

1 **Application of Artificial Intelligence (AI) in molecular brain**  
2 **imaging. Perspectives from the EANM.**

3 **Or**

4 **Perspectives from the EANM on the application of Artificial**  
5 **Intelligence (AI) in molecular brain imaging.**

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**Commented [ZK1]:** Would it be OK? The EANM representative advised us to omit the 'neuroimaging committee' from the title.

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68 **Abstract:**

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70 This paper discusses the opinion of the Neuroimaging Committee of the European  
71 Association of Nuclear Medicine regarding the role of artificial intelligence, the unmet  
72 needs of AI in standardized applications, and the increasing need for common ethical  
73 standards.

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75 The first part of this manuscript offers insight into the fundamentals of artificial  
76 intelligence (AI) and provides a general overview of the current role and functions of  
77 AI in nuclear medicine neuroimaging. AI methods offer opportunities for image quality  
78 enhancement, shortening image acquisition time, and potentially reduced dose of the  
79 utilized tracer. In addition, it can facilitate image reading, differential diagnosis and/or  
80 predict cognitive decline. Furthermore, AI-based segmentation can eliminate  
81 meticulous manual annotation and inter-observer variability and offers help to  
82 clinicians with differential diagnosis or automatization of reads (e.g. amyloid  
83 positive/negative), prediction of cognitive decline, detection of epileptogenic focus).

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85 In the second part, the current clinical applications of artificial intelligence and its  
86 future perspectives in nuclear medicine neuroimaging are reviewed with emphasis  
87 on the potential application of AI in brain oncology, neurodegeneration, epilepsy and  
88 psychiatric disorders.

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102 **1. Goal**

103 With an increasing availability of diagnostic and therapeutic options for nuclear  
104 neuroimaging and open science practices, a larger amount of data has become  
105 available, requiring a more complex evaluation (1).

106 Artificial Intelligence (AI) was first applied in neuroimaging in the early 2000s, when it  
107 was combined with functional magnetic resonance imaging (fMRI) to create more  
108 precise mapping of the activity of the human brain after various specific stimuli.  
109 Despite the potential of the technique being immediately clear, the first reports were  
110 pessimistic (2,3). This was because of the combined need for very large amounts of  
111 data and contemporary, state-of-the-art computing resources. Solutions became  
112 available only in the last decade, which is the reason for today's AI revolution (4).

113 Much has been written of the potential application of AI in neuroradiology and in most  
114 recent times in nuclear imaging in several fields, however, a detailed description of the  
115 mechanisms underlying the application of AI in nuclear neuroimaging has not been  
116 fully provided (5,6).

117 Indeed, the Neuroimaging Committee of the European Association of Nuclear  
118 Medicine believes that an easy-to understand- and position overview on the  
119 principles of AI in nuclear neuroimaging will bring important added value to clinical  
120 studies and to clinical teams.

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131 **2. Introduction and background of AI in neuroimaging**

132 **Introduction**

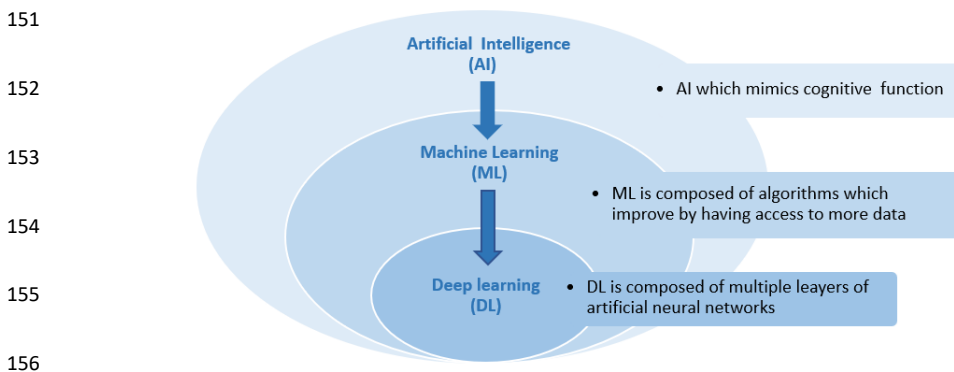
133 AI is designed to perform tasks that would otherwise require human labour. AI is a  
134 technique which enables programs to mimic human cognitive functions, i.e., human  
135 behaviour; therefore, these algorithms can learn from experience. AI essentially learns  
136 from processing large amount of data & recognize specific patterns in the dataset (7).

137 **Background and Nomenclature: machine learning vs. deep learning**

138 Machine learning (ML) is a subset of AI programs/algorithms which uses statistical  
139 methods on training data and which, by doing so, is able to improve. This is typically  
140 an iterative process (the more data we have/insert in the database, the more accurate  
141 is the result). In machine learning often the data is structured and pre-processed (e.g.  
142 radiomics) using well define features). For instance, ML can differentiate normal brain  
143 parenchyma from ischemic parenchyma by using pre-programmed patterns of an  
144 infarct (e.g. hypo attenuating brain tissue, obscuration of the basal ganglia, sulci  
145 effacement in CT) which are paired with the result in the AI computer database  
146 (infarcted brain tissue) (8,9).

147 Deep learning (DL) is a subset more complex evolution of machine learning. In this  
148 learning process, the 'raw' data are presented, and the algorithm learns how to extract  
149 the relevant features (Fig. 2) (10).

150 **Figure 2:** Relation between AI, Machine Learning and Deep Learning



157 DL was inspired by human brain structures/networks; therefore, this algorithm concept  
158 is called artificial neural network (ANN). It models artificial neurons that collect input  
159 data and weigh each of those inputs. This artificial neuron network operates with an  
160 activation function which combines the weighted average of the input into an output  
161 signal. This signal is received by connected neurons (Fig. 3) (8,10,11).

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163 **Figure 3:** Schematic structure of a Deep Learning method (Artificial Neural Network)

164 In deep learning the first step is to **i)** collect a large dataset of images / input layer (several MR  
165 sequences presented in the left-hand side of the figure). **ii)** Then the computer generates a  
166 set of “unusual images” named convolutional layers which is the main building block of CNN  
167 and contain abnormal findings (also named filters, e.g. abnormal density, intensity, edge,  
168 deviation of anatomical boundaries etc.). **iii)** Then the images are matched with a dataset of  
169 pre-acquired images with similar features (see the Fig. below: information of infarct,  
170 hemorrhage and metastasis were included in the dataset). Similarly, to what happens in the  
171 human brain, which pools information together, the several convolution layers from the images  
172 are connected each other. **iiii)** The computer then checks the (millions of) possible combined  
173 information (through several fully connected layers to identify a more complex picture  
174 (relationship between the features) in the database and will give the results based on the  
175 likelihood of similarity. Likewise to human brain, the more information we have, the more  
176 probability we have to make a correct assessment. In the same way, the more convolution  
177 layer information we feed the AI dataset system, the more accurate results will be generated.

