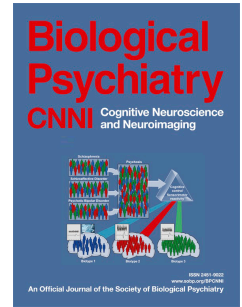


Journal Pre-proof

An Approach to Neuroimaging Interpersonal Interactions in Mental Health Interventions

James Crum, Xian Zhang, Adam Noah, Antonia Hamilton, Ilias Tachtsidis, Paul Burgess, Joy Hirsch



PII: S2451-9022(22)00025-8

DOI: <https://doi.org/10.1016/j.bpsc.2022.01.008>

Reference: BPSC 908

To appear in: *Biological Psychiatry: Cognitive Neuroscience and Neuroimaging*

Received Date: 12 July 2021

Revised Date: 31 December 2021

Accepted Date: 25 January 2022

Please cite this article as: Crum J., Zhang X., Noah A., Hamilton A., Tachtsidis I., Burgess P. & Hirsch J., An Approach to Neuroimaging Interpersonal Interactions in Mental Health Interventions, *Biological Psychiatry: Cognitive Neuroscience and Neuroimaging* (2022), doi: <https://doi.org/10.1016/j.bpsc.2022.01.008>.

This is a PDF file of an article that has undergone enhancements after acceptance, such as the addition of a cover page and metadata, and formatting for readability, but it is not yet the definitive version of record. This version will undergo additional copyediting, typesetting and review before it is published in its final form, but we are providing this version to give early visibility of the article. Please note that, during the production process, errors may be discovered which could affect the content, and all legal disclaimers that apply to the journal pertain.

© 2022 Published by Elsevier Inc on behalf of Society of Biological Psychiatry.

An Approach to Neuroimaging Interpersonal Interactions in Mental Health Interventions

James Crum^{1*}, Xian Zhang³, Adam Noah³, Antonia Hamilton¹, Ilias Tachtsidis², Paul Burgess¹, Joy Hirsch^{2,3,4,5}

¹Institute of Cognitive Neuroscience, University College London, London, UK.

²Department of Medical Physics and Biomedical Engineering, University College London, London, UK. Institute of Cognitive Neuroscience, University College London, London, UK

³Brain Function Laboratory, Department of Psychiatry, Yale School of Medicine, New Haven, CT, USA

⁴Department of Neuroscience, Yale School of Medicine, New Haven, CT, USA

⁵Department of Comparative Medicine, Yale School of Medicine, New Haven, CT, USA

*** Correspondence:**

James Crum

james.crum.16@ucl.ac.uk

17 Queen Square, London WC1N 3AR

Keywords: mental health; psychotherapy; functional near-infrared spectroscopy; neural coupling; interpersonal interaction; frontal lobe

Abstract

Background. Conventional paradigms in clinical neuroscience tend to be constrained in terms of ecological validity, raising several challenges to studying the mechanisms mediating treatments and outcomes in clinical settings. Addressing these issues requires real-world neuroimaging techniques that are capable of continuously collecting data during free-flowing interpersonal interactions and that allow for experimental designs which are representative of the clinical situations in which they occur.

Methods. In this work, we developed a paradigm that fractionates the major components of the human-to-human verbal interactions occurring in clinical situations and used functional near-infrared spectroscopy to assess the brain systems underlying clinician-client discourse (n = 30).

Results. Cross-brain neural coupling between people was significantly greater during clinical interactions compared to everyday-life verbal communication, particularly between the prefrontal cortex (PFC) (e.g., inferior frontal gyrus) and inferior parietal lobule (e.g., supramarginal gyrus). Interestingly, the clinical tasks revealed extensive increases in activity across the PFC, especially in rostral PFC (area 10) during periods in which participants were required to silently reason about the dysfunctional cognitions of the other person.

Conclusions. This work demonstrates a novel experimental approach to investigating the neural underpinnings of interpersonal interactions that typically occur in clinical settings, and its findings support the idea that particular prefrontal systems might be critical to cultivating mental health.

Introduction

A common framework of neuroimaging methods investigating the treatment of psychopathological disorders is to collect neuroimaging data periodically at particular stages of treatment rather than continuously, *in situ* (1). Although this framework is excellent for examining the effects of clinical interventions on behavioral, affective, and physiological responding (2), it creates an important explanatory gap regarding the nature of the neural systems by which these changes are brought about during the clinical interpersonal interactions that are central to a multitude of treatments (Figure 1). In other words, neuroimaging techniques are currently being used to study etiopathogenic mechanisms and cortical dysregulation as well as the effects and efficacy of (non-)psychopharmacological treatments on changes in neural activity and behavior, such as functional near-infrared spectroscopy (fNIRS) (2-5). However, observing only the effects of interventions, such as decreases in maladaptive behavior, emotion dysregulation, and functional dysconnectivity (6, 7), limits our understanding of the neurocognitive mechanisms by which adaptive changes in mental health are cultivated during treatment (8). For instance, what is it about the interpersonal interactions in clinical situations that fosters healthier thinking, feeling, and behaving on the part of patients? Second-person neuroscience approaches to investigating such neuropsychiatric questions might represent a path towards addressing this explanatory gap. Indeed, the neural systems in which *clinicians* engage to treat patients and those in which patients also probably learn to engage remain largely unclear.

Figure 1

The chief reason why data are not collected *in situ* is that there are inherent limitations to most neuroimaging methods that constrain the types of experimental designs that can be employed in intervention-type settings (see Ref. 1 & 2). So, to investigate the neurocognitive

mechanisms of interest during treatment, the method that should ideally be adopted is one that allows for 'real-world' paradigms and the collection of data relating to interpersonal information-processing dynamics. Recent cognitive neuroscientific research has acknowledged this need for a multi-person and, indeed, multi-modal framework by using the neuroimaging technique of hyperscanning to explore the inter-subject systems underpinning human-to-human interaction (e.g., Refs. 9-23). Hyperscanning measures hemodynamic changes and interpersonal brain synchronization between two or more individuals whilst engaging in interactive tasks in naturalistic or laboratory settings (see Refs. 24-27, for reviews). Neuroimaging methods such as functional magnetic resonance imaging and electroencephalography have used this technique in several studies, with a growing number of publications using fNIRS-based hyperscanning (28). For example, portable, wireless neuroimaging systems are methodological complements to experimental designs that are more naturalistic or 'ecological' (29). But what type of ecological experimental design is then appropriate for investigating clinically representative settings and situations, yet retains the degree of scientific control required in contemporary cognitive neuroscience? It is probably one that approaches the conundrum of clinical interpersonal interactions by attempting to *fractionate* their core modality: verbal communication.

Interestingly, that the dialog between clinicians and clients is typically dialectical in nature represents the most clinically significant use of language in verbal interventions (30-32). For example, clients express thoughts as statements or propositions about goal-incongruent events, reflecting specific dysfunctional cognitive schemas and appraisals (33, 34), and, in turn, clinicians use various adaptive strategies to challenge the veracity and utility of these thoughts (35, 36).

Importantly, what is perhaps most demanding of clinicians is their task that immediately precedes this verbal intervention: to critically think about and *recogitate* clients' beliefs (1, 2). A standard position that might be adopted from our knowledge of cognitive neuroscience so far might be that the brain systems taxed by such a process likely depend in part on executive subsystems based in the prefrontal cortex (PFC) that are dedicated to solving ill-structured, linguistically mediated reasoning problems (see Ref. 37, for review). And, in this case, these subsystems likely modulate a more posterior, semantic network in which maladaptive schema and appraisal processes are represented and stored (38). If this is the case, then the literature in this area of cognitive control (39-47) and emotion regulation (48-51; see Refs. 46 & 52, for reviews) suggest that rostral PFC (area 10) and middle frontal gyrus (area 46) might play a marked role in this 'thinking' task that potentially drives not only clinician-led verbal interventions but also eventual client-led ones independent of treatment settings.

A few fNIRS-based hyperscanning studies on verbal communication have recently been conducted to examine the neural underpinnings of dynamic coupling between people during natural dialog (e.g., Refs. 13, 18, 19, 22, 53, & 54), with common findings in subregions that have long been implicated in speech production and comprehension such as Broca's and Wernicke's areas, respectively, as well as in the PFC subregions mentioned above. Interpersonal synchronization has tended to be significantly greater between people during these verbal interactions as compared to random pairings of participants who nevertheless conversed, but not with each other. However, no study to our knowledge has developed an experimental design that can be adapted to different clinical settings to specifically assess the inter- and intra-neural dynamics of verbal exchanges in clinical situations, particularly their epochs (e.g., speaking, listening, and thinking), nor have such exchanges been compared to non-clinical verbal

communication to assess what is unique about clinical interactions that make the clinician successful or the interaction compelling to the client.

