

Abstract Neural Representations of Category Membership beyond Information Coding Stimulus or Response

Robert M. Mok^{1,2} and Bradley C. Love^{1,3}

Abstract

■ For decades, researchers have debated whether mental representations are symbolic or grounded in sensory inputs and motor programs. Certainly, aspects of mental representations are grounded. However, does the brain also contain abstract concept representations that mediate between perception and action in a flexible manner not tied to the details of sensory inputs and motor programs? Such conceptual pointers would be useful when concepts remain constant despite changes in appearance and associated actions. We evaluated whether human participants acquire such representations using fMRI. Participants completed a probabilistic concept learning task in which sensory, motor, and category variables were not perfectly coupled or entirely independent, making it possible to observe evidence for abstract representations or purely grounded representations. To assess how the learned concept structure is

INTRODUCTION

Concepts organize our experiences into representations that can be applied across domains to support higher-order cognition. How does the brain organize sensory input into an appropriate representation for categorization? Are concepts simply a combination of sensory signals and motor plans, or does the brain construct a separate concept representation, abstracted away from sensory-motor codes? Despite much research on how people organize sensory information into a format suited for categorization (e.g., Love, Medin, & Gureckis, 2004; Kruschke, 1992; Nosofsky, 1986) and its neural basis (e.g., Zeithamova et al., 2019; Bowman & Zeithamova, 2018; Mack, Love, & Preston, 2016; Folstein, Palmeri, & Gauthier, 2013; Mack, Preston, & Love, 2013; Davis, Love, & Preston, 2012a, 2012b; Cromer, Roy, & Miller, 2010; Seger & Miller, 2010; Freedman & Assad, 2006; Sigala & Logothetis, 2002), few have explicitly examined whether category representations exist independently of sensory-motor information (Figure 1A).

Some concepts seem to be "grounded" in sensory or motor experiences (Barsalou, 2008). For instance, the idea of "pain" is based on experiences of pain, and the metaphorical use of the word is presumably linked to those bodily experiences. Certain aspects of concepts are more represented in the brain, we examined brain regions implicated in flexible cognition (e.g., pFC and parietal cortex) that are most likely to encode an abstract representation removed from sensory–motor details. We also examined sensory–motor regions that might encode grounded sensory–motor-based representations tuned for categorization. Using a cognitive model to estimate participants' category rule and multivariate pattern analysis of fMRI data, we found the left pFC and human middle temporal visual area (MT)/V5 coded for category in the absence of information coding for stimulus or response. Because category was based on the stimulus, finding an abstract representation of category was not inevitable. Our results suggest that certain brain areas support categorization behavior by constructing concept representations in a format akin to a symbol that differs from stimulus–motor codes.

abstracted from first-hand experience and act more like symbols or pointers, which can support flexible cognition. For example, we know water can be used to clean the dishes, but when we are thirsty, we drink it. The same object can also appear entirely different in some contexts, such as a camouflaging stick insect appearing as a leaf or when a caterpillar changes into a butterfly. In such cases where sensory information is unreliable or exhibits changes, an amodal symbol working as an abstract pointer may aid reasoning and understanding. Cognitive science and artificial intelligence researchers discuss the use of amodal symbols-abstracted away from specific input patternsfor solving complex tasks, arguing they provide a foundation to support higher cognition (Marcus, 2001; Pylyshyn, 1984; Fodor, 1975; also see Markman & Dietrich, 2000). In contrast, theories of grounded cognition suggest that all "abstract" representations are grounded in, and therefore fully explained by, sensory-motor representations (Barsalou, 1999; Harnad, 1990). Indeed, sensory-motor variables and categories are often correlated in the real world, and the brain may never need to represent "category" in a way that can be disentangled from perception and action.