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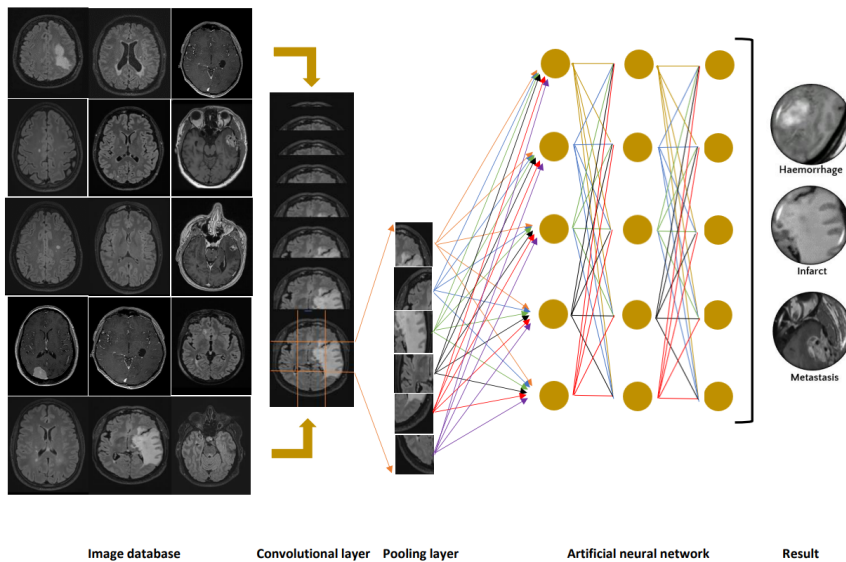
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190 An ANN is able to recognize complex, non-linear patterns in a wide range of complex  
191 data set and it can associate them for instance with specific disorders and estimate  
192 the onset of disease.

193 The nomenclature of NN/ANN/DL tends to be confusing. Hereafter, we refer to all  
194 neural network architectures as ANN, and if it is a conventional ANN, we denote that  
195 it is "fully-connected". DL, on the other hand, is a special type of ANN which does not  
196 just have fully-connected neural layers, but also has so-called convolutional layers that  
197 extract features from input data (Fig. 3) to create output data. Convolution layer  
198 consists of one or more filters (or Kernel) with different weights that are used to extract  
199 features from the input image (8,10,11).

200 These convolutional kernels are matched to the given input image at each coordinate  
201 and generate a "meta-image" (a.k.a. convolved image) which highlights several  
202 features such as regions, edges, patterns where the given kernel had a high ratio of  
203 matching.

204 This resulting "meta-image" will be weighted and compared to the database into the  
205 computer. The training process of ANN is not only of optimizing weights in the fully-  
206 connected network, but also to determine the values of the convolutional kernels.  
207 Hence, DL operates not only with hand-crafted features (e.g., shallow radiomics) but  
208 with learnt features (12–15).

209 Deep learning is the most used algorithm in medical imaging because it can make  
210 complex decisions on its own. It is worth to mention that, given the high number of  
211 heterogeneous parameters, DL requires a large training dataset to avoid  
212 under/overfitting. It is widely used in structural and functional MRI and positron  
213 emission tomography (PET) imaging. It is specifically designed for image processing,  
214 object identification and segmentation allowing unparalleled accuracy in the field of  
215 neuroradiology (16,17).

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218 **3. Physics, clinical aspects, and the need for exhaustive evaluation**  
219 **and validation in neuroimaging**

Commented [ZK2]: Should we rewrite to: 'Major challenges of AI' instead of 'Physics'

220 AI algorithms have shown many potential benefits for brain PET and SPECT, mainly  
221 related to the physics and clinical aspects of the studies. This section is focused on  
222 ensuring these advancements have been rigorously tested and achieved through a  
223 reproducible methodology, with a reliable training and verification method and,  
224 secondly, defining the corresponding ground-truth for an exhaustive validation and  
225 evaluation of AI algorithms.

226 ***Lack of generalizability and potential solutions***

227 The crescent interest in AI is not without problems, requiring large validation studies.  
228 Consortium datasets have emerge in molecular neuroimaging including Alzheimer's  
229 Disease Neuroimaging Initiative (ADNI), Parkinson's Progression Markers Initiative  
230 (PPMI) or Open Access Series of Imaging Studies (OASIS), however, more data are  
231 still needed to for the complete translation to clinical routine use.

232 Open standard datasets will be essential for the development of AI, even though it  
233 may involve significant costs. One possible cost-efficient solution is to make use of  
234 realistic Monte Carlo simulations techniques for generating in silico neuroimaging  
235 datasets, thus allowing for data augmentation from patient data (18). Another solution  
236 to address this challenge is federated learning, which allows AI to be trained on  
237 decentralized datasets from multiple hospitals, while ensuring data privacy and  
238 security. Federated learning has been already applied to training of AI models in  
239 different brain PET challenges, such as reconstruction, segmentation and denoising  
240 using brain PET datasets from multiple institutions (19–21). An even more recent  
241 improvement is swarm learning, that combine Federated learning with blockchain  
242 technologies to further ensure the robustness of the learning process (22).

243 ***The ground-truth for AI models***

244 The ground-truth for a given neuroimaging dataset is often uncertain, difficult to  
245 establish and strongly dependent on each application. For instance, ground-truth for  
246 AI models aimed at improving the spatial resolution can be obtained from high-  
247 resolution phantom studies, the ground-truth for models focused on denoising should  
248 be obtained from the corresponding raw data acquired during long scans (23). In



249 clinical applications, the ground-truth for AI models providing automated image  
250 analysis can be datasets analysed visually and processed manually by experienced  
251 nuclear medicine physicians (24). On the other hand, AI models focused on disease  
252 detection should use a ground-truth obtained from cases with a definite diagnosis  
253 confirmed by clinical follow-up as well as other relevant diagnostic tests or  
254 histopathological examination if available (25). Therefore, it is important to have a clear  
255 “ground truth” aim before processing and using any AI model; this process requires by  
256 all clinicians an understanding of the physics and clinical applications of Artificial  
257 intelligence.

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#### 259 **4. Image acquisition, reconstruction, segmentation, registration and** 260 **analysis**

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262 In this section we will discuss the potential application of AI to processes of image  
263 formation, which include data acquisition and image reconstruction steps (including  
264 data correction) and post-processing (including registration, normalization, and  
265 analysis).

##### 266 ***Acquisition and reconstruction***

267 In the data acquisition stage, deep learning models have been utilized to estimate  
268 Time-of-Flight (ToF) and improve the quantitative accuracy and diagnostic confidence  
269 of PET images reconstructed without ToF, specifically for brain PET (26,27). In  
270 tomographic reconstruction, AI has been employed to enhance the quality of PET and  
271 SPECT images by reducing noise and enhancing image contrast during reconstruction  
272 (28). Deep learning techniques have also demonstrated effectiveness in providing  
273 accurate and generalizable PET attenuation and scatter correction methods (29,30),  
274 and, interestingly, attenuation correction methods without CT (31). Finally, generative  
275 adversarial networks have been employed for motion correction in brain PET,  
276 effectively addressing the challenge of head motion artifacts (32). Also, they can be  
277 used to dramatically shorten scan times/activity amounts needed (33).