Accordingly, the aim of this work was to use a ‘real-world’ approach to developing a neuroimaging paradigm that addresses these theoretical and practical lacunae. It was predicted that, because clinical situations are inherently more interactive and normative than everyday instances of verbal communication, clinical interpersonal interactions will elicit greater cross-brain coherence in paired participants engaging in the roles of clinician and client compared to a control condition, and that within-brain contrasts will show cognitive resource consumption predominately across the PFC. Moreover, since the tasks of clinicians in real-world treatment settings are much less passive than those involved in everyday discourse, it was hypothesized that periods of verbal intervention, in which clinicians are required to dispute dysfunctional cognitions about the self, others, and world, should demonstrate changes in activity above and beyond normal speaking demands, particularly in rostral PFC (area 10) and more posterior areas related to the semantic network. It was further expected that, perhaps to a greater degree, this pattern of activity will also be demonstrated prior to verbal intervention when clinicians covertly reason about dysfunctional cognitions, namely in rostral PFC and right middle frontal gyrus (area 46).

Methods and Materials

Participants

Thirty healthy adults (15 pairs; 80% female; mean age = 30.17 ± 12.68 years; 97% right-handed) participated in the study (55). All participants provided written informed consent in accordance with guidelines provided by the Yale Human Investigation Committee (HIC

#1501015178), were reimbursed for participation. Dyads were assigned in order of recruitment and no individual participated in more than one dyad. Eligibility of participation was determined using two screening tasks, namely a right-handed finger-thumb tapping task and passive viewing of a reversing checkboard whilst fNIRS signals were acquired. A participant was selected for the hyperscanning experiment if counter-correlated HbO₂ and HbR signals were observed in the left motor hand-area for the finger-tapping task ($p < .05$) and in the bilateral occipital lobe for the passive viewing task ($p < .05$). This screening procedure attempted to ensure that the fNIRS signals of the sample were reliable and not confounded by irregularities in skull thickness, fat deposits, bone density, and blood chemistry (56-58).

Experimental paradigm

Participants were seated approximately 140 centimeters across a table and with a full field of vision of each other in a normal room (see Figure S1 in Supplementary Material). A computer screen was also positioned approximately 45° to the side of this face-to-face orientation and 70 centimeters from each participant's face; so, the participants in each dyad had their own computer screens from which to view stimuli and that only they could see, and at which they needed not to turn their heads to look. Participants engaged in four conditions (counterbalanced). The two factors classifying them were 'situation' and 'role'. In the clinical situation, each participant was able to act as both the clinician and client; in the control condition, each participant was able to act as the speaker and responder (see Figure S2). No participant was used more than once and each partner in a dyad was always different. The experimental design was therefore blocked and adopted a repeated-measures approach.

The subtasks across these conditions and within dyads included speaking, listening, and thinking epochs. (Figure 2). These subtasks, together with the stimuli, varied in nature depending

on whether the interpersonal interaction was clinical. Namely, all stimuli shown on the computer screens were linguistic propositions, but in clinical blocks they were affective, or *hot*, conceptual valuations (59) (i.e., cognitive appraisals [34]) and, more specifically, were dysfunctional in that they were irrational and unrealistic in terms of being ungrounded in logic, empiricism, and pragmatism (33), representing a conjunction of the major types of irrational thinking (e.g., catastrophizing, self-downing, demandingness, etc.). For example: “My friends must always treat me fairly,” whereas the propositions in control blocks were purely descriptive facts about the world, containing no evaluative or normative component: “It is cheaper to buy produce from a farmers market.”

Figure 2

Signal acquisition and optode localization

Functional NIRS signal acquisition of hemodynamics was acquired using a 80-fiber (108-channel) continuous-wave fNIRS system (LABNIRS, Shimadzu Corp., Kyoto, Japan) configured for hyperscanning (54 channels per person) and sampled at a rate of 27 Hz at three wavelengths of light (780, 805, and 830 nm). A light-emitting diode probe (Daiso Crop., Hiroshima, Japan) was used to achieve an orthogonal connection between the fNIRS optodes and scalp (i.e., to displace hair in the cap). Anatomical locations of optodes in relation to standard head landmarks, including inion and top center (Cz) and left and right tragi, were determined using a Patriot 3D Digitizer (Polhemus, Colchester, VT) and linear transform techniques (60-64). Montreal Neurological Institute (MNI) coordinates (65) for each channel were obtained using NIRS-SPM software (66) with MATLAB (Mathworks, Natick, MA).

Regions of interest (ROIs)

The anatomical coverage of the channel configuration was corresponded with eleven bilateral ROIs (Table 4; see Figure S3 in Supplementary Material): rostral PFC (Brodmann's area [BA] 10), middle frontal gyrus (BA46/9), inferior frontal gyrus (BA44/45/47), angular gyrus (BA39), supramarginal gyrus (BA40), middle temporal gyrus (BA21), superior temporal gyrus (BA22), somatosensory cortex (BA1/2/3), premotor and supplementary motor cortex (BA6), subcentral area (BA43), and primary auditory cortex (BA42). These ROIs were specified *a priori* based on recent hyperscanning research on human-to-human verbal communication (13, 18, 19, 22, 53, & 54), neuroimaging and cortical brain stimulation meta-analyses in emotion regulation (e.g., reappraisal [48-51]), and neuroimaging and neuropsychological research on frontal lobe functions (37, 46, & 47), particularly on the activation biasing of stimulus-independent attention (67) in favor of generating novel strategies (39-43, 45, 68, & 69). That is, the channel configuration was designed to achieve coverage only over these theoretically constrained ROIs (see Ref. 70).

Signal processing

Pre-processing of raw fNIRS signals consisted of removing global systemic effects such as respiration, heart rate, and blood pressure (71) using a principal component analysis (PCA) spatial filter (72, 73), a technique which uses the distributed optode coverage to distinguish signal components originating from local and distal (i.e., extracerebral) sources. Onsets and durations of the epochs of each trial of each block were extracted to generate the stimulus design, with which the canonical hemodynamic response function was then convolved using NIRS-SPM. A general-linear model (GLM) analysis then fitted these predicted signals to the data, yielding beta estimates for each parameter in the single-subject design matrices. The contrast effects of these data were then reshaped into 3-D volume images using SPM and normalized to standard

MNI space using linear interpolation. The results of second-level, random-effects analyses via summary statistics (74) based on these estimates and effects were rendered on a standard MNI brain template. Anatomical locations of peak voxel activity were identified using NIRS-SPM. Since the present study collected data only from the ROIs, and there were no whole-brain contrasts, corrections were not applied to the results; the false-discovery rate, for example, would have been too conservative for the nature of the study.

Inter-brain synchronization (cross-brain coherence) was evaluated across dyads ($n = 30$) for the comparison of the clinical and control interpersonal interactions using the wavelet analysis approach described in Ref. 75. Wavelet analysis assesses the extent to which two or more brains (i.e., hemodynamic signals) are correlated over time (58, 76), an indirect measure of non-symmetric coupled dynamic systems (77). The wavelet function was the Complex Gaussian 2 from the MATLAB wavelet toolbox, because of its proximity to the hemodynamic response function. The number of octaves was 4 and the range of frequencies was 0.4 to 0.025 Hz. The number of octaves was also four; so, there were 16 scales for which the wavelength difference was 2.5 s. Task regressors were also removed according to PsychoPhysiological (PPI) analysis convention (78) to examine coherence that was not related to task-specific processes, but rather to dynamic coupling processes. Neural synchrony of the wavelet components of these residuals was explored also for scrambled dyads (randomly matched pairs) to control for potential effects of shared component processes that were not unique to paired participants. As with the within-brain analyses, channels were grouped into anatomical regions (i.e., 11 ROIs) based on shared anatomy for wavelet analysis. Lastly, all analyses were conducted on both HbO₂ and HbR, but the interpretation of results was based on research suggesting that HbR signals are less affected by systemic confounds (79). For example, fNIRS paradigms involving overt as well as covert

speech tasks produce changes in arterial CO₂ that, likely due to changes in respiration, alter the HbO₂ signal to a greater degree than HbR (80, 81).

