non-linear
105 extension of the concept of entropy (16) that can detect the magnitude and direction of information
106 flow between physiological time series data. TE increases when future values of one time series can
107 be better predicted with knowledge of preceding values from a different time series – suggesting the
108 former is influenced by the latter (Figure 1). One advantage of TE is that it can measure the
109 bidirectional exchange of information between two nodes. For example, it allows us to separately
110 assess how changes in respiratory rate influence capillary oxygen saturation and how changes in
111 oxygen saturation affect respiratory rate. This allows for the assessment of directed interactions
112 between different physiological time series for network mapping based on available physiological
113 signals. For example, using TE, the strength of the cardiorespiratory network could be assessed in
114 experimental hypoxia in healthy participants (18). Assessment of the strength of the cardiorespiratory
115 network in critical illnesses is important in critical care as it may shed light on the pathophysiology of
116 compensatory mechanisms and help predict deterioration or poor outcomes. This is particularly

117 important in complex disorders such as sepsis which is associated with multiorgan failure and high
118 mortality (2,24).

119 This study therefore aimed to understand whether cardiorespiratory transfer entropy, measured from
120 bedside monitor data of patients with sepsis in the MIMIC-III database, could be used to assess their
121 physiological network strength and its relationship with 48-hour deterioration and mortality.

122

123 **Materials and methods**

124 This was a retrospective cohort study using the Waveform Database Matched Subset of the Medical
125 Information Mart for Intensive Care III (MIMIC-III) Clinical Database (25,26), reported in accordance
126 with the RECORD guidelines (27).

127

128 **Ethics statement:** The MIMIC-III was anonymized following HIPAA standards and the project received
129 approval from the Institutional Review Boards of Beth Israel Deaconess Medical Center and MIT (IRB
130 protocol nos. 2001P001699/14 and 0403000206, respectively) (25). The authors who handled the
131 data underwent required ethics training at MIT and were credentialed (ID 10304625).

132

133 **Participants and data extraction:** Details of patient enrolment flow diagram and data extraction is
134 described elsewhere (28). In brief, inclusion was limited to patients over 18 years of age, with a single
135 ICU stay who met the Sepsis-3 criteria on admission (an increase in SOFA score of ≥ 2 points and
136 suspicion of infection (1)). Initially, the complete MIMIC-III clinical dataset was downloaded to a
137 secured cloud storage of the University College London (UCL) and structure query language (SQL)
138 code was used to extract the required data based on the inclusion criteria. Patients' identity codes
139 from SQL data were used to extract the numeric physiological data using the WFDB toolbox
140 (<https://archive.physionet.org/physiotools/matlab/wfdb-app-matlab/>). Specifically, the earliest
141 numeric time-series within the first ICU admission were downloaded for each patient using the
142 "rdsamp" function. The extracted data were then curated and aligned with header files containing the
143 signal information, sampling frequency, and signal class (variable names) using the "wfdbdesc"
144 function. To ensure adequate data for stable estimation of TE, patients were included only if their
145 waveform records contained at least 30 minutes of continuous, noise-free signals sampled at a rate of
146 1 Hz (29). The first 30-minute segment of noise-free waveform data was used for analysis. Noise-free
147 data were defined as having a valid time-stamped value for every second in the waveform database.
148 Consequently, the included time series had no missing data, and no imputation was required. 79
149 records met these criteria when considering three waveforms - heart rate (HR), respiratory rate (RR)
150 and capillary oxygen saturation (SpO_2) – and formed the basis of the final cohort.

151 Matched information was retrieved from the Clinical Database on patient age, sex, SOFA scores,
152 Elixhauser comorbidity index, mechanical ventilation, and date of death. A 30-day survival data was
153 missing in 15 patients; therefore, 164 patients were included in the final survival analysis

154

155 **Definition of deterioration:** The SOFA score was extracted for the day when a patient's physiological
156 signals record was available and again 48 hours later. Deterioration was defined as SOFA score ≥ 2
157 points at 48 hours. Due to early discharge or death, 55% of 48-hour SOFA scores in this study required
158 imputation. To handle missing for data for 48 hour SOFA scores calculation, the maximum score of 24
159 was applied if the patient had already died (30), and a score of 1 applied if discharged alive from ICU.

160

161 **Calculation of transfer entropy (TE)**

162 An existing open-source algorithm (<https://www.physionet.org/content/tewp/1.0.0/>) was used to
163 calculate TE (in bits) for parallel physiological time-series. This algorithm employs an extension of
164 Darbellay-Vajda adaptive partitioning (22) to estimate a non-linear probability density function in a
165 computationally efficient manner. It calculates the probability of event B of a time lag window length
166 of t_b occurring after the outcome of event A of a time lag of window length of t_a was observed (Figure

167 1), where A and B are representations of the physiological parameters (e.g., HR, RR, and SpO₂). The
168 returned value of transfer entropy represents the amount of directional information transferred from
169 a data segment of one physiological time series to the future data segment of another time series. In
170 addition to probability density function estimation, TE magnitude also depends on the lag chosen
171 between the source and target time series. As the optimal lag for each node pair was not known *a*
172 *priori*, TE was measured for a range of time lag values that set equally for both t_A and t_B , at 1, 5, 10,
173 15, 20 and 25 seconds (Figure 1). This approach was conducted to ascertain the consistency of the
174 results and establish an optimal time lag for future transfer entropy computations. Based on these
175 results, a time lag value of 5 seconds was chosen to calculate the TE estimate for each edge for all
176 patients.

177

178 **Network visualization**

179 Network maps were constructed for qualitative assessment by conceptualising each physiological
180 signal as a node, with edges drawn between nodes showing the strength of any directional
181 information flow. TE edge strength was displayed as the average group value. Comparison of directed
182 transfer entropy values between physiological time-series were conducted at a time lag of 5 seconds,
183 with each mean transfer entropy calculation being compiled to form an adjacency matrix. This matrix
184 was then used to plot a bidirectional network graph in MATLAB.

185

186 **Network indices**

187 In the context of network science, “Centrality” measures the importance of a node within a network,
188 particularly in relation to the flow of information. Indegree (ID) and outdegree (OD) measure the
189 centrality of a node by calculating the information that each node receives (ID) or sends out (OD).
190 Indegree and outdegree centralities of SpO₂, HR, and RR were calculated for each patient using
191 respective transfer entropy adjacency matrices using MATLAB.

192

193 **Statistical analysis**

194 Data are shown as mean \pm SD unless stated otherwise. The mean differences in network edges and
195 node centralities between the groups (survivors vs non-survivors and deterioration vs no
196 deterioration) were calculated using the Student’s t-test or its non-parametric equivalent (Mann-
197 Whitney U-test).

198 Cox regression was used for estimation of hazard ratios with 95% confidence intervals. Multivariate
199 Cox regression was performed with covariates of SOFA, mechanical ventilation, Elixhauser
200 comorbidity score, and age. ROC curve analysis was used to find optimum cut-off point (Youden’s
201 index) with optimum sensitivity and specificity in prediction of 30-day mortality in the intensive care
202 unit and of deterioration. To visualise patient survival, the Kaplan Meier curves were applied and
203 analysed using a log rank (Mantel-Cox) method. P-value less than 0.05 was used for statistical
204 significance. Two-way ANOVA was used for assessment of the effect of time lag on TEs. We also
205 wondered if shorter time-series (namely, 20, 10, 5, 2 and 1-min) can estimate TE calculated from 30-
206 min time-series and predicts poor outcomes (mortality, deterioration) within this patient population.
207 Thus, Bland-Altman plots were used to identify bias in TE of time series of 20, 10, 5, 2, and 1 minutes
208 (starting from the beginning of recording) compared to the 30-min transfer entropy values. This
209 method is based on the quantification of the agreement between two quantitative measurements
210 (short time-series, A versus 30-min, B) by studying the relationship between $A - B$ and $(A + B)/2$
211 (Bland and Altman, 1999). The linear regression analysis was used to test for statistical significance of
212 the bias for the intercept and slope in the Bland-Altman plots.

