

1 **Machine Learning Applied to over 900 3D Printed Drug Delivery Systems**

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25 **Abstract**

26 Three-dimensional printing (3DP) is a transformative technology that is advancing
27 pharmaceutical research by producing personalized drug products. However, advances made
28 via 3DP have been slow due to the lengthy trial-and-error approach in optimization. Artificial
29 intelligence (AI) is a technology that could revolutionize pharmaceutical 3DP through
30 analyzing large datasets. Herein, literature-mined data for developing AI machine learning
31 (ML) models was used to predict key aspects of the 3DP formulation pipeline and *in vitro*
32 dissolution properties. A total of 968 formulations were mined and assessed from 114
33 articles. The ML techniques explored were able to learn and provide accuracies as high as 93%
34 for values in the filament hot melt extrusion process. In addition, ML algorithms were able to
35 use data from the composition of the formulations with additional input features to predict the
36 drug release of 3D printed formulations. The best prediction was obtained by an artificial neural
37 network that was able to predict drug release times of a formulation with a mean error of ± 24.29
38 minutes. In addition, the most important variables were revealed, which could be leveraged in
39 formulation development. Thus, it was concluded that ML proved to be a suitable approach to
40 modelling the 3D printing workflow.

41

42 **Keywords:** additive manufacturing and continuous manufacturing, personalized and precision
43 pharmaceuticals, machine learning and predictive analysis, digital health and digital
44 technologies, fused filament fabrication, drug delivery

45

46 **1 Introduction**

47 Three-dimensional printing (3DP), or additive manufacturing, is a cutting-edge fabrication
48 technology that involves the layer-by-layer fabrication of a 3D object based on a computer-
49 aided design (CAD) model [1-6]. Since the approval of the first 3D printed medicine,
50 Spritam®, 3DP has been touted as the next disruptor of the pharmaceutical manufacturing
51 industry [7, 8]. Promising bespoke medicines with precise dosing, pharmaceutical 3DP may
52 contribute to the clinical goal of precision medicines, allowing every individual to be able to
53 receive the right dose at the right time [9-14]. The growing interest in this field has led to an
54 ever-expanding number of 3DP technologies deemed suitable for fabricating tailored
55 medicines. These can be grouped based on the technique; (1) Material Extrusion, which
56 includes Fused Filament Fabrication (better known as Fused Deposition Modelling (FDM™))
57 [15-20], Semi-solid Extrusion (SSE) [21-25], and Direct Powder Extrusion (DPE) [26, 27]; (2)
58 Powder Bed Fusion, which includes Selective Laser Sintering (SLS) [28-32]; (3) VAT
59 Photopolymerization, which includes Stereolithography (SLA) [33-36]; and (4) Material
60 Jetting, which includes Inkjet Printing (IJP) [37-41]. Each of these technologies possess unique
61 features and advantages; for example, IJP is capable of printing unique patterns such as QR
62 codes that can help in the international war against counterfeit medicines [42, 43]. Amongst
63 these, FDM is the most actively explored 3DP technology in pharmaceuticals [7, 44-46].

64 FDM is a thermal material extrusion technology whose popularity is mainly attributed to
65 its affordability, versatility and compact size [7, 17, 47]. It involves processing raw
66 pharmaceutical material through hot melt extrusion (HME) to obtain long strands of filament,
67 which are subsequently fed into an FDM 3D printer [48]. The printer melts the filament and it
68 is deposited layer-by-layer onto a build plate to create a 3D object. The size and shape of the
69 object can be easily modified using software. This technology has been used within the
70 pharmaceutical arena to produce an array of drug products, ranging from printlets (3D printed
71 tablets) [49] and capsules [13], to transdermal microneedles [50], subcutaneous implants [51],
72 and other innovative drug delivery devices [52-55]. Yet, developments in pharmaceutical FDM
73 3DP has been hampered by the empirical process of formulation development. Numerous
74 parameters within this two-step process can influence the performance of the final product.
75 These include, but are not limited to, pre-HME variables (e.g. proportion of materials, object
76 design), HME variables (e.g. extrusion temperature, torque, extrusion speed), and FDM 3DP
77 variables (e.g. printing speed, printing temperature, platform temperature) [56, 57].
78 Consequently, in order to produce the desired product, researchers must undergo a process of

79 trial-and-error, slowly adjusting each parameter one at a time and evaluating the performance
80 of each prototype. Not only is this time-consuming and inefficient, it also necessitates large
81 amounts of material waste and monetary costs.

82 Therefore, to have a means of predicting the optimal parameters that will produce the 3D
83 printed object with the best performance would be desirable. Machine Learning (ML) may hold
84 the key to optimising this process [58, 59]. ML is an Artificial Intelligence (AI)-based, *state-*
85 *of-the-art* technology that enables pattern recognition from complex datasets [60-63]. Recent
86 years have seen AI receive immense and well-deserved media coverage, owing to its successes
87 in affording unparalleled insights and enhanced efficiency in numerous disciplines. For
88 instance, Google DeepMind's AI program (AlphaFold) determines the 3D shapes of proteins
89 from its amino-acid sequence, potentially saving computational biologists time and resources
90 compared to existing lab techniques such as X-ray crystallography [64]. Successful
91 applications of AI in other sectors have prompted the pharmaceutical industry to re-evaluate
92 the traditional costly and time-consuming process of bringing drugs into market [65-69].
93 Indeed, AI is a versatile and revolutionary technology that warrants consideration for
94 accelerating and transforming pharmaceutical 3DP [70].

95 We have previously reported an AI-based web application, named M3DISEEN
96 (<http://m3diseen.com>), that employs five ML techniques to enhance the efficiency of FDM
97 formulation development [71]. This software was successful at predicting four key process
98 parameters: extrusion temperature, filament mechanical characteristics, printing temperature
99 and printability. The dataset comprised a total of 614 drug-loaded formulations evaluated by
100 expert HME and FDM operators from University College London – School of Pharmacy and
101 the company FabRx, using 145 excipients and drugs. An advantage of ML is its ability to
102 improve its predictive performance as the sample size increases. Expanding the M3DISEEN
103 dataset could be achieved by conducting further experiments in-house, however, this approach
104 is time-consuming. Alternatively, a potentially more efficient strategy would be to data mine
105 FDM formulations from published studies. This strategy would also present the opportunity to
106 gather data generated by other research groups, thus minimising potential bias. In addition,
107 more information could be extracted from the literature e.g., drug dissolution results from
108 formulations.

109 As more intricate 3D designs are fabricated via FDM 3D printing, it may become more
110 difficult to gauge the drug release profile *a priori*. Thus, the ideal prediction model should
111 include this feature. Dissolution testing is a fundamental analysis in formulation development,
112 used to conclude the suitability of a drug product and for further development. As a product is

113 formulated, it is important to ensure that the drug release occurs in an appropriate manner. The
114 dissolution process may be time-consuming, particularly if the experiments are conducted over
115 weeks or months, which cannot be avoided. Due to its necessity, researchers have investigated
116 modelling techniques to predict dissolution behaviour, particularly for controlled release
117 systems [72, 73]. A mathematical description of the release profile is rather difficult, given the
118 numerous factors that will need to be considered. This is particularly true for FDM, since it
119 affords researchers the ability to produce different and intricate designs [48]. ML on the other
120 hand can utilise existing data, which is made possible by the abundance of dissolution data
121 published, to predict dissolution results of new formulations.

122 The present study reports the ML pipeline developed, using formulations mined from
123 previously published studies, to predict key HME and FDM 3D printing conditions and drug
124 dissolution properties. The key parameters predicted are extrusion temperature, filament
125 mechanical characteristics, printing temperature and printability. The work especially focussed
126 on the prediction of the drug dissolution performance of the 3D printed formulations and the
127 features that affected dissolution. This study will provide a critical analysis of the performance
128 of ML techniques for the prediction of different parameter of 3D printed formulations from
129 data obtained from the literature and the requirements of the collected data.

130

131 **2 Materials and methods**

132 **2.1 Data mining from literature**

133 PubMed, Google Scholar, and Web of Science were used to search for articles published in
134 English using the terms “hot melt extrusion”, or “fused deposition modelling”, or “fused
135 filament fabrication”, and “drug”, or “tablet”, or “capsule”, or “printlet”, or “drug device”, or
136 “printability” between Jan 1, 2013, and November 30, 2020.

137

138 **2.2 Data collection**

139 The data collection from the literature were arranged as shown in Table 1.

140 **2.2.1 Identification of the Formulation**

141 The formulations extracted from literature were identified by the article’s DOI, author ID,
142 formulation ID in the manuscript and year of publication.

143

144 **2.2.2 Composition**

145 The components and their respective weight ratio for each formulation was recorded. Any
146 formulations where the accumulative ratio did not sum to 1 (i.e. 100 w/w%) were removed
147 from the analysis.

148

Table 1. The variables used within this study

| | | | | |
|--|---|------------------------|------------------------|-----------|
| Identification of the formulation | Article DOI | DOI_1 | DOI_2 | ... DOI_n |
| | Author | Author_1 | Author_2 | Author_n |
| | Formulation ID | ID_1 | ID_2 | ... ID_n |
| Composition | Material 1 | 0.2 | 0.5 | |
| | Material 2 | 0.3 | 0 | |
| | ... | ... | ... | |
| | Material 410 | 0.1 | 0.1 | |
| Hot Melt Extrusion | Extruder (brand type) | HAAKE_MiniCTW | Noztek_Pro | |
| | Extrusion Speed (RPM) | 22.5 | 135 | |
| | Extrusion temperature (°C) | 145 | 169 | |
| | Extrusion torque (N.cm) | 15 | 15 | |
| | Filament aspect | Good | Good | |
| 3D printing | Printer (brand type) | Makerbot_Replicator_2X | Makerbot_Replicator_2X | |
| | Nozzle diameter (mm) | 0.4 | 0.4 | |
| | Printing Speed (mm/s) | 90 | 10 | |
| | Printing temperature (°C) | 210 | 200 | |
| | Platform temperature (°C) | 30 | 80 | |
| | Printability | Yes | Yes | |
| 3D printed formulation | Object | Tablet | Film | |
| | Shape | Cylinder | Square | |
| | Type of shell | 1 | 1 | |
| | Length (mm) | 10 | 20 | |
| | Width, Diameter (mm) | 10 | 20 | |
| | Depth, Thickness (mm) | 3.2 | 0.2 | |
| | Volume (mm3) | 258.97 | 80 | |
| | Surface area (mm2) | 257.61 | 816 | |
| | Surface area/volume | 0.995 | 10.2 | |
| | Weight (mg) | 181.02 | 112.8 | |
| | Layer thickness (mm) | 0.2 | 0.05 | |
| | Shell (top/bottom) (mm) | 0.2 | 0.4 | |
| | Shell (lateral) (mm) | 0.2 | 0.4 | |
| | Infill (%) | 0 | 60 | |
| | Infill type | Rectilinear | Hexagonal | |
| 3D printed product aspect | Good | Good | | |
| Dissolution test | Dissolution T20 (min) | 20 | y | |
| | Dissolution T50 (min) | 80 | y | |
| | Dissolution T80 (min) | 230 | y | |
| | pH of the dissolution media (pH) | Acid | Mixed | |
| | Volume of dissolution media (ml) | 900 | 50 | |
| | Dissolution apparatus | USP_II | bottle | |
| | Dissolution speed (RPM) | 50 | 50 | |
| Drug solubility | Drug Solubility (mg/L) | 0.1 | 0.007 | |

**"y" was used to represent information that could not be found

150 **2.2.3 Hot Melt Extrusion**

151 The HME process parameters recorded were extruder type, extrusion speed, extrusion
152 temperature (as per the temperature reported in the respective manuscripts; this may refer to
153 the nozzle temperature or maximum barrel temperature), extrusion torque, and filament
154 mechanical characteristics (good, brittle or flexible).