Results

Contrast effects: ROIs

Within-brain statistical comparisons of ROIs that were determined *a priori* for situation and role types and the relative subtasks of these conditions were conducted at the threshold of $\alpha = .01$. Examining the effects of clinical discourse interactions compared to non-clinical interpersonal interactions [Clinical > Control], collapsed across all subtasks and roles, revealed significant differences in orbitofrontal cortex (BA11), $p < .001$, $t(28) = 2.93$, inferior frontal gyrus (BA47), $p < .001$, $t(28) = 3.08$, rostral PFC (BA10), $p < .001$, $t(28) = 3.05$, and supramarginal gyrus (BA40), $p < .001$, $t(28) = 2.64$ (Figure 3).

Figure 3

Subtracting the activation in the thinking subtask of Repeaters in the control condition from that of the thinking subtask of Clinicians in the clinical condition [Clinical thinking > Control thinking] demonstrated a significant increase in the recruitment of left rostral PFC, $p < .001$, $t(28) = 3.13$, as well as in a cluster covering right middle frontal gyrus and inferior frontal gyrus, particularly pars orbitalis, $p < .001$, $t(28) = 3.21$, and in a cluster over the subcentral area (BA43) and primary auditory cortex, $p < .001$, $t(28) = 3.18$ (Figure 4).

Figure 4

Comparing the verbal intervention subtask of Clinicians in the clinical condition against the repeating subtask of Repeaters in the control condition [Intervention > Repeating] that

occurred subsequent to the ‘thinking’ epochs showed significant—albeit less—activation in rostral PFC, $p < .001$, $t(28) = 2.91$, angular and supramarginal gyri (BA39), $p < .001$, $t(28) = 2.58$, and pre-motor and supplementary motor cortex, $p < .001$, $t(28) = 3.02$ (Figure 5). Results including cluster sizes, MNI coordinates, probability estimates, and hemispheric localizations of these contrasts are presented in Table 1-3.

Figure 5

Dynamic neural coupling

Cross-brain coherence between dyads during clinical discourse interactions [Clinical situation > Control situation] significantly increased between inferior frontal gyrus (BA44) and supramarginal gyrus, $p = .002$, $t(29) = 3.35$ (uncorrected; see Figure 6). Changes in coherence (y-axis) are plotted over 30 second periods of time (x-axis). This coherence was not observed when the partners were computationally shuffled (right panel): that is, randomly paired with every participant except the original partner, which is consistent with the idea that neural coupling is dyad-specific.

Figure 6

Discussion

This study adapted the recent approaches of multi-person neuroscience paradigms investigating aspects of verbal communication (e.g., Refs. 13, 18, 19, 22, 53, & 54) to capture human-to-human interactions that might be clinically significant. The development and application of this novel paradigm constitute a proof of principle, but the results were surprisingly consistent with the prediction that interpersonal interactions in the context of psychotherapy place unique demands on neural systems that normal verbal communication does

not. More specifically, the within- and cross-brain coherence evidence found in the clinical condition exhibited a pattern of mutual engagement of subregions along the anterior-posterior axis of the lateral surface of the cerebral cortex, particularly in the PFC and inferior parietal lobule. That the clinical condition showed greater dynamic neural coupling between pairs of participants is consistent with other observations of physiological synchronization (heart and breathing rates) between clinicians and clients (82-85), which stresses the need for a more multi-modal approach. Indeed, additional neuroimaging techniques could complement temporal and spatial resolutions and other dependent measures such as eye-gaze and facial-cues could enhance researchers' ability to index coupling between systems during clinical interactions (20, 86). One explanation for these findings is that they might derive from normative nature of the commutation; it was largely dialectical and discourse in everyday life is typically not. An additional element worth considering is the prosocial efforts on the part of the clinician to positively influence the dysfunctional information processing of the client, which could be a more specific source of influence on the strength of interactivity between individuals in these situations.

Interestingly, the within-brain findings support the role of specific PFC subregions in carrying out the task of clinicians to verbally intervene and restructure clients' dysfunctional thinking. Significant activation was observed in left rostral PFC (BA10) and right middle frontal gyrus (BA46) during the clinical thinking task, with the largest cluster being recruited in BA10 (-32, 52, 0). These results are in line with the postulation that this task largely depends on a cognitive ability (i.e., recogitation) that reasons about propositional attitudes in open-ended situations to produce changes that are conducive to well-being (1). Such an ability should place marked demands on stimulus-independent operations that support self-initiated procedures for

generating and testing novel hypotheses about linguistic propositions (40-45, 68, & 69; see Refs. 37 & 46). If this is the case, then it makes sense that such a manipulation of self-generated information would rely on sustained activation biasing in the rostral attentional gateway (67). The actual testing and rejecting of thought hypotheses are potentially mediated by dorsolateral PFC (right BA46) in checking whether semantic criteria—stored in more posterior areas such as BA39 and BA40—are satisfied; it is also possible that dorsal anterior cingulate cortex might be involved in this procedure (87). Future research might explore these possibilities.

The findings relating to periods of verbal intervention support not only the importance of the PFC but also that of more posterior subregions of the inferior parietal lobule, namely angular gyrus (BA39) and supramarginal gyrus (BA40). These two subregions comprise what is often termed Geschwind's territory in the language literature, which is an area associated with multi-sensory integration of information such as sight, sound, and body sensation, and it is thicker in humans than in other primates and one of the last areas of the brain to mature—other than rostral PFC (88); it also mediates bidirectional information processing between Broca's and Wernicke's areas via the arcuate fasciculus (89). What is unique about these regions having been recruited is that the clinicians' pattern of activation strongly reflects that which is typically found in the participants of emotion regulation paradigms, particularly ones involving cognitive reappraisal (see Refs. 90, 92, & 92, for reviews). It appears that, whilst restructuring the dysfunctional cognitive processes of others', clinicians engaged the same brain regions associated with the semantic network in modifying conceptual valuations during cognitive change strategies. In other words, clinicians are experts at using potentially the same systems at which they aim for clients to become adept. This possibility raises two interesting questions. First, would it be possible, then, to distinguish between experienced and inexperienced clinicians? Indeed, recent

research has shown interesting differences between novice and expert surgeons (93). Such an investigation in the context of psychotherapy might have implications for developing training programs. Second, could examining discrepancies in patterns of activation between healthy populations (e.g., clinicians) and clinical ones lead to insights that would inform efforts to reduce these differences (e.g., cognitive training paradigms to help clients recogitate their dysfunctional thoughts)? Changes in such functional variations might serve as reliable biomarkers for how clients respond to treatment at the level of the brain and be predictive of treatment outcome measures. These possibilities are in line with recent literature on the potential applications of multi-person neuroscience to neuropsychiatry (94, 95). In addition, within the framework of the Interactive Brain Hypothesis⁹⁵, inter-brain synchronization—or lack thereof—in clinical situations might be interpreted as a ‘dialectical misattunement’ of coupled, dynamical systems (97; see Ref. 98). Clearly, these possibilities warrant further research and there is yet much to learn from the brains of clinicians (1).

That the present sample did not consist of licensed clinicians suggests something more general about the findings, namely that the evidenced neural systems represent aspects of the normal human functions that work towards modifying propositional attitudes; clinicians are simply a population of experts at engaging these systems. Some of these functions are individually well-understood in the areas of language, social interaction, emotion regulation, and executive function, but less-well understood in their confluence towards achieving the recogitation of not only dysfunctional cognitions but also everyday thoughts people have about the world, others, and self. The present study has shown that aspects of rostral PFC, inferior and middle frontal gyri, and supramarginal and angular gyri are potentially key to this general network. The sample also did not consist of clients with real diagnoses, and so it will be

important when working with a clinical sample to assess the ways in which activation trends might differentiate from healthy participants during verbal intervention (e.g., Ref. 99). However, it is worth noting that clinicians and clients should be able to interact naturally whilst neuroimaging data are collected—without computer-mediation. To achieve this, interpersonal interactions could be fractionated in similar ways to the epochs of the present design, but with brain-first approaches to extracting the stimulus design whereby significant functional events in particular brain regions are estimated from observed HbO₂ and HbR signals (100). Portable and wireless neuroimaging devices (28) seem also to be a prerequisite to collecting data in authentic clinical settings (1). Moreover, it will be important to include additional measures of people's phenomenological experience of clinical settings in which neuroimaging data are collected to account for factors that might influence the information-processing systems of interest, such as nervousness, novelty, attitudes toward the 'therapeutic alliance', and so forth.