##### 278 ***Segmentation and registration:***

279 In post-processing, AI-based segmentation can overcome the time-consuming and  
280 observer-dependent process of manual annotation of brain structures in PET images

**Commented [ZK3]:** Should we rewrite to: ‘Image formation and analysis’

281 (34,35). AI can also assist in the registration of neuroimaging data, via the alignment  
282 of images from different imaging modalities or timepoints and learning the mapping  
283 between images and different modalities (36). Furthermore, AI can facilitate the  
284 extraction of meaningful quantitative parameters from the images, such as, improved  
285 amyloid PET quantification without non-specific contributions (37) and amyloid PET  
286 quantification without using MRI (38). This advance can contribute to the development  
287 and routine accessible use of biomarkers for early diagnosis and personalized  
288 treatment. Moreover, AI might provide non-invasive estimations of the arterial input  
289 function for brain PET studies, facilitating adoption of absolute quantification in clinical  
290 settings (39).

### 291 ***Interpretability Analysis***

292 Lastly, interpretability and robustness are essential aspects of AI applications in  
293 neuroimaging. By improving interpretability and robustness, we can enhance the  
294 trustworthiness, and clinical utility of AI models and promote the development and  
295 translation of AI technologies in clinical settings. Additionally, we can help identify  
296 potential biases, errors, or limitations in the model, which can be addressed to improve  
297 its performance and generalizability (40). Similarly, some of the AI methods can be  
298 easily supervised. A segmentation task can be easily checked once the segmentations  
299 are generated, so the correctness of the segmentation is easily verified/ supervised.  
300 Some other tasks of AI cannot be easily supervised and require external validation  
301 and, if possible, some explainability testing is of importance. So called explainable AI  
302 techniques are rapidly emerging to improve interpretability, including feature  
303 visualization, saliency maps, and decision trees. These can reveal the key features  
304 and patterns that contribute to the model's predictions or decisions. Another approach  
305 is to incorporate robustness measures, such as adversarial training, regularization,  
306 and uncertainty quantification, into the AI model to increase its resilience to various  
307 types of noise, artifacts, or uncertainties (41).

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311 **5. AI in molecular imaging in neuro-oncology. A review of the current**  
312 **knowledge and perspectives.**

313 In neuro-oncology, one of the specificities of neuro-oncological applications of AI is a  
314 relatively rare incidence of brain tumors with an annual global age-standardized  
315 incidence of primary malignant brain tumors of about 3 per 100,000 (42), requiring  
316 special modelling workflows or data augmentation techniques (43,44). Radiomics  
317 studies should follow the IBSI (Image Biomarker Standardization Initiative) guidelines  
318 (45). These guidelines cover the image pre-processing, tumor segmentation, and the  
319 image biomarker computation. All the extracted radiomics features are used in a  
320 modelling step, performed in most of the cases with machine learning models. Studies  
321 using deep learning approaches, which can be applied to the entire analysis or to  
322 specific parts of the workflow (46), are for the moment scarce.

323 ***Machine learning studies***

324 The first studies using AI in neuro-oncology were based on machine learning models  
325 with conventional PET features for initial characterization of brain lesions (47),  
326 predicting molecular characteristics of gliomas (48–50) including features from  
327 multiparametric MRI (48), and search of recurrences (51) with higher diagnostic  
328 performances as compared to results obtained only with a conventional approach.

329 ***Radiomics studies***

330 Most of the radiomics studies in neuro-oncology focused on amino-acid PET  
331 radiotracers in gliomas, at initial diagnosis for grading (52,53) or prediction of important  
332 molecular characteristics (54–59) according to the latest WHO classifications of  
333 gliomas (60), for prognosis (61–63), for search of recurrences (64–66), including the  
334 search for early progression in glioma patients after chemoradiation (67). Interestingly,  
335 some studies investigated radiomics derived from both static but also dynamic  
336 acquisitions at initial diagnosis (68,69), for the prognosis (70) or search for glioma  
337 recurrences (71). The combination of PET radiomics features extracted from several  
338 PET radiotracers (64) or in combination with MRI radiomics features (59) is also of  
339 interest in the field of neuro-oncology. It is also important to perform radiomics  
340 analyses in a multicentric approach ensuring a better guarantee of generalizability of  
341 the obtained results (71). Some studies were focused on methodological approaches

342 regarding patient preparation (72) or PET imagereconstruction processes (73) and  
343 their influence on radiomics analyses. Importantly, two methodological studies with  
344  $^{18}\text{F}$ -FET relied on the features repeatability (43) and harmonization (44), two crucial  
345 steps for considering the generalization of the results obtained. PET radiomics studies  
346 in gliomas with other radiotracers than amino-acid ones are limited, with  $^{18}\text{F}$ -FDG (74–  
347 76) or TSPO PET imaging (44). Table 1 summarizes the main radiomics studies in  
348 gliomas compliant with the IBSI guidelines.

349 Radiomics studies in other brain tumors are relatively limited, mainly to brain  
350 metastases for the initial differential diagnosis (77) and the search for recurrences  
351 (78,79). Rare studies also included primary CNS lymphomas for the differential  
352 diagnosis (80,81).

### 353 ***Deep learning studies***

354 The first studies used deep learning for specific tasks like the tumor segmentation with  
355 PET (82,83) or the attenuation correction in PET/MRI (84). More clinically tasks were  
356 then investigated with equivalent diagnostic performances than expert consensus for  
357 the diagnosis of tumor progression (85), but lower diagnostic performances for the  
358 prediction of molecular characteristics (86).

### 359 ***Perspectives***

360 AI in neuro-oncology is intensively evaluated allowing simplifying steps in radiomics  
361 pipeline such as tumor segmentation, increasing data comparability between  
362 observers and more importantly extracting new features from the images of brain  
363 tumor patients (87). AI is currently primarily represented by radiomics analyses, which  
364 must be performed according to the steps described in the IBSI guidelines to ensure  
365 standardization of processes (45,88), providing promising results with good diagnostic  
366 performances in various clinical indications, including methodological approaches.  
367 Some improvements are nevertheless required for the generalization of the observed  
368 diagnostic performances, by identifying specific radiomic signatures that are easily  
369 transposable across centers. Notably, these efforts concern the feature repeatability  
370 and harmonization through well-defined multicentric studies. This is even more  
371 meaningful for the field of neuro-oncology since CNS tumors are rare diseases with  
372 therefore a limited number of patients, requiring data collection from different centers.

373 Studies of PET multi-tracer radiomics analyses and/or combination with  
374 multiparametric MRI and clinical parameters are also encouraged. Another important  
375 point is that diagnostic performances of radiomics models should systematically be  
376 compared to conventional parameters to really appreciate the added value of AI-  
377 related methods in each clinical indication before implementation in clinical routine.  
378 Finally, an important effort may be developed to make accessible radiomics data  
379 accessible at the individual level, providing an additional clinical tool to assist the  
380 nuclear medicine physicians in their decisions.

