Electrospinning Optimisation of Drug-Loaded Eudragit E PO for Paediatric Oral Drug Delivery
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PURPOSE
Currently there is a lack of age appropriate formulations. Liquids can taste bad, and solids are difficult to swallow, leading to poor compliance in the paediatric population. Manufacturing a novel dosage form that is palatable and is easy to swallow could be made possible by using a novel technique such as electrospinning. By combining a bitter drug, Chlorpheniramine Maleate (CPM), with a taste masking polymer, Eudragit E PO (E- EPO), taste masked fibres can be manufactured.

OBJECTIVE
Electrospinning is affected by process, solution and environmental factors [1]. The aim of this study is to utilise a design of experiment approach (DoE) to efficiently optimise the quality of the fibres produced.

METHOD(S)
All solutions were prepared to 100% using absolute ethanol. Ratios of 1:6 of CPM :E- EPO were used in the drug loaded fibres. Spraybase® electrospinning apparatus was used to manufacture the fibres. A Scanning Electron Microscope (SEM) FEI Quanta 200FEG, was used to image the fibres. ImageJ 1.46R was used to measure diameters. JMP Pro 12.0.1 was used to create the fractional design and for data analysis. Parameters investigated are shown in Table 1.

Table 1 - A table displaying the factors and the three corresponding levels for each factor

<table>
<thead>
<tr>
<th>Factor</th>
<th>Low</th>
<th>Medium</th>
<th>High</th>
</tr>
</thead>
<tbody>
<tr>
<td>Applied voltage (kV)</td>
<td>10.0</td>
<td>17.50</td>
<td>25.0</td>
</tr>
<tr>
<td>Flow rate (mL/h)</td>
<td>0.50</td>
<td>1.25</td>
<td>2.00</td>
</tr>
<tr>
<td>Gap distance (mm)</td>
<td>150</td>
<td>200</td>
<td>250</td>
</tr>
<tr>
<td>E- EPO concentration (%w/v)</td>
<td>25.0</td>
<td>35.0</td>
<td>45.0</td>
</tr>
<tr>
<td>Water in solvent (%v/v)</td>
<td>0.00</td>
<td>10.0</td>
<td>20.0</td>
</tr>
</tbody>
</table>

The desired fibres were manufactured with the morphology and ease of operation as the optimisation criteria, namely reducing beading, and fibre diameter.

RESULT(S)
Initially placebo fibres were optimised, as shown in Figs 1a, 1b and 1c.

DoE modelling tool predicted optimum conditions that maximise desirability - 35% E- EPO, 0.5mL/h flow rate, 150 mm gap distance, 15-20 kV applied voltage were predicted to form fibres with an average diameter of 621 nm and minimal beading. When validated experimentally smooth non-beaded fibres with an average diameter of 1508 nm (± 250 ) were formed (Fig 1b).

When the drug was added, the solution properties changed and hence re-optimisation was required. SEM images shown in Figs 2a, 2b and 2c.

Increased polymer concentration was found to be the most significant factor in increasing placebo fibre diameter, p-value = 0.008, and decreasing beading, p-value = 0.004.

Similar to placebo fibres, concentration was found to be the most influential factor affecting fibre morphology. At a concentration of 40% E- EPO, smooth ribbons were formed, however, needle clogging halted the smooth running of the electrospinning process.

Generally, the conditions for producing good drug-loaded fibres were the same as with placebo fibres, when the drug was added at a 1:6 ratio to the polymer.

CONCLUSION(S)
The fractional factorial DoE approach reduced the number of runs required to optimise the placebo fibres from 3⁶ or 243 runs, to 12 runs. The design identified the most influential manufacturing conditions for nano-diameter fibres and absence of beading as well as the prediction of optimal conditions for both outcomes. The study has therefore not only suggested parameters for producing E- EPO fibres but has also developed an approach for the rational choice of electrospinning conditions.

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REFERENCE