213

214 **Results**

215 Descriptive characteristics of the participants are shown in Table 1. Overall, 130 patients survived
216 after a 30-day follow-up period. The non-survivors (n = 34) were older (65 ± 18 vs. 75 ± 12 , $P=0.003$)
217 and had higher SOFA scores (4.1 ± 2.3 vs. 6.8 ± 4.1 , $P<0.001$). The comorbidity index (Elixhauser) was

218 higher in non-survivors ($P=0.027$). Changes in SpO_2 mean and pattern of fluctuations in this cohort has
219 been reported elsewhere (28). In brief, the average SpO_2 was marginally higher in the survivors
220 compared to the non-survivors (97.4 ± 2.2 vs. 96.0 ± 6.3 , $P = 0.033$). Mean HR was lower in survivors
221 compared to the non-survivors (83.5 ± 18.3 vs. 94.0 ± 23.8 beats/min, $P = 0.0063$). There was no
222 statistical difference in RR between survivors and non-survivors (19.7 ± 4.8 vs. 21.2 ± 6.0 breath/min,
223 $P=0.117$). There was no difference in distribution of gender or ethnicity between survivors and non-
224 survivors.

225

226 **Association of transfer entropy and network indices with 30-day mortality**

227 The TE values are subsequently denoted as follows:

228

229 From heart rate to respiratory rate: TE (HR \rightarrow RR)

230 From heart rate to oxygen saturation: TE (HR \rightarrow SpO_2)

231 From respiratory rate to heart rate: TE (RR \rightarrow HR)

232 From respiratory rate to oxygen saturation: TE (RR \rightarrow SpO_2)

233 From oxygen saturation to heart rate: TE (SpO_2 \rightarrow HR)

234 From oxygen saturation to respiratory rate: TE (SpO_2 \rightarrow RR)

235

236

237 As shown in Table 2, the highest average value of TE was during the transfer of information from SpO_2
238 to RR. The lowest TE between physiological signals was during the transfer of information from HR to
239 SpO_2 . TE values in most directions were significantly higher in survivors compared to non-survivors
240 after 30 days of follow-up (Table 2).

241

242 *Network indices:* To assess the importance of each node within the network, centrality indices
243 (indegree and outdegree) were measured and compared between the groups. The results indicate
244 that within the HR-RR- SpO_2 network, the RR node receives the highest amount of information from
245 other nodes (highest indegree), and the SpO_2 node sends the highest amount of information to other
246 nodes (highest outdegree). Table 3 shows details of the network indices between groups. There is a
247 significant difference between survivors and non-survivors in indegree or outdegree indicating that all
248 nodes have higher information flow in survivors compared with non-survivors.

249

250 *Survival analysis:* Cox regression analysis was conducted to evaluate the risk of 30-day mortality
251 associated with TE and network indices (Table 4). Reduction in TE or centrality of individual nodes
252 were associated with increased chance of mortality in this cohort of patients with sepsis. Since non-
253 survivors were older and had higher SOFA scores and comorbidities, we considered whether these
254 characteristics might confound the association between TE and mortality. Additionally, factors such as
255 mechanical ventilation and drugs such as the use of beta blockers could affect transfer of information
256 between physiological signals and potentially influence these findings. To address these concerns, we
257 conducted a multivariate Cox regression analysis to evaluate the dependence of individual network
258 indices on factors such as age, SOFA score, Elixhauser comorbidity index, mechanical ventilation, and
259 beta blocker (propranolol, metoprolol, or esmolol) use. The results indicated that among network
260 indices, TE (SpO_2 \rightarrow HR), TE (HR \rightarrow RR), TE (RR \rightarrow HR), Indegree of HR, all outdegrees (HR, RR and SpO_2)
261 as well as the sum of TEs were independent predictors of 30-day mortality (Supplementary material
262 1). Lower TE values in the group that went on to die, suggests reduced connectivity and weakened
263 cardiorespiratory network in non-survivor. Graphical visualization of these network edges is shown in
264 Figure 2.

265

266 The results of the multivariate Cox regression analysis indicated that higher age, higher SOFA scores,
267 and mechanical ventilation were independent predictors of mortality (Supplementary material 1). As

268 expected, mechanical ventilation altered the transfer of information between physiological signals,
269 leading to reduced TE (SpO₂ → RR), TE (HR → SpO₂), TE (HR → RR) and TE (RR → SpO₂) values compared
270 to spontaneously breathing patients (Supplementary material 2A). To further investigate the influence
271 of mechanical ventilation on TEs and network indices within our cohort, we compared TEs and
272 network indices between survivors and non-survivors after excluding patients who received
273 mechanical ventilation. The results again demonstrated that TE (SpO₂ → HR), TE (HR → RR), TE (RR →
274 HR), the indegree of HR and RR, and all outdegrees (HR, RR, and SpO₂) were significantly lower in non-
275 survivors compared to survivors among patients with spontaneous breathing (Supplementary
276 material 2B). These findings are consistent with the results of the multivariate Cox regression analysis,
277 which demonstrated the independence of TE (SpO₂ → HR), TE (HR → RR) and TE (RR → HR) from
278 mechanical ventilation in predicting mortality within this cohort.
279

280 *The effect of time lag on transfer entropy:* To ensure that an optimized time lag value is used for TE
281 calculation, TE was measured for a range of time lag values at 1, 5, 10, 15, 20 and 25 second. Survivor
282 group consistently had higher transfer entropy values at all time lags (Figure 3). It is noteworthy that
283 when the calculation was set between a time lag of 5 and 25, the resulting transfer entropy values fell
284 within a comparable range, as opposed to when a time lag of 1 was utilized. This substantiates the
285 use of time lag 5 seconds in transfer entropy calculation. TE (SpO₂ → HR), TE (HR → RR) and TE (RR →
286 HR) were chosen for this analysis as they demonstrated a significant predictive power in multivariate
287 Cox regression analysis for mortality.
288

289 **Association of transfer entropy and network indices with 48-hours deterioration**

290 31 (18.9%) patients had an increase in SOFA score ≥ 2 points at 48 hours. TE values and network
291 indices of this group were compared with the rest of the patients who didn't show 48-hour
292 deterioration. As shown in Table 5, TE (SpO₂ → HR), TE (HR → RR) and TE (RR → HR) were significantly
293 lower in the group that exhibited deterioration. Likewise, the centrality measures of all nodes, except
294 for indegree SpO₂, were significantly lower in the deteriorating group (Table 6).
295

296 *Survival analysis:* Cox regression analysis showed that reduction in most TE or network indices of
297 individual nodes were associated with increased chance of 48-hour deterioration in this cohort of
298 patients with sepsis (Table 7). However, after controlling for age, SOFA, Elixhauser comorbidity index
299 and mechanical ventilation, only TE (HR → RR) and TE (RR → HR) remained statistically significant
300 suggesting that these edges provide information on 48-hour deterioration independent of other
301 clinical covariates. A summary of multivariate Cox regression analysis is shown in Supplementary
302 material 3. Graphical visualization of these network edges is shown in Figure 4.
303

304 **Diagnostic performance of network indices for 30-day mortality**

305 ROC curve analysis was performed to evaluate diagnostic performance of TEs and network indices for
306 mortality (Figure 5), where TE (HR → RR) and outdegree HR showed the highest accuracy for
307 sensitivity and specificity than the other classifiers (AUC > 0.5, P < 0.01 for all variables).
308

309 Kaplan-Meier survival plots were constructed to compare survival between different directional TE
310 groups and between outdegrees of TE, categorised based on the Youden index threshold of ROC for
311 30-day mortality. Kaplan-Meier plots (Figure 6 and 7) showed separation of these groups' survival
312 curves based on the thresholds for TE (SpO₂ → HR), TE (HR → RR), TE (RR → HR) and all outdegrees
313 with statistical significance assessed using the log rank test ($p < 0.001$). Indegree of HR is also a
314 significant predictor of mortality in the log rank test. Data not shown.
315
316

317 Discussion

318

319 This study takes an integrative approach through network analysis to investigate sepsis and aims to
320 identify differences in the information transfer and connectivity of organ systems between sepsis
321 survivors and non-survivors. To optimize the mapping method's network analysis, we investigated the
322 suitable range of time lag for transfer entropy calculation. Transfer entropy has rarely been applied in
323 sepsis prognosis or organ deterioration assessment, even though HR, RR, and SpO₂ signals are closely
324 monitored in clinical settings, and transfer entropy calculation has a well-established algorithm. Using
325 HR, RR, and SpO₂ as clinical variables to represent the cardio-respiratory system, the study
326 investigated the transfer entropy values of 164 sepsis patients in the ICU.