Here, we consider several competing accounts. Closely related to "grounded cognition," some researchers emphasize a central role of action for cognition (Wolpert & Witkowski, 2014; Wolpert & Ghahramani, 2000; Rizzolatti, Riggio, Dascola, & Umiltá, 1987), such that category

© 2020 Massachusetts Institute of Technology. Published under a Creative Commons Attribution 4.0 International (CC BY 4.0) license

¹University College London, ²University of Cambridge, ³The Alan Turing Institute, London, UK

representations could simply consist of the appropriate stimulus-motor representations and associations (Figure 1B). An alternative view holds that categorymodulated stimulus representations are key for categorization, where stimulus information is transformed into a representation suited for categorization (as in cognitive models: e.g., Love et al., 2004; Kruschke, 1992). In these models, an attention mechanism gives more weight to relevant features so that within-category stimuli become closer and across-category stimuli are pushed apart in representational space (Figure 1C). Finally, the brain may recruit an additional amodal, symbol-like concept representation (Marcus, 2001; Pylyshyn, 1984; Newell, 1980; Fodor, 1975) to explicitly code for category, separate from sensory-motor representations. For instance, sensory information is processed (e.g., modulated by category structure) and then transformed into an abstract category representation before turning into a response (Figure 1D). This representation resembles an amodal symbol in that it has its own representational format (e.g., orthogonal to sensory-motor codes) and acts as a pointer between the relevant sensory signals (input) and motor responses (output). The advantage of such a representation is that it can play a role in solving the task and can persist across superficial changes in appearance and changes in motor commands. People's ability to reason and generalize in an abstract fashion suggests the brain is a type of symbol processor (Marcus, 2001).

Here, we aimed to test whether the brain constructs an abstract concept representation separate from stimulus and motor signals, if the "category" code consists of category-modulated stimulus representations and motor codes, or if it simply consists of stimulus–motor mappings. We designed a probabilistic concept learning task where the stimulus, category, and motor variables were not perfectly coupled nor entirely independent, to allow participants to naturally form the mental representations required to solve the task, and used multivariate pattern analysis (MVPA) on fMRI data to examine how these variables were encoded across the brain. For evidence supporting the amodal account (Figure 1D), some brain regions should encode category information but not the stimulus or response. For the category-modulated sensory account (Figure 1C), regions should encode both stimulus and category information, with no regions that encode category without stimulus information. Finally, for the sensory-motor account (Figure 1B), regions should code for category, stimulus, and motor response (separately or concurrently), with no regions encoding category without sensory or motor information.

We recruited participants to an initial behavioral session where they first learned the task and invited a subset of participants who performed relatively well to partake in an fMRI study. To assess how the learned concept structure is represented in the brain, we focused on brain regions implicated in flexible cognition, including pFC and parietal cortex, which are strong candidates for representing the abstract concept structure without being tied to sensorymotor variables, and sensory-motor regions that are involved in stimulus processing and may encode grounded representations such as category-modulated stimulus representations as the basis of concept knowledge. We focused on these regions to test for category representations after learning rather than testing regions that might be involved in learning (e.g., hippocampus, medial pFC),

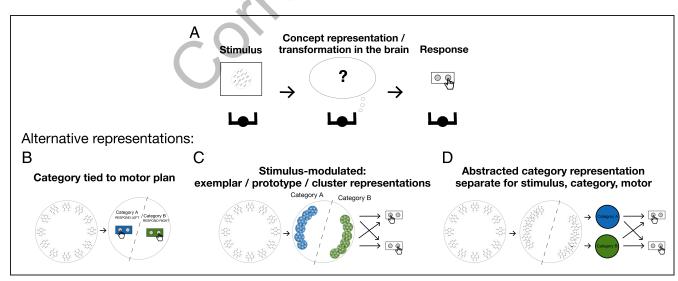


Figure 1. How the brain transforms stimulus into a concept representation for categorization. Stimuli are 12 motion dot patterns (100% coherent), from 0° to 330° in 30° steps. Blue and green colors denote the two categories. (A) An observer must transform the percept into intermediate representations for accurate categorization behavior. (B–D) Possible representations the brain might use for categorization. (B) Each stimulus is associated with a motor response, where the category representation is grounded in sensory–motor codes. (C) Stimulus-modulated representations as category representation. The stimulus representation is modulated by the category structure, which is turned into a motor representation for the response. (D) The category-modulated stimulus representation is associated with an abstract representation of each category with a different representational format to the sensory motor codes (blue and green circles), which is then turned into a response.

because participants spent a significant amount of time learning the category structure in a prior behavioral session (see Methods).

METHODS

Participant Recruitment and Behavioral Session

We recruited participants to partake in a behavioral session to assess their ability to learning the probabilistic concept learning task. One hundred thirty-one participants completed the behavioral session, and we invited a subset of higher performing participants who were MRI compatible to participate in the fMRI study. We set the threshold for being invited to no lower than 60% accuracy over two blocks of the task (50% chance). Only two participants in the behavioral session performed below 60% accuracy.