381 **Table 1. Summary of PET radiomics studies compliant with the IBSI guidelines in**  
382 **gliomas**

**Commented [ZK4]:** Alexander Hammers:  
"The order in which the references are listed is not clear - broadly year of publication per category? But that's not consistent.  
A subheading per column would also be useful - currently it only says "patients". (For number of participants, I would find it useful to add any controls, like in the epilepsy table (Table 2).  
The latter also has a column denoting the AI method used - please consider this here as well, to clearly differentiate from classical radiomics studies.  
Finally, we should use the consensus nomenclature for radiotracers (summary in <https://www.ncbi.nlm.nih.gov/pmc/articles/PMC6465410/>) just like we insist on IBSI guidelines; I have amended in the table (and elsewhere)"

**Commented [ZK5R4]:** Prof. Hammers advised fundamental modifications in all the added tables Francesco, including the structures/content/abbreviation etc.

I have modified what I was able to, however:

This is the only suggestion type I cannot fully conduct/finish, and I ask you to leave (omit) what I could not fulfil. Everything else Prof. Hammers asked so, I added carefully (again).

	Radiotracer	Number of Patients	Task	Main finding
<b>Initial diagnosis</b>				
Russo et al., 2021 (53)	[ <sup>11</sup> C]-methionine	56	Grading	AUC of 0.64
Zhou et al., 2021 (57)	[ <sup>18</sup> F]-FET	58	IDH mutation prediction	AUC of 0.91 combining PET and CT features
Li et al., 2021 (68)	[ <sup>18</sup> F]-FET	159	TERTp mutation prediction in glioblastomas	AUC of 0.82
Zaragori et al., 2022 (73)	[ <sup>18</sup> F]-FDOPA	72	IDH mutation and 1p19q codeletion prediction	AUC of 0.83 for IDH mutation and 0.72 for 1p19q codeletion
Zhang et al., 2022 (89)	[ <sup>18</sup> F]-FDG	102	ATRX mutation prediction in IDH-mutant gliomas	AUC of 0.96 combining PET and MRI features
Cao et al., 2022 (77)	[ <sup>18</sup> F]-FDG	100	Differentiation between glioblastoma and brain metastases	AUC of 0.84 combining PET and MRI features
Papp et al., 2023 (56)	[ <sup>11</sup> C]-methionine	35	IDH mutation prediction	Radiomics signature differ according to sex
<b>Prognosis</b>				
Li et al., 2023 (70)	[ <sup>18</sup> F]-FET	141	Survival in newly-diagnosed glioblastomas	AUC of 0.74 combining PET and clinical features
Carles et al., 2021 (62)	[ <sup>18</sup> F]-FET	32	Survival in recurrent glioblastomas	AUC of 0.66 for recurrence location.

Radiomics signature associated to survival.

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**Recurrence**

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Wang et al., 2020 (64) [18F]-FDG and 11C-methionine 160

Differentiation of treatment-related changes from glioma progression

AUC of 0.91 with an integrated model involving radiomics signature, the mean of tumor-background ratio of 18F-FDG, maximum of TBR of 11C-MET PET, and patient age

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Ahrari et al., 2021 (71) [18F]-FDOPA 85

Differentiation of treatment-related changes from glioma progression

AUC of 0.83

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Müller et al., 2022 (66) [18F]-FET 151

Differentiation of treatment-related changes from glioma progression

AUC of 0.85

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**Methodological**

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Gutsche et al., 2021 (43) [18F]-FET 50

Features repeatability

In tumor VOIs, 73% of first-order features and 71% of features extracted from the gray level co-

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			occurrence	383
			matrix showed	384
			high	385
			repeatability.	386
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			Carbidopa	387
			impacted 81% of	388
			radiomics	389
Bros et al., 2021 (72)	[ <sup>18</sup> F]-FDOPA	54	Effects of features,	390
			Carbidopa	391
			premedication	392
			significantly	392
			modified when	393
			using ratios to	394
			healthy brain.	395
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Ahrari et al., 2022 (73)	[ <sup>18</sup> F]-FDOPA	57	Effects of the Point	396
			Spread Function	397
			deconvolution	398
			AUC of 0.83 vs.	399
			0.79 for the IDH	399
			mutation after	399
			applying PSF.	399
<hr/>				
			Feature	400
			distributions	400
			could be	401
			successfully	402
Zounek et al., 2023 (44)	[ <sup>18</sup> F]-FET and [ <sup>18</sup> F]-GE-180	19	Features	403
			harmonization for	403
			pooling data	403
			aligned using	403
			ComBat except	403
			for some features	403
			affected by	403
			changes in	403
			patients rank.	408

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414 **6. AI in molecular imaging of Epilepsy: A review of the current**  
415 **knowledge and perspectives.**

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417 Epilepsy is one of the most common neurological disorders characterized by abnormal  
418 excessive firing and synchronisation of neurons leading to seizures. The accurate  
419 identification of the epileptogenic foci is essential to avoid misdiagnosis and select the  
420 correct treatment, especially when resective surgery is necessary as in drug-resistant  
421 epilepsy (90). While nuclear medicine neuroimaging is the key diagnostic tool, allowing  
422 to evaluate metabolic, neurotransmission or perfusion abnormalities occurring in  
423 people with epilepsy, there is an increasing need to define accurate computer-aided  
424 tools to support clinicians. In this context, AI-based tools pave the way for solving such  
425 tasks, fostered by the exceptional advancement in the models we have witnessed in  
426 the last years. ML and DL are currently explored for diverse tasks as cortical lesion  
427 localization (mainly for focal cortical dysplasia - FCD), epileptic focus  
428 detection/lateralization and brain region segmentation (e.g., hippocampus), or for the  
429 diagnosis and prognosis of different epilepsy types. Still, AI has been mostly applied  
430 to MRI or EEG recordings (especially for seizure identification and forecasting), while  
431 their exploitation in the nuclear medicine-epilepsy field is still in its infancy, with a few  
432 studies largely limited to [<sup>18</sup>F]FDG-PET briefly reviewed in the followings.

433

434 ***Machine Learning studies***

435 In conventional ML, the classification/regression tasks are combined with an initial step  
436 of feature engineering to extract the image-derived phenotypes to be included in the  
437 different models. The voxel-wise glucose uptake levels have been used in a few  
438 studies (91,92), also combined with dimensionality reduction methods as Principal  
439 Component Analysis (PCA) (92). However, regional measures are still the primary  
440 choice, usually defined as asymmetry/laterality indices calculated from glucose mean  
441 values in a single representative region (93) or in a series of ROIs from common  
442 atlases as Anatomical Automatic Labelling Atlas (AAL) or Freesurfer parcellation  
443 (94,95). All these measures combined with other ML methods (e.g., support vector  
444 machine, random forest and multivariate pattern analysis) have been successfully  
445 applied for lateralization tasks in temporal lobe epilepsy (92,93,95), seizure recurrence  
446 prediction and prognostic assessment in drug-resistant epilepsy (94,96,97), or disease

447 classification (patients vs controls) (91,93), with improved performance compared to  
448 conventional and visual approaches.