155

156 **2.2.4 3D Printing**

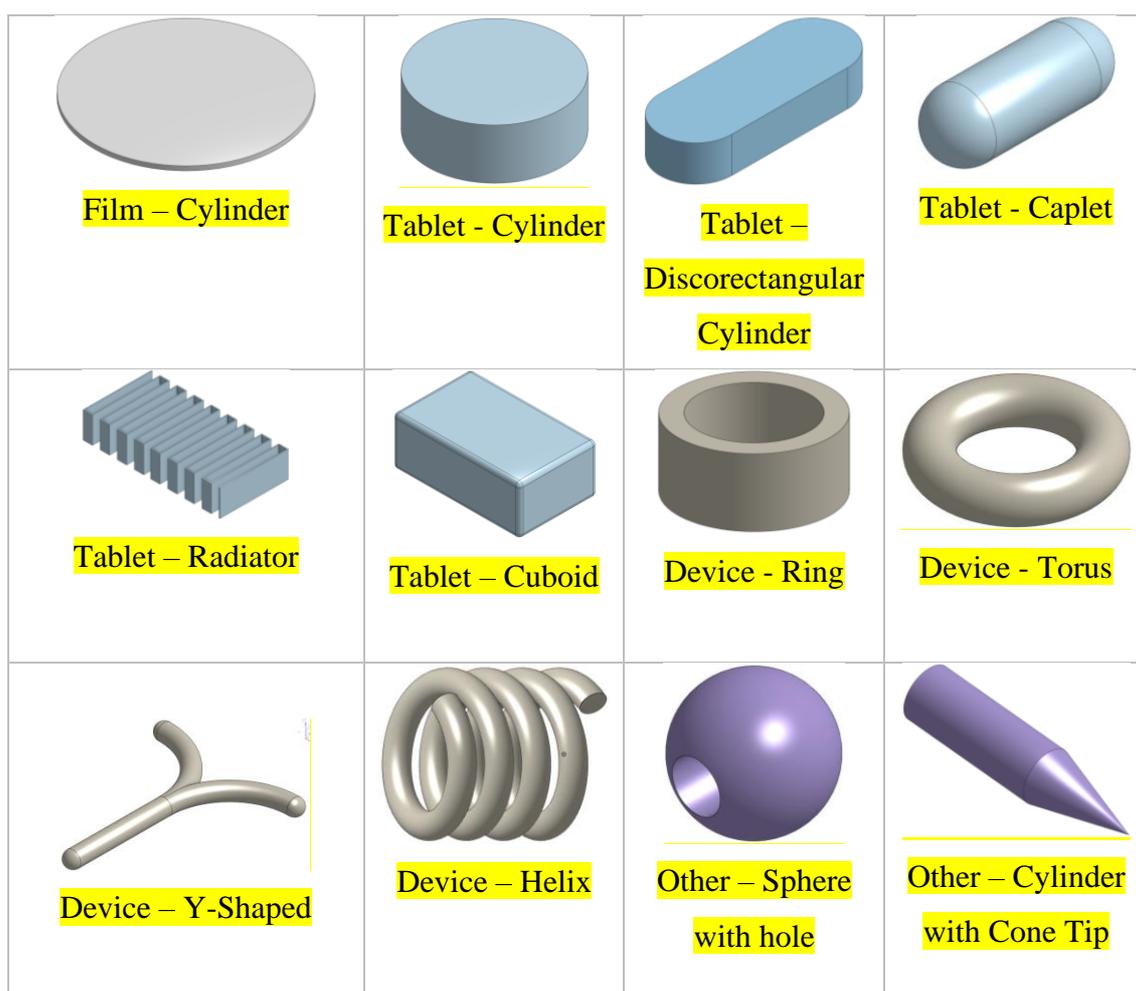
157 The FDM printing process parameters recorded were printer brand and type (e.g. direct drive),
158 nozzle diameter, printing speed, printing temperature, platform temperature, and if the
159 formulation was printable or not.

160

161 **2.2.5 3D Printed Formulations**

162 This part included the information about the object printed, shape of the object, dimensions of
163 the object (Length x Width x Height), weight, layer thickness, the type of shell, thickness of
164 the shell, and percentage infill. The printed products were classed by a feature called ‘object’
165 that refers to the type of delivery system, either a tablet, film, device or other. Since 3D printing
166 can produce complex shapes, a feature called ‘shape’ was created to detail the shape of the
167 delivery system. This feature helped to elaborate whether a film was cylindrical or square; or
168 whether a tablet was a cylinder or in the shape of a unique structure, such as a radiator [74].
169 Examples of objects and shape can be found in Figure 1.

170

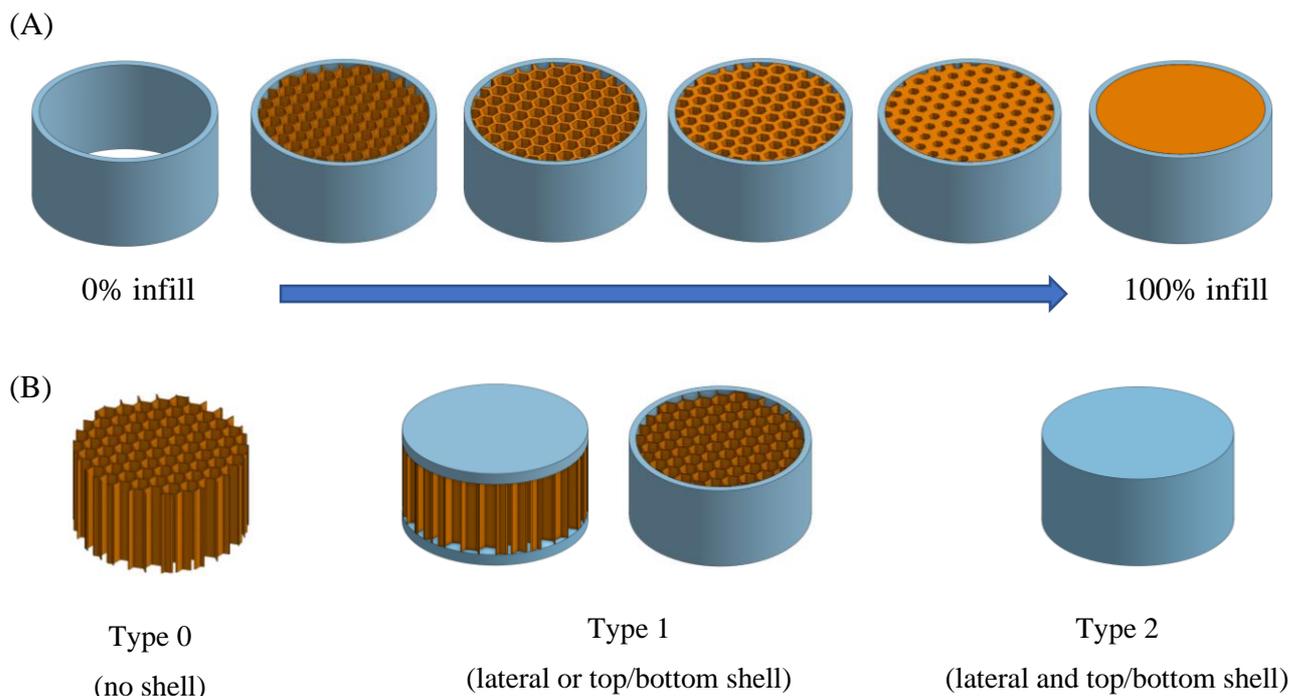


172 Figure 1. Examples of some 3D designs of objects and shapes found in the literature (object –
173 shape)

174

175 Any 3D printed object consists of an external structure called *shell* that provides the
176 shape to the object, and the internal structure called *infill* (Figure 2). The information about the
177 percentage of infill of the 3D printed object was also recorded. The information related to the
178 type of shell were represented through 3 options: “0” - no shell, “1” represented an object with
179 lateral or top/bottom shell, and “2” represented an object with lateral and top/bottom shells.
180 Cylindrical objects that were printed with 100% infill were consistently regarded as having
181 both lateral and top/bottom shells, i.e. shell type 2. The formulations that contain multiple drugs
182 or structures with different composition for the shell and the infill (e.g. 3D printed enteric
183 coating) were not taken into account for the prediction of the dissolution profiles.

184



185

186 Figure 2. Schematic representation of (A) cylinder with different infill percentage (from 0%
 187 left to 100% right) and of (B) different shell type “0” represented “with no shell”, “1”
 188 represented “with lateral or top/bottom shell”, and “2” represented “with lateral and top/bottom
 189 shells”. The composition of the shell and the infill is the same in all the analysed formulation,
 190 the different colour is for visualization purposes.

191

192 Shell thickness was extracted from the information from the articles or calculated by
 193 multiplying the thickness of the FDM extrudate by the number of shells for the lateral shell
 194 thickness; and multiplying the layer height by the number of shells for either the top or bottom
 195 shell thickness.

196 The volume and surface area were calculated using the dimensions of the object, as
 197 reported in the respective articles, and basic geometric formulas. However, for objects with
 198 complicated structures, image processing techniques in MATLAB (version R2020a,
 199 MathWorks, USA) were used to estimate their volume and surface area. Briefly, the images
 200 were first binarized according to their colour, which allowed the image of the drug product to
 201 be separated from the background. By calculating the area of the segmented image, it was
 202 possible to determine the surface area, volume and surface area to volume.

203

204 **2.2.6 Drug Solubility**

205 Drug solubility values in water were obtained from the relevant supplier datasheets or from
206 reported literature. The parameter called weighted drug solubility was calculated using the drug
207 solubility of the drug multiplied by the percentage of drug in each formulation.

208

209 **2.2.7 Dissolution Test**

210 The dissolution profiles reported in previous studies varied in scale, whereby different studies
211 measured the drug release to different time points. Instead, the time taken to reach 20% (T20),
212 50% (T50) and 80% (T80) drug release were recorded to ensure a consistent and complete
213 feature was created. As most articles reported results from drug release studies in the form of
214 graphs, an online software named Digitizer (version 4.3, Ankit Rohatgi, USA) was used to
215 determine the time at the relevant percentage drug release. Each dissolution figure was
216 uploaded to the software, which was able to determine the time points by defining the axes.
217 For sustained release formulations where the dissolution test did not reach a specific percentage
218 the time was omitted from the dataset. Other dissolution features included; volume and pH of
219 the dissolution media, type of dissolution apparatus and its speed. The pH of the dissolution
220 media was recorded in the dataset as “acid” for tests conducted in stomach pH-simulating
221 media (taken as media less than pH 4.5) and “basic” intestinal pH-simulating media (taken as
222 media more than pH 4.5). The rationale for choosing pH 4.5 as the threshold between the two
223 types of media is based on gastric pH typically ranging from 1.5 to 4.5. The dissolution studies
224 performed partially in acid media and then in basic media were recorded as “mixed” pH.

225

226 **2.2.8 General considerations**

227 Information fields that were relevant but were not reported in the article were represented using
228 “y”. Examples of such information include extrusion torque if the filament was extrudable, and
229 dissolution time if the 3D object was printable but not evaluated in dissolution tests. The
230 notation “x” was used to represent information when downstream processes were not
231 applicable, e.g. printing speed and temperature were marked “x” when the filament was not
232 extrudable.

233

234 **2.3 Predicted target variables**

235 The key parameters that the study aimed to predict were the extrusion temperature, filament
236 mechanical characteristics, printing temperature, printability, and T20, T50 and T80 (Table 2).
237 These are referred to as *targeted variables*.