Participants (fMRI Study)

Thirty-nine participants took part in the fMRI study (most returned ~2–4 weeks after the behavioral session). Six participants were excluded because of lower-than-chance performance, misunderstanding the task, or falling asleep during the experiment. The remaining 33 participants (23 women) were aged 19–34 years (mean = 24.04 years, *SEM* = 0.61 years). The study was approved by the University College London Research Ethics Committee (reference: 1825/003).

Stimuli and Apparatus

Stimuli consisted of coherently moving dots produced in PsychoPy (Peirce et al., 2019), images of faces and buildings (main task), and images of flowers and cars (practice). In each dot-motion stimulus, there were 1000 dots, and dots were 2 pixels in size and moved at a velocity of $\sim 0.8^{\circ}$ per second. The dot-motion stimuli and images were 12° in diameter (or on longest axis). The fixation point was a black circle with 0.2° diameter. A gray circle (1° diameter) was placed in front of the dot stimulus but behind the fixation point to discourage smooth pursuit. The natural images were provided by members of Cognitive Brain Mapping Lab at RIKEN BSI. The task was programmed and run in PsychoPy in Python 2.7. The task was presented on an LCD projector (1024×768 resolution), which was viewed through a tilted mirror in the fMRI scanner. We monitored fixation with an eye tracker (Eyelink 1000 Plus, SR Research) and reminded participants to maintain fixation between runs as necessary.

Behavioral Task

To examine how the brain constructs an appropriate mental representation for categorization, we designed a probabilistic concept learning task to be first performed in a behavioral session and then the same probabilistic categorization task in the fMRI session. Specifically, we set out to test whether any brain regions coded for an abstract category signal separate from stimulus and motor signals, if the category signal mainly consisted of categorymodulated sensory signals, or if the category signal was simply a combination or coexistence of sensory-motor signals. To this end, we designed a probabilistic categorization task where the task variables (category, stimulus, and motor response) were not perfectly coupled or entirely independent.

On each trial, participants were presented with a set of moving dots moving coherently in one direction and were required to judge whether it belonged to one category ("Face") or another ("Building") with a corresponding left or right button press. The motion stimulus was presented for 1 sec, followed by an ISI ranging from 1.8 to 7.4 sec (jittered), then the category feedback (Face or Building stimulus) for 1 sec. The intertrial interval was 1.8 sec. Naturalistic images were used to encourage task engagement and to produce a strong stimulus signal.

The moving-dot stimuli spanned 12 directions from 0° to 330° in 30° steps, with half the motion directions assigned to one of two categories determined by a category bound. For half of the participants, the category bound was placed at 15° , so that directions from 30° to 180° were in one category, and directions from 210° to 330° and 0° were in the other category. For the other half of the participants, the objective category bound was placed at 105° , so that directions from 270° were in one category, and directions from 120° to 270° were in one category, and directions from 0° to 90° and 300° to 330° were in the other category.

The corrective category feedback consisted of a face or building stimulus, which informed the participant which category the motion stimulus was most likely part of. The feedback was probabilistic such that the closer to the bound a stimulus was, the more probabilistic the feedback was (see Figure 2A). In the practice sessions, participants were introduced to a deterministic version of the task before the probabilistic task (see Experimental Procedure: Behavioral Session section below).

Behavioral Task Rationale

Probabilistic category feedback was used to decouple the stimulus from the category to a certain extent. Most previous concept learning studies used deterministic feedback, such that each stimulus was always associated with the same (correct) category feedback. In terms of conditional probability, the probability of a stimulus belonging to a given category (Pr(category A | stimulus x)) with deterministic category feedback is 1. With probabilistic category feedback, the conditional probability is less than 1, and as the stimulus–feedback association becomes weaker (more probabilistic), it approaches 0.5 (not predictive). In this way, the stimulus and category are weakly coupled and may lead participants to form a category representation abstracted from the more concrete experimental variables (such as stimulus and motor response). On the other hand,