449

#### 450 **Deep Learning studies**

451 Besides two pioneering works focusing on epilepsy lateralization with ANNs  
452 architectures (98,99), DL has been only recently introduced in such domain. DL has  
453 the undeniable advantage of avoiding feature extraction by learning directly from the  
454 images, allowing to improve the classification/prediction performance compared to all  
455 the other approaches. Only few examples are available in the current literature, aiming  
456 at improving the epilepsy lesion characterization (100) or structure segmentation  
457 (101). One study evaluated ANN along with other ML-based approaches for predicting  
458 surgical outcome in mesial temporal lobe epilepsy (92), and one study focused on the  
459 identification of the epileptic foci in paediatric patients with a symmetry-driven  
460 Siamese CNN, going beyond visual assessment and conventional SPM analysis (89).  
461 Another used DL to predict an individual patient's "healthy" FDG PET based on their  
462 MRI, which was then subtracted from the real FDG PET to identify metabolic lesions  
463 (Subtraction Interictal PET Co-registered to MRI, "SIPCOM"), again performing better  
464 than conventional SPM analysis (102).

465

#### 466 **Perspectives**

467 Despite the methodological advancements, AI applications in molecular imaging of  
468 epilepsy are still limited and confined to specific epilepsy types, possibly because of  
469 the difficulties in finding large (and annotated) datasets to train and generalize the  
470 complex AI-based models, the high heterogeneity of patients with epilepsy and the  
471 need to perform patient-specific fingerprinting, especially when comes to clinics. Multi-  
472 centre initiatives, coupled with advanced DL models (e.g., multi-task CNNs,  
473 autoencoders) and data augmentation methods (e.g., generative adversarial networks  
474 or large simulated databases) (100), might help to overcome part of such limitations,  
475 providing more generalizable models and a precise fine-grained characterization of  
476 inter-individual patient variability to progress towards personalized medicine.

477 Some recent studies have also underlined the importance of combining multi-modal  
478 imaging data, such as metabolic PET with structural or functional MRI, often  
479 leveraging the value of simultaneous PET/MRI acquisitions. These multi-modal data  
480 coupled with AI models can increase the accuracy in predicting the surgical outcomes

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The reference has the wrong authors, I need to modify manually before submission.

((PET image enhancement using artificial intelligence for better characterization of epilepsy lesions.  
Flaus A, Deddah T, Reilhac A, Leiris N, Janier M, Merida I, Grenier T, McGinnity CJ, Hammers A, Lartizien C, Costes N. Front Med (Lausanne). 2022 Nov 16;9:1042706. doi: 10.3389/fmed.2022.1042706. eCollection 2022.))

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Wrong reference again, I need to adjust manually before submission. Correct title:

PET image enhancement using artificial intelligence for better characterization of epilepsy lesions.  
Flaus A, Deddah T, Reilhac A, Leiris N, Janier M, Merida I, Grenier T, McGinnity CJ, Hammers A, Lartizien C, Costes N. Front Med (Lausanne). 2022 Nov 16;9:1042706. doi: 10.3389/fmed.2022.1042706. PMID: 36465898

481 (103,104) and detecting focal epilepsy lesions such as FCD (105,106). All these  
 482 approaches therefore deserve further investigations for fully exploiting their potential  
 483 and exploring their generalizability in the epilepsy workflow (see the summary of the  
 484 cited articles in Table 2).

485 **Table 2:** Summary of cited papers

486

	<b>Study cohort</b>	<b>Task</b>	<b>AI method</b>	<b>Main finding</b>
Wu et al., 2021 [87]	23 MTLE patients and 24 HC	Classification	MVPA + SVM	AUC of 0.996
Beheshti et al., 2020 [88]	56 TLE patients (MRI negative)	Focus lateralization	T-test Feature ranking + SVM	Accuracy of 96.43%
Peter et al., 2018 [89]	17 TLE patients and 23 HC	Focus lateralization and classification	Lateralization indices + LR	AUC of 0.8 (lateralization); AUC of 0.44 (classification)
Kini et al., 2021 [90]	89 TLE patients	Prediction of long-term seizure recurrence	RF	Mean out-of-bag accuracy of 0.71
Shih et al., 2021 [91]	104 MTLE patients	Focus lateralization	Lateralization indices + 7 ML classifiers	Accuracy of ~ 96% (validation), 100% (test)
Sinclair et al., 2021 [92]	82 MTLE patients	Prediction of surgical outcome	LR, SVM, RF, ANN	AUC of 0.75–0.81
Lee et al., 2000 [93]	261 epilepsy patients	Epilepsy diagnosis (NA, LTLE, RTLE)	ANN + LDA	Average agreement between ANN and human experts of 85% (test)
Kerr et al., 2013 [94]	105 epilepsy patients	Diagnosis and lateralization of TLE	MLP	Accuracy of 88% (RTLE) and 83% (LTLE); accuracy for simultaneous diagnosis and lateralization of 76%
Flaus et al., 2022 [95]	Simulated data and 10 epilepsy patients	PET image quality enhancement	ResNet	Improved image quality; improvement of visual lesion

					detection from 38 to 75%
Sundar et al., 2022 [96]	10 HC and 14 non-lesional epilepsy patients (brain dataset)	Segmentation	nnU-Net		89% of the cerebral areas with DSC > 0.80
Zhang et al., 2021 [97]	201 pediatric TLE patients and 24 HC	Localization + Classification	Siamese CNN		DSC of 0.51; AUC of 0.92 (classification)
Tang et al., 2022 [98]	141 epilepsy patients	Prediction of seizure outcomes after surgery	ResNet-34 + multi-kernel SVM		AUC from 0.799 to 0.952 (higher for multi-modality)
Wang et al., 2022 [99]	39 mTLE-HS patients and 22 HC	Prediction of seizure outcomes after surgery	GBDT + LR		AUC of 0.905 (multi-modality, test)
Lin et al., 2020 [100]	22 epilepsy patients with FCD	Automatic detection of FCD lesion	XGBoost		Accuracy of 91% (multi-modality)
Tan et al., 2018 [101]	28 epilepsy patients with FCD and 23 TLE patients (MRI negative)	Automatic detection of FCD lesion	SVM		Sensitivity of 93% (multi-modality)

*MTLE = mesial temporal lobe epilepsy; HC = healthy controls; MVPA = machine learning-based multivariate pattern analysis; SVM = support vector machine; LR = logistic regression; RF = random forest; ANN = artificial neural network; NA = no abnormal findings; LDA = linear discriminant analysis; MLP = multilayer perceptron; CNN = convolutional neural network; DSC = dice coefficient; mTLE-HS = medial temporal lobe epilepsy due to hippocampal sclerosis; GBDT = gradient boosting decision tree; FCD = focal cortical dysplasia. (Note: all studies used 18F-FDG radiotracer)*

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495 **7. AI in molecular imaging of dementia and movement disorders: A**  
496 **review of the current knowledge and perspectives.**  
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498 The differential diagnosis of neurodegenerative and movement disorders can be quite  
499 complex and is highly dependent on the expertise of the reader. Therefore, AI may  
500 help in the (early) differential diagnosis, especially for less experienced readers.  
501 Multimodal imaging with structural and functional information combined with fluid-  
502 based biomarkers is becoming the standard in the diagnostic landscape. In this  
503 multimodal setting AI can be particularly helpful for feature selection. Moreover, AI  
504 might give additional clues about the prognosis. However, the biggest challenge in the  
505 field of AI in neurodegenerative disease is located in a very limited number of available  
506 standards of truth assessments, i.e. autopsies in previously imaged patients. In the  
507 next paragraphs we will review the AI approaches used in the literature and the  
508 perspectives of AI in molecular imaging of degenerative disorders.

