Robustness of CSF Aβ42/40 and Aβ42/P-tau181 measured using fully automated immunoassays to detect AD-related outcomes

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Abstract

Introduction: This study investigated the comparability of cerebrospinal fluid (CSF) cutoffs for Elecsys immunoassays for amyloid beta (Aβ)42/Aβ40 or Aβ42/phosphorylated tau (p-tau)181 and the effects of measurement variability when predicting Alzheimer’s disease (AD)-related outcomes (i.e., Aβ-PET visual read and AD neuropathology).

Methods: We studied 750 participants (BioFINDER study, Alzheimer’s Disease Neuroimaging Initiative [ADNI], and University of California San Francisco [UCSF]). Youden’s index was used to identify cutoffs and to calculate accuracy (Aβ-PET visual read as outcome). Using longitudinal variability in Aβ-negative controls, we identified

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1 | INTRODUCTION

Alzheimer’s disease (AD) is the most common cause of dementia and is characterized neuropathologically by the presence of extracellular amyloid beta (Aβ) plaques and intracellular neurofibrillary tangles composed of hyperphosphorylated tau. These features can be detected in vivo using well-validated cerebrospinal fluid (CSF)-based biomarkers, including Aβ42 in ratio to Aβ40 (Aβ42/Aβ40) and tau phosphorylated at threonine 181 (Aβ42/p-tau181).2 Because the accuracy of clinical criteria for AD is suboptimal (when using autopsy data as a reference standard),3-4 CSF biomarkers are increasingly used in the workup of patients with cognitive impairment to rule out AD as an underlying cause, and have been incorporated in research diagnostic guidelines for AD5-7 and clinical trials for participant enrichment.

Despite the broad use of CSF Aβ and p-tau181 in clinical practice in several countries, significant variability in measured concentrations has been reported between laboratories and across sample batches,8,9 hampering the establishment of uniform global cutoff values that can be used across sites for defining abnormality. This variability can be traced to (1) pre-analytical (i.e., due to differences in the collection, handling, and storage of samples),10 (2) analytical (i.e., due to differences in how the assays are run as well as variability in kit components between assay lots),8,11 and (3) biological/patient-related (i.e., confounding factors inherent to a given patient, such as age) factors. For a given CSF biomarker, the variability stemming from these three sources results in a “total error” for that measure that can be established by collecting and testing samples on at least two different occasions. The total allowable error (TAE) of a biomarker, by contrast, is the maximum total error for which a biomarker still performs well in its intended clinical use.12

While biological/patient-related factors do not appear to pose a significant problem for CSF AD biomarkers,13,14 pre-analytical (e.g., sample handling and storage) and analytical (e.g., between/within differences in laboratory procedures) variability is known to affect biomarker values from enzyme-linked immunosorbent assays (ELISA),15 which are widely used for routine CSF biomarker analysis. This has been shown to result in interlaboratory variation up to 15%.15 This can be addressed through the use of standardized protocols for CSF collection and storage16 and fully automated platforms such as the Roche Elecsys immunoassays that have high test–retest reliability (<5%) and low laboratory- and kit-associated variability.13 These show excellent concordance with manual ELISAs17 and have been well validated against Aβ-potisol emission tomography (PET)18-20 and postmortem data.21 Despite the low variability levels described for fully automated assays, total error levels may result in variable classification (i.e., an individual is classified as having normal AD biomarker findings at one time point and abnormal at another), increasing the diagnostic uncertainty at the individual patient level.

In the present study, we aimed to (1) assess the comparability of CSF cutoffs for Elecsys-based Aβ42/Aβ40 and Aβ42/p-tau181 across three separate cohorts to assess the impact of different preanalytical protocols and (2) assess the effects of variability over repeated CSF measurements (test–retest variability) on AD-related outcomes (i.e., Aβ-PET visual read and a measure of overall AD neuropathologic change). Further, given the interest in blood tests for Aβ pathology, the performance of CSF Aβ42/Aβ40 was compared to that for plasma Aβ42/Aβ40 measured using Elecsys immunoassays in a subset of participants. We hypothesized that: (1) we would obtain similar cutoffs for Aβ42/Aβ40 and Aβ42/p-tau181; (2) CSF Aβ42/p-tau181 would prove more robust to longitudinal variation, compared to CSF Aβ42/Aβ40;
and (3) CSF Aβ42/Aβ40 would prove superior to plasma Aβ42/Aβ40 in terms of the percentage of individuals showing uncertain outcomes.