327

328 Summary of results and interpretation

329 This study demonstrated several important new findings:

330 Firstly, the study found that the group means of all transfer entropy values were significantly higher in
331 survivors than in non-survivors, indicating more active physiological systems and greater information
332 transfer in patients with better prognoses. This supports the hypothesis that decreased homeostatic
333 interorgan connectivity is associated with poor prognosis in critically ill sepsis patients, which is also
334 consistent with previous studies on organ systemic dysfunction in critically ill patients (13) and
335 patients with cirrhosis (14). In normal health, heart rate, cardiac output, blood pressure, respiratory
336 rate, tidal volume and many other measurable aspects of cardiorespiratory physiology are intricately
337 linked via positive and negative feedback systems. Exactly how mutual effects are mediated is still not
338 perfectly understood (31), but increases in blood pressure stimulate arterial baroreceptors, leading to
339 slowing of respiration (32), and changes in arterial oxygen saturation can similarly be precipitated by
340 changes in the cardiovascular system, as these affect arterial oxygen tension via altered ventilation-
341 perfusion matching in the lung. The mechanism and benefits of respiratory sinus arrhythmia (changes
342 in HR in each respiratory cycle) is well documented (33). The effect of RR on HR and blood pressure,
343 via changes in intrathoracic pressure, is already used widely in anaesthesia and intensive care
344 medicine to understand intravascular volume status (34). There is also a wealth of evidence showing
345 that heart rate variability (HRV) is lower in patients with worse ICU outcomes (35), something which
346 would be consistent with partial uncoupling of organ-systems and reduced TE in pairs that included
347 heart rate. Likewise, reduced oxygen saturation entropy has recently been reported in non-surviving
348 patients with sepsis (28) which is line with reduced transfer of information between nodes that
349 included SpO₂ in patients with poor prognosis. Reduced transfer of information between physiological
350 signals may represent uncoupling of organ systems during a pathologic challenge (e.g. infection).
351 While it is expected that compensatory mechanisms lead to enhanced coupling of physiological
352 subsystems during physiologic challenges, in the group of patients who have uncoupled physiological
353 networks, this may lead to deterioration and death (Figure 8). The reason behind the uncoupling of
354 organ systems in life-threatening sepsis is not well understood. Experimental reports suggest end-
355 organ hypo-responsiveness to autonomic neural stimulation (36,37), decreased controllability of the
356 cardiac pacemaker (38), and/or impaired neural processing within the brainstem autonomic
357 regulatory centres (e.g., the Nucleus of the Solitary Tract) (39) during experimental sepsis.

358

359 Secondly, the study demonstrated that directed transfer entropy from physiological time-series can
360 predict mortality and 48-hour organ function deterioration in critically ill patients with sepsis,
361 independent of SOFA score, comorbidity and ventilation status. These findings highlight the potential
362 of transfer entropy in filling the gap in foreseeing the potential underlying dysfunctional connections
363 between organ systems of complex diseases. Measurement of HR, RR, and SpO₂ is easy both at the
364 ICU bedside and during fieldwork (e.g., in poorly resourced or extreme environment settings using
365 wearable devices). TE-based network measures can be added to ICU digital monitors or portable
366 devices. The current survival prediction and analysis score in the ICU leaves room for foreseeing the
367 potential underlying dysfunctional connections between organ systems in complex diseases. In this

368 case, TE and network indices can be continuously calculated and monitored as a digital value for
369 tracking individuals who require more attention and for making important clinical decisions during
370 patient care. The independence of TEs from SOFA in predicting deterioration and outcomes means
371 that network indices have the potential to be used in conjunction with SOFA and other
372 clinical/laboratory measures in patient care. The independence of TE-based network indices in
373 predicting poor outcomes also provides insight into the pathophysiology of sepsis and emphasizes the
374 importance of an integrated network approach in understanding the mechanisms of dysregulated
375 host responses to infection. Organ system connectivity probably plays an important role in the
376 regulated host physiological response to infection, a concept that is not typically assessed in most
377 cellular/molecular studies, which are carried out using a reductionistic approach (40).

378
379 Thirdly, the findings in Figure 3 optimized the transfer entropy calculation by demonstrating that TE
380 ($\text{SpO}_2 \rightarrow \text{HR}$), TE ($\text{HR} \rightarrow \text{RR}$) and TE ($\text{RR} \rightarrow \text{HR}$) reaches a plateau at a time lag of approximately 5
381 seconds and remains stable afterward. This finding is interesting and aligns with previous reports that
382 attempted to estimate the memory length within the cardiorespiratory system (41,42). In the context
383 of physiological time-series, memory is a statistical feature that persists for a period and distinguishes
384 the time-series from a random, or memory-less, process (41). Shirazi et al. developed a method for
385 quantifying memory in physiological time-series and reported that the memory length is estimated to
386 be around 5 to 25 seconds in the cardiorespiratory system in both health and disease (41). This means
387 any intrinsic perturbation within the physiological system would affect the system for a limited time
388 before the effect dissipates. This limited memory length makes the system more controllable, as
389 prolonged memory can impair the adaptability of the physiological system (38,43). Furthermore, a
390 time lag of 5 seconds also represents approximately two respiratory cycles, which aligns with the
391 known physiological interaction between RR and HR within this time frame (e.g., respiratory sinus
392 arrhythmia).

393
394 In the analysis of mortality and deterioration prediction, we found that only two directed transfer
395 entropy values showed a consistent pattern of significance for all statistical analyses were $\text{HR} \rightarrow \text{RR}$ and
396 $\text{RR} \rightarrow \text{HR}$. In the context of $\text{HR} \rightarrow \text{RR}$ and $\text{RR} \rightarrow \text{HR}$, a study of directional coupling between the cardio-
397 respiratory system may explain the clinical significance of transfer entropy. In a recent study,
398 Borovkova et al. revealed the presence of bidirectional couplings between cardiac and respiratory
399 cycles across all age groups in healthy participants (44). Their findings showed that the coupling from
400 respiration to the parasympathetic control of HR is stronger than the coupling in the opposite
401 direction in health. They also suggested that the directed interaction between RR and HR may be
402 disrupted in complex diseases such as sleep apnoea, leading to an increase in the directional coupling
403 from the main heart rhythm to respiration (44). This interpretation may also apply to sepsis, where
404 the information transfer is disrupted from RR to HR in patients with poor prognoses due to the loss of
405 directional coupling. Our study indicates that both TE ($\text{HR} \rightarrow \text{RR}$) and TE ($\text{RR} \rightarrow \text{HR}$) are reduced in non-
406 surviving patients with sepsis compared to survivors. However, a full interpretation of these findings
407 awaits further research involving physiological network mapping in health as well as transition from
408 health to disease. We wondered if TE ($\text{RR} \rightarrow \text{HR}$) shows any correlation with the degree of respiratory
409 sinus arrhythmia and thus measured short-term HRV in this cohort using the Poincaré plot, where
410 SD1 is commonly used as a measure of respiratory sinus arrhythmia (42,45). We observed that SD1
411 exhibits a statistically significant correlation with TE ($\text{RR} \rightarrow \text{HR}$) (data not shown). Further studies are
412 required to elucidate the exact interpretation of TE ($\text{HR} \rightarrow \text{RR}$) and its interaction with TE ($\text{RR} \rightarrow \text{HR}$) in
413 health and disease.
414

415 To shed light on the effect of mechanical ventilation on network indices, we compared the reciprocal
416 interactions between RR, HR, and SpO₂ between mechanically ventilated and spontaneously
417 breathing patients using the concept of TE. Our results showed that TE (SpO₂ → RR), TE (HR → SpO₂),
418 TE (HR → RR) and TE (RR → SpO₂) were significantly lower in mechanically ventilated patients
419 compared to spontaneously breathing patients (Supplementary material 2A). This finding is expected,
420 as mechanical ventilation minimises the spontaneous physiological feedback loops involved in
421 respiratory pattern control. Our multivariate Cox regression analysis demonstrated that network
422 indices predict survival independently of mechanical ventilation (Supplementary material 1). Similarly,
423 in spontaneously breathing patients without mechanical ventilation, network indices were
424 significantly higher in survivors in comparison with non-survivors (Supplementary material 2B). These
425 findings suggest that mechanical ventilation has not introduced bias into our results. Interestingly,
426 even in mechanically ventilated patients, RR and SpO₂ time-series show subtle fluctuations, which
427 might be linked to ventilator settings such the Assist-Control mode (where each breath can be either
428 patient-initiated or controlled by the ventilator). Such variations in respiratory cycles in mechanically
429 ventilated patients may activate physiological feedback loops within the patient control system,
430 potentially resulting in information transfer that, while weaker, still exists in mechanically ventilated
431 patients. Details on ventilator settings are not readily available in the MIMIC-III dataset, preventing
432 their inclusion in our analysis. Future prospective studies could investigate these settings to gain a
433 deeper understanding of their impact on cardio-respiratory information transfer in critically ill
434 patients with sepsis.

