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Enhanced Non-invasive Characterisation of Renal Tumour Microstructure with VERDICT-MRI

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Synopsis

Keywords: Kidney, Kidney, Microstructure Imaging

Motivation: Diffusion-weighted (DW)-MRI may characterise renal cell carcinoma (RCC) by reflecting cellularity, but results using the apparent diffusion coefficient (ADC) model are inconclusive.

Goal(s): Use advanced modelling with VERDICT-MRI to characterise renal tissue in two different grades and subtypes of RCC, and compare performance to ADC.

Approach: Fit VERDICT and ADC models to DW-MRI data from two patients and compare performance in terms of accuracy of fitted signal and parameter estimates.

Results: The VERDICT model captures the DW-MRI signal more accurately than ADC. It discriminates between tissue types, and shows high cellularity and low vasculature in the grade 3 tumour, agreeing with independent CT.

Impact: We show that VERDICT-MRI can be used to accurately characterise tumour and benign tissue microstructure in two patients with RCC of diferent grade and subtype, improving performance over ADC and reflecting histological tissue properties such as cellularity and vasculature.

Introduction

Renal cell carcinoma (RCC) arises from renal epithelium, and accounts for >90% of kidney cancers¹. MRI is routinely used for RCC diagnosis², and diffusion-weighted MRI (DW-MRI) can provide additional sensitivity by probing tissue microstructure³. Most DW-MRI RCC studies use the apparent diffusion coefficient (ADC), which has been shown to be lower in tumour tissue than benign^{4,5}, but cannot differentiate between cancer subtypes, producing contradictory results⁶⁻⁹.

The Vascular, Extracellular and Restricted DIffusion for Cytometry in Tumours (VERDICT)-MRI framework, consisting of a specific DW-MRI acquisition and a biophysical model for tumour microstructure¹⁰, has been used for prostate¹¹⁻¹³, brain¹⁴ and rectal¹⁵ tumours, showing enhanced tumour characterisation over ADC^{16,17}. We demonstrate the first application of VERDICT-MRI in renal cancer, in two patients with grade 2 and 3 RCC. Results show VERDICT predicts the renal DW-MRI signal more accurately than ADC, showing promise for improved tissue type diferentiation by reflecting histological features.

Figures

VERDICT-MRI was performed on a 3T MRI system (Ingenia; Philips, Best, the Netherlands), using a pulsed-gradient spinecho sequence with echo-planar imaging readout in the coronal plane. The imaging parameters were: repetition time, 2000–3349ms; echo time (TE), 54–87ms field of view, 220x200mm; voxel size, 1.25x1.25x5mm; no interslice gap; acquisition matrix, 176x176. The VERDICT acquisition protocol for kidney is: $b=[70, 90, 150, 500, 1000, 1500, 2000, 2200, 2500]$ s/mm²; d=[4.8,4.8,4.8,12.0,12.0,26.3,16.8,16.8,21.4]ms; D=[27.0,27.0,27.0,34.0,34.0,47.0,37.5,37.5,43.5]ms. We acquired a separate b=0 image for each TE. Acquisition time was ~40 min.

Pre-processing

The pre-processing pipeline^{12,13} included denoising using MP-PCA¹⁸ (MrTrix3¹⁹ 'dwidenoise'), and correction for Gibbs ringing²⁰. We applied mutual-information rigid and affine registration¹³, and divided the DW-MRI volumes by their matched b=0 for normalisation. The regions of interest (ROIs) were drawn by a board-certified study radiologist on corresponding T2-weighted images.

VERDICT Model

The VERDICT model has three compartments that characterise diffusion in the intracellular (IC), vascular (VASC) and extracellular-extravascular space (EES) in tumours¹⁰. For renal tissue, the IC compartment is an impermeable sphere of radius R with diffusivity of d_{IC}=2µm²/ms and the EES compartment is Gaussian free diffusion with diffusivity d_{EES}=2μm²/ms. The vascular compartment is randomly-oriented sticks with pseudo-diffusivity d_{VASC}=50μm²/ms to reflect the high vascularity of kidney tissue²¹. We estimate f_{IC} (IC volume fraction), f_{EES} (EES volume fraction) and cell radius R. The vascular volume fraction is f_{VASC} =1– f_{IC} – f_{EES} .The total DW-MRI signal is: 2 2 VASC 2 IC (IC VOIUME Haction), I_{EES}

Figure 2 shows maps of ADC and the estimated VERDICT parameters. For patient 1 (grade 2), we see higher $f_{\sf IC,}$ $f_{\sf VASC}$ and R and lower f_{EES} in the solid tumour region than in benign tissue, and no clear trends for ADC. We also observe higher $\sf f_{\sf EES}$ and lower $\sf f_{\sf IC}$ in the necrotic tumour region. For patient 2 (grade 3), we see lower ADC, $\sf f_{\sf EES}$ and $\sf f_{\sf VASC}$, and higher $\sf f_{\sf IC}$ and R in the tumour region than in benign tissue.