2. METHODS

2.1. Participants

We included 750 participants with Elecsys CSF Aβ42/Aβ40 and Aβ42/p-tau181 and Aβ-PET from three separate cohorts: 172 from the Swedish BioFINDER study (clinical trial no. NCT01208675), scanned with [18F]flutemetamol (85 cognitively unimpaired [CU] and 87 with mild cognitive impairment [MCI]), 318 from the Alzheimer’s Disease Neuroimaging Initiative (ADNI; clinical trial NCT00106899; 54 CU, 22 MCI, 37 AD dementia, and 146 with various non-AD disorders) who were scanned with [11C]Pittsburgh compound B ([11C]PiB). Inclusion criteria for individuals with and without cognitive impairment have been described elsewhere and are described in the supporting information. Written informed consent was obtained from all participants, either directly or from a legally authorized representative, with patient assent. Studies were approved by local institutional review boards.

To obtain estimates of the total variability of Aβ42/Aβ40 and Aβ42/p-tau181 over time (i.e., between different CSF collections), we also included 315 CU individuals from BioFINDER with biannual longitudinal CSF data extending up to 8 years (partially overlapping with the main cohort, but without requiring Aβ-PET). To focus on non-AD-related variability, we defined Aβ positivity in this group at baseline using a stringent threshold derived with Gaussian mixture modeling (GMM) of CSF Aβ42/Aβ40 at baseline. The GMM analysis identified two modes, representing the Aβ-negative and Aβ-positive CUs. We used the upper 95% confidence limit of the leftward (i.e., Aβ-positive) distribution as the cutoff for subject inclusion. Sensitivity analyses for estimates of variability were also performed using an alternative cutoff to define Aβ negativity, generated by the maximum separation of modes in the GMM analysis. A final sensitivity analysis for estimates of variability was done using an additional dataset from 38 participants randomly selected from the clinical practice of the Memory Clinic at Skåne University Hospital (test–retest cohort) who completed two lumbar punctures (morning and evening) and blood sampling within 6 to 10 weeks (average 7.4 ± 1.05 weeks). The collection procedure, amount of fluid collected, and pre-analytical handling protocol was identical across visits. Approximately half (47.4%) were Aβ-positive.

2.2. CSF biomarkers

Lumbar puncture and CSF handling in BioFINDER has previously been described in detail. After collection and centrifugation at three centers, CSF supernatant was stored in 1 ml aliquots in polypropylene tubes at −60°C. In ADNI, CSF collection was performed as described in the ADNI procedures manual (http://www.adni-info.org/). Within 1 hour of collection CSF samples were frozen on dry ice and shipped to the ADNI Biomarker Core laboratory at the University of Pennsylvania Medical Center. Aliquots (0.5 ml) were prepared from these and stored in barcode-labeled polypropylene vials at ≤−80°C. For UCSF samples, CSF was obtained following ADNI protocols and transferred from collection tubes into polypropylene tubes and frozen within 1 hour of sampling. Aβ42, Aβ40, and p-tau181 were measured at three different centers using the Elecsys immunoassays on a Cobas e 601 analyzer: the Clinical Neurochemistry Laboratory, University of Gothenburg, Sweden (BioFINDER); the Biomarker Research Laboratory, University of Pennsylvania, USA (ADNI); and the Clinical Chemistry Department at Skåne University Hospital, Malmö, Sweden (UCSF), according to the preliminary kit manufacturer’s instructions and as described previously.