435
436 In this study, we focused on cardio-respiratory information transfer to explore physiological networks
437 in patients with sepsis. The potential application of network physiology in critically ill patients has
438 been suggested by other investigators (13,46) for prognostication as well as for evaluating weaning
439 readiness from mechanical ventilation (47-49). The results of the present study are promising and
440 may pave the way for extending the analysis and applying the reconstruction of causal networks in
441 physiology and critical care using other non-linear methods (50-52) and machine learning approaches
442 (53,54).

443
444 Linear methods (e.g., correlation analysis) and non-linear methods have been extensively used to
445 study the coupling of cardio-respiratory systems in sepsis (55,56). The advantage of non-linear
446 methods, such as transfer entropy, is that they provide an interpretation of the complexity of
447 physiological signal fluctuations in terms of the amount of information (in bits) exchanged between
448 different physiological processes. However, other entropy-based measures can also be used to
449 analyse the coupling of physiological time-series, such as cross-entropy and mutual information
450 (57,58). Cross-entropy measures the synchronization between two parallel signals (59). While
451 synchronization is often observed in the context of physiological rhythms, the exchange of
452 information between two processes does not necessarily lead to synchronization. Thus, TE can
453 estimate information transfer more accurately. Although mutual information does not share the same
454 limitation as cross-entropy, it lacks directionality (60). In contrast, the exchange of information
455 between physiological processes (e.g., heart rate and respiratory rate) is inherently directional.
456 Therefore, the use of TE for assessing directed information transfer is justified in the present study.
457 Future investigations, however, should aim to extend the analysis to identify the optimal analytical
458 methodology that can be used and validated in prospective studies.

459 460 **Limitations**

461 There were important limitations to this study. The principal ones were the small cohort size and the
462 use of only three physiological signals. These related issues were due to the relatively low proportion
463 of patients in MIMIC-III with waveform data; the relatively demanding requirement of 30 minutes
464 simultaneous signals with no missing data; and the *a priori* choice to limit inclusion to a Sepsis-3
465 cohort to reduce the heterogeneity seen in ICU patients. This lack of appropriate data in MIMIC-III

466 may portend issues with TE measurement in the real world: as probes are removed for toileting or
467 other transfers, it may be difficult to obtain unbroken waveform records of sufficient duration for
468 stable estimation of TE and this may limit its potential as a monitor of health. We wondered if shorter
469 time-series can estimate TE calculated from 30-minute time-series and predict poor outcomes
470 (mortality, deterioration) within this patient population. Therefore, we analysed 20-, 10-, 5-, and 1-
471 minute time-series for the calculation of TEs (see Supplementary material 4). Using Bland-Altman
472 analysis, the results showed that different TEs are subject to varying degrees of bias when shorter
473 time-series are used. The most robust TEs were TE (HR → RR) and TE (RR → HR), where 10- and 20-
474 minute time-series could estimate TEs calculated from 30-minute time-series (Supplementary
475 material 4-B2 and B3). Survival analysis also indicated that TE (HR → RR) and TE (RR → HR) calculated
476 from 20-minute time-series could predict mortality and 48-hour deterioration independently of age,
477 SOFA, mechanical ventilation, and comorbidity (Supplementary material 4C). This finding is promising
478 as it shows that shorter time-series can be used for network mapping, which facilitates clinical
479 translation.

480
481 It should also be noted that due to early discharge or death, 55% of 48-hour SOFA scores in this study
482 required imputation. While we used a reasonable method imputation of 48-hour SOFA, our findings
483 on prediction of deterioration may be subject to bias and a larger sample size in future studies could
484 provide more solid evidence for the value to TE-based network mapping in prediction of deterioration
485 in sepsis.

486
487 This study has potential confounders, including the effects of medications (e.g., dexmedetomidine)
488 and arrhythmias (e.g., atrial fibrillation), which may influence the dynamics of physiological signals.
489 Data on the presence or absence of atrial fibrillation during the collection period were unavailable
490 and, therefore, not included in this analysis. Future studies can investigate the impact of atrial
491 fibrillation on TE and network indices. Further limitations were the impact of mechanical ventilation
492 and of excessive supplemental oxygen on the measurement of TE. Both of these factors are partially
493 under the control of the clinician, meaning that measured TE may not always directly reflect the
494 patient's own physiology. In this study, "mechanical ventilation" was defined as both patients
495 undergoing positive pressure ventilation and those using spontaneous breathing modes. Those who
496 were positive pressure ventilated, and in particular paralysed, may have had very low TE values, even
497 if this ventilation was temporary for patients with relatively normal lung function (for example,
498 postoperatively). Supra-normal oxygen saturation levels were also sometimes seen due to excessive
499 supplemental oxygen, both in ventilated and non-ventilated patients. Accidental excessive oxygen
500 administration is common in real world clinical practice (61), but it may have major effect on TE
501 calculation, as it can result in ceiling oxygen saturation (100%) being recorded for every value in the
502 waveform record. These patients then have low or zero TE edge estimates – as target values can be
503 predicted using past information from the target alone. While our results showed that the prognostic
504 value of TEs was independent of mechanical ventilation, future studies can investigate the effect of
505 respiratory support on TEs further.

506
507 The retrospective design of this study may introduce unaccounted bias. Hence, a prospective study is
508 essential to evaluate both classical scoring systems and novel physio-markers for the early diagnosis
509 of sepsis, enabling the development of a smart alarm for proactive clinical intervention.

510 511 **Conclusion**

512 This work has confirmed the potential of transfer entropy measurement as a novel digital biomarker
513 in intensive care. Extension of the current methodology to larger datasets is needed to fully
514 understand the interactions of individual TE edges and the impact of patient confounders and
515 mechanical ventilation on its predictive ability.

516

517 **SUPPLEMENTAL MATERIALS**

518

519 Supplemental material 1: <https://doi.org/10.6084/m9.figshare.27881040>

520 Supplemental material 2: <https://doi.org/10.6084/m9.figshare.27882240>

521 Supplemental material 3: <https://doi.org/10.6084/m9.figshare.27883869>

522 Supplemental material 4: <https://doi.org/10.6084/m9.figshare.27884325>

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526

527

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530

531 **Conflict of interest:** None

532

533 **Authors contribution:**

534 Conceived and designed research (MW, WL, ARM), analysed data (CM, MW, QL, EI, CT, P-YC, AC, TO,
535 ARM), interpreted results of experiments (CM, MW, QL, WL, ARM), prepared figures (CM, MW, CT,
536 QL, ARM), drafted manuscript (MW, QL, ARM), edited and revised manuscript (CM, EI, CT, P-YC, WL),
537 approved final version of manuscript (All authors).

538

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811 Tables:

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813 **Table 1.** Summary of descriptive results.

Variable	Summary value
Age (years) (median, Interquartile range)	68 (53-84)
Male/Female (count, %)	93/71 (57%/43%)
Ethnicity (count, %)	
White	125 (76%)
Black	10 (6%)
Hispanic	5 (3%)
Asian	3 (1%)
Other	3 (1%)
Unknown	18 (11%)
Hospital admission primary diagnosis (count, %)	
Neurological	46 (28%)
Cardiac	35 (21%)
Infective	34 (21%)
Gastrointestinal	9 (5%)
Orthopaedic	4 (2%)
Other	35 (21%)
Elixhauser index (median, Interquartile range)	3 (0-7)
Mechanically ventilated during TE measurement (count, %)	45 (27.4%)
SOFA score on day of TE was measured (median, Interquartile range)	4 (2-6)
SOFA score 48 hours after TE was measured (median, Interquartile range)	1 (1-5)
Deterioration in SOFA score \geq 2 points at 48 hours (count, %)	31 (18.9%)
30-day mortality (count, %)	34 (20.7%)

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829 **Table 2:** Comparison of Transfer Entropy Means between Survivors and Non-survivors:

	Survivors	Non-Survivors	P-value
TE(SpO ₂ →HR)	0.537 ± 0.144	0.449 ± 0.182	0.003
TE(HR→SpO ₂)	0.336 ± 0.187	0.245 ± 0.185	0.013
TE(HR→RR)	0.532 ± 0.163	0.390 ± 0.195	<0.001
TE(RR→HR)	0.510 ± 0.143	0.417 ± 0.207	0.083
TE(SpO ₂ →RR)	0.582 ± 0.168	0.490 ± 0.212	0.083
TE(RR→SpO ₂)	0.361 ± 0.198	0.272 ± 0.208	0.022

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831 **Table 3:** Comparison of Network Indices (Indegree and Outdegree) between Survivors and Non-
832 Survivors

	Survivors	Non-Survivors	P-value
Indegree SpO ₂	0.696 ± 0.380	0.517 ± 0.388	0.016
Indegree HR	1.046 ± 0.277	0.866 ± 0.382	0.034
Indegree RR	1.113 ± 0.316	0.880 ± 0.378	<0.001
Outdegree SpO ₂	1.118 ± 0.224	0.939 ± 0.248	<0.001
Outdegree HR	0.868 ± 0.285	0.636 ± 0.283	<0.001
Outdegree RR	0.870 ± 0.224	0.689 ± 0.249	<0.001

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835 **Table 4:** Monivariate Cox regression analysis to predict 30-day mortality based on Transfer Entropies,
836 and Network Indices (Indegrees and Outdegrees):

	B	SE	P-value	Exp(B)	Confidence Interval (95%)
TE(SpO ₂ →HR)	-2.633	0.901	0.003	0.072	0.012 – 0.421
TE(HR→SpO ₂)	-2.070	0.881	0.019	0.126	0.022 – 0.709
TE(HR→RR)	-3.357	0.789	<0.001	0.035	0.007 – 0.166
TE(RR→HR)	-2.694	0.898	0.003	0.068	0.012– 0.393
TE(SpO ₂ →RR)	-2.122	0.763	0.005	0.120	0.027 – 0.535
TE(RR→SpO ₂)	-1.765	0.821	0.032	0.171	0.034 – 0.856

Indegree SpO ₂	-0.965	0.426	0.023	0.381	0.165 – 0.877
Indegree HR	-1.382	0.453	0.002	0.251	0.103 – 0.610
Indegree RR	-1.421	0.388	<0.001	0.242	0.113 - 0.517
Outdegree SpO ₂	-2.476	0.629	<0.001	0.084	0.025 – 0.289
Outdegree HR	-2.015	0.511	<0.001	0.133	0.049 – 0.363
Outdegree RR	-2.629	0.693	<0.001	0.072	0.019 – 0.281

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Table 5: Comparison of Transfer Entropy Means between Patients with 48-hour Deterioration and without Deterioration.

	Deterioration	No Deterioration	P-value
TE(SpO ₂ →HR)	0.451 ± 0.173	0.534 ± 0.149	0.007
TE(HR→SpO ₂)	0.282 ± 0.180	0.325 ± 0.191	0.247
TE(HR→RR)	0.391 ± 0.211	0.528 ± 0.161	0.005
TE(RR→HR)	0.428 ± 0.195	0.505 ± 0.151	0.016
TE(SpO ₂ →RR)	0.479 ± 0.234	0.582 ± 0.161	0.231
TE(RR→SpO ₂)	0.325 ± 0.213	0.346 ± 0.200	0.590

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Table 6: Comparison of Network Indices (Indegree and Outdegree) between Patients with 48-hour Deterioration and without Deterioration

	Deterioration	No Deterioration	P-value
Indegree SpO ₂	0.606 ± 0.388	0.672 ± 0.388	0.398
Indegree HR	0.878 ± 0.365	1.0395 ± 0.288	0.009
Indegree RR	0.870 ± 0.426	1.11 ± 0.304	0.017
Outdegree SpO ₂	0.929 ± 0.268	1.116 ± 0.220	<0.001
Outdegree HR	0.673 ± 0.312	0.854 ± 0.286	0.002
Outdegree RR	0.752 ± 0.241	0.852 ± 0.237	0.038

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Table 7: Monivariate Cox regression analysis to predict 48-hour Deterioration based on Transfer Entropies, and Network Indices (Indegrees and Outdegrees)

	B	SE	P-value	Exp(B)	Confidence Interval (95%)
TE(SpO ₂ →HR)	-2.267	0.955	0.018	0.104	0.016 – 0.674
TE(HR→SpO ₂)	-0.969	0.928	0.296	0.380	0.062 – 2.340
TE(HR→RR)	-2.842	0.842	0.001	0.058	0.011 – 0.304
TE(RR→HR)	-2.032	0.950	0.032	0.131	0.020 – 0.843
TE(SpO ₂ →RR)	-1.998	0.788	0.011	0.136	0.029 – 0.635
TE(RR→SpO ₂)	-0.427	0.876	0.626	0.652	0.117 – 3.631
Indegree SpO ₂	-0.347	0.453	0.444	0.707	0.291 – 1.718
Indegree HR	-1.115	0.481	0.020	0.328	0.128 – 0.842
Indegree RR	-1.267	0.409	0.002	0.282	0.126 – 0.628
Outdegree SpO ₂	-2.247	0.657	<0.001	0.106	0.029 – 0.383
Outdegree HR	-1.478	0.549	<0.007	0.228	0.078 – 0.669
Outdegree RR	-1.330	0.714	0.062	0.264	0.065 – 1.071

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851 **Figure legends:**

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853 **Figure 1.** A schematic diagram to explain the concept of transfer entropy (TE). The transfer of
854 information from a physiological time-series A to another parallel time-series B is annotated as TE (A
855 → B) and is defined as how much additional information the past of the A time-series contains about
856 the future observation of the B time-series (red arrows) independently of our knowledge of the past
857 state of B (black arrow). Such transfer of information can be presented as an edge in a network
858 connecting directed information from nodes A to B. t_A : time lag in A from present. t_B : time lag in B
859 from present. As the optimal lag for each node pair is not known *a priori*, TE in this study is measured
860 for a range of time lag values that set equally for both t_A and t_B , at 1, 5, 10, 15, 20 and 25 seconds.

861

862 **Figure 2.** Network maps for survivors and non-survivors, showing mean TE values (in bits) for each
863 edge. Red: TEs which are significant predictors of mortality, independent of covariates (age, SOFA,
864 comorbidity index and mechanical ventilation). Edge weighting correspond to magnitude of
865 information flow. HR: heart rate; RR: respiratory rate; SpO₂: oxygen saturation.

866

867 **Figure 3:** Comparison of Transfer Entropies [TE (SpO₂ → HR), TE (HR → RR) and TE (RR → HR)] between
868 survivors and non-survivors at different time lags. Data are shown as mean standard error or mean.
869 Two-way ANOVA showed that group (Survivors/Non-Survivors) and time lag both significantly affect
870 TEs ($P < 0.001$ for all TEs) and there is no interaction between group and time-lag.

871

872 **Figure 4.** Network maps for patients with 48-hour deterioration and no deterioration, showing mean
873 TE values (in bits) for each edge. Edge weighting correspond to magnitude of information flow. HR:
874 heart rate; RR: respiratory rate; SpO₂: oxygen saturation.

875

876 **Figure 5.** ROC Curves for Prediction of 30-day mortality based on Transfer Entropies (A) and Network
877 Indices (B)

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879 **Figure 6:** Kaplan Meier Graphs for Visualization of Prediction of Mortality based on Transfer Entropies.
880 ROC curves were used to obtain optimum cut-off points.

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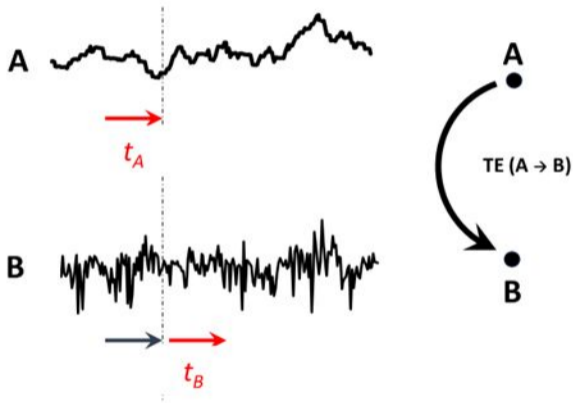
882 **Figure 7:** Kaplan Meier Graphs for Visualization of Prediction of Mortality based on Network Indices.
883 ROC curves were used to obtain optimum cut-off points.