Table 2. Summary of the predicted targeted variables

| Targeted variables | Values | Analysis Type |
|-------------------------------------|---|-----------------------|
| Extrusion temperature | HME temperature (°C) | Regression |
| Filament mechanical characteristics | Unextrudable, Flexible, Good or Brittle | Multi-classification |
| Printing temperature | Printing temperature (°C) | Regression |
| Printability | Yes or No | Binary Classification |
| Dissolution time (T20, T50 and T80) | Time (min) | Regression |

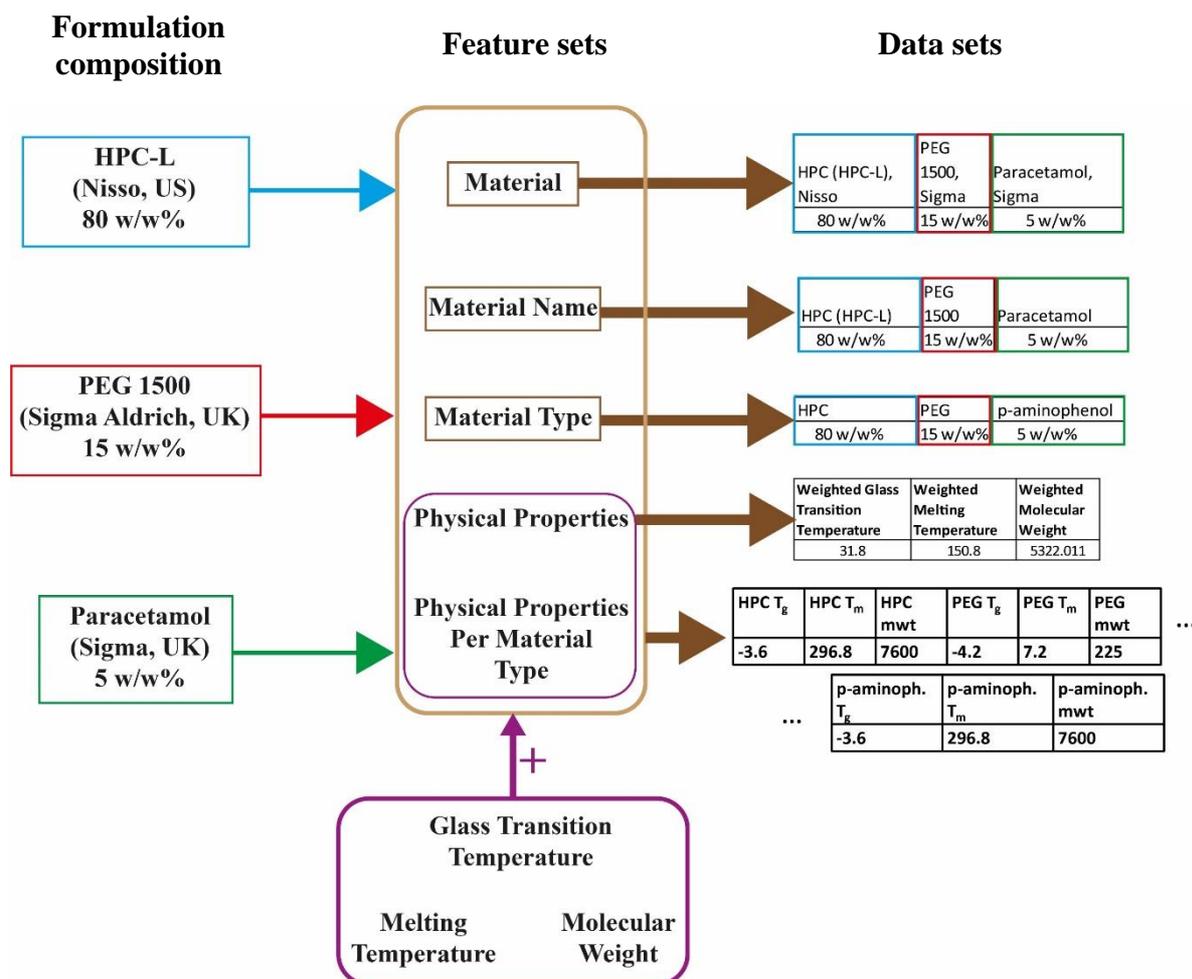
239

240 Regression analyses were used to predict the HME temperature, FDM printing
 241 temperature and dissolution time, since these target variables were continuous numerical
 242 values. Classification analyses were performed to predict the filament mechanical
 243 characteristics and printability [71], since these target variables are categorical. The labels used
 244 for filament mechanical behaviour were either ‘Good’, ‘Brittle’, ‘Flexible’ or ‘Unextrudable’
 245 based on the comments found in the reported studies. The definition of ‘Good’, ‘Flexible’,
 246 ‘Brittle’ and ‘Unextrudable’ can be found in a previous publication [71]. Printability was
 247 classified as either ‘Yes’ or ‘No’ to indicate whether the filament was printable via FDM, given
 248 the selected printing parameters. The drug release results reported in the studies varied in scale
 249 because different studies measured the drug release at different time points. For dissolution
 250 prediction, the time in minutes taken to reach 20% (T20), 50% (T50) and 80% (T80) drug
 251 release were recorded to ensure the feature was consistent.

252

253 2.4 Feature set selection and creation

254 Five feature sets used herein were *material*, *material name*, *material type*, *physical properties*
 255 *and physical properties per material type*. The feature sets were created similarly to those
 256 previously reported [71]. Briefly, material refers to the individual excipient or drug, respective
 257 of supplier, and uses the weight fraction of the material as input. Material name is the same as
 258 material, but materials from different suppliers were grouped together (Figure 3). The feature
 259 set material type groups materials by their chemical structure, whereas physical properties uses
 260 the weighted glass transition temperature, melting temperature and molecular weight as inputs.
 261 The final feature set is a combination of physical properties and material type, where the
 262 materials are grouped by their chemical structures and the input is the weighted physical
 263 properties. Schematics illustrating the creation of the feature sets are presented in Figure 3.



264

265 **Figure 3.** Schematic illustrating how materials from the formulations were classified in the
 266 different feature sets: material, material name, material type, physical properties and physical
 267 properties per material type.

268

269 2.5 Data analysis - Machine learning (ML) techniques

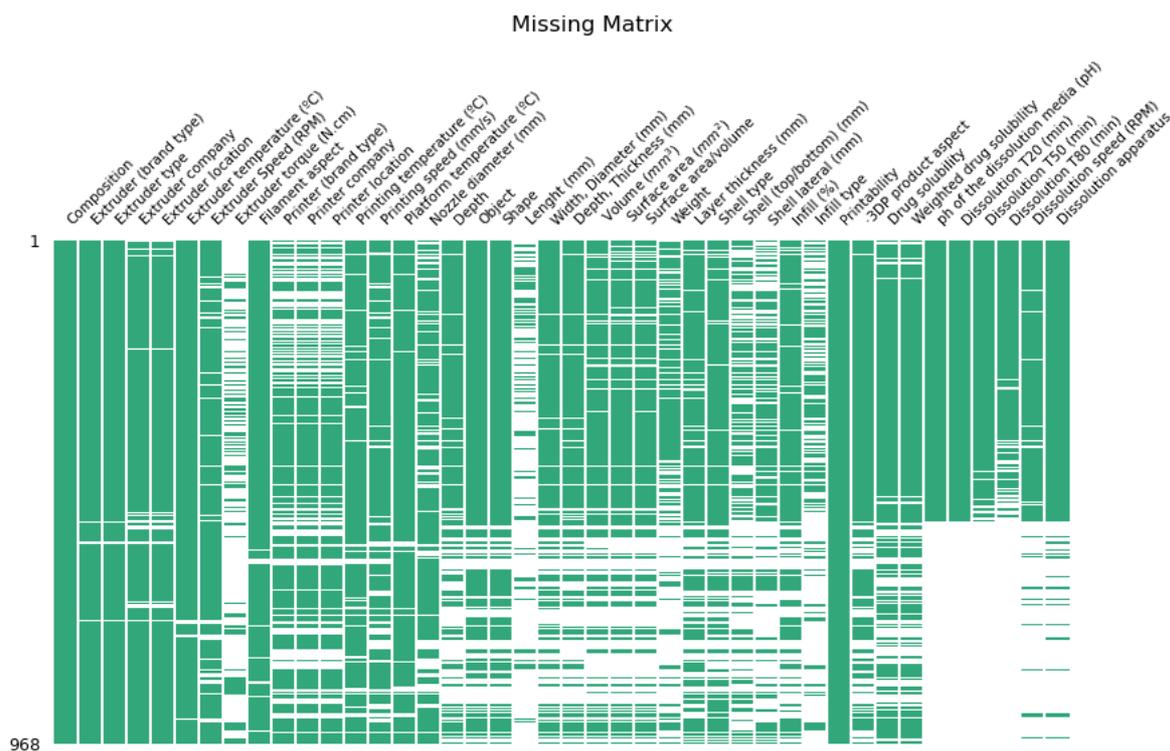
270 A standard PC (running on Operative system: Debian 5.4.19-1 x86_64) was used for the data
 271 analysis and the development of the algorithms described below (Processor: Intel® Xeon®
 272 CPU E5620 (2.40 GHz), RAM Memory: 32 GB).

273 **Five different ML techniques** were used in this study for classification tasks, which were
 274 support vector machines (SVM), random forests (RF), artificial neural networks (ANN), K-
 275 nearest neighbors (KNN) and logistic regression (LR). Different ML techniques were used
 276 since each ML technique has its own learning characteristics. Three different ML techniques
 277 were used for regression task, which were SVM, RF and ANN. Multi-linear regression and
 278 KNN were unable to result in meaningful predictions, and hence the results are not included in
 279 this study **for regression analyses**. Brief explanations of each ML technique can be found in a

280 previous study [71]. The ML techniques were developed using python 3.7 (Python Software
281 Foundation), using the Scikit-Learn package (scikit-learn package, v0.21.3). A 75:25 split was
282 used for training and testing the ML techniques.

283 For developing models to predict the dissolution time the original five feature sets
284 (Figure 3) were used, however additional features were taken into account (Table 1, sections
285 3D printed formulation, Dissolution test, Drug solubility). These features (e.g. surface area,
286 weight, infill, pH of the media) were included since they could affect the drug dissolution
287 results and could be considered dissolution-related data.

288 Predicting the dissolution profile was more demanding than, for example, predicting
289 printability or printing temperature. This was because not every literature mined 3D printed
290 formulation contained dissolution data, and hence the results had to be discarded prior to
291 performing ML. Additionally some articles may report some features (e.g. weight of the
292 formulation) but not others (e.g. infill or shell thickness), whereas ML techniques need to be
293 fed with complete dataset, without missing values. The more data fed into the ML algorithms
294 the greater their performance would be, but due to the missing values in some features, feeding
295 the algorithms with all the dissolution related features would reduce the number of rows
296 (formulations). For example, if weight, shape, pH and dissolution speed were included and
297 then any row containing any null values were removed, which resulted in a 351 formulations
298 dataset; if infill, weight and dissolution speed were selected, then this resulted in 336
299 formulations. Generally, it was observed that including more features resulted in a higher
300 percentage of missing data, and hence the smaller the size of the data set and the number of
301 formulations included (Figure 4). To avoid this situation, different combinations of input
302 features were tested and compared in terms of the ML algorithms prediction performance.



303
 304 Figure 4. Diagram representing the dataset, used to illustrate the missingness of the data for
 305 each of the 968 formulations. Green indicates information was available in the literature,
 306 whereas white areas indicates the data was missing.

307
 308 In this study each possible combination of the 12 features that can affect drug dissolution
 309 were computed (shape, type of shell, surface area/volume, weight (mg), infill (%), infill type,
 310 pH of the dissolution media (pH), volume of dissolution media (ml), dissolution apparatus,
 311 dissolution speed (RPM), drug solubility (mg/L), weighted solubility). This led to a to 2 to the
 312 power of 12 ($2^{12} = 4096$) combinations of features that were merged with the 5 feature sets that
 313 take in to account the composition of the formulations (Figure 3). We disregarded those
 314 datasets that lost more than the 40% of the original formulations and used the rest for training
 315 a ML model for each algorithm (RF, SVM and ANN). This led us to consider a total of $(2^{12}) \times$
 316 5×3 different ML experiments. Additionally, each experiment was tested in 50-fold random-
 317 split cross validation to avoid the negative impact of outliers (Figure S1). The dissolution data
 318 is spread on a considerably large scale (e.g. T20 could be either 5 min or 2000 min), where the
 319 effect of randomly splitting the data into training and testing had a pronounced effect on the
 320 results and an undesirable impact in the metrics. The ML pipeline for predicting the dissolution
 321 times is detailed and illustrated in the supplementary document (Figure S1). Categorical values
 322 (e.g. print shape) were label encoded, and numerical values (e.g. surface area, dissolution time)

323 with large ranges were quantile transformed. Label encoding is one means of vectorising
324 categorical data. Using shape features as an example, cylinder, caplets and capsules were
325 represented as 0, 1 and 2, respectively.

326

327 **2.6 Data evaluation**

328 Different metrics were used for scoring the accuracy of the ML techniques, as no single metric
329 conveys a complete picture of a model's performance. A brief explanation of each metric can
330 be found in our previous study [71]. For classification analyses, **five** classification metrics were
331 used; *accuracy*, *Cohen's kappa*, *precision*, *recall*, and *F1*. For the processing temperature and
332 dissolution time predictions, **two** regression metrics were used: the *mean absolute error*
333 (MAE), and the *coefficient of determination* (R^2).

334 An additional metric that we called RADOC (Real Area Difference Of Curves) was
335 developed for predicting the dissolution times. The metric is used to compare two "curves", in
336 a two-dimensional space, formed by the two series of points (the experimental and the
337 predicted points) respectively connected by straight lines. RADOC computes the area
338 corresponding to the absolute difference between those two curves (Figure S2 (A)). The smaller
339 this difference area, the more similar the shape of the two curves will be, leading to a more
340 fine-grained measure of the dissolution dynamics. That difference area is then relativized
341 against the area under the real curve (Figure S2 (B) and (C)) (leading to a [0%, ∞ %] error
342 range), which helped us to also address the scale problem.