2.3. Aβ-PET acquisition and processing

For BioFINDER, [18F]flutemetamol studies were performed using a Philips Gemini TF PET/computed tomography (CT) scanner (Philips Medical Systems), 90 to 110 minutes post-injection; data were acquired in list mode and binned into frames using an iterative Vue...
Point HD algorithm (six subsets, 18 iterations with 3 mm filter and no time-of-flight correction).

For ADNI, $[^{18}F]$florbetapir data were acquired 50 to 70 minutes post-injection. For UCSF, $[^{11}C]$PiB data were acquired 50 to 70 minutes post-injection on a Siemens Biograph PET/CT scanner. All participants completed T1-weighted magnetization-prepared rapid gradient echo magnetic resonance imaging scans for MET image co-registration and template normalization.

2.4 | Visual read of $\text{A}^\beta$-PET images

Banked $[^{18}F]$flutemetamol (BioFINDER) or $[^{18}F]$florbetapir (ADNI) PET images were re-evaluated by three independent readers at Molecular Neuroimaging, New Haven, Connecticut, USA. A similar approach was used for $[^{11}C]$PiB.

2.5 | Neuropathology

Neuropathological assessments were available for 90 participants from the UCSF cohort. Assessments were performed according to previously described procedures—blinded to CSF results—and included the AD Thal amyloid phase, indicating topographical extent of $\text{A}^\beta$ plaque pathology; Braak neurofibrillary tangle stage, indicating the topographical extent of tau neurofibrillary pathology; and Consortium to Establish a Registry for Alzheimer’s Disease (CERAD) score, indicating the density of neocortical neuritic plaques. Thal stage, Braak stage, and CERAD score were aggregated in the Alzheimer’s Disease Neuropathological Change (ADNC) score. ADNC has four levels: none, low, intermediate, or high. These were combined into none/low (negative ADNC) and intermediate/high (positive ADNC).

2.6 | Statistical analyses

All analyses were performed in R, version 4.1.2. Youden’s index was used to identify optimal cutoffs for $\text{A}^\beta_{42}/\text{A}^\beta_{40}$ and $\text{A}^\beta_{42}/\text{p-tau}_{181}$ that separated $\text{A}^\beta$-positive and $\text{A}^\beta$-negative individuals based on $\text{A}^\beta$-PET visual read. Using these cutoffs, sensitivity, specificity, and accuracy (i.e., percentage of correctly classified individuals) were calculated within and between cohorts.

To assess classification stability and identify a gray zone around cut points where there is a risk of misclassification (i.e., those with a >5% chance of having a different predicted outcome due to measurement variability if they were to have two CSF measurements close in time), we first determined the longitudinal variability of $\text{A}^\beta_{42}/\text{A}^\beta_{40}$ and $\text{A}^\beta_{42}/\text{p-tau}_{181}$ in $\text{A}^\beta$-negative CU individuals. This was calculated as the standard deviation (SD) of the average relative percent change between biomarker values across measurements. Next, we randomly varied CSF biomarker values for each participant based on a random sample from a normal distribution with mean equal to zero and SD equal to the longitudinal variability estimate for each biomarker.

This simulation was run over 1000 bootstrap trials to obtain 95% confidence interval (CI)-based gray zones for cutoffs. We report the percentage of study participants whose predicted outcomes ($\text{A}^\beta$-PET visual read and AD neuropathologic change) changed when biomarkers were randomly varied. The proportions of individuals within the gray zones for $\text{A}^\beta_{42}/\text{A}^\beta_{40}$ and $\text{A}^\beta_{42}/\text{p-tau}_{181}$ were compared using Fisher’s exact test. In addition, constrained generalized additive models were used to examine the estimated risk of having an abnormal $\text{A}^\beta$-PET scan across different levels of CSF $\text{A}^\beta_{42}/\text{A}^\beta_{40}$ and $\text{A}^\beta_{42}/\text{p-tau}_{181}$. These models were fit using the R cgam package version 1.17. Last, in the subset of individuals from BioFINDER that had both plasma and CSF $\text{A}^\beta_{42}/\text{A}^\beta_{40}$ ($n=139$), a receiver operating characteristic (ROC) analysis was performed using CSF $\text{A}^\beta_{42}/\text{A}^\beta_{40}$ status as outcome and plasma $\text{A}^\beta_{42}/\text{A}^\beta_{40}$ as predictor.