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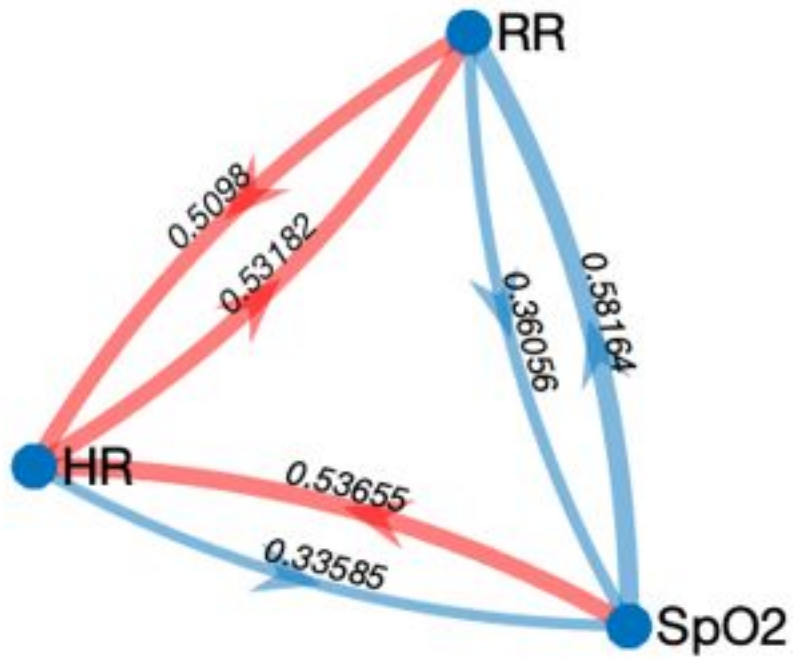
885 **Figure 8.** Graphical representation of possible underlying relationship between physiological
886 stress and TE

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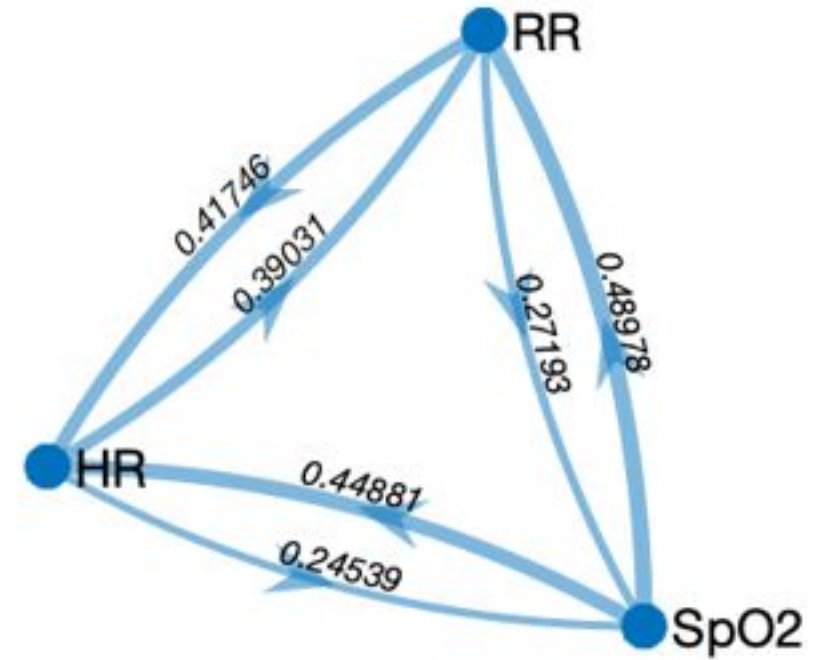
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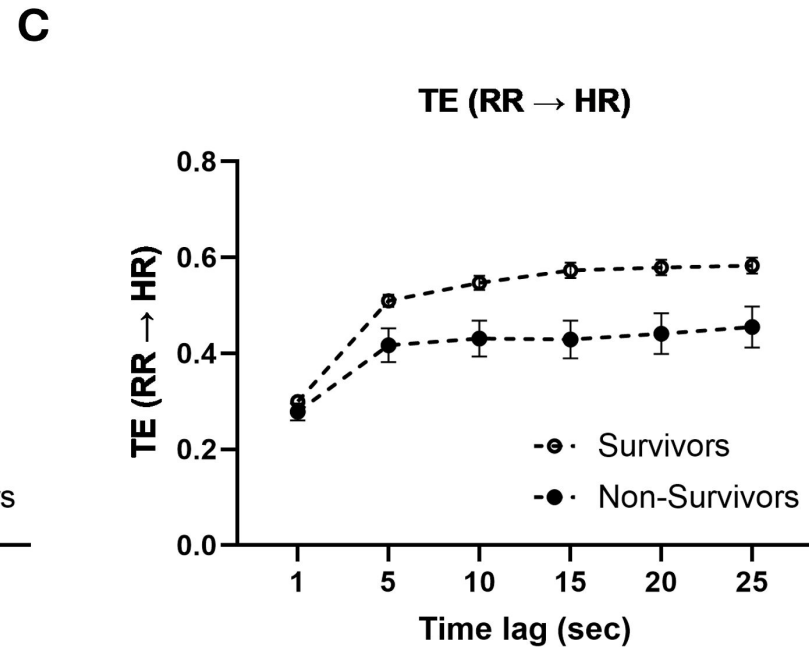
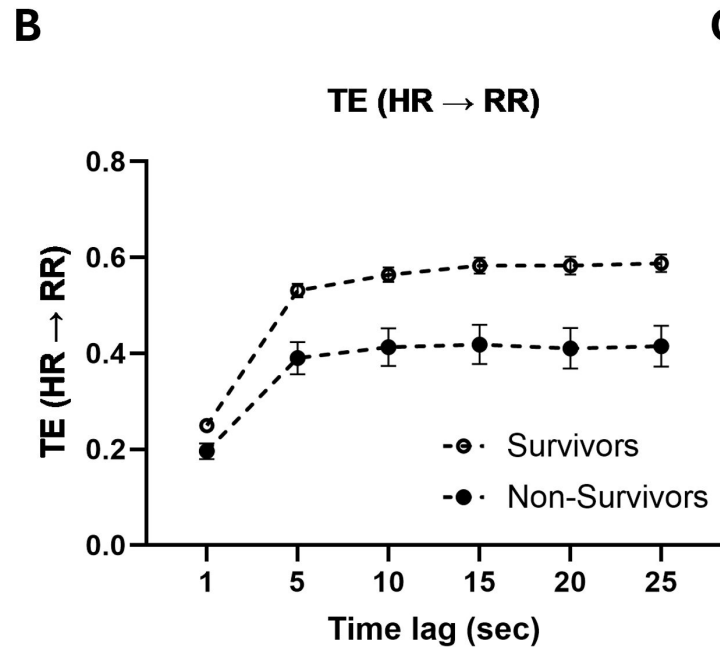
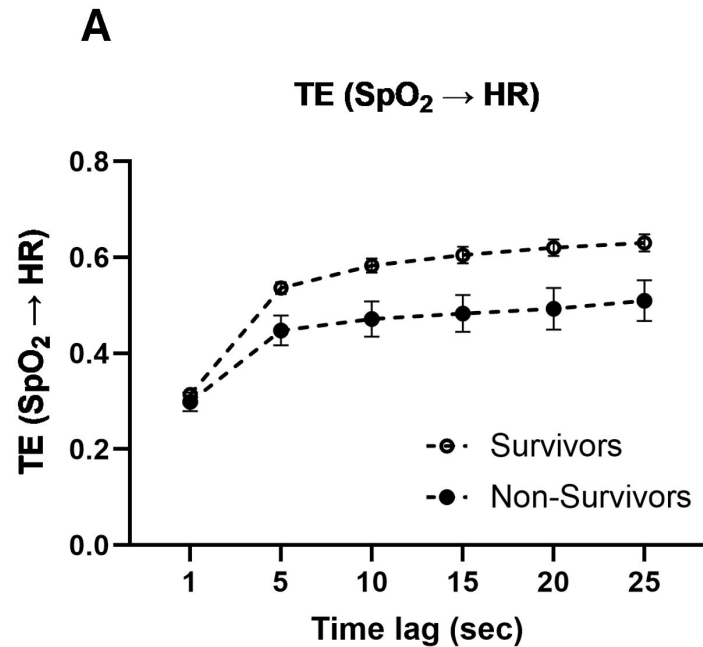