In sum, the practical applications of using ecological designs, tasks, and methods to investigate clinically relevant phenomena are numerous, and the findings of the present study demonstrate a precedent for the real-world neuroimaging of inter- and intra-brain systems supporting the interpersonal interactions that have long been integral to psychotherapeutic treatment. If it is the case that understanding the intervention tasks of clinicians at the levels of the brain and information processing is crucial to explaining treatment outcomes, such as improvements in emotion regulation, adaptive behavior, and functional connectivity, and also the case that these are the same or markedly similar tasks in which clinicians aim to cultivate in clients, then the recruitment the neural subsystems supporting these tasks on the part of clients might relate to their ability to identify, dispute, and modify their own affective valuations about goal-incongruent events and, therefore, to the success of downregulating negative emotion.

Future research would benefit from using a hybrid experimental design that takes advantage of the periodic measurement framework of existing designs and the continuous, *in situ* approach of the present study to investigate the neurocognitive mechanisms by which psychiatric change is achieved as a consequence of evidence-based treatments for the pathogenesis of psychopathological symptoms.

Journal Pre-proof

Acknowledgements: This research was partially supported by the National Institute of Mental Health of the National Institutes of Health under award numbers R01MH107513 (JH), R01MH119430 (JH), and R01MH111629 (JH). The content is solely the responsibility of the authors and does not necessarily represent the official views of the National Institutes of Health. All data reported in this paper are available upon request from the corresponding author. Pilot studies for this project originated from the Institute of Cognitive Neuroscience, with support from the Department of Medical Physics and Biomedical Engineering, University College London.

Conflict of Interest: The authors report no biomedical financial interests or potential conflicts of interest.

References

1. Crum, J. (2020). Future applications of real-world neuroimaging to clinical psychology. *Psychological Reports*. <https://doi.org/10.1177/0033294120926669>
2. Ehlis, A. C., Barth, B., Hudak, J., Storchak, H., Weber, L., Kimmig, A. C. S., et al. (2018). Near-infrared spectroscopy as a new tool for neurofeedback training: Applications in psychiatry and methodological considerations. *Japanese Psychological Research*. Blackwell Publishing Ltd. <https://doi.org/10.1111/jpr.12225>
3. Ehlis, A.-C., Schneider, S., Dresler, T., & Fallgatter, A. J. (2014). Application of functional near-infrared spectroscopy in psychiatry. *NeuroImage*, 85, 478–488. <https://doi.org/10.1016/j.neuroimage.2013.03.067>
4. Ho, C. S. H., Zhang, M. W. B., & Ho, R. C. M. (2016). Optical topography in psychiatry: A chip off the old block or a new look beyond the mind-brain frontiers? *Frontiers in Psychiatry*. Frontiers Media S.A. <https://doi.org/10.3389/fpsy.2016.00074>
5. Irani, F., Platek, S. M., Bunce, S., Ruocco, A. C., & Chute, D. (2007). Functional near infrared spectroscopy (fNIRS): An emerging neuroimaging technology with important applications for the study of brain disorders. *Clinical Neuropsychologist*.
6. Gross, J. J. (Ed.). (2014). *Handbook of emotion regulation* (2nd ed.). New York, NY: Guilford Press.
7. Hofmann, S. G. (Ed.). (2014). *The Wiley handbook of cognitive behavioral therapy*. Chichester, West Sussex, UK: Wiley Blackwell, a John Wiley & Sons, Ltd.

8. Crum J. (2021). Understanding mental health and cognitive restructuring with ecological neuroscience. *Front. Psychiatry*, 12:697095. DOI: 10.3389/fpsyt.2021.697095
9. Cui, X., Bray, S., Bryant, D. M., Glover, G. H., & Reiss, A. L. (2011). A quantitative comparison of NIRS and fMRI across multiple cognitive tasks. *NeuroImage*, 54(4), 2808–2821. <https://doi.org/10.1016/j.neuroimage.2010.10.069>
10. Dommer, L., Jäger, N., Scholkmann, F., Wolf, M., & Holper, L. (2012). Between-brain coherence during joint n-back task performance: A two-person functional near-infrared spectroscopy study. *Behavioural Brain Research*, 234(2), 212–222. <https://doi.org/10.1016/j.bbr.2012.06.024>
11. Duan, L., Liu, W. J., Dai, R. N., Li, R., Lu, C. M., Huang, Y. X., et al. (2013). Cross-brain neurofeedback: scientific concept and experimental platform. *PLoS ONE*, 8(5). <https://doi.org/10.1371/journal.pone.0064590>
12. Funane, T., Kiguchi, M., Atsumori, H., Sato, H., Kubota, K., & Koizumi, H. (2011). Synchronous activity of two people's prefrontal cortices during a cooperative task measured by simultaneous near-infrared spectroscopy. *Journal of Biomedical Optics*, 16(7), 077011. <https://doi.org/10.1117/1.3602853>
13. Hirsch, J., Noah, J. A., Zhang, X., Dravida, S., & Ono, Y. (2018). A cross-brain neural mechanism for human-to-human verbal communication. *Social Cognitive and Affective Neuroscience*, 13(9), 907–920. <https://doi.org/10.1093/scan/nsy070>
14. Hirsch, J., Zhang, X., Noah, J. A., & Ono, Y. (2017). Frontal temporal and parietal systems synchronize within and across brains during live eye-to-eye contact. *NeuroImage*, 157, 314–330. <https://doi.org/10.1016/j.neuroimage.2017.06.018>

15. Holper, L., Scholkmann, F., & Wolf, M. (2012). Between-brain connectivity during imitation measured by fNIRS. *NeuroImage*, 63(1), 212–222.
<https://doi.org/10.1016/j.neuroimage.2012.06.028>
16. Jiang, J., Chen, C., Dai, B., Shi, G., Ding, G., Liu, L., et al. (2015). Leader emergence through interpersonal neural synchronization. *Proceedings of the National Academy of Sciences of the United States of America*, 112(14), 4274–4279.
<https://doi.org/10.1073/pnas.1422930112>
17. Jiang, J., Dai, B., Peng, D., Zhu, C., Liu, L., & Lu, C. (2012). Neural Synchronization during Face-to-Face Communication. *Journal of Neuroscience*, 32(45), 16064–16069.
<https://doi.org/10.1523/jneurosci.2926-12.2012>
18. Liu, Y., Piazza, E.A., Simony, E., et al. (2017). Measuring speaker– listener neural coupling with functional near infrared spectroscopy. *Scientific Reports*, 7, 43293.
19. Liu, N., Mok, C., Witt, E.E., et al. (2016). Nirs-based hyperscanning reveals inter-brain neural synchronization during cooperative jenga game with face-to-face communication. *Frontiers in Human Neuroscience*, 10(82), 11.
20. Noah, J. A., Zhang, X., Dravida, S., Ono, Y., Naples, A., McPartland, J. C., et al. (2020). Real-Time Eye-to-Eye Contact is Associated with Cross-Brain Neural Coupling in Angular Gyrus. *Frontiers in Human Neuroscience*, 14.
<https://doi.org/10.3389/fnhum.2020.00019>
21. Piva, M., Zhang, X., Noah, A., Chang, S.W., Hirsch, J. (2017). Distributed neural activity patterns during human-to-human competition. *Frontiers in Human Neuroscience*, 11, 571.

22. Nozawa, T., Sasaki, Y., Sakaki, K., Yokoyama, R., & Kawashima, R. (2016). Interpersonal frontopolar neural synchronization in group communication: An exploration toward fNIRS hyperscanning of natural interactions. *NeuroImage*, *133*, 484–497.
<https://doi.org/10.1016/j.neuroimage.2016.03.059>
23. Tang, H., Mai, X., Wang, S., Zhu, C., Krueger, F., Liu, C. (2016). Interpersonal brain synchronization in the right temporo-parietal junction during face-to-face economic exchange. *Social Cognitive and Affective Neuroscience*, *11*(1), 23–32.
24. Crivelli, D., & Balconi, M. (2017). Near-infrared spectroscopy applied to complex systems and human hyperscanning networking. *Applied Sciences*, *7*(9), 922.
<https://doi.org/10.3390/app7090922>
25. Czeszumski, A., Eustergerling, S., Lang, A., Menrath, D., Gerstenberger, M., Schubert, S., et al. (2020). Hyperscanning: A valid method to study neural inter-brain underpinnings of social interaction. *Frontiers in Human Neuroscience*. Frontiers Media S.A.
<https://doi.org/10.3389/fnhum.2020.00039>
26. Redcay, E., & Schilbach, L. (2019). Using second-person neuroscience to elucidate the mechanisms of social interaction. *Nature Reviews Neuroscience*, *20*(8), 495–505.
<https://doi.org/10.1038/s41583-019-0179-4>
27. Scholkman, F., Holper, L., Wolf, U., & Wolf, M. (2013). A new methodical approach in neuroscience: assessing inter-personal brain coupling using functional near-infrared imaging (fNIRI) hyperscanning. *Frontiers in human neuroscience*, *7*, 813.
28. Pinti, P., Tachtsidis, I., Hamilton, A., Hirsch, J., Aichelburg, C., Gilbert, S., et al. (2018). The present and future use of functional near-infrared spectroscopy (fNIRS) for cognitive