2.7 | Plasma $\text{A}^\beta_{42}/\text{A}^\beta_{40}$ in BioFINDER

Blood samples collected at the same time as CSF samples were available in a subset of participants from BioFINDER ($n=139$) and in the test–retest cohort ($n=38$). Non–AD-related variability in plasma $\text{A}^\beta_{42}/\text{A}^\beta_{40}$ was determined in the same fashion as for CSF (i.e., SD of the average relative percent change between biomarker values across measurements) in the subset of $\text{A}^\beta$-negative CU participants with available longitudinal plasma samples ($n=248$). Details surrounding plasma collection have been described previously and are included in the supporting information. Plasma $\text{A}^\beta_{42}$ and $\text{A}^\beta_{40}$ were measured using the Elecsys immunoassays on a Cobas e 601 analyzer at the Clinical Neurochemistry Laboratory, University of Gothenburg, Sweden. Performance of plasma $\text{A}^\beta_{42}/\text{A}^\beta_{40}$ was compared to that for CSF $\text{A}^\beta_{42}/\text{A}^\beta_{40}$ in the same subjects, using $\text{A}^\beta$-PET visual read as outcome ($n=46$).

3 | RESULTS

3.1 | Accuracies of CSF biomarkers to predict $\text{A}^\beta$-PET

Participant selection and characteristics are summarized in Figure S1 in supporting information and Table 1. Youden index–based cutoffs ($\text{A}^\beta$-PET visual read as outcome) by cohort were as follows: BioFINDER (<0.059 [95% CI, 0.052–0.063] for $\text{A}^\beta_{42}/\text{A}^\beta_{40}$ and <41.90 [95% CI, 34.26–54.98] for $\text{A}^\beta_{42}/\text{p-tau}_{181}$), ADNI (<0.056 [95% CI, 0.052–0.060] for $\text{A}^\beta_{42}/\text{A}^\beta_{40}$ and <39.20 [95% CI, 29.02–56.29] for $\text{A}^\beta_{42}/\text{p-tau}_{181}$), and UCSF (<0.058 [95% CI, 0.050–0.067] for $\text{A}^\beta_{42}/\text{A}^\beta_{40}$ and <46.02 [95% CI, 34.20–51.54] for $\text{A}^\beta_{42}/\text{p-tau}_{181}$). Using these cutoffs, average accuracies of $\approx90\%$ were achieved for both $\text{A}^\beta_{42}/\text{A}^\beta_{40}$ (range 90.70%–94.03%) and $\text{A}^\beta_{42}/\text{p-tau}_{181}$ (range 89.77%–94.13%). Accuracies—along with sensitivities/specificities—are reported in Table 2. Cross-validation of cutoffs between cohorts showed that accuracies were stable across cohorts and cutoffs (Figure S2 in supporting information).
TABLE 1  Participant characteristics

<table>
<thead>
<tr>
<th>BioFINDER</th>
<th>ADNI</th>
<th>UCSF</th>
</tr>
</thead>
<tbody>
<tr>
<td>Total n</td>
<td>172</td>
<td>318</td>
</tr>
<tr>
<td>CU/CI, n</td>
<td>85/87</td>
<td>54/264</td>
</tr>
<tr>
<td>Age, years</td>
<td>70.39(5.40)</td>
<td>71.06(7.16)</td>
</tr>
<tr>
<td>Female, n (%)</td>
<td>72 (42%)</td>
<td>163 (51%)</td>
</tr>
<tr>
<td>Education, years</td>
<td>11.63 (3.27)</td>
<td>16.16 (2.77)</td>
</tr>
<tr>
<td>APOE ε4+, n (%)</td>
<td>79 (46%)</td>
<td>170 (53%)*</td>
</tr>
<tr>
<td>MMSE</td>
<td>27.94 (1.70)</td>
<td>27.95 (1.79)</td>
</tr>
<tr>
<td>Elecsys Aβ42/Aβ40</td>
<td>0.068 (0.030)</td>
<td>0.053 (0.023)</td>
</tr>
<tr>
<td>Elecsys Aβ42/P-tau181</td>
<td>63.61 (43.49)</td>
<td>42.74 (33.04)</td>
</tr>
<tr>
<td>Aβ-PET, visual read, n (%)</td>
<td>77 (45%)</td>
<td>191 (60%)</td>
</tr>
</tbody>
</table>

