

Optimising ablation strategies to treat ventricular fibrillation

Peter Taggart¹, Martyn P. Nash^{2,3}, Pier Lambiase^{1,4}

¹Institute of Clinical Sciences, University College London, London, UK

²Auckland Bioengineering Institute, University of Auckland, New Zealand

³Department of Engineering Science, University of Auckland, New Zealand

⁴Barts Heart Centre, Dept. of Cardiology, St Bartholomews Hospital, London, UK

Since the earliest documented accounts of ventricular fibrillation (VF) over 3000 years ago [1] the mechanisms responsible have been the source of ongoing debate. During the early part of last century, both focal and re-entrant mechanisms were proposed, and more recently the re-entry mechanisms have polarised into the multiple wavelet and mother rotor hypotheses. The multiple wavelet hypothesis, originally put forward by [2] to explain atrial fibrillation, implies that VF is sustained by multiple circulating unstable wavelets perpetuated by a sequence of wavebreaks and self-generating re-entry. The mother rotor hypothesis [3] proposes that VF is maintained by a single rapid periodic source that is unable to sustain uniform 1:1 conduction throughout the myocardium resulting in intermittent conduction block with multiple irregular activation patterns. Early studies from several groups across a range of animal species have provided evidence in support of one or other hypothesis. A subsequent study using multi-electrode total epicardial mapping in patients undergoing routine surgical procedures showed that both mechanisms appeared to be operative during the first 20 to 40 seconds of human VF [4]. These findings are now generally accepted, although the relative contributions of focal and rotor activity are still debated. Recently, there has been a revival of interest in focal mechanisms with studies indicating a role of the Purkinje system as both a trigger and in the maintenance of VF [1,5].

These mechanistic considerations are of great importance, not only for our understanding of VF mechanisms, but also as they underpin therapeutic ablation strategies. Traditional targets include sites with structural features

that stabilise and perpetuate functional re-entry and focal sources, which can be identified using VF mapping [6]. Quantitative methods for analysing VF date back over three decades [7], with methods for identifying re-entrant activity being pioneered by Gray and colleagues [8], who used phase techniques to analyse optical maps of cardiac electrical activity during VF. Nash and colleagues [4] translated these techniques to studying VF in cardiac patients using electrocardiac mapping with arrays of contact electrodes across the entire ventricular epicardium. These techniques are now well established for studying cardiac fibrillation [9,10,11], though care must be taken over data interpretation, particularly with respect to the spatial resolution of recordings [12].

Non-invasive quantification of VF using phase analysis relies on the ability to determine the spatio-temporal electrical activity of the heart from body surface recordings. A variety of theoretical ECG imaging (ECGI) methods have been proposed to address this need by predicting epicardial potentials [13]; equivalent dipole layers [14]; or the ventricular activation sequence [15]. However, in vivo validation of these techniques has faced many challenges [16], and studies comparing ECGI predictions against directly measured cardiac electrograms have yielded mixed results. Sophisticated ECGI validation work has been performed using carefully controlled isolated perfused hearts in torso tanks [17,18], and while some in-situ validation studies have demonstrated good reproducibility (e.g. [19]), others have shown variable correlation (e.g. [20,21,22]) due to factors such as sensitivity to geometric inputs for the ECGI computations. Nevertheless, ECGI has been applied to study cardiac arrhythmias in patients (e.g. [23,24]), but there remains a paucity of data demonstrating the clinical validation of ECGI in patients with VF, primarily because of the technically challenging and demanding protocols.

In the current issue, Haïssaguerre and colleagues [25] studied 54 patients with structural heart disease presenting with VF in the absence of preceding VT. Electrophysiological mapping was used to optimise the strategy for targeted ablation therapy. The mapping techniques incorporated both endocardial and epicardial contact electrode mapping together with body surface ECGI during an initial period (mean of 16 seconds) immediately following the onset of VF. Key findings were: (i) activities during the initial period of VF arose from parts

of the structural substrate and Purkinje system prior to propagating through the ventricular mass; (ii) Purkinje arrhythmogenic activity may be elicited by programmed stimulation; (iii) ablation, targeting the main sources of activation, prevented recurrence in 83% of patients over a five year follow up period.

This study is an important contribution in the management of idiopathic VF and prevention of recurrent cardiac arrest. The findings shed light on strategies to identify triggers and target the substrate - key elements enabling the development of VF - and presents a coherent case for the efficacy of combining myocardial substrate characterisation, Purkinje mapping and VF mapping to optimise ablation therapy. The use of ECGI to visualise ectopics on the ward, or during exercise testing, presents an advantage. The mapping of abnormal substrate during induced VF is an important further contribution, as this aids optimisation of ablation when ectopy is not present. Several questions arise: what specific features of these VF foci distinguish them as key source locations, or are they simply anchor sites for VF rotors in the myocardium? Moreover, can specific markers from electrograms and/or conduction-repolarisation dynamics distinguish key areas to target for ablation in idiopathic VF? Data from Brugada Syndrome and a proportion of early repolarisation idiopathic VF patients would indicate that specific depolarisation abnormalities with fractionation are important markers of 'VF substrate'. The challenge remains to ensure that bystander areas are not ablated so as to create a partial lesion that may later act as a nidus for VF. Future studies focusing on these electrophysiological characteristics would help to inform ablation strategies to standardise procedures. The main question here is which dynamic features are important? Example contenders include steep restitution slopes, specific degrees of functional block, and localised repolarisation alternans, to mention a few. Such features require detailed interrogation of the tissue, and this is becoming more accessible using high density multipolar grid catheters to streamline the techniques. Furthermore, the exact aetiology of these sites remains to be elucidated - are they due to the effect of previous micro-infarction, inflammation or somatic mutations in the tissue that can cause localised electrophysiological anomalies? Such knowledge may help inform more targeted small molecule or novel anti-arrhythmic drug strategies.