Survivors

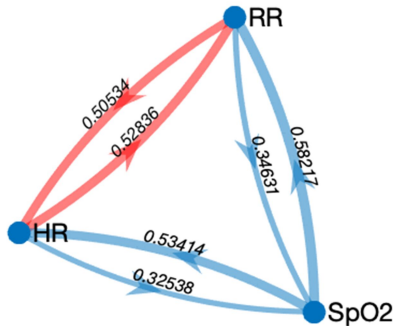


Non-Survivors

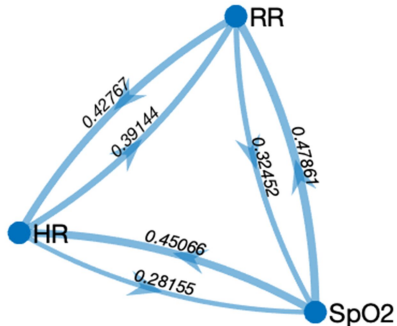


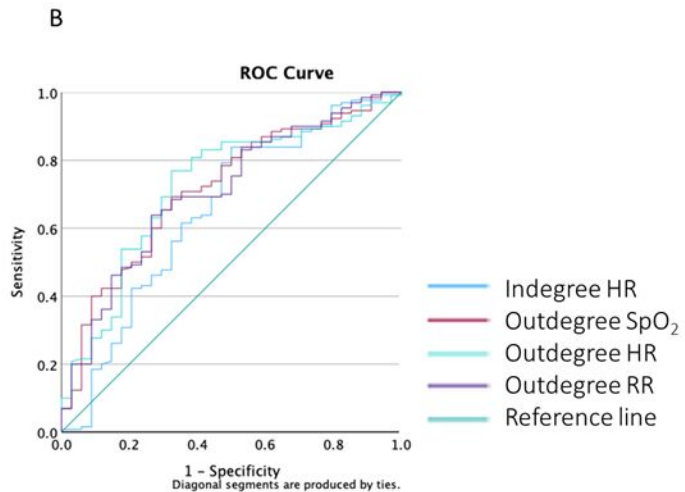
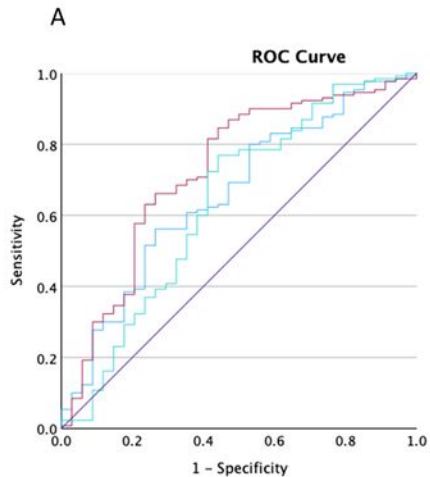


No Deterioration

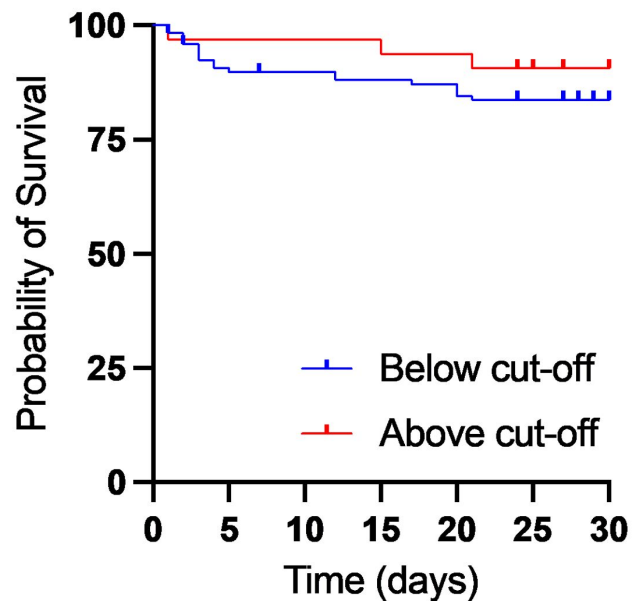


Deterioration



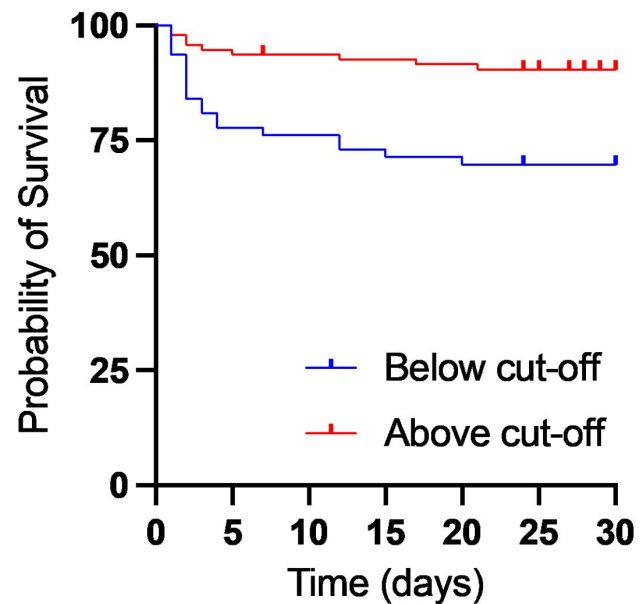


A

TE (SpO₂ → HR)