Abbreviations: Aβ, amyloid beta; ADNI, Alzheimer’s Disease Neuroimaging Initiative; APOE, apolipoprotein E; CI, cognitively impaired; CU, cognitively unimpaired; MMSE, Mini-Mental State Examination; PET, positron emission tomography; p-tau, phosphorylated tau; UCSF, University of California San Francisco.

*APOE data missing for 26 participants. **MMSE data missing for 21 participants.

TABLE 2  Performance of Youden index–based cutoffs

<table>
<thead>
<tr>
<th>CSF measure</th>
<th>Cohort</th>
<th>Cutoff [95% CI] (Youden-based)</th>
<th>Sensitivity [95% CI]</th>
<th>Specificity [95% CI]</th>
<th>Accuracy [95% CI]</th>
</tr>
</thead>
<tbody>
<tr>
<td>Aβ42/Aβ40</td>
<td>BioFINDER</td>
<td>&lt;0.059 [0.052, 0.063]</td>
<td>93.97 [90.45, 96.98]</td>
<td>83.92 [79.22, 88.24]</td>
<td>88.33 [85.24, 91.41]</td>
</tr>
<tr>
<td></td>
<td>ADNI</td>
<td>&lt;0.056 [0.051, 0.060]</td>
<td>98.24 [96.48, 99.56]</td>
<td>87.40 [81.11, 92.91]</td>
<td>94.34 [91.82, 96.54]</td>
</tr>
<tr>
<td></td>
<td>UCSF</td>
<td>&lt;0.058 [0.050, 0.067]</td>
<td>95.12 [90.24, 98.78]</td>
<td>91.01 [86.52, 94.94]</td>
<td>93.08 [90.0, 96.15]</td>
</tr>
<tr>
<td>Aβ42/p-tau181</td>
<td>BioFINDER</td>
<td>&lt;41.90 [34.26, 54.98]</td>
<td>91.46 [87.44, 94.97]</td>
<td>86.27 [81.57, 90.21]</td>
<td>88.55 [85.02, 90.97]</td>
</tr>
<tr>
<td></td>
<td>ADNI</td>
<td>&lt;39.20 [29.40, 56.20]</td>
<td>95.81 [92.67, 96.54]</td>
<td>91.34 [86.61, 96.10]</td>
<td>94.03 [91.19, 96.54]</td>
</tr>
<tr>
<td></td>
<td>UCSF</td>
<td>&lt;46.02 [34.20, 51.54]</td>
<td>95.12 [90.21, 98.78]</td>
<td>92.70 [88.76, 96.63]</td>
<td>93.46 [90.38, 96.15]</td>
</tr>
</tbody>
</table>

Note: Youden-based cutoffs were based on Aβ-PET visual read as outcome.

Abbreviations: Aβ, amyloid beta; ADNI, Alzheimer’s Disease Neuroimaging Initiative; CI, confidence interval; CSF, cerebrospinal fluid; PET, positron emission tomography; p-tau, phosphorylated tau; UCSF, University of California San Francisco.

3.2 Longitudinal variability and robustness of predictions using CSF biomarkers

Using longitudinal CSF data from a separate cohort of Aβ-negative CU individuals (n = 269), the observed variability (SD of the average relative percent change between biomarker values) was 11.18% for Aβ42/Aβ40 and 19.35% for Aβ42/p-tau181—no significant differences were seen in accuracy across cohorts (Table S1 in supporting information).