Patients with renal tumours were identified at the Royal Free Hospital. Patient 1: age 77, grade 2 clear-cell RCC (ccRCC) confirmed post-surgery. Patient 2: age 71, grade 3 RCC of unspecified non-ccRCC subtype confirmed from previous biopsy.

Data Acquisition

Figure 1 shows the normalised signal from each patient (symbols), with the predicted VERDICT and ADC signal in tumour and benign tissue (lines). We observe lower mean-squared error (MSE) for VERDICT than ADC.

Figure 3 presents average parameter estimates for each slice of the ROIs in three tissue types, revealing similar trends to the maps (Fig. 2). We plot estimates for both patients in the tumour region, showing lower f_{IC}, higher f_{vASC} and higher ADC for patient 1 (grade 2 RCC) than for patient 2 (grade 3 RCC).

Figure 4 presents CT images of both patients, showing stronger enhancement for patient 1 (90HU) than patient 2 (50HU).

Discussion and Conclusion

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This work demonstrates the first use of VERDICT-MRI for renal tissue microstructure in two patients with diferent grade and subtype RCC. We show that VERDICT captures the DW-MR signal trends and discriminates tumour from benign tissue more efectively than ADC.

VERDICT revealed lower f_{VASC} in the tumour region for patient 2 than for patient 1, reflecting the reduced vascularity of the grade 3 tumour over the grade 2 ccRCC. This agrees with Fig. 4, as ccRCC are generally hypervascular, whilst other subtypes are often hypovascular²³. Additionally, the grade 3 RCC has higher f_{IC} than the grade 2, demonstrating increased cellularity in the higher-grade tumour²⁴. This suggests VERDICT reflects specific histological properties, showing potential for non-invasive discrimination of RCC subtype. IC

Future work will recruit more patients for statistical analysis, and identify an economical acquisition protocol.

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\frac{S(b)}{S_0} = f_{VASC} S_{VASC}(d_{VASC}, b) + f_{IC} S_{IC}(d_{IC}, R, b) + f_{EES} S_{EES}(d_{EES}, b)
$$

where b is the b-value, S $_{\rm 0}$ is the b=0 signal intensity. The model is fit to the data using supervised deep learning with a multilayer perceptron^{12,13,22}.

Results

Figure 1: Plots of the normalised signal from each patient as symbols, with the predicted VERDICT and ADC signal in tumour (purple) and benign (black) tissue as lines. We observe lower mean-squared error in both tissue types when fitting VERDICT over ADC, for both patients. The DW-MR signal appears isotropic, hence we do not observe differences between the three directions.

Figure 2: Parameter maps with tumour ROI (purple) and benign ROI (black). **A**) patient 1 (benign ROI on ipsilateral) shows higher $f_{IC,}$ f_{VASC} and R and lower f_{EES} in the solid tumour region than benign. **B**) patient 1, whole tumour (white) with necrotic region outside purple solid tumour, shows higher f $_{\sf EES}$ and lower f_{IC} in the necrotic tumour region. **C**) and **D**) patient 2 (benign ROI on contralateral) shows lower ADC, f_{EES} and f_{VASC}, and higher f_{IC} and R in the tumour region than benign.

Methods

Patient Cohort

Figure 3: Violin plots showing VERDICT and ADC parameter values in tumour region, ipsilateral and contralateral benign kidney for both patients, and comparisons between patient parameter estimates in the tumour region, where μ is the mean. For both patients, we observe higher f_{IC} and R and lower f $_{\sf EES}$ in the tumour region than benign, and for patient 2 we see lower f_{VASC} and ADC in the tumour. Patient 1 shows lower f_{IC} and higher f_{VASC} and ADC in the tumour region than patient 2.

Figure 4: Nephrographic phase coronal computerised tomography (CT) scan slices through the right renal tumours of (a) patient 1, 90 Hounsfield units (HU) and (b) patient 2, 50 HU. The lower enhancement of patient 2 can be attributed to the tumour subtype, which has reduced vascularity in comparison to clear-cell RCC subtype of patient 1.