- neuroscience. *Annals of the New York Academy of Sciences*.
<https://doi.org/10.1111/nyas.13948>
29. Pinti, P., Aichelburg, C., Gilbert, S., Hamilton, A., Hirsch, Burgess, W. P., et al. (2018). A review on the use of wearable functional near-infrared spectroscopy in naturalistic environments. *Japanese Psychological Research*. <https://doi: 10.1111/jpr.12206>
30. Beck, A. T. (1976). *Cognitive therapy and the emotional disorders*. New York, NY: International University Press.
31. Ellis, A. (1962). *Reason and emotion in psychotherapy*. New York, NY: Stuart.
32. Ellis, A. (1994) *Reason and emotion in psychotherapy* (Rev. ed.). Secaucus, NJ: Carol Pub, Group.
33. David, D., Lynn, S., & Ellis, A. (2010). *Rational and irrational beliefs: Research, theory, and clinical practice*. New York, NY: Oxford University Press.
34. Scherer, K. R., Schorr, A., & Johnstone, T. (Eds.). (2010). *Appraisal processes in emotion: Theory, methods, research*. New York, NY: Oxford University Press.
35. Clark A. D. (2014). Cognitive restructuring. In S. G. Hofmann (Ed.), *The Wiley handbook of cognitive behavioral therapy*, Vol 1. (pp. 23–44). Chichester, West Sussex, UK: Wiley Blackwell, a John Wiley & Sons, Ltd.
36. Crum, J. E. (2019). A clinical strategy to strengthen the connection between cognition, emotion, and behavior: From philosophical principles to psychotherapy practice. *Journal*

- of Rational-Emotive and Cognitive-Behavior Therapy*, 37(3), 241–250.
<https://doi.org/10.1007/s10942-018-0308-4>
37. Shallice, T., & Cipolotti, L. (2018). The prefrontal cortex and neurological impairments of active thought. *SSRN*. <https://doi.org/10.1146/annurev-psych-010416-044123>
38. Binder, J. R., Desai, R. H., Graves, W. W., & Conant, L. L. (2009). Where is the semantic system? A critical review and meta-analysis of 120 functional neuroimaging studies. *Cerebral Cortex*, 19(12), 2767–2796. <https://doi.org/10.1093/cercor/bhp055>
39. Cipolotti, L., Spanò, B., Healy, C., Tudor-Sfetea, C., Chan, E., White, M., et al. (2016). Inhibition processes are dissociable and lateralized in human prefrontal cortex. *Neuropsychologia*, 93, 1–12. <https://doi.org/10.1016/j.neuropsychologia.2016.09.018>
40. Goel, V., & Grafman, J. (2000). Role of the right prefrontal cortex in ill-structured planning. *Cognitive Neuropsychology*, 17(5), 415–436. <https://doi.org/10.1080/026432900410775>
41. Goel, V., Stollstorff, M., Nakic, M., Knutson, K., & Grafman, J. (2009). A role for right ventrolateral prefrontal cortex in reasoning about indeterminate relations. *Neuropsychologia*, 47(13), 2790–2797.
<https://doi.org/10.1016/j.neuropsychologia.2009.06.002>
42. Goel, V., Tierney, M., Sheesley, L., Bartolo, A., Vartanian, O., & Grafman, J. (2007). Hemispheric specialization in human prefrontal cortex for resolving certain and uncertain inferences. *Cerebral Cortex*, 17(10), 2245–2250. <https://doi.org/10.1093/cercor/bhl132>

43. Goel, V., & Vartanian, O. (2005). Dissociating the roles of right ventral lateral and dorsal lateral prefrontal cortex in generation and maintenance of hypotheses in set-shift problems. *Cerebral Cortex*, *15*(8), 1170–1177. <https://doi.org/10.1093/cercor/bhh217>
44. Robinson, G. A., Cipolotti, L., Walker, D. G., Biggs, V., Bozzali, M., & Shallice, T. (2015). Verbal suppression and strategy use: A role for the right lateral prefrontal cortex? *Brain*, *138*(4), 1084–1096. <https://doi.org/10.1093/brain/awv003>
45. Volle, E., De Lacy Costello, A., Coates, L. M., McGuire, C., Towgood, K., Gilbert, S., et al. (2012). Dissociation between verbal response initiation and suppression after prefrontal lesions. *Cerebral Cortex*, *22*(10), 2428–2440. <https://doi.org/10.1093/cercor/bhr322>
46. Shallice, T. & Cooper, R. P. (2011). *The organization of mind*. Oxford: Oxford University Press.
47. Knight, R. T., & Stuss, D. T. (2013). *Principles of frontal lobe function*. Oxford [etc.: Oxford university press.
48. Buhle, J. T., Silvers, J. A., Wage, T. D., Lopez, R., Onyemekwu, C., Kober, H., et al. (2014). Cognitive reappraisal of emotion: A meta-analysis of human neuroimaging studies. *Cerebral Cortex*, *24*(11), 2981–2990. <https://doi.org/10.1093/cercor/bht154>
49. Diekhof, E. K., Geier, K., Falkai, P., & Gruber, O. (2011). Fear is only as deep as the mind allows. *NeuroImage*, *58*(1), 275–285. <https://doi.org/10.1016/j.neuroimage.2011.05.073>
50. Kohn, N., Eickhoff, S. B., Scheller, M., Laird, A. R., Fox, P. T., & Habel, U. (2014). Neural network of cognitive emotion regulation - An ALE meta-analysis and MACM analysis. *NeuroImage*, *87*, 345–355. <https://doi.org/10.1016/j.neuroimage.2013.11.001>

51. Messina, I., Bianco, S., Sambin, M., & Viviani, R. (2015). Executive and semantic processes in reappraisal of negative stimuli: Insights from a meta-analysis of neuroimaging studies. *Frontiers in Psychology*, *6*. <https://doi.org/10.3389/fpsyg.2015.00956>
52. Braunstein, L. M., Gross, J. J., & Ochsner, K. N. (2017). Explicit and implicit emotion regulation: A multi-level framework. *Social Cognitive and Affective Neuroscience*, *12*(10), 1545–1557. <https://doi.org/10.1093/scan/nsx096>
53. Cañigueral, R., Zhang, X., Noah, J. A., Tachtsidis, I., Hamilton, A., & Hirsch, J. (2021). Facial and neural mechanisms during interactive disclosure of biographical information. *NeuroImage*, *226*, 117572.
54. Hirsch, J., Tiede, M., Zhang, X., Noah, J. A., Salama-Manteau, A., & Biriotti, M. (2021). Interpersonal agreement and disagreement during face-to-face dialogue: an fNIRS investigation. *Frontiers in human neuroscience*, *14*, 601.
55. Oldfield, R. C. (1971). The assessment and analysis of handedness: The Edinburgh inventory. *Neuropsychologia*, *9*(1), 97–113. [https://doi.org/10.1016/0028-3932\(71\)90067-4](https://doi.org/10.1016/0028-3932(71)90067-4)
56. Owen-Reece, H., Smith, M., Elwell, C. E., & Goldstone, J. C. (1999). Near infrared spectroscopy. *British Journal of Anaesthesia*, *82*(3), 418–426. <https://doi.org/10.1093/bja/82.3.418>
57. Okada, E., & Delpy, D. T. (2003). Near-infrared light propagation in an adult head model I Modeling of low-level scattering in the cerebrospinal fluid layer. *Applied Optics*, *42*(16), 2906. <https://doi.org/10.1364/ao.42.002906>