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3.3 CSF biomarker status in relation to Aβ-PET and ADNC scores

To examine whether participants in the gray zone for CSF Aβ42/Ab40 and Aβ42/p-tau181 were close to the cutoffs for Aβ-PET, we plotted Aβ42/Ab40 and Aβ42/p-tau181 status (negative, positive, or in the gray zone using Aβ-PET visual read as outcome) in relation to Aβ-PET standardized uptake value ratio and ADNC scores (Figure S6 in supporting information). Using a priori cutoffs for Aβ-PET, an average of 73.38% (BioFINDER-1, 73.68%; ADNI, 73.08%) and 91.16% (BioFINDER-1, 90%; ADNI, 92.30%) of gray zone cases were Aβ-PET positive using Aβ42/Ab40 and Aβ42/p-tau181, respectively. In the UCSF cohort, 14.81% and 7.41% of gray zone cases had intermediate/high ADNC scores for Aβ42/Ab40 and Aβ42/p-tau181, respectively.

3.4 Longitudinal variability and robustness of predictions using plasma biomarkers

In the 139 participants that had Aβ42/Ab40 measured in both CSF and plasma (Table S5 in supporting information), 9.35% fell within the interval associated with >5% chance of having a different predicted Aβ-PET visual read over time. For plasma—in which the longitudinal variation for Aβ42/Ab40 was 7.49% in Aβ-negative CU participants (average follow-up, 3.65 ± 1.57 years)—30.93% of participants fell within the interval associated with a >5% chance of having a different predicted outcome over time when using Aβ-PET visual read as outcome. Improved findings (28.78% with uncertain outcome) were obtained when plasma Aβ42/Ab40 variation was derived from the test–retest cohort (4.10%). Data points for Aβ40 and Aβ42 (CSF and plasma) are shown in relation to the cutoffs for Aβ42/Ab40 in Figure S7 in supporting information. ROC analysis using CSF Aβ42/Ab40 status as outcome (binarized as positive/negative using the Youden-based cutoff of <0.0610) showed that plasma Aβ42/Ab40 had an area under the curve (AUC) of 0.834 (95% CI, 0.762–0.907).

3.5 Online individualized risk prediction tool

We provide an illustrative online tool at https://brainapps.shinyapps.io/CSFpredict_GZ/, where individualized predictions can be made for Aβ-PET using CSF Aβ42/Ab40 and Aβ42/p-tau181. Illustrative cases showing positive, negative, and gray zone CSF results for Aβ42/p-tau181 are shown in Figure 3.
FIGURE 2  Estimated risk of Aβ-PET positivity for CSF Aβ42/Aβ40 and Aβ42/p-tau181 in BioFINDER. The estimated risk of being Aβ-PET positive is shown for CSF Aβ42/Aβ40 (A and B) and Aβ42/P-tau181 (C and D), assuming a prevalence of ≈30% Aβ-PET positivity (dashed gray line). Results are shown using ratios (A and C) and percentiles (B and D). While the risk of being Aβ-PET positive was low for both Aβ42/Aβ40 and Aβ42/p-tau181 at higher (normal) levels, the risk of Aβ-PET positivity was greater for Aβ42/p-tau181 at lower (abnormal) levels. Aβ, amyloid beta; ADNI, Alzheimer’s Disease Neuroimaging Initiative; CSF, cerebrospinal fluid; PET, positron emission tomography; p-tau, phosphorylated tau; UCSF, University of California San Francisco