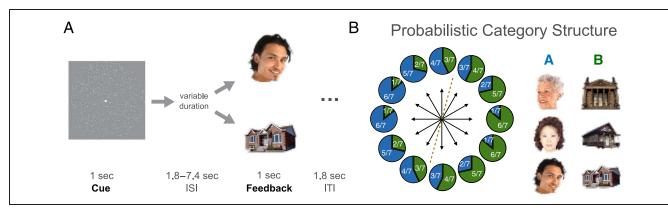


Figure 2. Behavioral task. (A) On each trial, a dot-motion stimulus was presented and participants judged whether it was in Category A or B. At the end of each trial, probabilistic category feedback (a face or building stimulus) informed the participant which category the motion stimulus most likely belonged to. (B) Probabilistic category structure. For motion stimuli to the left of the category bound (dotted line), the feedback will most likely be a face (Category A), and stimuli to the right will most likely be a building (Category B). For example, for the motion direction where the blue section is 4/7, the participant will see a face four out of seven times and a building three out of seven times (corresponding to the 3/7 green section). The closer the motion direction to the category bound, the more probabilistic the feedback.

participants could still perform the task at greater accuracy than chance if they relied heavily on the stimulus, grounding the category in the stimulus representations.

Furthermore, the category–response association was flipped after each block (e.g., left button press for Category A in the first block, right button press for Category A in the second block), to discourage participants simply associating each category with a motor response across the experiment. Of course, it was still possible for participants to associate the category with a motor plan and change this association across blocks, leading to a category representation based on motor planning.

In summary, the task required participants to learn the category that each motion-dot stimulus belonged to by its probabilistic association to an unrelated stimulus (face or building as category feedback), whereby the probabilistic feedback could lead participants to form an abstract or grounded category representation. In addition, the category–motor association was flipped across blocks. Together, the category, stimulus, and motor variables were weakly coupled, allowing us to assess whether there are brain regions that code for these variables together or independently of one another.

Experimental Procedure: Behavioral Session (Practice and Main Experiment)

To ensure participants understood the main experimental task, they were given four practice task runs with each version gradually increasing in task complexity. In the first three runs, the task was the same as described above except that the images used for feedback were pictures of flowers and cars. In the fourth run, it was a practice run of the main task described above. Before each run, the experimenter explained the task to the participant.

Participants were instructed to learn which motion directions led to the appearance of Flower images and which led to the Car images. Specifically, they were told that, when the moving dot stimulus appears, they should press the left (or right) button if they think a Flower will appear or the right (or left) button if they think a Car will appear. In the first run, the category boundary was at 90° (up-down rule), and motion directions were presented in sequential order around the circle. The category ("Flower" or "Car") feedback was deterministic such that each dot-motion stimulus was always followed by the same category stimulus feedback. For feedback, participants were presented with the image in addition to a color change in the fixation point (correct: green, incorrect: red, too slow: yellow). In the second run, the task was the same except the motion directions were presented in a random order. In the third run, participants were told that the feedback is probabilistic, meaning that the feedback resembles the weather report: It is usually correct, but sometimes it is not. For example, of the five times you see that motion direction, you will be shown a flower stimulus as feedback four times, but you will be shown a car once. So the feedback is helpful on average, but sometimes it can be misleading. In the fourth run, participants were introduced to a new task to be used in the main experiment, with a new probabilistic category boundary (15° or 105°) and with face and building images as feedback.

Once participants completed the practice runs and were comfortable with the task, they proceeded to the main experimental session where they learnt the category rule from trial and error. In each block, participants completed seven trials per direction condition, giving 84 trials per block. The experimenter informed participants that the category–response association flipped after each block. Participants completed three or four experimental runs.

Experimental Procedure: fMRI Session

A subset of participants was invited to attend an fMRI session. Participants were given one practice block run as a reminder of the task and then proceeded to complete the main experiment in the scanner. Participants learned through trial and error. They were not informed about the location of the category boundary in either the behavioral or fMRI session, which partially explains why their performance was not at ceiling. A cognitive model fit to individuals' behavior indicates that participants' category boundaries differed from the optimal boundary (see below).

Participants completed three or four blocks of the probabilistic category learning task (four participants performed an extra block because of low performance on early block runs), then a motion localizer block, and a face–scene localizer block (block order for localizer runs was counterbalanced across participants). After the scan session, participants completed a postscan questionnaire to assess their understanding of the task and to report their subjective category rule.

Each task block took approximately 12 min, and the whole scan session (main task, localizers, and structural scans) took slightly over an hour. Including preparation, practice, and postexperiment debriefing, the whole session took approximately 2 hr.