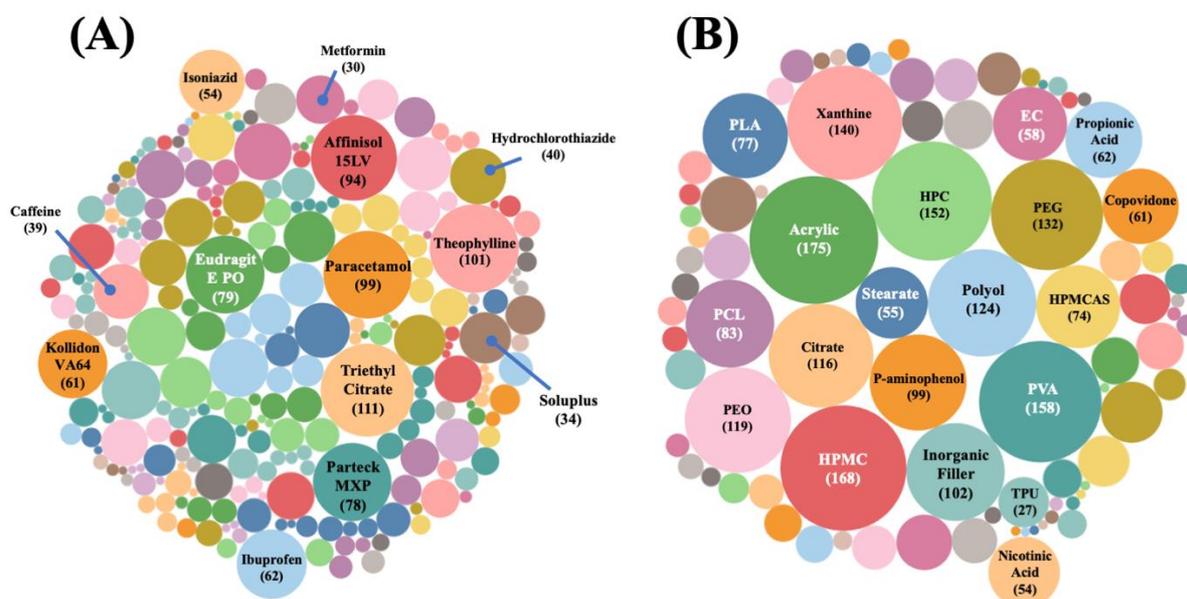
343

344 **3 Results and Discussion**

345 **3.1 Exploratory data analysis**

346 A total of 968 formulations were literature mined from 114 articles, and only formulations
347 incorporating drugs were added to the database. Information relating to the starting materials,
348 HME process, 3DP and drug dissolution was obtained, which were identified as having a
349 potential effect on the fabrication workflow and drug release profile. Figure 4 illustrates the
350 distribution of the data collected. During the data collection stage, it was clear that there was a
351 lack of data in some of the selected parameters, which could be a potential problem for the
352 machine learning (ML) algorithms. It is worth mentioning that only 57.02% of FDM articles
353 reported the drug dissolution profile of their printed product.

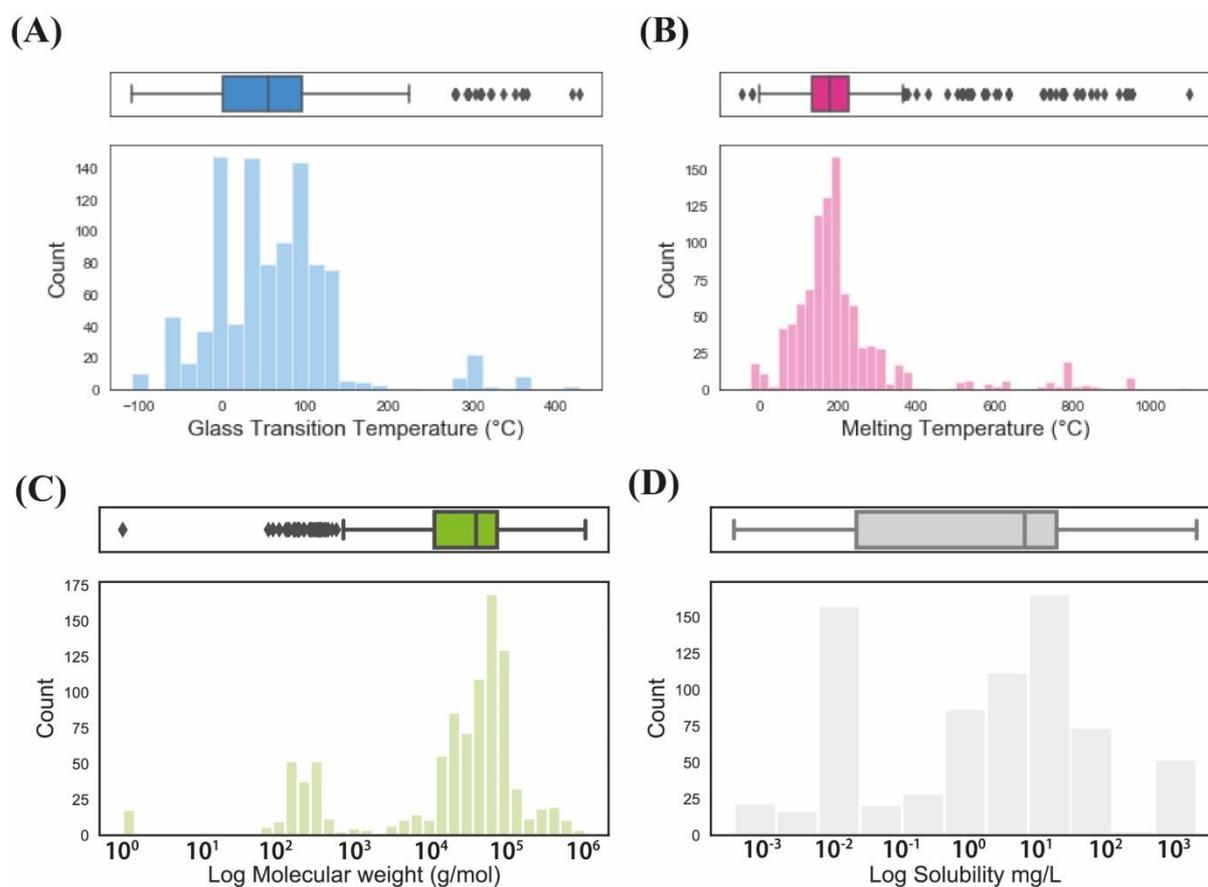
354 In total, 411 excipients and drugs were recorded from 121 different suppliers. Grouping
 355 similar materials together, irrespective of supplier, resulted in a total of 254 materials,
 356 presented as packed bubble diagrams in Figure 5, where it is evident that a large number of
 357 excipients had been used. Figure 5 (B) presents the materials when grouped by similar chemical
 358 structure. From both analyses, it appears that materials were used evenly, displaying equal
 359 distribution. The most widely used excipient type was acrylics, which was used slightly more
 360 used than HPMC and PVA. Similarly, the most used drug was theophylline, which was
 361 marginally more used than paracetamol.
 362



363
 364 **Figure 5.** Packed bubble diagrams to illustrate the distribution of (A) individual materials used
 365 and (B) material types.

366 Four different physical properties pertaining to each material were recorded in the
 367 present study. The glass transition temperatures (T_g) of the individual materials ranged from -
 368 107.65 to 1201.85°C, with the majority possessing a T_g below 200 °C (Figure 6 (A)). The
 369 melting temperatures (T_m) of the materials ranged from -76 °C to 1,974 °C, with the majority
 370 of materials possessing T_m values below 400 °C (Figure 6 (B)). The small number of outliers
 371 with high T_m and T_g values correspond to inorganic fillers, such as titanium dioxide and barium
 372 sulphate. The molecular weight of materials ranged from 58.4 to 7,000,000 g/mol (Figure
 373 6(C)). Drug solubility is also a determinant of the dissolution behaviour, and the value for each
 374 formulation was recorded, ranging from 0.0004 to 2,450 mg/L (Figure 6 (D)).

375

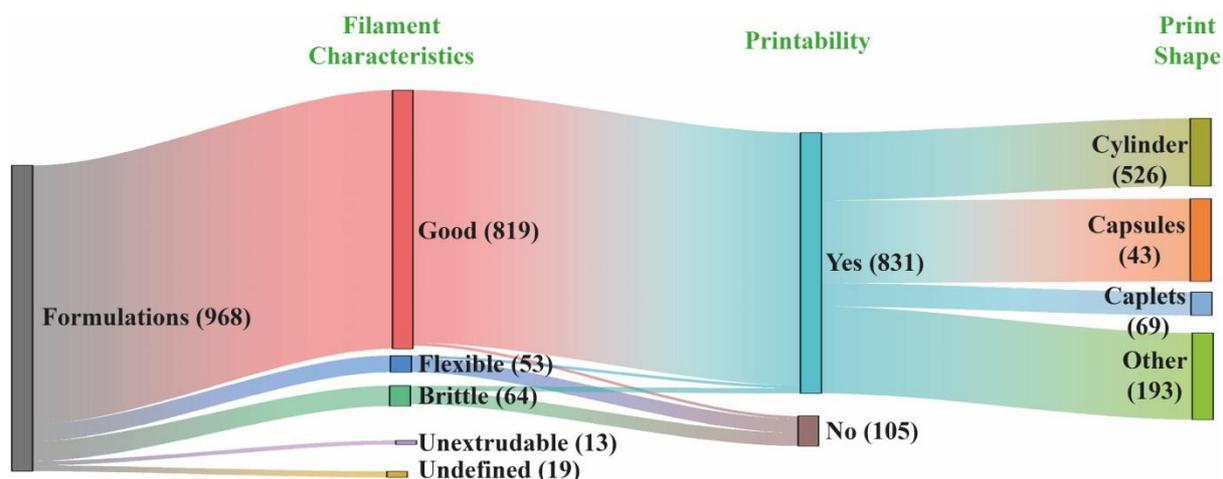


376

377

378 Figure 6. Box plot-histogram depicting the distribution of (A) glass transition temperature, (B)
 379 melting temperature, (C) molecular weight and (D) drug solubility of the formulation.

380 Exploratory data analysis of the outcome of HME revealed that 84.6% of the filaments
 381 reported in the literature were identified as ‘Good’ with respect to filament characteristics
 382 (Figure 7). These values are likely to be positively skewed, due to bias reporting wherein
 383 researchers are incentivised to only publish positive results. As illustrated by the Sankey
 384 diagram in Figure 7, the majority of ‘Good’ filaments were printable. Conversely, filaments
 385 exhibiting either ‘Flexible’ or ‘Brittle’ characteristics were found to mainly yield unprintable
 386 formulations. Nevertheless, the majority of the 968 formulations reported in the literature were
 387 printable (85.74%), which highlight again that most of the articles only report positive results.
 388



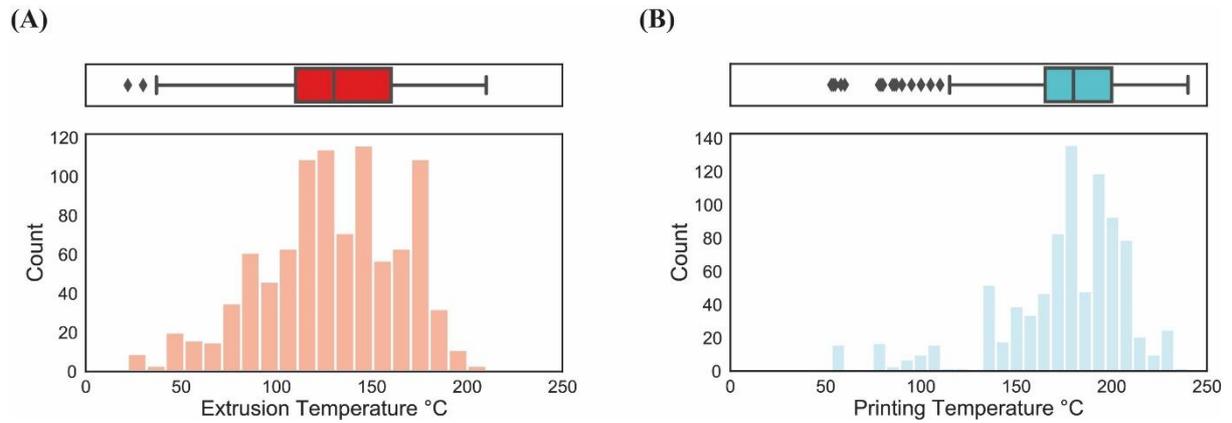
389
 390 Figure 7. Sankey diagram depicting the flow of literature-mined formulations across three
 391 different features.