Finally, the authors should be congratulated on an outstanding contribution to clinical electrophysiology research, which adds to our understanding of VF, and will no doubt contribute to future therapeutic strategies for its management.

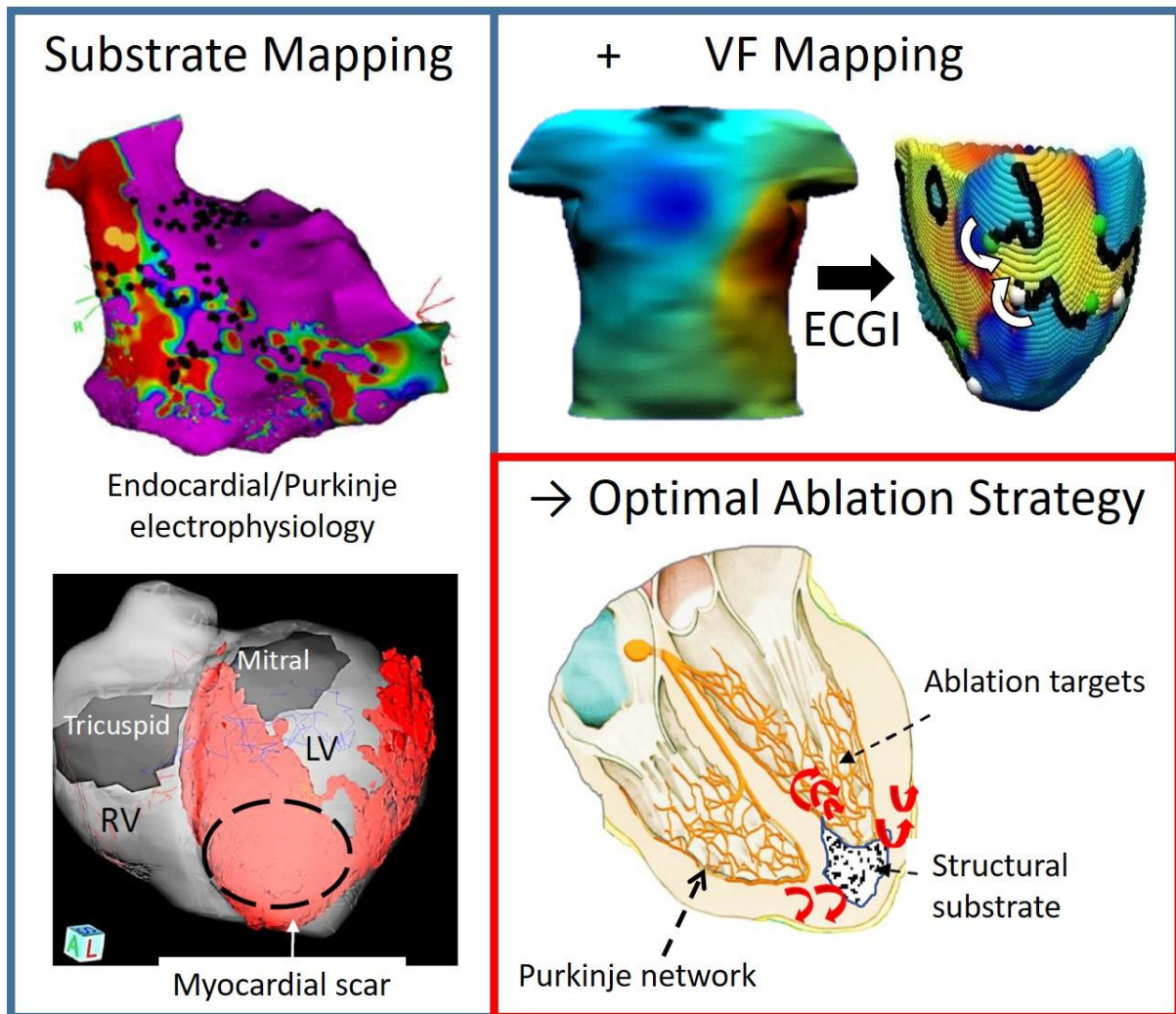


Figure: Electrophysiological/Purkinje mapping and structural imaging of the heart (left) can be used to characterise the triggers and substrate for ventricular fibrillation (VF). Combination of this myocardial substrate mapping with functional imaging of VF, via non-invasive electrocardiographic imaging (ECGI; upper right), can be used to optimise the strategy and identify targets for ablation therapy. LV/RV: left/right ventricles.

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