Localizer Tasks

To localize the face-selective fusiform face area (FFA; Allison, Puce, Spencer, & McCarthy, 1999; Kanwisher, McDermott, & Chun, 1997) and place-sensitive parahippocampal place area (PPA; Epstein & Kanwisher, 1998) in individuals, participants completed an event-related localizer scan where they were presented with faces and buildings and made a response when they saw an image repeat (1-back task), which was followed by feedback (the fixation point changed to green for correct and red for incorrect). On each trial, an image of a face or building was presented for 1 sec with ISIs between stimulus and feedback (green/ red fixation color change) ranging from 1.8 to 7.4 sec (jittered), with an intertrial interval of 1.8 sec. A total of 42 faces and 42 buildings were presented in a random order. Participants also completed a motion localizer run that was not used here.

MRI Data Acquisition

Functional and structural MRI data were acquired on a 3-T TrioTim scanner (Siemens) using a 32-channel head coil at the Wellcome Trust Centre for Neuroimaging at University College London. An EPI-BOLD contrast image with 40 slices was acquired in 3-mm³ voxel size, repetition time (TR) = 2800 msec, and echo time (TE) = 30 msec, and the flip angle was set to 90°. A whole-brain field map with 3-mm³ voxel size was obtained with a first TE = 10 msec, second TE = 12.46 msec, and TR = 1020 msec, and the flip angle was set to 90°. A T1-weighted (T1w) structural image was acquired with 1-mm³ voxel size, TR = 2.2 msec, and TE = 2.2 msec, and the flip angle was set to 13°.

Behavioral Model and Data Analysis

The probabilistic nature of the feedback meant that participants did not perform exactly according to the objective category rule determined by the experimenter, and inspection of behavioral performance curves suggested that most participants formed a category rule slightly different to the objective rule. To get a handle on the category rule participants formed, we applied a behavioral model to estimate each participant's subjective category boundary from their responses.

The model contains a decision bound defined by two points, b_1 and b_2 , on a circle (0°–359°). Category A proceeds clockwise from point b_1 , whereas Category B proceeds clockwise from b_2 . Therefore, the positions of b_1 and b_2 define the deterministic category boundary between Categories A and B. To illustrate, if $b_1 = 15^\circ$ and $b_2 =$ 175°, stimulus directions from 15° to 175° would be in one category, and stimulus directions from 175° to 359° and from 0° to 15° would be in the other category. Note that the number of stimulus directions is not constrained to be equal across categories, as illustrated in this example (five and seven directions in each category). Despite this, there were six stimulus directions in each category for most participants.

The only source of noise in this model are the positions of b_1 and b_2 , which are normally distributed as $\mathcal{N}(0, \sigma)$. As the σ parameter—the standard deviation of the positions of b_1 and b_2 —increases, the position of the boundary for a given trial becomes noisier, and therefore it becomes more likely that an item may be classified contrary to the position of the boundary. In practice, no matter the value of σ , it is always more likely that an item will be classified according to the positions of b_1 and b_2 . The standard deviation parameter provides an estimate of how uncertain participants were of the category boundary. If a participant responded perfectly consistently according to a set of bounds (deterministically), σ would be low, whereas if the participant was more uncertain of the bound locations and responded more probabilistically, σ would be higher.

The probability a stimulus x is an A or B is calculated according to whichever boundary b_1 or b_2 is closer. This is a numerical simplification as it is possible for the further boundary to come into play and even for boundary noise to lead to b_1 or b_2 to traverse the entire circle. However, for the values of σ we consider, both of these possibilities are highly unlikely. The probability that stimulus x is labeled according to the mean positions of b_1 and b_2 is

$$1 - p\left(z > \frac{|x - b_x|}{\sigma}\right)$$

where z is distributed according to the standard normal distribution and b_x is b_1 or b_2 , whichever is closer to x. Intuitively, the further the item is from the boundary position, the more likely it is to be classified according to the boundary position as noise (i.e., σ) is unlikely to lead to sufficient boundary movement in that trial. The probability an item is labeled in the alternative category (i.e.,

"incorrect" responses against the bound defined by the mean positions of b_1 and b_2) is simply 1 minus the above quantity.