392 The extrusion temperatures used in HME ranged from 22 to 210 °C, with a mean of 132
 393 °C (Figure 8 (A)). Twenty-four extruder brands were used to prepare filaments, with the
 394 Thermo Scientific Process 11 filament extruder and the HAAKE MiniCTW found to be the
 395 most used. Extrusion speeds ranged from 5 to 200 rpm. Values of torque during extrusion were
 396 reported in some articles but, due to low levels of reporting, this feature was not further
 397 analysed. The printing temperatures used in FDM 3DP ranged from 53 to 240 °C, with a mean
 398 of 174 °C (Figure 8 (B)). As evidenced by the box-plot, there are a notably larger number of
 399 outliers in the printing temperature compared to the HME temperatures. Outliers due to
 400 incorrect information can negatively impact modelling performance since the ML techniques
 401 will be making predictions based on incorrect relationships. However, these outliers, although
 402 statistically determined as outliers by the box-plot, were in fact correct values. These outliers
 403 reflect that, despite being a relatively high-temperature fabrication process (> 100 °C), a small
 404 number of studies have investigated whether certain formulations can be printed at lower
 405 temperature. Keeping the outliers in the dataset provides the potential to develop a modelling
 406 technique for low-temperature FDM processing, which will benefit researchers investigating
 407 thermally labile drugs.

408 The platform temperature is also an important feature because it can affect the
 409 adherence of the formulations to the build plate while printing. These values ranged from 16
 410 to 115 °C, with a mean of 41 °C, although in 47% studies the temperature was not controlled,
 411 and hence the value was room temperature. A total of thirty different types of printer brands
 412 were used in the studies, with Makerbot Replicator 2X and Prusa i3 3D desktop printer being

413 the most commonly used, and with nozzle diameters ranging from 0.2 to 0.5 mm (mode 0.4
414 mm). Values of Printing Speed ranged from 0.5 to 500 mm/s, with a mode of 90 mm/s.

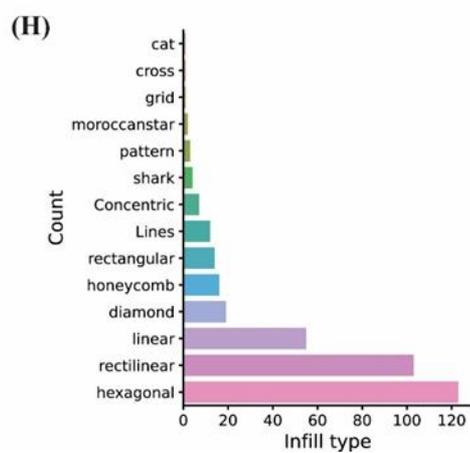
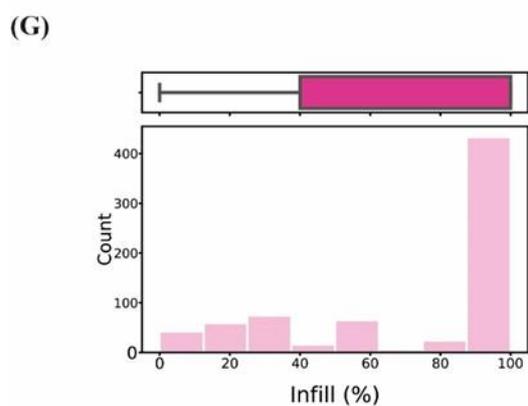
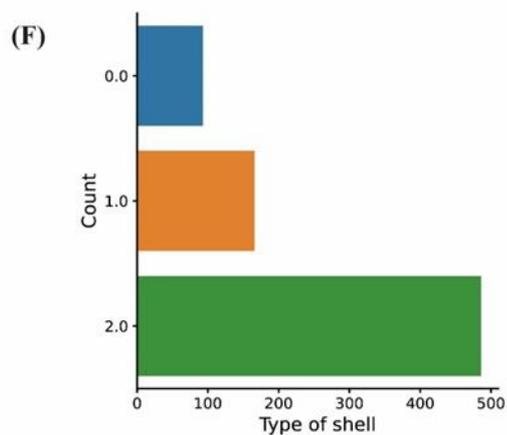
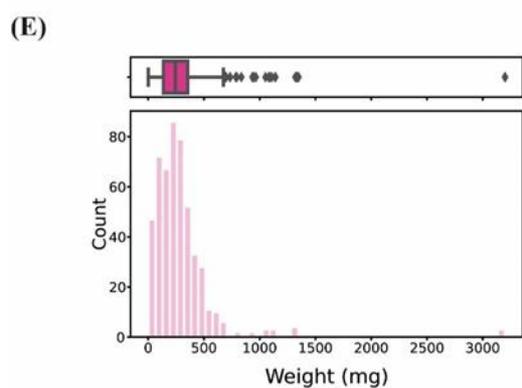
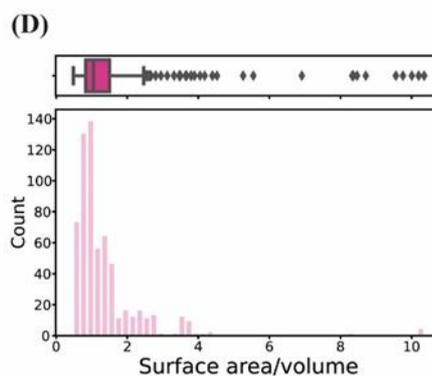
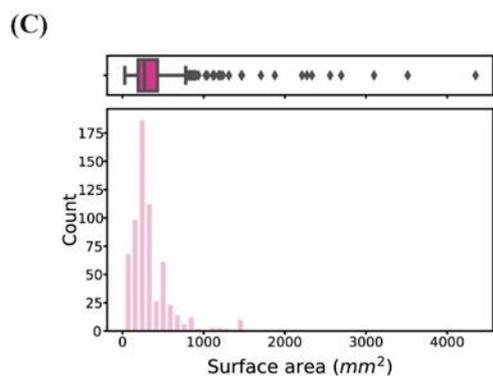
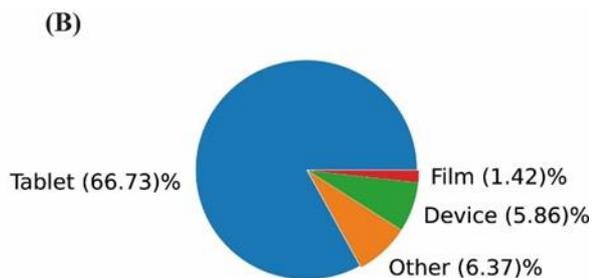
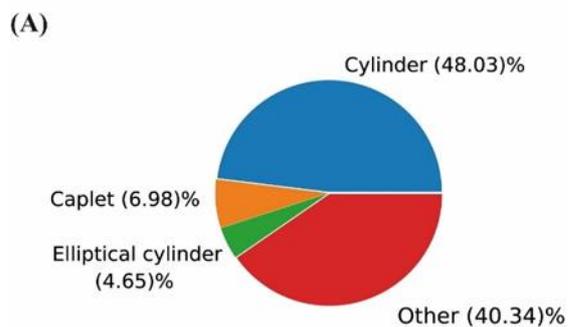
415



416

417 Figure 8. Box plot-histogram plots depicting the distribution of (A) extrusion and (B) printing
418 temperatures recorded in the dataset.

419 Regarding the 3D printed objects, FDM 3DP can be used to fabricate a range of items,
420 however the majority of objects printed were oral formulations that were encoded as “tablets”,
421 with a comparatively smaller proportion of “films” and “devices” printed (Figure 9 (A)).
422 Although 3DP can print complex geometries, most of the literature has focused on developing
423 cylinders, capsules and caplets (Figure 9 (B)). Overall, a total of 38 different shapes were
424 recorded, with the most common shape printed being a cylinder (48.03%), followed by caplets
425 (6.98%) and elliptical cylinder (4.65%).



427 Figure 9. Pie charts, box plot-histograms and bar charts illustrating the proportion of (A)
428 objects and (B) shapes printed, (C) surface area, (D) surface area to volume ratio, (E) weight,
429 (F) type of shell, (G) infill and (H) infill type.

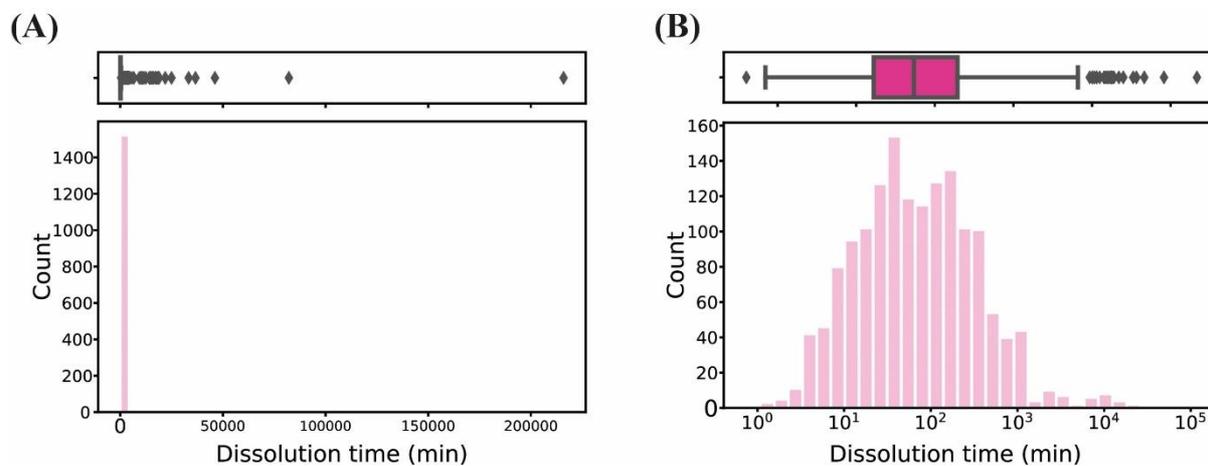
430

431 Other physical characteristics of the 3D printed objects that could be relevant due to
432 their potential effect on the drug release from the formulation were collected and analysed
433 (Figure 9). The dimension of the objects (length, width, diameter, depth) were collected and
434 were used to derive features like volume (ranged from 10.6 mm³ to 1658.8 mm³, with a mean
435 of 332.8 mm³), surface area (ranged from 26.6 to 4350.4 mm², with a mean of 384.8 mm²), and
436 surface area to volume ratio (ranged from 0.5 to 10.4, with a mean of 1.5) (Figure 9).

437 The weight of the printed object ranged from 30 to 3200 mg, with a mean of 308.5 mg
438 and the layer thickness ranged from 0.05 to 0.5 mm, with a mean of 0.18 mm. Most of these
439 objects (65.2 %) were printed with including lateral and top/bottom shells (Figure 9). Only
440 12.5 % of the objects did not include any external shell. The thickness of top/bottom shells
441 ranged from 0.05 to 2.4 mm with a mean of 0.4 mm, and thickness of the lateral shells ranged
442 from 0.1 to 2.4 mm, with a mean of 0.7 mm. A wide range of infill percentages were used
443 (from 0 to 100 %) with a mode of 100 %. Fourteen types of infills were used in the mined
444 studies, with rectilinear and hexagonal infills being the most used. Due to the missing data, the
445 feature infill type was not used for further analysis.

446 Data mining the literature allowed the extraction of the dissolution behaviour of 3D
447 printed formulations. The results revealed that 48.04% of the printable formulations were
448 analysed for their drug releasing characteristics. The distribution of times taken for the
449 formulation to reach 20%, 50% and 80% drug release are presented in Figure 10. The times
450 spanned several orders of magnitude, ranging from 0.4 min to 46,123 min (32 days). This
451 reflects the ability of FDM to be applied in a range of drug delivery systems capable of both
452 immediate and extended-drug release. However, the data is positively skewed, highlighting
453 that the majority of studies focused on release in the order of hours. Skewed data is known to
454 negatively impact ML techniques, and hence the data will need to be transformed prior to
455 modelling. Skewed data will result in ML techniques being trained on a disproportionately
456 higher number of shorter dissolution times, and will be less likely to accurately predict times
457 for larger dissolution times. Addressing this issue usually involves collecting more data to
458 balance the distribution, which is not feasible since all the published results have already been
459 collected. Alternatively, the majority class can be minimised to balance the distribution, but

460 this will come at the expense of a smaller dataset. Hence, in this instance, it is better to
461 transform the data. The log transformed data highlights that when the data is transformed it
462 results in a near-normally distributed data across several orders of magnitude (Figure 10 (B)).
463



464
465 Figure 10. Histogram and boxplot depicting (A) the distribution of time taken to reach 20%,
466 50% and 80% drug release and (B) the log transformed data. The log transformation clearly
467 illustrates the distribution of dissolution times were recorded across several orders of
468 magnitude.