58. Cui, X., Bryant, D. M., Reiss, A. L. (2012). Nirs-based hyperscanning reveals increased interpersonal coherence in superior frontal cortex during cooperation. *Neuroimage*, 59(3), 2430–7.
59. Ochsner, K. N., & Gross, J. J. (2014). The neural bases of emotion and emotion regulation: A valuation perspective. In J. J. Gross (Ed.), *Handbook of emotion regulation* (2nd ed., pp. 23-42). New York, NY: Guilford Press.
60. Eggebrecht, A. T., Ferradal, S. L., Robichaux-Viehoever, A., Hassanpour, M. S., Dehghani, H., Snyder, A. Z., et al. (2014). Mapping distributed brain function and networks with diffuse optical tomography. *Nature Photonics*, 8(6), 448–454.
<https://doi.org/10.1038/nphoton.2014.107>
61. Eggebrecht, A. T., White, B. R., Ferradal, S. L., Chen, C., Zhan, Y., Snyder, A. Z., et al. (2012). A quantitative spatial comparison of high-density diffuse optical tomography and fMRI cortical mapping. *NeuroImage*, 61(4), 1120–1128.
<https://doi.org/10.1016/j.neuroimage.2012.01.124>
62. Ferradal, S. L., Eggebrecht, A. T., Hassanpour, M., Snyder, A. Z., & Culver, J. P. (2014). Atlas-based head modeling and spatial normalization for high-density diffuse optical tomography: In vivo validation against fMRI. *NeuroImage*, 85, 117–126.
<https://doi.org/10.1016/j.neuroimage.2013.03.069>
63. Okamoto, M., & Dan, I. (2005). Automated cortical projection of head-surface locations for transcranial functional brain mapping. *NeuroImage*, 26(1), 18–28.
<https://doi.org/10.1016/j.neuroimage.2005.01.018>

64. Singh, A. K., Okamoto, M., Dan, H., Jurcak, V., & Dan, I. (2005). Spatial registration of multichannel multi-subject fNIRS data to MNI space without MRI. *NeuroImage*, *27*(4), 842–851. <https://doi.org/10.1016/j.neuroimage.2005.05.019>
65. Mazziotta, J., Toga, A., Evans, A., Fox, P., Lancaster, J., Zilles, K., et al. (2001). A probabilistic atlas and reference system for the human brain: International Consortium for Brain Mapping (ICBM). *Philosophical Transactions of the Royal Society B: Biological Sciences*. Royal Society. <https://doi.org/10.1098/rstb.2001.0915>
66. Ye, J. C., Tak, S., Jang, K. E., Jung, J., & Jang, J. (2009). NIRS-SPM: Statistical parametric mapping for near-infrared spectroscopy. *NeuroImage*, *44*(2), 428–447. <https://doi.org/10.1016/j.neuroimage.2008.08.036>
67. Burgess, P. W., Dumontheil, I., & Gilbert, S. J. (2007). The gateway hypothesis of rostral prefrontal cortex (area 10) function. *Trends in Cognitive Sciences*, *11*(7), 290–298. <https://doi.org/10.1016/j.tics.2007.05.004>
68. Roca, M., Torralva, T., Gleichgerrcht, E., Woolgar, A., Thompson, R., Duncan, J., et al. (2011). The role of Area 10 (BA10) in human multitasking and in social cognition: A lesion study. *Neuropsychologia*, *49*(13), 3525–3531. <https://doi.org/10.1016/j.neuropsychologia.2011.09.003>
69. Seyed-Allaei, S., Avanaki, Z. N., Bahrami, B., & Shallice, T. (2017). Major thought restructuring: The roles of different prefrontal cortical regions. *Journal of Cognitive Neuroscience*, *29*(7), 1147–1161. https://doi.org/10.1162/jocn_a_01109
70. Poldrack, R. A., Mumford, J. A., & Nichols, T. (2012). *Handbook of functional MRI data analysis*. Cambridge: Cambridge University Press.

71. Tachtsidis, I., & Scholkmann, F. (2016). False positives and false negatives in functional near-infrared spectroscopy: issues, challenges, and the way forward. *Neurophotonics*, 3(3), 039801. <https://doi.org/10.1117/1.nph.3.3.039801>
72. Zhang, X., Noah, J. A., Dravida, S., & Hirsch, J. (2017). Signal processing of functional NIRS data acquired during overt speaking. *Neurophotonics*, 4(04), 1. <https://doi.org/10.1117/1.nph.4.4.041409>
73. Zhang, X., Noah, J. A., & Hirsch, J. (2016). Separation of the global and local components in functional near-infrared spectroscopy signals using principal component spatial filtering. *Neurophotonics*, 3(1), 015004. <https://doi.org/10.1117/1.nph.3.1.015004>
74. Friston, K. J., Ashburner, J., Kiebel, S., Nichols, T., & Penny, W. D. (2007). *Statistical parametric mapping: The analysis of functional brain images*. Amsterdam: Elsevier/Academic Press.
75. Zhang, X., Noah, J. A., Dravida, S., & Hirsch, J. (2020). Optimization of wavelet coherence analysis as a measure of neural synchrony during hyperscanning using functional near-infrared spectroscopy. *Neurophotonics*, 7(01), 1. <https://doi.org/10.1117/1.nph.7.1.015010>
76. Torrence, C., & Compo, G. P. (1998). A Practical Guide to Wavelet Analysis. *Bulletin of the American Meteorological Society*, 79(1), 61–78. [https://doi.org/10.1175/1520-0477\(1998\)079<0061:APGTWA>2.0.CO;2](https://doi.org/10.1175/1520-0477(1998)079<0061:APGTWA>2.0.CO;2)
77. Hasson, U., & Frith, C. D. (2016). Mirroring and beyond: Coupled dynamics as a generalized framework for modelling social interactions. *Philosophical Transactions of the Royal*

- Society B: Biological Sciences*. Royal Society of London.
<https://doi.org/10.1098/rstb.2015.0366>
78. Friston, K. J. (2011). Functional and effective connectivity: A review. *Brain Connectivity*, *1*(1), 13–36. <https://doi.org/10.1089/brain.2011.0008>
79. Dravida, S., Noah, J. A., Zhang, X., & Hirsch, J. (2017). Comparison of oxyhemoglobin and deoxyhemoglobin signal reliability with and without global mean removal for digit manipulation motor tasks. *Neurophotonics*, *5*(01), 1.
<https://doi.org/10.1117/1.nph.5.1.011006>
80. Scholkmann, F., Gerber, U., Wolf, M., & Wolf, U. (2013). End-tidal CO₂: An important parameter for a correct interpretation in functional brain studies using speech tasks. *NeuroImage*, *66*, 71–79. <https://doi.org/10.1016/j.neuroimage.2012.10.025>
81. Scholkmann, F., Wolf, M., & Wolf, U. (2013). The effect of inner speech on arterial CO₂ and cerebral hemodynamics and oxygenation: A functional NIRS study. In *Advances in Experimental Medicine and Biology* (Vol. 789, pp. 81–87). Springer New York LLC.
https://doi.org/10.1007/978-1-4614-7411-1_12
82. Palumbo, R. V., Marraccini, M. E., Weyandt, L. L., Wilder-Smith, O., McGee, H. A., Liu, S., et al. (2017). Interpersonal autonomic physiology: A systematic review of the literature. *Personality and Social Psychology Review*, *21*(2), 99–141.
<https://doi.org/10.1177/1088868316628405>
83. Tschacher, W., & Meier, D. (2019). Physiological synchrony in psychotherapy sessions. *Psychotherapy Research*. <https://doi.org/10.1080/10503307.2019.1612114>

84. Ellingsen, D. M., Isenburg, K., Jung, C., Lee, J., Gerber, J., Mawla, I., et al. (2020). Dynamic brain-to-brain concordance and behavioral mirroring as a mechanism of the patient-clinician interaction. *Science advances*, 6(43), eabc1304.
85. Anzolin, A., Isenburg, K., Grahl, A., Toppi, J., Yücel, M., Ellingsen, D. M., et al. (2020). Patient-clinician brain response during clinical encounter and pain treatment. In *2020 42nd Annual International Conference of the IEEE Engineering in Medicine & Biology Society (EMBC)* (pp. 1512-1515). IEEE.
86. Chen, P. H. A., Cheong, J. H., Jolly, E., Elhence, H., Wager, T. D., & Chang, L. J. (2019). Socially transmitted placebo effects. *Nature human behaviour*, 3(12), 1295-1305.
87. Bush, G., Vogt, B. A., Holmes, J., Dale, A. M., Greve, D., Jenike, M. A., et al. (2002). Dorsal anterior cingulate cortex: A role in reward-based decision making. *Proceedings of the National Academy of Sciences of the United States of America*, 99(1), 523–528.
<https://doi.org/10.1073/pnas.012470999>
88. Carter, R., Aldridge, S., Page, M., & Parker, S. (2019). *The human brain book*. New York, NY: DK Publishing.
89. Catani, M., & Jones, D. K. (2005). Perisylvian language networks of the human brain. *Annals of neurology*, 57(1), 8-16.
90. Ochsner, K. N., & Gross, J. J. (2005). The cognitive control of emotion. *Trends in Cognitive Sciences*. Elsevier Ltd. <https://doi.org/10.1016/j.tics.2005.03.010>