In other words, the probability stimulus in a certain category is a Gaussian function of the distance to the closest bound, where the further away the stimulus is from the bounds, the more likely it is to be a part of that category (see Figure 3A for an illustration of the model). Maximum likelihood estimation was used to obtain estimates for each participant (using the optimize function in SciPy). Model estimates of the subjective category bound fit participant behavior as expected. Specifically, there was high accuracy (concordance) with respect to the estimated subjective category bound (mean proportion correct = 0.82, *SEM* = 0.01; see Figure 3B).

Modeling and analyses were performed in Python 3.7.

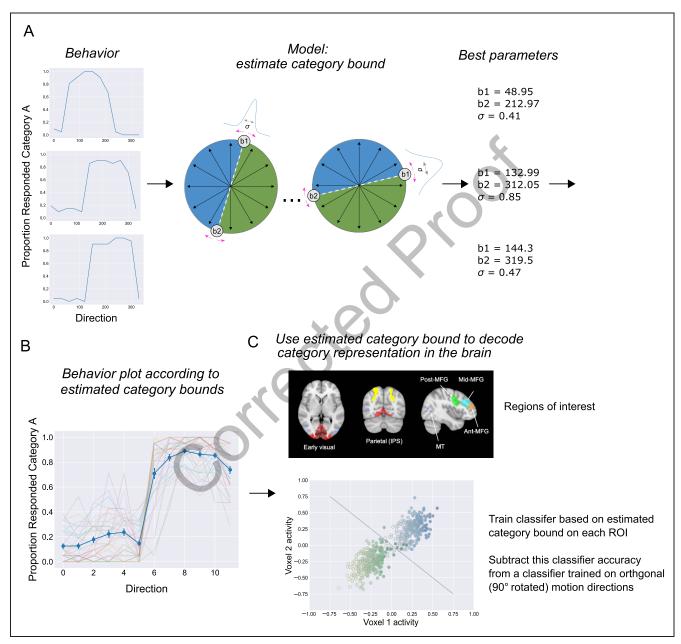


Figure 3. Task model, behavioral results, and model-based fMRI analysis procedure. (A) The model takes individual participant behavior as input and estimates their subjective category bound (b_1 and b_2) and standard deviation (σ). (B) Categorization behavior. Proportion Category A responses plotted as a function of motion directions ordered by individual participants' estimated category boundary. Blue curve represents the mean, and error bars represent *SEM*. Translucent lines represent individual participants. (C) Model-based fMRI analysis procedure illustration. Voxel activity patterns are extracted from each ROI for each motion direction condition (top), and a classifier was trained (SVM) to decode the category based on the model-based estimation of the category boundary for each participant (bottom). The data in the scatterplot were generated to illustrate example patterns of voxel activity evoked by the motion direction stimuli (two voxels shown here) belonging to each category (blue for Category A, green for Category B). The line is a possible support vector plane that reliably discriminates voxel patterns elicited by stimuli in Category A from stimuli in Category B. To test for an abstract category signal, we subtracted the classification accuracy for the category SVM by an SVM trained to discriminate orthogonal (90° rotated) directions (see Methods for details).

fMRI Preprocessing

Results included in this article come from preprocessing performed using fMRIprep 1.2.3 (Esteban et al., 2019; RRID:SCR_016216), which is based on Nipype 1.1.6-dev (Gorgolewski et al., 2011; RRID:SCR_002502).

Anatomical Data Preprocessing

The T1w image was corrected for intensity nonuniformity using N4BiasFieldCorrection (Avants, Tustison, & Song, 2009; ANTs 2.2.0) and used as T1w reference throughout the workflow. The T1w reference was then skull-stripped using antsBrainExtraction.sh (ANTs 2.2.0), using OASIS as the target template. Spatial normalization to the ICBM 152 Nonlinear Asymmetrical template version 2009c (Fonov, Evans, McKinstry, Almli, & Collins, 2009; RRID: SCR 008796) was performed through nonlinear registration with antsRegistration (ANTs 2.2.0, RRID:SCR 004757; Avants, Epstein, Grossman, & Gee, 2008), using brainextracted versions of both T1w volume and template. Brain tissue segmentation of cerebrospinal fluid (CSF), white matter (WM), and gray matter (GM) was performed on the brain-extracted T1w using fast (FSL 5.0.9, RRID: SCR 002823; Zhang, Brady, & Smith, 2001).