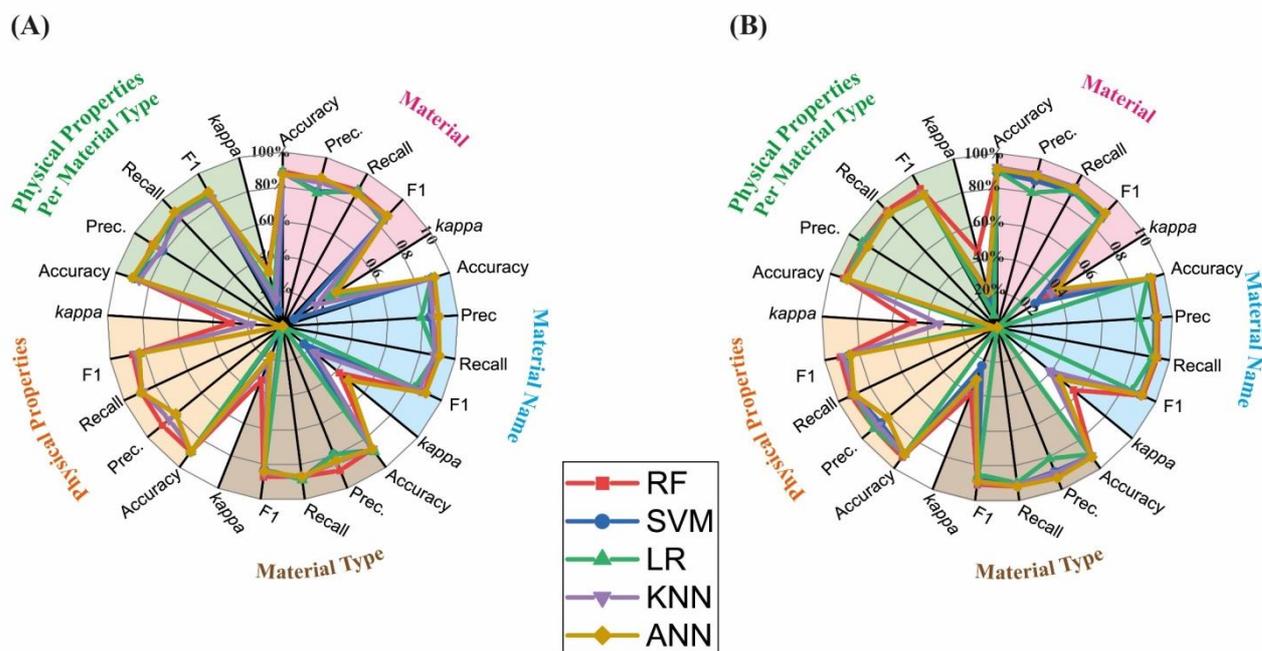
469
470 The values of other dissolution test parameters that could affect the drug dissolution
471 rate were also collected and analysed. 45.2% of the formulations were tested in simulating
472 intestinal pH condition using a “basic” dissolution media (pH media higher than pH 4.5),
473 36.5% of tests were conducted in stomach pH-simulating conditions (pH media lower than pH
474 4.5) and some studies (14.3%) evaluated the formulations first in acid and then in basic pH
475 media, simulating the transit through the GI tract (Figure S3). Some studies (3.9%), especially
476 for formulations made with materials that are pH dependent, e.g. enteric polymers, evaluated
477 the drug release of the same formulations using acid and basic pH media. The volume of
478 dissolution media ranged from 1 to 1000 mL, with a mode of 900 mL. The main type of
479 dissolution apparatus used in those studies was USP type II, and the dissolution speeds ranged
480 from 10 to 200 rpm, with a mode of 50 rpm (Figure S3).
481

482 3.2 Predictability evaluation

483 3.2.1 Predicting Filament Mechanical Characteristics

484 ML techniques were used to predict the filament characteristics using the literature dataset.
485 ANN obtained the highest accuracy of 91%, with the feature set Material Name (Figure 11
486 (A)). Similarly, this feature obtained the highest *kappa* value of 0.49.

487 For imbalanced datasets, using the accuracy as a metric to compare different datasets
488 can be misleading, particularly if one dataset has a greater imbalance. For example, the
489 literature-mined dataset contained 84.6% labelled as ‘Good’ for printability. If as prediction
490 criterion, one blindly assigned all formulations as ‘Good’, then one would trivially obtain an
491 accuracy of 84.6%. This high accuracy value may incorrectly seem a good result while, in
492 reality, the trivial ML “algorithm” would not be learning any patterns as it would just be
493 predicting the majority class for all formulations. Thus, despite the simplicity for calculating
494 the accuracy, it is more informative to use a metric that factors in a baseline value, such as the
495 *kappa* value. The *kappa* value factors in the probability of a chance agreement (i.e. random
496 guessing), and measures the predictive performance of an ML technique compared to random
497 guessing. *Kappa* values can be negative, indicating the ML technique performed worse than
498 random guessing; 0, indicating a performance comparable to random guessing; or a positive
499 value, indicating the performance was better than random guessing. From the results presented
500 in Figure 11, it can be concluded that ML techniques are able to perform better than random
501 guessing. There were some exception, primarily with using the Physical Properties feature set
502 as input, where the *kappa* value was 0 for ANN, SVM and LR. Nevertheless, from a practical
503 sense, and using the Material name feature set, ML will provide researchers with an enhanced
504 accuracy in predicting the filament characteristics compared to random guessing. The precision
505 and recall metrics are equally informative for 3DP researchers from a practical perspective.
506 These metrics reveal how well a model is able to predict the positive class (‘Good’, in the
507 current study).



509

510 Figure 11. Radar plot with the metrics result for the (A) filament mechanical characteristics
 511 and (B) printability. RF - random forests, SVM - support vector machines, LR - logistic
 512 regression, KNN - K-nearest neighbors, ANN - artificial neural networks. Please see Table S1
 513 & S2 for the specific values.

514

515 3.2.2 Predicting printability

516 The printability metrics for the literature are presented in Figure 11 (B). The feature set
 517 Material was found to produce the highest metrics, which were obtained using RF. The
 518 accuracy and kappa values were 93% and 0.56, respectively. The positive label was set to ‘Yes’
 519 for precision and recall, since there is more interest in knowing if a filament will be printable.
 520 The precision and recall values were 82% and 83%, respectively. In a practical sense, the recall
 521 value suggests that for every ten formulations, there will be 1.7 formulations that are printable
 522 but incorrectly predicted as unprintable by RF.

523 As previously mentioned, overall, the classification analyses revealed that the Material
 524 features set produced the highest metrics. This feature set possessed the largest number of
 525 features, a total of 411, and hence provided comparatively the most comprehensive information
 526 pertaining to the materials. Equally, the Physical Properties feature set comprised of only three
 527 features, which could explain why the lowest predictive accuracies were obtained with it. It
 528 should also be noted that more effective models could be developed if the dataset was more

529 balanced. However, the imbalance reflects the current state of academic publishing, which is
530 to publish mainly the positive results.

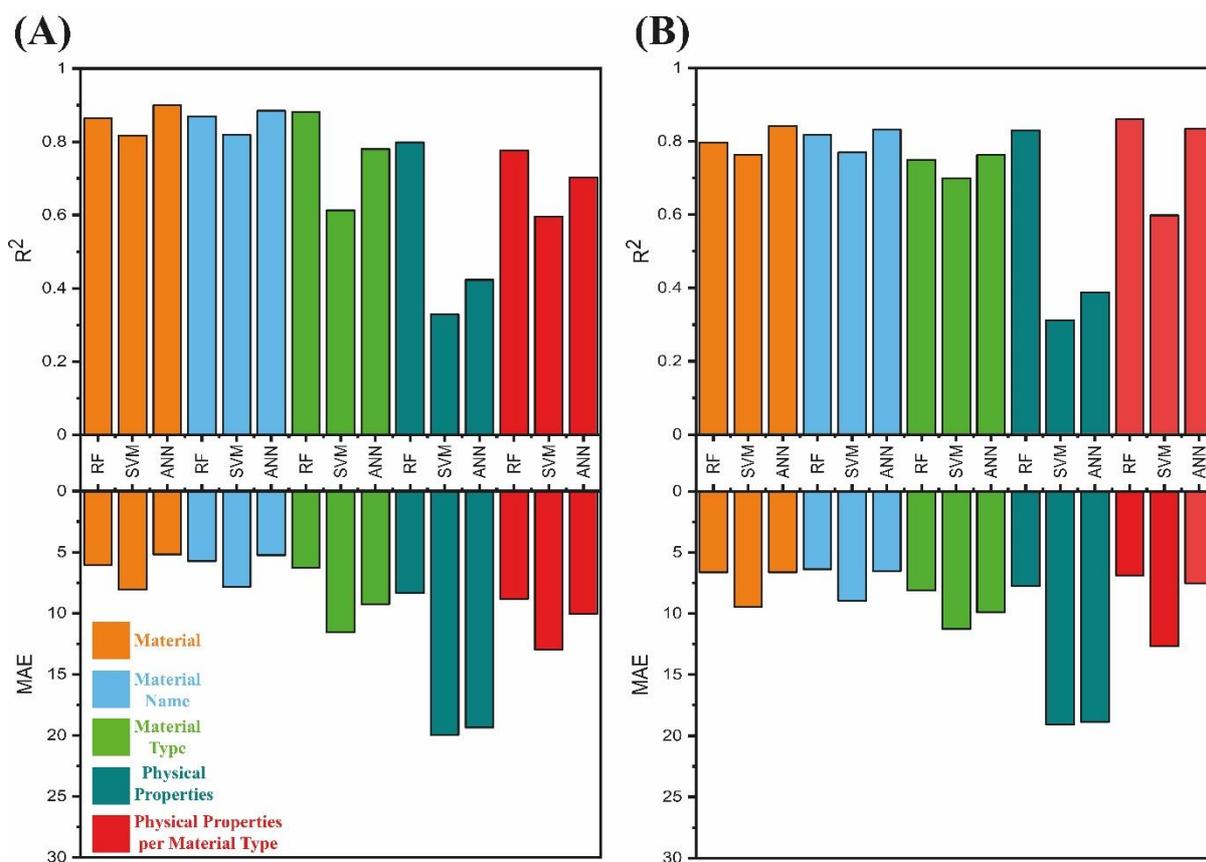
531

532 **3.2.3 Predicting extrusion temperature**

533 The extrusion temperature is a parameter difficult to anticipate, especially without prior
534 knowledge. The values are continuous, ranging from 20 to 220 °C, and thus a regression task
535 was performed to predict the individual temperature values for each formulation. The metrics
536 used were the coefficient of determination (R^2) and the mean absolute error (MAE). R^2
537 measures the variance in the data between the actual temperature and the predicted temperature,
538 with a perfect prediction resulted in an R^2 of 1.00. For more practical usage, the MAE measures
539 the absolute errors between the actual and predicted temperatures. The lower the error the more
540 accurate the prediction, with a perfect prediction producing an MAE of 0 °C. MAE is more
541 practical because a value, e.g. of 5 °C indicates that on average, the predicted temperature will
542 deviate by ± 5 °C.

543 The optimal MAE and R^2 were achieved with ANN; 5.18 °C and 0.90, respectively,
544 again using the Material feature set (Figure 12 (A)). These results were an improvement over
545 previous work, that used a smaller dataset [71], wherein the MAE and R^2 were 10.8 °C and
546 0.56, respectively. This was despite the present work possessing a wider temperature range,
547 where a larger error would have been expected to account for the wider range. The increase in
548 R^2 clearly highlights the significant improvement in the predictive performance of the present
549 study, suggesting that collecting data from the literature could be a suitable approach for
550 predictions, and is even better than generating the data in house.