509

510 ***Machine Learning studies***

511 Machine learning already showed tremendous success in the differential diagnosis of  
512 neurodegenerative disorders by pattern recognition of Parkinsonian syndromes using  
513 FDG-PET images more than a decade ago (107). A recent review confirmed that the  
514 performance of a multimodal machine learning model using both structural and  
515 functional data is higher than single modality models (108). In prodromal AD and  
516 Parkinsonian syndromes, artificial intelligence not only showed potential in the early  
517 differential diagnosis, but also to predict future pathological protein accumulation and  
518 clinical deterioration (109–112). Furthermore, machine learning was evaluated for the  
519 discrimination of patients with amyotrophic lateral sclerosis from controls in a  
520 prospective study (113). Apart from differential diagnosis and prognosis, Subtype-and-  
521 Stage Inference (SuStaln) modelling was applied for data-driven identification of four  
522 major subtypes in the Alzheimer's disease (AD) continuum (108,111,113–115).

523

524 ***Deep Learning studies***

525 Artificial intelligence using deep learning may help to extract hidden information in  
526 multimodal imaging approaches of neurodegenerative diseases. For example, it can  
527 assist the biomarker discovery, physiology exploration and so on.

528 The application of deep learning has been ranged from image quality enhancement  
529 (116), biomarker discovery (117,118)) cross-modality synthesis (117,119,120),  
530 quantification improvement (37,38), phenotype discovery (121) to clinical differential  
531 diagnosis (24,122–124). Brain segmentation, a crucial task to obtain quantitative  
532 parameters such as regional volume or radiotracer uptake, has been successfully  
533 performed by CNN models with high accuracy and fast processing time (125).

534 Deep learning models trained on normal data of FDG PET can effectively identify a  
535 wide range of brain abnormalities (126). For Alzheimer's disease a multimodal deep  
536 learning framework - combining clinical parameters with MRI-data - demonstrated a  
537 high accuracy to discriminate between Lewy body, Alzheimer's and vascular dementia  
538 (127). Furthermore, a deep learning model using FDG PET scans could demonstrate  
539 the cognitive dysfunction in patients with isolated rapid REM sleep behaviour disorder  
540 (iRBD) (128). Here, iRBD is considered as a very early preclinical symptom of  
541 synucleinopathies such as Parkinson's disease, Lewy body dementia and multiple  
542 system atrophy. Also, for prognosis AI with deep learning can help since convolutional  
543 neural networks obtained an accuracy of 75% to discriminate between patients with  
544 mild cognitive impairment who will progress to Alzheimer and patients with stable mild  
545 cognitive impairment (114). Several studies have highlighted the use of deep learning  
546 in predicting and differentiating dementia and its related conditions. Deep learning  
547 models achieved notable accuracy in predicting MCI's progression to AD and  
548 outperformed human readers in predicting AD's final clinical diagnosis (129,130).  
549 Other research further emphasized deep learning's accuracy in differentiating and  
550 diagnosing various forms of dementia using diverse radiotracers (24,131–133). Deep  
551 learning has been effective in classifying and diagnosing movement disorders. Notable  
552 results include the consistent accuracy in classifying FDG PET (118,134), DAT PET  
553 (124) or SPECT (135,136) imaging and differentiating PD or parkinsonian types.

554  
555 Several investigations focused on refining image analysis and predictive models using  
556 deep learning (137). Studies have shown that deep learning can improve the  
557 association between specific amyloid load (37), cognitive signature (138,139),  
558 enhance spatial normalization (38), and extract longitudinal trajectories (121).  
559 Research has explored the potential of deep learning in generating synthetic PET  
560 images of scarce tracers (120), generating MR images from amyloid PET (119), and  
561 harmonizing image discrepancies (140,141).

562

563 **Perspectives**

564 Future studies need to overcome the lack of validation studies across different centres  
565 and the lack of harmonization of generally accepted AI algorithms to aid in diagnosis  
566 across the neurodegenerative diseases spectrum. Moreover, all AI models are data-  
567 driven, so pre-processing of imaging data plays a crucial role. Therefore, pre-  
568 processing software also needs to be harmonized and validated. Accommodation of  
569 substantial numbers with standard of truth assessments for validation of AI application  
570 in PET imaging of neurodegenerative disorders remains a challenge and may be  
571 solved by large cohorts such as BioFINDER or ADNI (142,143). Conversely, PET itself  
572 may also be used as a standard of truth assessment for AI driven analysis of fluid  
573 biomarkers or omics data with the goal to find cheap and versatile tools for  
574 characterization of neurodegenerative disorders.

575

576 **Table 3:** Summary of the cited references as they vary in patient numbers

577

	<b>Radiotracer</b>	<b>Number of Patients</b>	<b>Task</b>	<b>Main finding</b>
<b>Anomaly discovery</b>				
Choi et al. 2019 (126)	18F-FDG	1303	Unsupervised identification of abnormalities of various disorders	Deep learning trained only by normal data was applicable for identifying wide-range of abnormalities in brain diseases
<b>Dementia</b>				
Lu et al. 2018 (37)	18F-FDG	1242	A multimodal and multiscale deep neural work to predict the risk of MCI in conversion to AD	82.4% accuracy in identifying the individuals with MCI who will convert to AD at 3 years prior to conversion
Ding et al. 2019 (130)	18F-FDG	1042	Convolutional neural network to predict final diagnosis of AD and MCI	Predicted AD final clinical diagnosis 75.8 months earlier, surpassing reader performance
Lee et al. 2022 (117)	18F-FDG	511	Deep learning-based signature from FDG PET to objectively and quantitatively evaluate cognitive function	DL-based cognitive signature using FDG PET discriminated stroke patients with dementia with AUC of 0.75
Etminani et al. 2022 (24)	18F-FDG	757	3D deep learning model to predict final diagnosis of	Superior AUC for predicting final diagnoses: DLB