4 | DISCUSSION

As universal cutoffs are a key prerequisite for the widespread use of Aβ42/Aβ40 and Aβ42/p-tau181 in clinical practice, we examined how comparable cutoffs were across cohorts and the impact of different cutoffs on accuracy (i.e., percentage of correctly classified individuals). Despite the CSF samples having been analyzed in different laboratories using several preanalytical protocols—and there being differences in cohort composition and Aβ-PET tracers—we did not observe significant differences in either cutoffs or accuracies across measures and cohorts, nor in accuracies using a common (average) cutoff across cohorts for Aβ42/Aβ40 and Aβ42/p-tau181. These findings are in line with previous work using CSF Elecsys AD biomarkers, in which it was shown that a cutoff combining Aβ42 and P-tau181 established in BioFINDER and validated in ADNI showed high concordance with visual read Aβ-PET classification.23 Though these results suggest, overall, that Elecsys Aβ42/Aβ40 and Aβ42/p-tau181 may prove relatively robust to methodological differences, numeric differences of ≈3% between cohorts indicate that a unified preanalytical protocol for CSF handling may nevertheless be optimal to facilitate the establishment of global cutoff values required for routine use of CSF biomarkers in clinical practice.38,39

Across the investigated outcomes (Aβ-PET visual read, and ADNC score), the percentage of individuals at risk for misclassification was lower for Aβ42/p-tau181, compared to Aβ42/Aβ40. The superior performance of Aβ42/p-tau181 may reflect the greater TAE of this measure. Despite having a greater estimate of measurement variability (19.35% vs. 11.18% for Aβ42/Aβ40 using the SD of the average relative percent change between biomarker measurements from longitudinal data in Aβ-negative CU individuals), fewer subjects fell within the range associated with a > 5% chance of varying back and forth across the cutoff threshold. This can likely be explained by the fact that data points for Aβ42/Aβ40 are closer to the cutoff than for Aβ42/p-tau181. The superiority of Aβ42/p-tau181 when using Aβ-PET visual read and ADNC score as outcomes may also be due to this marker combining measures of two different pathologic processes into a single measure. As CSF Aβ42 and p-tau181 concentrations are thought to change at different points in the disease course (earlier for Aβ42, later for p-tau181),41 their combination may improve performance when predicting measures of disease stage, such as Aβ-PET status, measures of clinical progression, or post mortem estimates of AD pathology burden. Moreover, in clinical settings in which Aβ-PET is increasingly used, risk curves based on constrained generalized additive models clearly showed that abnormal Aβ42/p-tau181 ratio values carried a
FIGURE 3  Online individualized risk prediction tool for Aβ-PET. BioFINDER-based individualized risk predictions are shown for Aβ-PET using CSF Aβ42/Aβ40 and Aβ42/p-tau181 levels that are (A) positive, (B) negative, and (C) in the gray zone for either marker. Cutoffs and associated intervals used to define gray zones were 0.059 [0.052, 0.063] for CSF Aβ42/Aβ40 and 41.90 [34.40, 54.98] for CSF Aβ42/p-tau181. Aβ, amyloid beta; CI, confidence interval; CSF, cerebrospinal fluid; PET, positron emission tomography; p-tau, phosphorylated tau.

In the present study we estimated the percentage of cases whose predicted status (normal vs. abnormal) on different AD-related outcomes would have a >5% chance to differ after repeated lumbar punctures. Our results call attention to the importance of such gray zones when using CSF AD biomarkers. While the number of participants falling within this zone was relatively low (e.g., 11.04%, on average, for Aβ42/Aβ40, and 5.81% for Aβ42/p-tau181 when using Aβ-PET status as outcome), these figures nevertheless translate into significant case numbers when extrapolated to scenarios in which these biomarkers are used in clinical practice. Gray zones have been previously described for Aβ42/p-tau181 measured using INNOTEST ELISAs in patients with dementia, and have also been described in recommendations for the use of CSF in the diagnostic workup of MCI patients. Similarly to other areas of medicine, including oncology and cardiology, recommendations have included that the analysis be repeated or that an imaging-based investigation be performed. The
upper and lower boundaries defining the gray zone for a given marker could even be used in the clinical chemistry laboratory providing the CSF results to clinicians, such that a gray zone result would result in immediate re-testing of the sample. Should the result still fall within the gray zone for that measure, a new lumbar puncture could be ordered, or an imaging biomarker ordered. Our findings on the percentage of gray zone cases that were Aβ-PET positive support this approach, particularly for Aβ42/p-tau181 (where ≈90% were Aβ-PET positive, compared to ≈73% for Aβ42/Aβ40).