551



553

554 Figure 12. The R^2 and MAE for the (A) extrusion and (B) printing temperatures for the
 555 different ML algorithms. RF - random forests, SVM - support vector machines, ANN -
 556 artificial neural networks

557

558 3.2.4 Predicting printing temperature

559 The printing temperature is an important variable that affects the printability of a formulation
 560 but predicting its value is a time-consuming approach without prior knowledge. Similar to
 561 HME, the incorrect temperature can result in nozzle blockage if the temperature is too low, or
 562 blockage caused by degradation of the polymer and the drug if the temperature is too high. To
 563 date, there is no *rule-of-thumb* or an established model for pre-determining the printing
 564 temperature, other than the assumption that the printing temperature should be higher than the
 565 extrusion temperature in the HME. The optimal MAE and R^2 were obtained by RF, which were
 566 6.87 °C and 0.86, respectively, using the Physical Properties per Material Type feature set
 567 (Figure 12 (B)). The MAE and the R^2 values were better than the values in the previous study
 568 (8.3 °C and 0.83, respectively) [71], where all the data was obtained using the same FDM 3D
 569 printer brand and generated in-house. These new results were remarkable, indicating that

570 printing temperature data obtained from the literature, published by many different research
571 groups using many different FDM printer models, were comparable or even better at predicting
572 printing temperature. Nevertheless, the MAE infers that using the literature-mined data can
573 yield an accuracy of ± 6.87 °C, which is a narrow range considering that the printing
574 temperatures attempted to date vary from 40 to 260 °C.

575

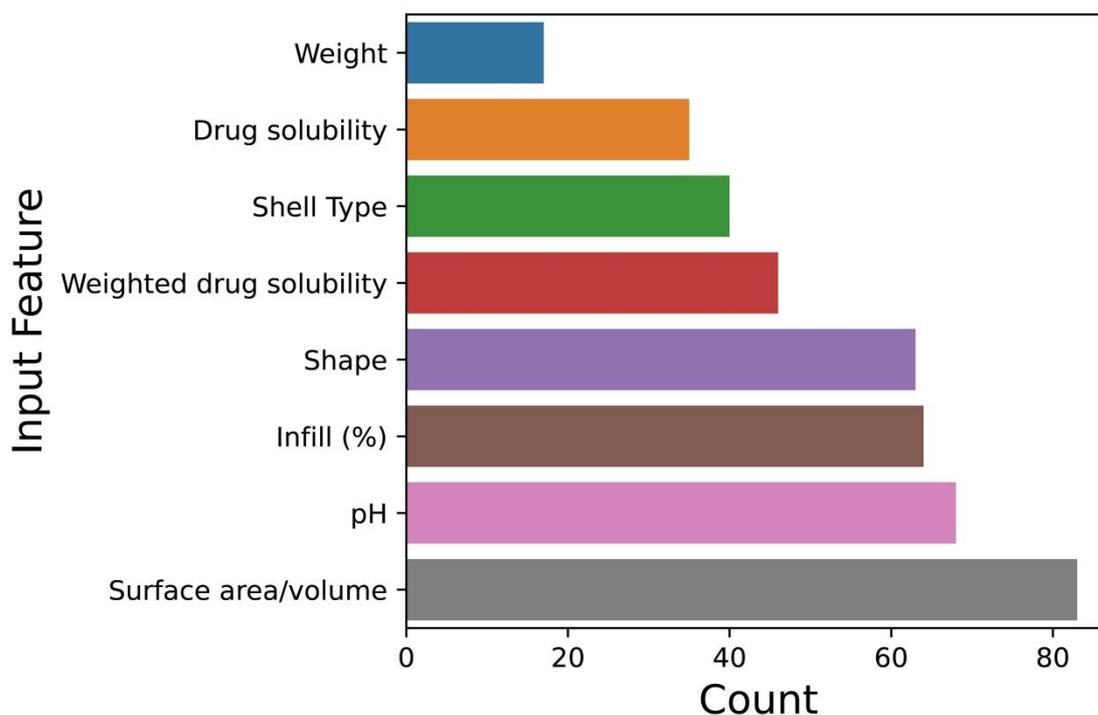
576 **3.2.5 Predicting Dissolution Behaviour**

577 The drug dissolution behaviour of the formulations is affected by more than just the material
578 components of the delivery system. The drug dissolution is influenced by design parameters of
579 the formulation, such as weight and surface area-to-volume ratio [8, 48], drug solubility [75];
580 and the dissolution conditions, such as media pH and volume. The physical characteristics of
581 the 3D printed object, the conditions of the dissolution test and the solubility of the drug were
582 therefore used as inputs for each one of the feature configurations. Hence, developing a
583 predictive model requires additional inputs to those used for modelling printability. The
584 complete list of input variables that could affect drug dissolution profiles are detailed in Table
585 1.

586 The analysis began by incorporating the new added features and finding the best
587 configuration of features to obtain the highest predictive performance. The best configurations
588 were selected based on a new metric used herein, which is referred to as RADOc, due to the
589 shortcomings of the other metrics. The pragmatism of MAE is useful since the units for this
590 metric are the same as the data under analysis. The MAE is a scale-dependent metric that
591 requires the data, including during the training-test partition, to be on the same scale. However,
592 this was not the case for predicting the dissolution time, where some partitioning exhibited
593 longer dissolution times. Due to the scale difference between T20, T50 and T80, relative
594 metrics such as R^2 or the mean absolute percentage error (MAPE) are more suitable for this
595 task. However, although a high score in those metrics would normally mean the evolution of
596 both profiles is also similar, this is not the case when having only three points (T20, T50 and
597 T80). To address this problem, when selecting the best model, the RADOc metric was used.
598 RADOc is both scale-free and capable of capturing the evolution of the graphs, and hence is
599 suitable for predicting the dissolution times (Figure S2). RADOc compares the relative
600 difference between the area under the curve for both the actual and predicted curves, where the
601 smaller the value the smaller the deviation between the two curves. This helped to determine
602 which configuration provided the best predictive performance. The training-test split

603 partitioning was performed 50 times using different random splits. This was due to the
604 incompleteness of data, whereby certain formulations would be missing values for particular
605 features (Figure 4). As a result, the same random split could not be achieved for each
606 configuration, which made it difficult to determine the true optimal configuration. Performing
607 the analysis 50 times with varying random splits provided a more holistic determination of the
608 optimal configuration. Again, the RADOC metric proved to be useful when comparing the
609 optimal configuration due to the variability in random splitting.

610 The features that were the most occurring in the best 100 analyses, in terms of
611 producing the lowest RADOC value, are presented in Figure 13. The main features used in the
612 best analyses were, in descending order, Surface area-to-volume ratio, pH, infill, shape,
613 weighted drug solubility, shell type, drug solubility and weight. The mean RADOC for the best
614 100 analyses was 48.01 and a standard deviation of 12.37.



615
616 Figure 13. Histogram depicting the feature importance. The count number indicates the number
617 of times a feature was used in the best 100 analysis.

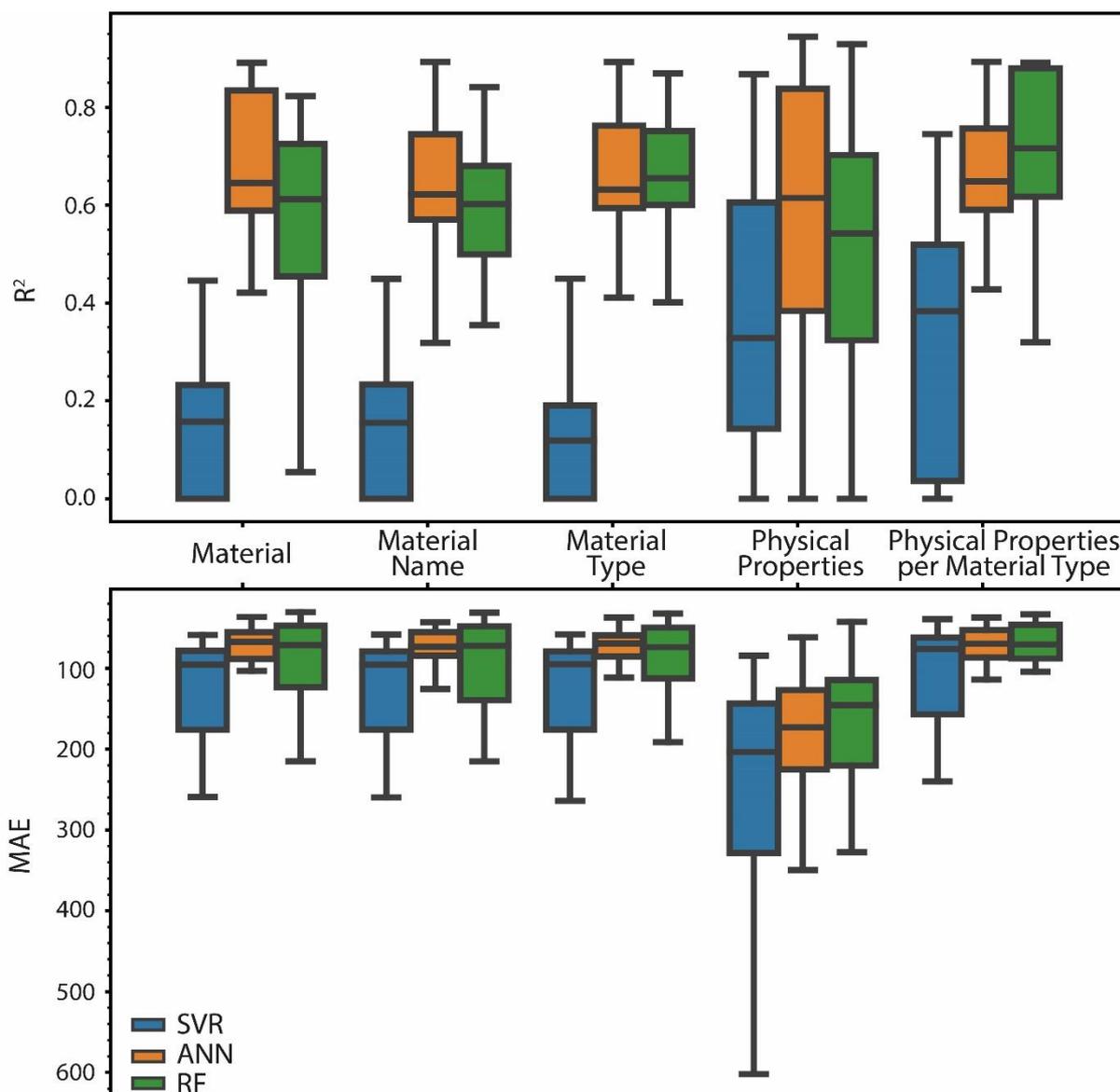
618
619 The feature surface area-to-volume ratio was identified as the most important feature
620 and was used in more than 80 of the best predictions. The feature was already identified as a
621 relevant parameter to control dissolution of 3D printed formulations in one of the first studies

622 in 2015 [48]. This feature is also related to the shape of the 3D printed object that was also
623 identified as a relevant feature, used in more than 60 on the best 100 predictions.

624 The pH of the media is the second most relevant parameter that needs to be controlled
625 when performing the dissolution test. The pH is not a characteristic of the 3DP formulation but
626 the dissolution media. The pH is included in more than 65 of the best 100 predictions. It is
627 important because some materials used to prepare 3D printer medicines show different
628 properties or solubility in different pH. The best example of this is the enteric polymers that do
629 not dissolve at pH acid (lower than 4.5) but disintegrate/dissolve when the pH is close to 5.
630 Dissolution studies performed in acidic media are typically for immediate release formulations,
631 so the selection of the pH of the media is partially linked to the type of formulations that are
632 evaluated in the dissolution test too.

633 The infill percentage of the formulations is the third most important feature and was
634 also identified as a relevant in previous studies [76, 77]. Higher infill percentage is associated
635 with longer dissolution times. Other important features are solubility and weighted solubility
636 of the drug used in 45 and 35 of the 100 best predictions, respectively. Higher solubility of the
637 drug leads to faster dissolution. The shell type is a feature that affect the dissolution and it is
638 related to the surface area-to-volume ratio feature; formulations without external shells tend to
639 release the drug faster due to easier penetration of dissolution media to the inner part of the
640 formulations. Moreover, the weight of the formulations also affects the dissolution process,
641 and in some cases higher weight leads to longer dissolution times.