			AD, DLB, MCI-AD and cognitively normal	96.2%, AD 96.4%, MCI-AD 71.4%, CN 94.7%, surpassing human reader performance.
Son et al. 2020 (131)	18F-Florbetaben	430	Validate DL's feasibility over visual rating for assessing diagnosis in subjects with equivocal amyloid PET	In equivocal scans, DL detected a significant MMSE score change difference over 1.76 years than visual reading
Park et al. 2023 (132)	18F-Flortaucipir	276	DL integrate multimodal data in differentiating cognitively unimpaired from MCI or AD	AUC of 0.976 for classification of AD and 0.850 for classification of MCI
Jo et al. 2020 (133)	18F-Flortaucipir	300	DL to identify informative features from tau PET for AD classification	Average accuracy of 90.8% based on five-fold cross-validation in classifying AD from cognitively normal
Ryoo et al. 2022 (128)	18F-FDG	50	Test the DL-based cognitive signature derived from AD for cognitive assessment of iRBD	AUC of 0.70 distinguishes RBD-MCI from RBD-nonMCI. The baseline DL-based cognitive signature is significantly higher in iRBD patients who

experienced  
cognitive decline  
over 2 years  
compared to those  
who didn't

**Movement  
Disorders**

Wenzel et al. 2019 (135)	123I-FP-CIT	645	deep convolutional neural networks for automatic classification of DAT SPECT	DL achieved consistent accuracy for the classification of DAT SPECT with variable site-, camera-, or scan-specific image characteristics
Shen et al. 2019 (134)	18F-FDG	350	Group Sparse Belief Network for discriminating PD and normal control subjects based on FDG-PET	Lasso Deep DL classification of PD and NC outperformed conventional approaches with strong correlation to UPDRS and H&Y scores
Adams et al. 2021 (136)	123I-FP-CIT	252	DL to predict clinical motor function evaluation scores from longitudinal DAT SPECT and non-imaging clinical measures	DL with DAT SPECT and UPDRS enhances 4-year motor function prediction
Wu et al. 2022 (118)	18F-FDG	2228	Metabolic imaging indices	DL achieved high accuracy in

			based on deep learning support differential diagnosis of parkinsonism	differentiating to parkinsonism in internal and external tests
Zhao et al. 2022 (124)	11C-CFT	1017	Decode the discriminative information DAT imaging using DL for the differential diagnosis of parkinsonism	Sensitivity of 90.7%, 84.1%, 78.6% and specificity of 88.4%, 97.5% 93.3% in the blind test for the differential diagnosis of IPD, MSA and PSP
Lu et al. 2023 (129)	18F-Florzolotau		A normalization-free deep-learning model for differentiation of PSP and MSA-P	DL-guided radiomic features correlated with clinical severity of PSP
<b>Quantification &amp; Methodology</b>				
Liu et al. 2021 (37)	11C-PIB	172	Using DL to correct non-specific binding due to cerebrovascular disease	Specific amyloid load after DL-correction increased association with cognitive and functional test scores by up to 67%
Kang et al. 2023 (38)	18F-Flutemetamol, 18F-Florbetaben,	1130	DL-based spatial normalization for automatic quantification of	Quantification using DL-based spatial normalization shows better correlation with that using MRI

	18F- Florbetapir		amyloid PET without MRI	FreeSurfer using MRI SPM	than
Reith et al. 2021 (139)	18F- Florbetapir	1224	Combine DL-based imaging feature and other clinical data to predict future image features	A root mean squared error of $0.0339 \pm 0.0027$ for amyloid SUVR prediction	
Choi et al. 2020 (138)	18F-FDG	1364	DL-based cognitive signature of FDG PET adaptable for PD and AD	DL-based signature developed from AD applies to predict the conversion of MCI to AD and PD dementia	
Hong et al. 2022 (121)	18F- Flortaucipir	1080	Identify the tau trajectory and quantify the tau progression in a data-driven approach with the continuous latent space learned by variational autoencoder	Identified 4 clusters corresponds to different tau progression. The inferred tau trajectory agreed with the Braak staging	
<b>Cross-modality synthesis</b>					
Wang et al. 2021 (120)	18F-FDG	54	Generate synthetic PET images of less-available tracers such as synaptic density and amyloid from FDG PET	SUVR bias for synthesizing 11C-UCB-J: $-0.3\% \pm 7.4\%$ (AD), $-0.5\% \pm 7.3\%$ (CN); for 11C-PiB: $-1.3\% \pm 7.5\%$ (AD), $-2.0\% \pm 6.9\%$ (CN)	

Choi et al. 2018 (119)	18F- Florbetapir	261	Deep generative networks to generate structural MR images from amyloid PET for MR-less quantification	Mean absolute error of SUVR by MR-based method was $0.04 \pm 0.03$ , significantly lower than other MR-less methods.
Kim et al. 2021 (141)	18F-FDG	1533	deep learning based amyloid PET prediction based FDG PET	AUC of 0.86 for predicting amyloid-positive patients using FDG PET in external test
Shah et al. 2022 (140)	11C-PiB, 18F-florbetapir	138	A Residual Inception Encoder-Decoder Neural Network to harmonize the difference between different amyloid PET imaging	Significantly stronger between-tracer correlations ( $P < .001$ ) were observed after harmonization for both global amyloid burden indices and voxel-wise measurements

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589 **8. AI in molecular imaging in psychiatry: A review of the current**  
590 **knowledge and perspectives.**

591 Diagnosis and evaluation of psychiatric disorders rely almost exclusively on clinical  
592 interviews using the Diagnostic and Statistical Manual of Mental Disorders (DSM)  
593 nosography, with so far limited impact of neuroimaging beyond the issue of differential  
594 diagnosis. Yet, the DSM reliability is regularly questioned by its iterative modifications,  
595 lack of reproducibility of current diagnoses, and therapeutic resistance of many  
596 patients (144–146). In this context, more transdiagnostic approaches are emerging  
597 (147), in -addition to the development of invasive and non-invasive brain stimulation  
598 (148), for which relevant biomarkers are crucial to identify brain signatures, guide  
599 therapeutics and evaluate their effects (145). PET and SPECT imaging could be  
600 particularly relevant to explore such disorders mainly characterized by dysfunction, in  
601 the absence of morphological lesions, with the possible implementation of various  
602 targets such as the perfusion, metabolism, neurotransmission and neuroinflammation,  
603 and especially the individual application of artificial intelligence tools for precision  
604 medicine (149,150). In this line, machine learning classification from controls has  
605 suggested accurate performance to identify patients with attention-deficit and  
606 hyperactivity disorder using multimodal serotonergic brain PET imaging (151),  
607 patients with cocaine dependence using brain perfusion SPECT imaging (152),  
608 patients with internet game disorder using metabolic brain PET imaging (153), patients  
609 with major depression using serotonergic PET imaging (154), or brain metabolic PET  
610 imaging, also demonstrating the value of this last exploration to predict the response  
611 of deep brain stimulation in this context (155). Machine-learned analysis of  
612 [<sup>18</sup>F]FDOPA PET scans of patients with schizophrenia also showed good performance  
613 for identifying treatment responders and non-responders, with large potential  
614 healthcare cost savings (156). This translation from research to clinical applications  
615 will need more numerous multicentric studies, and to be supported by a paradigm  
616 change in psychiatry towards modern approaches of precision medicine.

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622 **9. Role of the EANM in advancing the use of AI in molecular brain**  
623 **imaging**

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625 As for the whole nuclear medicine community, there is great interest in the molecular  
626 brain imaging field to advance the use of AI in research, translational and potentially  
627 also in daily clinical routine settings. In good time, the EANM has recognized this  
628 desire and leads efforts moving this exciting development forward.