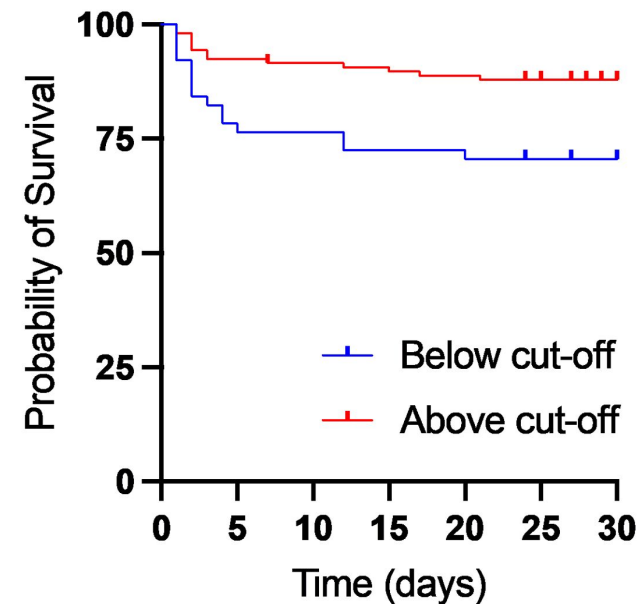
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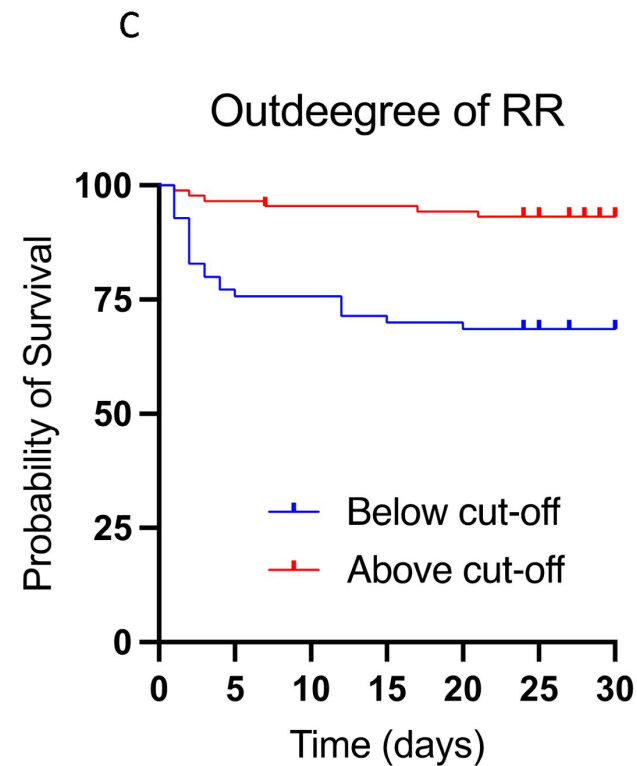
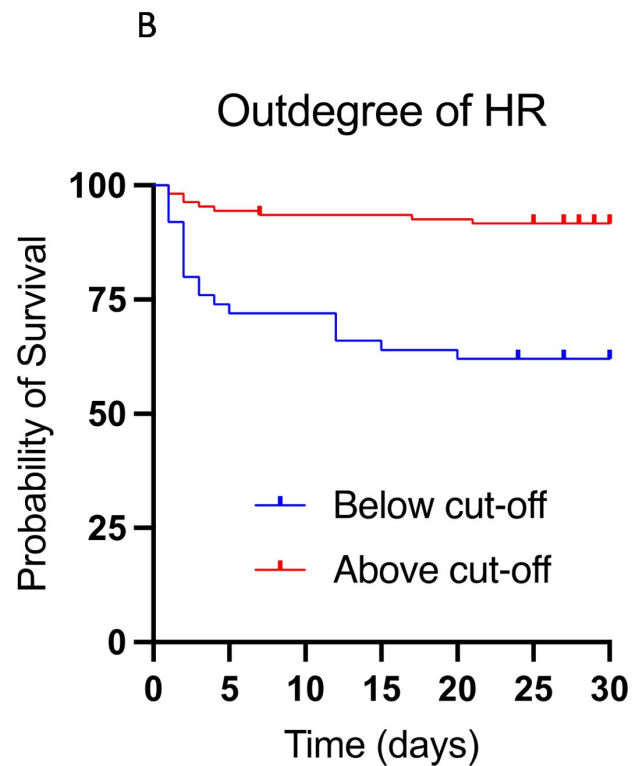
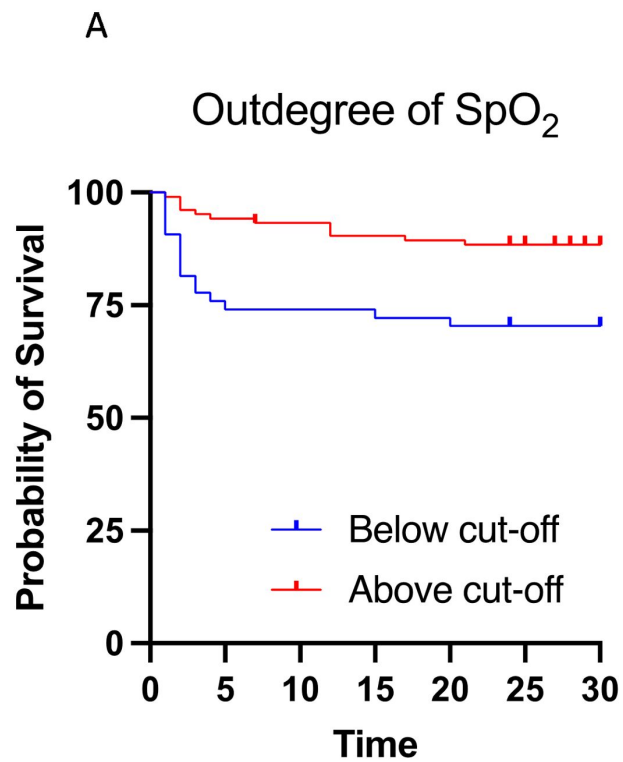
TE (HR → RR)

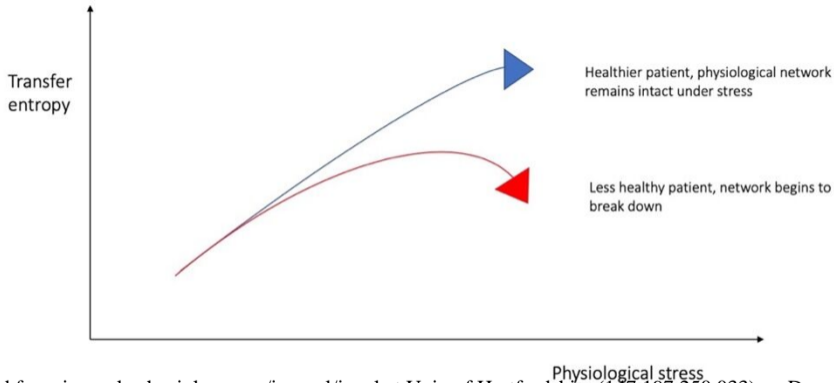


C

TE (RR → HR)







Decreased cardio-respiratory information transfer is associated with deterioration and a poor prognosis in critically ill patients with sepsis

METHODS

Recruitment of critically ill patients with sepsis (MIMIC III)

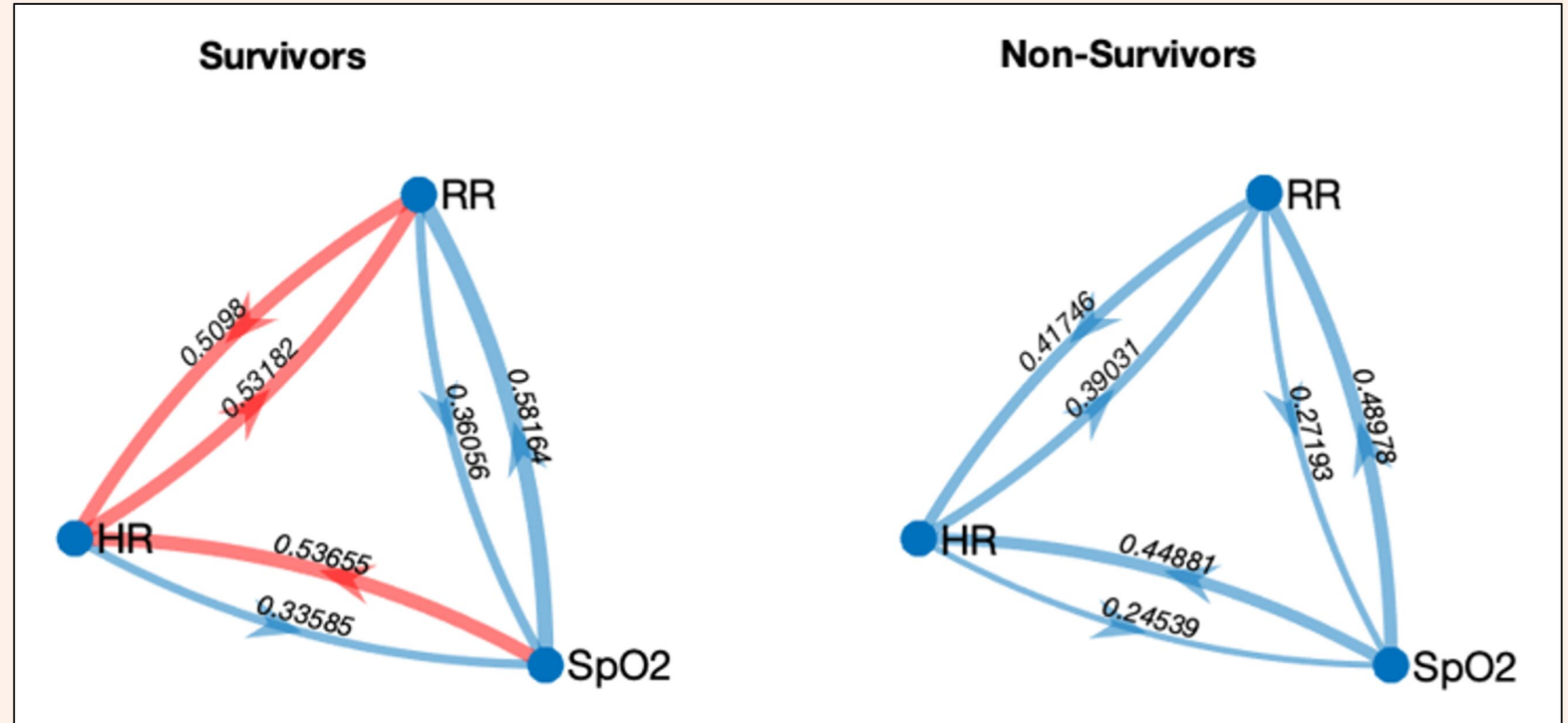
30-min heart rate (HR), respiratory rate (RR) and oxygen saturation (SpO₂)

Physiological network mapping by calculation of information transfer between physiological signals (Transfer Entropy)

Outcome measures:
a. 30-day survival, b. 48-h deterioration

Survival analysis

OUTCOMES



CONCLUSIONS

Greater information flow between heart rate, respiratory rate, and capillary oxygen saturation was associated with reduced mortality, independent of age, disease severity, mechanical ventilation and comorbidities.