91. Ochsner, K. N., & Gross, J. J. (2008). Cognitive emotion regulation: Insights from social cognitive and affective neuroscience. *Current Directions in Psychological Science*, *17*(2), 153–158. <https://doi.org/10.1111/j.1467-8721.2008.00566.x>
92. Ochsner, K. N., Silvers, J. A., & Buhle, J. T. (2012). Functional imaging studies of emotion regulation: a synthetic review and evolving model of the cognitive control of emotion. *Annals of the New York Academy of Sciences*, *1251*(1), E1–E24. <https://doi.org/10.1111/j.1749-6632.2012.06751.x>
93. Leff, D. R., Orihuela-Espina, F., Atallah, L., Darzi, A., & Yang, G.-Z. (2007). Functional near infrared spectroscopy in novice and expert surgeons--a manifold embedding approach. *Medical Image Computing and Computer-Assisted Intervention: MICCAI ... International Conference on Medical Image Computing and Computer-Assisted Intervention*, *10*(Pt 2), 270–7. Retrieved from <http://www.ncbi.nlm.nih.gov/pubmed/18044578>
94. Schilbach, L., Timmermans, B., Reddy, V., Costall, A., Bente, G., Schlicht, T., et al. (2013). Toward a second-person neuroscience. *Behavioral and Brain Sciences*, *36*(4), 393-414. doi:10.1017/S0140525X12000660
95. Schilbach, L. (2016). Towards a second-person neuropsychiatry. *Philosophical Transactions of the Royal Society B: Biological Sciences*, *371*(1686), 20150081.
96. Di Paolo, E., & De Jaegher, H. (2012). The interactive brain hypothesis. *Frontiers in Human Neuroscience*, *6*. <https://doi.org/10.3389/fnhum.2012.00163>

97. Bolis, D., Balsters, J., Wenderoth, N., Becchio, C., & Schilbach, L. (2018). Beyond autism: Introducing the dialectical misattunement hypothesis and a bayesian account of intersubjectivity. *Psychopathology*. S. Karger AG. <https://doi.org/10.1159/000484353>
98. Hasson, U., Ghazanfar, A. A., Galantucci, B., Garrod, S., & Keysers, C. (2012). Brain-to-brain coupling: A mechanism for creating and sharing a social world. *Trends in Cognitive Sciences*. <https://doi.org/10.1016/j.tics.2011.12.007>
99. Husain, S. F., Tang, T. B., Yu, R., Tam, W. W., Tran, B., Quek, T. T., et al. (2020). Cortical haemodynamic response measured by functional near infrared spectroscopy during a verbal fluency task in patients with major depression and borderline personality disorder. *EBioMedicine*, *51*, 102586.
100. Pinti, P., Merla, A., Aichelburg, C., Lind, F., Power, S., Swingler, E., et al. (2017). A novel GLM-based method for the Automatic IDentification of functional Events (AIDE) in fNIRS data recorded in naturalistic environments. *NeuroImage*, *155*, 291–304. <https://doi.org/10.1016/j.neuroimage.2017.05.001>

Tables

Table 1

Voxel-Wise GLM Contrast Comparisons (deOxyHb signals) of Situations Type

Contrast	Coordinates ¹	t value	p	Anatomical Regions in Cluster	BA ³	Probability	Voxels
Situation [Clinical > Control]	(38, 50, -8)	2.93	0.003	Orbitofrontal Area	11	0.63	28
				Rostral Prefrontal Cortex	10	0.27	
				Inferior Frontal Gyrus	47	0.10	
	(-54, 38, -4)	3.08	0.002	Inferior Frontal Gyrus	47	0.71	24
				Inferior Frontal Gyrus	45	0.15	
	(34, 53, 4)	3.05	0.002	Rostral Prefrontal Cortex	10	0.99	29
	(-60, -52, 38)	2.64	0.005	Supramarginal Gyrus	40	0.87	10
				Angular Gyrus	39	0.13	
Situation [Control > Clinical]	(66, -22, 16)	-2.63	0.007	Primary Auditory Association Cortex	42	0.39	18
				Supramarginal Gyrus	40	0.18	
				Subcentral Area	43	0.18	
				Superior Temporal Gyrus	22	0.15	

Note. Threshold $p = 0.01$. $df = 28$. ¹Coordinates are based on the MNI system and (-) indicates left hemisphere. ² $df =$ degrees of freedom. ³BA= Brodmann's Area.

Table 2

Voxel-Wise GLM Contrast Comparisons (deOxyHb signals) of Verbal Task

Contrast	Coordinates ¹	t value	p	Anatomical Regions in Cluster	BA ³	Probability	Voxels
Intervention [Verbal Intervention > Verbal Repeating]	(-44, 52, 6)	2.91	0.003	Rostral Prefrontal Cortex	10	0.36	31
				Middle Frontal Gyrus	46	0.20	
				Inferior Frontal Gyrus	47	0.17	
	(-52, -56, 30)	2.58	0.008	Angular Gyrus	39	0.49	10
				Supramarginal Gyrus	40	0.49	
	(50, 0, 42)	3.02	0.003	Pre- and Supplementary Motor Cortex	6	0.80	326
Intervention [Verbal Repeating > Intervention]	(-66, -4, 18)	-2.92	0.003	Pre- and Supplementary Motor Cortex	6	0.36	12
				Subcentral Area	43	0.20	
				Superior Temporal Gyrus	22	0.17	

Note. Threshold $p = 0.01$. $df = 28$. ¹Coordinates are based on the MNI system and (-) indicates left hemisphere. ²df = degrees of freedom. ³BA= Brodmann's Area.

Table 3

Voxel-Wise GLM Contrast Comparisons (deOxyHb signals) of Reasoning Task

Contrast	Coordinates ¹	t value	p	Anatomical Regions in Cluster	BA ³	Probability	Voxels
Thinking [Clinical > Control]	(-32, 52, 0)	3.13	0.002	Rostral Prefrontal Cortex	10	0.97	305
				Middle Frontal Gyrus	46	0.49	58
	(46, 38, 6)	3.21	0.002	Inferior Frontal Gyrus	47	0.24	
				Inferior Frontal Gyrus	45	0.17	
				Rostral Prefrontal Cortex	10	0.11	
	(-66, -14, 18)	3.18	0.002	Primary and Auditory Association Cortex	42	0.25	188
				Subcentral Area	43	0.22	
				Superior Temporal Gyrus	22	0.14	
				Pre and Supplementary Motor Cortex	6	0.11	
Thinking [Control > Clinical]	(-52, 34, 20)	-3.17	0.002	Middle Frontal Gyrus	46	0.71	17
				Inferior Frontal Gyrus	45	0.28	
	(50, 38, 20)	-2.85	0.004	Middle Frontal Gyrus	46	0.72	13
				Middle Frontal Gyrus	9	0.17	
	(-34, 26, 34)	-3.45	0.0009	Middle Frontal Gyrus	9	0.76	57
				Frontal Eye Fields	8	0.24	
	(-64, -26, 42)	-2.80	0.005	Supramarginal Gyrus	40	0.41	10
				Primary Somatosensory Cortex	2	0.23	
				Pre and Supplementary Motor Cortex	6	0.12	
				Primary Somatosensory Cortex	1	0.11	
(-58, -12, 44)	-2.70	0.006	Pre and Supplementary Motor Cortex	6	0.59	10	
			Primary Somatosensory Cortex	3	0.18		
			Primary Somatosensory Cortex	1	0.10		

Note. Threshold $p = 0.01$. $df = 28$. ¹Coordinates are based on the MNI system and (-) indicates left hemisphere. ² $df =$ degrees of freedom. ³BA= Brodmann's Area.