Though measuring Aβ reliably in blood has proven challenging using traditional ELISA technology, plasma Aβ42/40 determined using high-precision immunoprecipitation-coupled mass spectrometry (IP-MS) has been shown to correlate with Aβ-PET and to accurately identify individuals who are Aβ-positive using PET. More recent work using fully automated immunoassay platforms—including the Elecsys platform from Roche—have shown accuracies for predicting Aβ-PET that approach those for MS-based Aβ42/40 measures. We therefore compared the performance of CSF Aβ42/40 to that for plasma Aβ42/40, both measured using the Elecsys platform. Compared to CSF Aβ42/40, the number of participants that fell within the range associated with >5% chance of having a different predicted outcome over time was ≈1.5 to 3 times greater when using plasma Aβ42/40. This is likely because the data points for Aβ42/Aβ40 in plasma are closer to the cutoff than those for CSF. Though we were unable to compare CSF Aβ42/40 with plasma Aβ42/40 measured using a different immunoassay, the difference in performance between CSF and plasma would likely have been even greater as a recent head-to-head comparison of several IP-MS and immunoassays showed that Aβ42/40 measured using Elecsys immunoassays was the best performing in terms of AUC values using CSF Aβ42/40 and Aβ-PET status as outcome. The superior performance of Aβ42/40 in CSF, compared to plasma, can be attributed to the fact that Aβ brain pathology results in a decrease in plasma Aβ42/40 of 8% to 15%, compared to a decrease of ≈50% in CSF. This difference is thought to relate to peripheral Aβ production, binding to peripheral blood proteins that are present at approximately 200-fold higher concentrations in plasma than in CSF, and liver metabolic rates.

Strengths of this study include its large sample size, the use of three separate cohorts, and the use of multiple AD-related outcomes. Moreover, CSF biomarkers were measured using the same type of (Elecsys) platform at three different sites and the variability estimates for Aβ42/Aβ40 and Aβ42/p-tau181 were determined using several approaches. Also, we compared the performance of Aβ42/Aβ40 in CSF and plasma measured in the same individuals using the same immunoassays. We also provide an online prediction tool to illustrate the possible future use of such a tool in clinical settings, though future studies will be required to address its performance in other cohorts. A limitation of this study was that there were differences in the clinical composition of cohorts and the outcome used to set Youden-based cutoffs (i.e., Aβ-PET visual read) involved three different Aβ-PET tracers ([18F]Flutemetamol, [18F]Florbetapir, and [11C]PIB); despite these differences, however, the percentage of correctly classified individuals (i.e., accuracy) was similar across cohorts. Moreover, such methodological differences are likely representative of the variability in current clinical practice. Further, though Aβ-PET visual read analysis has been shown to be well correlated with Aβ pathology post mortem, visual read remains a proxy for histopathology and is partially subjective and reader dependent. Last, the included pathology cohort was small, which likely explains the trend level finding when using ADNC scores as outcome. This warrants further work in a larger post mortem cohort.

In conclusion, we here showed that similar cutoffs could be applied across centers to Elecsys CSF Aβ42/Aβ40 and Aβ42/p-tau181 and that Aβ42/p-tau181 was more robust to the effects of measurement variability in terms of AD-related outcomes than Aβ42/Aβ40, using three separate cohorts with different populations, preanalytical protocols, and Aβ-PET tracers. These findings suggest that Aβ42/p-tau181 may be the preferred Elecsys-based measure in clinical settings and clinical trials. Future studies are required, however, addressing gray zone cases.

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CONFLICTS OF INTEREST

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**SUPPORTING INFORMATION**

Additional supporting information can be found online in the Supporting Information section at the end of this article.

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