Functional Data Preprocessing

For each of the five or six BOLD runs found per subject (three or four task runs plus two localizer runs), the following preprocessing was performed. First, a reference volume and its skull-stripped version were generated using a custom methodology of fMRIPrep. A deformation field to correct for susceptibility distortions was estimated based on a field map that was coregistered to the BOLD reference, using a custom workflow of fMRIPrep derived from D. Greve's epidewarp.fsl script and further improvements of HCP Pipelines (Glasser et al., 2013). On the basis of the estimated susceptibility distortion, an unwarped BOLD reference was calculated for a more accurate coregistration with the anatomical reference. The BOLD reference was then coregistered to the T1w reference using flirt (FSL 5.0.9; Jenkinson & Smith, 2001) with the boundary-based registration (Greve & Fischl, 2009) cost-function. Coregistration was configured with 9 degrees of freedom to account for distortions remaining in the BOLD reference. Head-motion parameters with respect to the BOLD reference (transformation matrices, and six corresponding rotation and translation parameters) are estimated before any spatiotemporal filtering using mcflirt (FSL 5.0.9; Jenkinson, Bannister, Brady, & Smith, 2002). BOLD runs were slice-time corrected using 3dTshift from AFNI 20160207 (Cox & Hyde, 1997; RRID:SCR 005927). The BOLD time series (including slice-timing correction when applied) were resampled onto their original, native space by applying a single, composite transform to correct for head-motion and susceptibility distortions. These

resampled BOLD time series will be referred to as preprocessed BOLD in original space or just preprocessed BOLD. The BOLD time series were resampled to MNI152NLin2009cAsym standard space, generating a preprocessed BOLD run in MNI152NLin2009cAsym space. First, a reference volume and its skull-stripped version were generated using a custom methodology of fMRIPrep. Several confounding time series were calculated based on the preprocessed BOLD: framewise displacement, DVARS, and three region-wise global signals. Framewise displacement and DVARS are calculated for each functional run, both using their implementations in Nipype (following the definitions by Power, Barnes, Snyder, Schlaggar, & Petersen, 2012). The three global signals are extracted within the CSF, the WM, and the whole-brain masks. In addition, a set of physiological regressors were extracted to allow for component-based noise correction (CompCor; Behzadi, Restom, Liau, & Liu, 2007). Principal components are estimated after high-pass filtering the preprocessed BOLD time series (using a discrete cosine filter with 128-sec cutoff) for the two CompCor variants: temporal (tCompCor) and anatomical (aCompCor). Six tCompCor components are then calculated from the top 5% variable voxels within a mask covering the subcortical regions. This subcortical mask is obtained by heavily eroding the brain mask, which ensures it does not include cortical GM regions. For aCompCor, six components are calculated within the intersection of the aforementioned mask and the union of CSF and WM masks calculated in T1w space, after their projection to the native space of each functional run (using the inverse BOLDto-T1w transformation). The head-motion estimates calculated in the correction step were also placed within the corresponding confounds file. All resamplings can be performed with a single interpolation step by composing all the pertinent transformations (i.e., head-motion transform matrices, susceptibility distortion correction when available, and coregistrations to anatomical and template spaces). Gridded (volumetric) resamplings were performed using antsApplyTransforms (Advanced Normalization Tools), configured with Lanczos interpolation to minimize the smoothing effects of other kernels (Lanczos, 1964). Nongridded (surface) resamplings were performed using mri vol2surf (FreeSurfer).

Many internal operations of fMRIPrep use Nilearn 0.4.2 (Abraham et al., 2014; RRID:SCR_001362), mostly within the functional processing workflow. For more details of the pipeline, see the section corresponding to workflows in fMRIPrep's documentation.

ROIs

To study how the brain represented category, stimulus, and response variables in the probabilistic categorization task, we focused on a set of visual, parietal, and prefrontal brain ROIs hypothesized to be involved in coding these variables after learning. We selected anatomical masks from Wang et al. (2014; scholar.princeton.edu/napl/resources) to examine areas involved in early visual processing, motion processing, and attention, including early visual cortex (EVC; V1, V2, and V3 merged), motion-sensitive human middle temporal visual area (MT)/V5 (Dubner & Zeki, 1971), and the intraparietal sulcus (IPS). We included EVC to assess stimulus-related representations including orientation and direction. The IPS is implicated in both attention (Kastner & Ungerleider, 2000; Corbetta, Miezin, Shulman, & Petersen, 1993; Mesulam, 1981) and category learning (Freedman & Assad, 2016; Seger & Miller, 2010). However, we did not have strong reasons to focus on specific parts of the IPS, so we merged IPS1 to IPS5 to make a large IPS ROI.