Table 4

Group Median Coordinates, Anatomical Regions, and Atlas Probabilities of Channels

<i>Left Hemisphere</i>					<i>Right Hemisphere</i>				
Channel #	Coordinates	Anatomical Region	BA	Probability	Channel #	Coordinates	Anatomical Region	BA	Probability
1	-49, -44, 57	Supramarginal Gyrus	40	0.97	28	53, -48, 55	Supramarginal Gyrus	40	1
2	-45, 38, 32	Middle Frontal Gyrus	46	0.68	29	62, -38, 48	Supramarginal Gyrus	40	0.9
3	-54, 14, 38	Middle Frontal Gyrus	9	0.78	30	63, -15, 45	Pre-Motor Cortex	6	0.53
4	-58, -11, 47	Pre-Motor Cortex	6	0.7	31	60, 8, 38	Pre-Motor Cortex	6	0.46
5	-58, -36, 51	Supramarginal Gyrus	40	0.82	32	50, 33, 31	Middle Frontal Gyrus	46	0.7
6	-16, 60, 34	Middle Frontal Gyrus	9	0.54	33	61, -53, 38	Supramarginal Gyrus	40	0.96
7	-44, 48, 22	Middle Frontal Gyrus	46	0.52	34	67, -27, 40	Supramarginal Gyrus	40	0.46
8	-57, 24, 21	Inferior Frontal Gyrus	45	0.54	35	66, -4, 37	Pre-Motor Cortex	6	0.99
9	-62, -2, 35	Pre-Motor Cortex	6	0.92	36	60, 20, 25	Inferior Frontal Gyrus	45	0.42
10	-64, -25, 41	Supramarginal Gyrus	40	0.26	37	50, 43, 22	Middle Frontal Gyrus	46	0.8
11	-61, -51, 40	Supramarginal Gyrus	40	0.99	38	29, 56, 33	Middle Frontal Gyrus	9	0.6
12	-55, 32, 12	Inferior Frontal Gyrus	45	0.57	39	68, -41, 29	Supramarginal Gyrus	40	0.94
13	-63, 6, 19	Pre-Motor Cortex	6	0.5	40	70, -18, 30	Primary Somatosensory Cortex	2	0.21
14	-68, -16, 27	Subcentral Area	43	0.27	41	66, 5, 23	Pre-Motor Cortex	6	0.55
15	-67, -41, 30	Supramarginal Gyrus	40	0.96	42	59, 30, 16	Inferior Frontal Gyrus	45	0.56
16	-19, 71, 13	Rostral Prefrontal Cortex	10	1	43	65, -56, 17	Superior Temporal Gyrus	22	0.6
17	-53, 42, 1	Inferior Frontal Gyrus	47	0.53	44	71, -32, 20	Supramarginal Gyrus	40	0.42
18	-58, 17, 2	Superior Temporal Gyrus	22	0.29	45	70, -9, 18	Subcentral Area	43	0.44
19	-67, -9, 13	Subcentral Area	43	0.35	46	63, 13, 10	Inferior Frontal Gyrus	44	0.51
20	-69, -32, 18	Superior Temporal Gyrus	22	0.4	47	56, 40, 7	Middle Frontal Gyrus	46	0.52
21	-66, -55, 17	Superior Temporal Gyrus	22	0.67	48	31, 67, 12	Rostral Prefrontal Cortex	10	1
22	-32, 66, -1	Rostral Prefrontal Cortex	10	0.97	49	70, -47, 6	Superior Temporal Gyrus	22	0.63
23	-48, 49, -6	Inferior Frontal Gyrus	47	0.54	50	73, -24, 4	Superior Temporal Gyrus	22	0.45
24	-54, 27, -8	Inferior Frontal Gyrus	47	0.87	51	68, -4, -2	Middle Temporal gyrus	21	0.62
25	-66, -4, -11	Middle Temporal gyrus	21	1	52	59, 27, 1	Inferior Frontal Gyrus	47	0.62
26	-70, -24, 0	Middle Temporal gyrus	21	0.49	53	53, 47, 0	Inferior Frontal Gyrus	47	0.48
27	-69, -46, 4	Superior Temporal Gyrus	22	0.52	54	40, 63, 1	Rostral Prefrontal Cortex	10	1

Figure Legends

Figure 1. Data collection in psychotherapy. Neuroimaging and psychological methods typically collect physiological, behavioral, cognitive, and affective data *periodically*, such as pre-treatment, between treatment sessions, and post-treatment, to examine the effects of an intervention on the dependent variables of interest over time, leaving an explanatory gap regarding the potential neurocognitive mechanisms by which these effects are actuated and cultivated within treatment sessions. Adopting a more *in situ* approach that collects data within particular treatment sessions should address this issue. So, a hybrid approach of the former and latter stands the best chances of capturing the changes facilitating mental health.

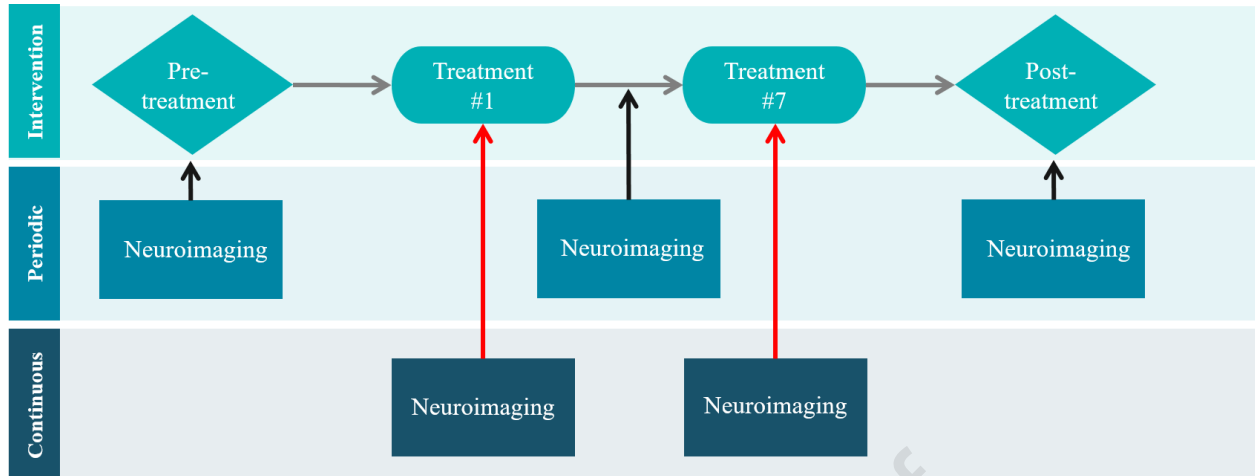
Figure 2. Epochs. In a single trial of a clinical block, the patient read a statement representing an affective valuation whilst the clinician listened. The clinician was required to first silently reason (recogitate) about how the statement was dysfunctional and, then, explain this reasoning whilst the patient listened. In a single trial of a control block, the speaker read a statement representing a descriptive proposition whilst the repeater listened. The repeater was required to first silently solve a problem relating to the language of the statement and, then, repeat the statement multiple times.

Figure 3. Clinical topic interaction. Contrast comparison of situation type [Clinical > Control] collapsed across role type and all subtasks for the ROIs ($n = 30$). Greater activation during the clinical blocks is represented in red. The clinical situation uniquely elicited right orbitofrontal cortex (BA11) and rostral PFC (BA10), and left inferior frontal gyrus (BA47) and supramarginal gyrus (BA40). See Table 1.

Figure 4. Recogitation. Contrast comparison of the thinking subtask of the clinical condition (i.e., internal reasoning about dysfunctional appraisals) [Clinical thinking > Control thinking] for the ROIs (n = 30). Greater activation during the thinking subtask of the clinical condition is represented in red. The cognitive resource demands of this type of recogitation (Crum, 2020) significantly recruited left rostral PFC (BA10), subcentral area (BA43), and primary and auditory association cortex (BA42), and right pars orbitalis (BA47) and middle frontal gyrus (BA46). See Table 3.

Figure 5. Verbal intervention. Contrast comparison of verbal intervention [Intervention > Repeating] for the ROIs (n = 30). Greater activation during verbal intervention in the clinical condition is represented in red. The cognitive resource requirements of verbal reasoning about dysfunctional appraisals significantly recruited left rostral PFC (BA10), angular gyrus (BA39), and supramarginal gyrus (BA40), and right pre-motor and supplementary motor cortex (BA6). See Table 2.

Figure 6. Neural synchronization. Coherence of brain-to-brain signals between clinical and control blocks collapsed across all roles and subtasks (n = 30). Signal coherence between dyads (y-axis) is plotted against the period (x-axis) for the clinical (red) and control (blue) conditions. Bar graphs indicate significance levels for the separations between the two conditions for each of the period values on the x-axis. The upper horizontal dashed line indicates ($p \leq 0.01$) and the lower line indicates ($p \leq 0.05$). Left panel shows coherence between actual partners and right panel shows coherence between shuffled partners. Cross-brain coherence is greatest in the clinical condition between inferior frontal gyrus and supramarginal gyrus.



Journal Pre-proof