629

630 A series of publications of AI in neuroimaging have emerged in the latest years,  
631 focusing on several different aspects of this complex modality. As often in the past  
632 with methodological imaging advancements, the brain is perfect as the organ of  
633 interest to start with testing such new developments. This is not only as multi-modality  
634 image co-registration is much easier for the head as compared to other body parts,  
635 and as large image databases are easily accessible in case of brain imaging.  
636 However, standardization of clinical brain image recording and imaging protocols as  
637 well as efficient dissemination of data will be essential before data from different  
638 centers can be used as input by AI (157–159).

639

640 As with medical imaging in general, in case of molecular brain imaging, the process  
641 from data acquisition to diagnosis involves numerous steps (e.g. image  
642 reconstruction, image segmentation, extraction of imaging biomarkers, image  
643 classification, patient stratification). AI methods have now been developed and tested  
644 for one specific step at a time. One could expect in the future that AI based algorithms  
645 could automatically handle all steps in a transparent fashion to the user, though, on  
646 the other hand, the process still needs to be guided by the clinical needs. Results and  
647 type of AI behavior or generalizability need to be evaluated (160–162).

648 The Neuroimaging committee of the EANM and neuro-nuclear medicine opinion  
649 leaders in general believe the future potential of AI will mainly be (i) to increase image  
650 quality that would translate into a higher diagnostic accuracy and confidence, (ii) to  
651 reduced tracer dose/radiation exposure, (iii) to reduced PET or SPECT scan times,  
652 (iv) to standardize and harmonize image data acquisition, processing and analysis  
653 across centers, and (v) to improve the reporting/communication of the scan results  
654 with the patients, their caregivers and the referring doctors.

655

**Commented [ZK8]:** "EANM should not be mentioned as a 3<sup>rd</sup> person in the last paragraph (9)" – from EANM Felix

Is it OK to rewrite like: "The EANM has recognised" --> "We have recognised"

"The EANM should focus" --> "We should focus.." etc

If it's fine, I will rewrite these accordingly.

**Commented [ZK9]:** I am adding here AH's Fair AI idea It will take 2-3 days to make it nice and comprehensive – I believe it is important to him.

Alexander Hammers:

"Fair AI is close to my heart, and in my opinion still vastly under-recognised - I've added the citation elsewhere but perhaps worth repeating in this summary section along the lines of "Standardisation of clinical data recording and imaging protocols, clear demographic characterisation of controls and patients for Fair AI (REF: Ioannou S et al.), as well as efficient dissemination of data will be essential before data from different centres can be optimally used as input for AI (125 - 127)"

[\(A study of demographic bias in cnn-based brain mr segmentation](#)

S Ioannou, H Chockler, A Hammers, AP King, ...  
International Workshop on Machine Learning in Clinical Neuroimaging, 13-22"

656 In clinical practice, it is difficult to foresee what will be happening in the future in  
657 molecular neuroimaging as well in other medical and non-medical fields, e.g. in how  
658 far the human being will be replaced by AI.

659 All these procedures will help even less experts' nuclear physicians, all over the globe,  
660 to interpret the images and address the patient to the appropriate specialist, with a  
661 timely management.

662 In our opinion the role of nuclear medicine physicians will be to supervise the work of  
663 AI, which will decide on the specific subject the technical parameters to adopt, the  
664 scan type, the image reconstruction technique, the count of photons and possible  
665 inclusion of scatter, the clinical information/potential risk assessment and or potential  
666 treatment options. Incorporation of AI into this envisioned automated workflow (from  
667 acquisition and pre-processing to disease and risk identification) will be useful for  
668 complex cases that will benefit the most from expert clinical analysis in situations of  
669 massive data overflow (157).

670 Most excitingly, the next years will also show whether AI is, in case of molecular brain  
671 imaging, suitable to support or even - at least in some applications - replace the  
672 nuclear medicine physician. General pros for AI in this regard are its availability without  
673 quality/reproducibility differences on a 24/7 base, stable quality, and a potential to  
674 improve over time. As examples, rather straightforward binary decisions like positivity  
675 vs. negativity in case of amyloid PET imaging, or rather complex and experience-  
676 dependent differential diagnoses like those obtained by FDG PET imaging in dementia  
677 disorders or atypical Parkinsonian syndromes might be better obtainable in the future  
678 by AI.

679

680 The role of nuclear medicine physicians is likely to evolve as soon as these new AI  
681 techniques (and us, as nuclear medicine experts should by ourselves drive this  
682 developments). will be fully integrated into their practice, and it is therefore important  
683 that the acquisition of a basic understanding of these methods and concepts will  
684 become part of their training (163), a matter the EANM should likewise focus on.

685

686 Nevertheless, there are ongoing challenges to AI in the healthcare system. In clinical  
687 practice, the most prominent and time-consuming obstacle is the implementation of AI  
688 into the already existing workflow. AI can only function at a high level if it is treated as  
689 a fundamental part of the routine protocols rather than a simple add-on within the



690 system. More specifically, successful integration of AI into the operation of an  
691 organization requires at the very least a high computational power of the facility, and  
692 proper education of the staff on how to correctly implement AI-generated results, which  
693 most likely take years to be implemented satisfactorily. Consequently, successful  
694 deployment of AI demands international actions led by the EANM and other  
695 stakeholders in the field, including standardized procedures for different AI  
696 applications worldwide (164–166).

697  
698 Taken together, the role of organizations like EANM is to define and foresee these  
699 current and potential upcoming issues regarding nuclear medicine related AI  
700 applications. With clear objectives, supported by similarly large organizations  
701 overcoming these issues can be accelerated (167,168). This also refers to setting up  
702 quality standards on publications dealing with AI in molecular imaging (169).

703  
704 Lastly, another concurrent call for EANM is to set internationally recognized ethical  
705 standards for the deployment of AI in nuclear medicine and its associated counterpart  
706 fields. The EANM has recently acknowledged a prominent set of ethical principles from  
707 Currie et al. (170) for the application of AI in nuclear medicine (Fig. 4), however; as AI  
708 algorithms and their reliability will increase, EANM will likely evolve these ethical  
709 codes.

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711 **Figure 4:** Decision making of the ethical principles from Currie et al.

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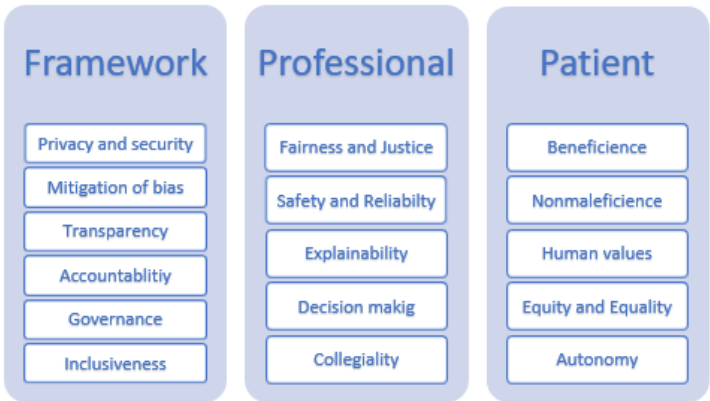
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**Commented [ZK10]: REMINDER FOR ME**  
- AH and I.Galazzo notes (before submission)  
- AH two extra in the table

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