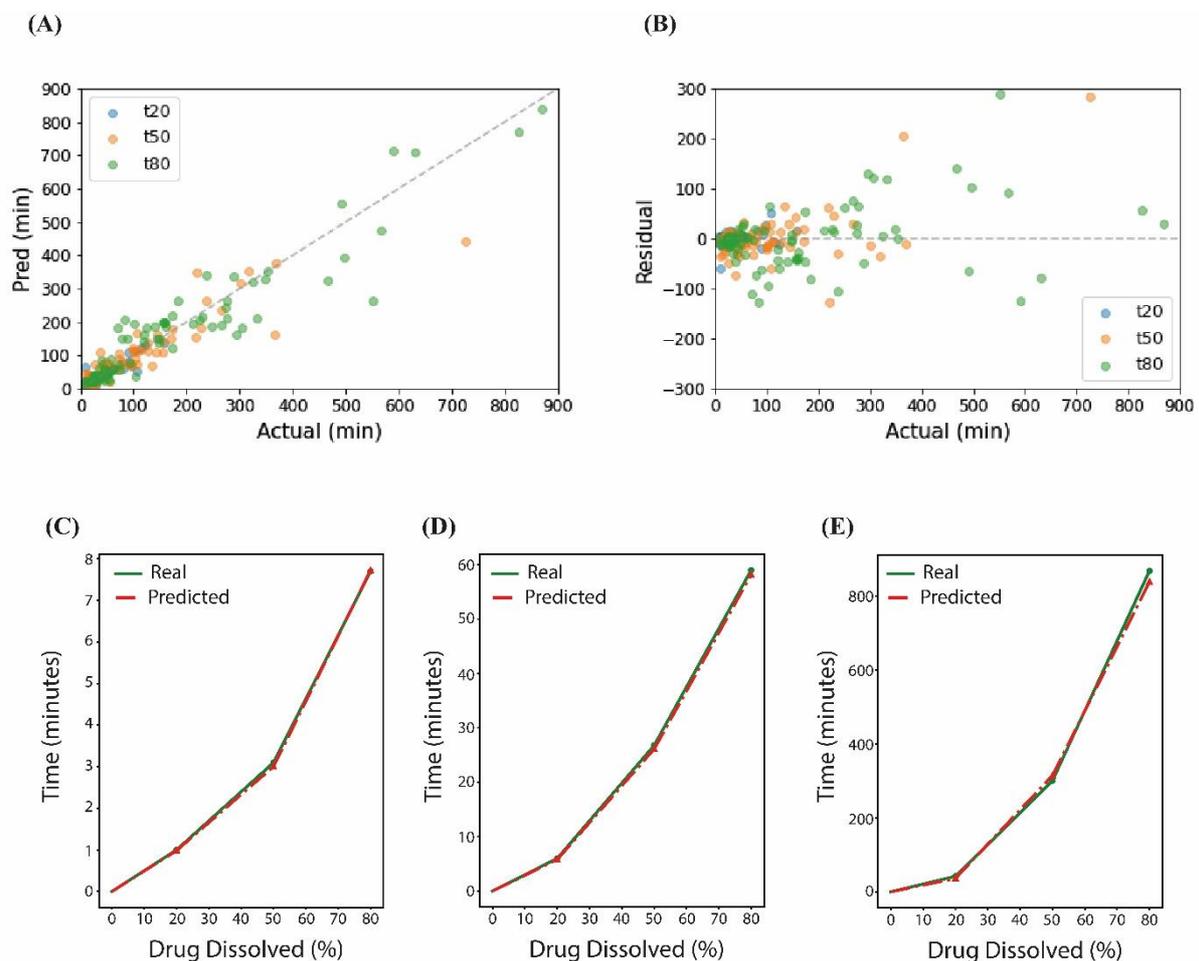
642 The incorporation of the additional feature inputs resulted in a good predictive
643 performance. The results from the 50-fold random split, for each feature set and algorithms are
644 presented in Figure 14. It was evident that the selected random split and configuration can
645 affect the predictive performance of the MLTs. For example, if the test split contained higher
646 dissolution times, then this was found to increase the error rate. The best prediction was
647 obtained by an ANN algorithm that used the material feature set combined with the surface
648 area-to-volume ratio, volume dissolution media, weighted solubility shape and pH of the media
649 as additional input features. Although each of the inputs gathered in (Table 1) were considered
650 important variables by the authors of this study prior to the ML analyses, they were not all used
651 by the ML algorithms. The ANN algorithm achieved an MAE of 24.29 minutes and a R^2 of
652 0.86 in the test set, which means that on average it is able to predict the dissolution times (T20,
653 T50 and T80) of a formulation with an error of ± 24.29 minutes. This is remarkable considering
654 that some of the dissolution tests run for days.



655
 656 Figure 14. R^2 and mean absolute error results of the 50-fold random split for each of the MLTs,
 657 and across the different feature sets for predicting drug dissolution profiles. The results
 658 demonstrate that the random split can affect the results of the MLTs, due to the wide range in
 659 dissolution times. RF - random forests, SVM - support vector machines, ANN - artificial neural
 660 networks.

661
 662 Figure 15 illustrate the prediction vs actual results from the best performing model. The
 663 MAE is an average of the absolute errors and thus influenced by large errors which, as
 664 expected, were obtained from sustained release data. This was evidenced when examining both
 665 the scatter plot and residual plot (Figure 15(A & B)). The residual plot (Figure 15 (B)) revealed
 666 a common trend, whereby an increase in residuals is observed as the actual dissolution time
 667 increases, with the exception of a few anomalies. Figure 15 (C-E) presents examples of three

668 different release studies, illustrating that ML techniques were able to produce accurate
669 simulations of the released drug, thereby confirming the models suitability for both immediate
670 and sustained release. Figure 15 (C-E) also demonstrated that the ML techniques were able to
671 learn the trajectory of the dissolution profile insofar as learning that the concentration of drug
672 release increases over time. A benefit of ML is that multiple predictions can be made from the
673 same data point (i.e. formulation). This was leveraged in the present study by investigating
674 whether the three time points could be predicted simultaneously, rather than developing
675 separate models for each time point, which is a faster approach to model development. This
676 feature was not coded into the ML techniques, and hence all three ML techniques were able to
677 independently learn the graph trajectory.
678



679
680
681 Figure 15. (A) Scatter plot illustrating the actual vs. predicted scatter plots, and (B) the
682 corresponding residual plot of the best performing ML technique. (C-E) Are three
683 representative actual vs predicted dissolution profiles, across three different time scales (8, 60
684 and 850 min).

685

686 The predictive performance of the ML strategy applied herein were considered
687 satisfactory. Considering that dissolution studies are performed from days to weeks, an MAE
688 in the order of minutes will indeed prove to be an asset to researchers. Previous work using
689 ML to predict the dissolution profile of 3D printed products has demonstrated that high
690 accuracies can be attained using ML [78, 79]. However, a current limitation of the previous
691 work for predicting dissolution profiles was that the formulations were developed in-house and
692 limited to one drug. In contrast, the model developed herein offers prediction to a larger
693 material pool. Moreover, the information was gathered from different researchers, making it
694 less susceptible to bias and thus providing greater generalisability for making new predictions.
695

696 **3.2.6 General consideration**

697 This study integrated data from articles published by researchers all over the world, with
698 different materials, methodologies and objectives, which produced ML models that were
699 successfully able to generalize for predicting the targeted variables (extrusion temperature,
700 filament mechanical characteristics, printing temperature, printability and drug dissolution
701 performance). Even though the same MLTs were used as in the previous study, higher
702 predictive performances were obtained in this study, particularly with the HME and FDM
703 temperatures [71]. This was expected as the current study consisted of more formulations. It is
704 also worth acknowledging that in the previous study it took six years to achieve an in-house
705 dataset of 614 formulations, whereas in the same time period 968 formulations were published
706 – an increase of 58% in data – highlighting the fast data generation nature of literature mining.
707 While the data used in the previous study was very straightforward to use, it was somewhat
708 limited, since the data was obtained from the same laboratory and using the same equipment,
709 work methodology and objectives.

710 Although the findings of the present study provided additional benefits to the previous
711 study in modelling key aspects of the 3DP workflow [71], the integration of the literature-
712 mined data presented several challenges. One salient disadvantage is that the data is not
713 structured and hence it is not machine-learning compatible, requiring an exhaustive and time-
714 consuming pre-processing step to collect and structure the data. For example, for unifying
715 dissolution time in different scales (immediate release, long-term release, etc), the authors had
716 to collect the data as “time to reach a certain percentage of release” rather than “percentage of
717 drug released after a certain time”.

718 The literature data is biased towards positive results which may have reduced the
719 learning performance of the ML techniques in predicting printability. Most researchers only
720 publish the good results in their studies. Even though there are some unsuccessful formulations
721 in the articles, the information is limited. As a result, most information about the filament
722 aspect and printability is positive, which causes a deficiency of negative examples and this is
723 not ideal for training ML algorithms, as they tend to learn the majority class. In addition, part
724 of the data in this study was estimated by using relevant software. Although estimation is a
725 common data generation technique, it may have contributed and additional error in some of the
726 data, and consequently may have reduced the accuracy of the prediction.

727 Finally, different articles missed different features when presenting data. For the ML
728 algorithms to work, rows containing null values (i.e. missing) must be removed from both
729 training and test sets, which is known to negatively impact the accuracy of ML algorithms due
730 to fewer learning instances. In addition, removing these null values forced additional pre-
731 processing workload to the ML pipeline. If the literature data was more complete then a simpler
732 pre-processing methodology could have been used, and potentially better results could be
733 achieved for drug dissolution prediction. To assist in developing more effective ML models,
734 the authors of this study encourage other authors in the field to publish complete data including
735 both positive and negative results. All the articles should provide the sufficient information
736 even if the data may not be relevant for the specific aim of the study. Ideally, standards on
737 which data and how it should be reported would avoid some of the problems encountered in
738 this study regarding missing information. The minimum parameters that we consider should
739 be published are included in Table 1, although additional data could be useful for future studies.
740 The features selected herein are known determinants of the target variables. The research in
741 3DP of pharmaceuticals remains nascent, and as the research develops more information will
742 come to light. This could potentially lead to an improved feature selection, enabling ML
743 techniques to attain a higher accuracy.

744 Current ML algorithms have the potential to overcome some of the challenges that the
745 field of 3DP of pharmaceuticals faces, including the optimization of the fabrication parameters,
746 reducing the inefficient empirical trial approach, and the requirements of expert knowledge.
747 The performance of the AI tools is expected to drastically improve in the following years,
748 however, one of the main needs of these algorithms to exploit its full potential is Big Data,
749 which means having data with several orders of magnitude of cardinality bigger than the data
750 set used for this study. While in other fields ML is applied to massive amounts of automatically

751 generated historical data, the application of ML to 3DP of medicines is based on experimental
752 data. This data requires big investment in time and resources as well as human intervention to
753 be generated and reviewed. The optimal amount of data will only be achieved via an open
754 sharing and collaboration-based program. Even if one institution or company were capable of
755 reaching a good amount of data alone, data from different sources would be preferable since it
756 would produce less biased or unbalanced datasets, which subsequently will be more
757 appropriate for training ML models.

758 Considering the future trajectory of 3DP medicines, the ultimate goal will be to digitally
759 simulate the entire 3DP workflow in an effort to move towards sustainable research, where
760 both costs and material waste are minimised, as well as the time needed to realise the research
761 hypothesis. In essence, the ML models developed could expedite developments in the field of
762 3DP pharmaceuticals. In addition, digital simulations can offer insight that otherwise would be
763 difficult to experimentally determine. The present study demonstrates that ML could be an
764 effective component of such digital simulation by offering high predictive performance and in
765 rapid time. Moreover, the low computational demands of ML mean that it can be deployed as
766 a web-based software, or seamlessly integrated into other modelling tools similar to the
767 M3DISEEN web-based service. The aim with ML will be to produce an end-to-end model that
768 can simulate the entire 3DP workflow. 3DP and ML (and other AI tools) offer a unique
769 opportunity to move the pharmaceutical development to the next level, and this will indeed
770 depend on the availability of data and the quality thereof.

771 **4 Conclusion**

772 The study investigated the use of literature-mined data for developing artificial intelligence
773 (AI) machine learning (ML) techniques models to predict key aspects of the 3D printing
774 formulation pipeline. The analysis of the literature mined data revealed that positive results are
775 overwhelmingly published, which consequently resulted in an imbalanced dataset for filament
776 aspect and printability. Nevertheless, the ML techniques explored herein were able to learn and
777 provide high predictive accuracies for the values of the filament hot melt extrusion processing
778 temperature, filament aspect, printing temperature and printability. ML algorithms using data
779 based on the composition of the formulations and additional input features that could influence
780 drug release (e.g. surface area/volume, weight, infill percentage, pH and volume of dissolution
781 media, drug solubility) were used to predict the drug release profile of FDM printed
782 formulations. The best prediction was obtained by an ANN algorithm, which was able to

783 predict the dissolution times (T20, T50 and T80) of a formulation with an error of ± 24.29
784 minutes. Thus, it was concluded that data mined from the literature was an efficient approach
785 to modelling 3D printing workflow. It was also concluded that a structured repository for 3DP
786 data will greatly facilitate the creation of new knowledge via ML.

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