Because these masks are provided in T1 structural MRI space (1-mm³), when they were transformed into individual participant functional space (3 mm³), several masks did not cover GM accurately (too conservative, thereby excluding some GM voxels). Therefore, we applied a small amount of smoothing to the mask (with a Gaussian kernel of 0.25 mm, using fslmaths) for a more liberal inclusion of neighboring voxels, before transforming it to individual-participant space. In addition, several potential ROIs were too small to be mapped onto our functional scans. Specifically, there were several participants with zero voxels in those masks after transforming to functional space, even with smoothing. This included the motion-sensitive area MST and the superior parietal lobule (SPL1), which were not included.

pFC is strongly implicated representing abstract task variables (Duncan, 2001; Miller & Cohen, 2001) and task-relevant sensory signals (e.g., Jackson, Rich, Williams, & Woolgar, 2017; Erez & Duncan, 2015; Roy, Riesenhuber, Poggio, & Miller, 2010; Meyers, Freedman, Kreiman, Miller, & Poggio, 2008; Goldman-Rakic, 1995). We selected prefrontal regions implicated in cognitive control and task representations (Fedorenko, Duncan, & Kanwisher, 2013; Duncan, 2010; imaging.mrc-cbu.cam.ac.uk/imaging /MDsystem) including the posterior, middle (approximately Area 8), and anterior (approximately Area 9) portion of the middle frontal gyrus.

Primary motor cortex was selected to examine representations related to the motor response and to test for any stimulus or category signals. Primary motor cortex masks were taken from the Harvard-Oxford atlas.

We also localized and examined brain responses in the FFA and PPA, to assess whether face and place regions, involved in processing stimuli at the feedback phase, were involved in representing the learned category (see procedure below). For example, if participants learnt that a set of motion directions belonged to Category A, which was associated with face stimuli as feedback, the FFA might show information about the learnt category during the motion direction stimulus phase (i.e., not to the face but according to the learnt category bound). It is worth noting that we are interested in assessing the information coding the learnt category (Category A vs. B), not the probabilistically presented face versus building feedback stimulus.

Apart from the FFA and PPA (where bilateral ROIs were used; see below), we included both left and right ROIs. Masks were transformed from standard Montreal Neurological Institute space to each participant's native space using Advanced Normalization Tools (Avants et al., 2009).

fMRI General Linear Model

We used the general linear model (GLM) in FMRI Expert Analysis Tool (Woolrich, Ripley, Brady, & Smith, 2001; FMRIB Software Library Version 6.00; fsl.fmrib.ox.ac.uk/fsl/) to obtain estimates of the task-evoked brain signals for each stimulus, which was used for subsequent MVPAs.

For the main GLM, we included one explanatory variable (EV) to model each motion stimulus trial (estimating trialwise betas for subsequent MVPA) and an EV for each category feedback stimulus linked to each motion stimulus condition (12 EVs, not used in subsequent analyses; see trial-wise GLM examining the feedback response below). No spatial smoothing was applied. Stimulus EVs were 1 sec with ISIs between stimulus and feedback ranging from 1.8 to 7.4 sec (jittered), and the intertrial interval was 1.8 sec. Each block run was modeled separately for leave-one-run-out cross-validation for MVPA.

To examine motor-related brain responses, we performed an additional GLM using the same number of EVs except the EVs were time-locked to the response rather than the motion stimulus (stimulus time plus RT) and modeled as an event lasting 0.5 sec, with the assumption that the motor events were shorter than the stimulus (although this made little difference to the results). For trials without a response, the stimulus was modeled from stimulus onset as done in the main GLM and then excluded in subsequent motor-related analyses. Feedback stimuli were modeled with a single EV as above.

To localize the face-selective FFA and place-sensitive PPA, we performed an additional GLM in SPM12 (www.fil .ion.ucl.ac.uk/spm/software/spm12/). We applied spatial smoothing using a Gaussian kernel of FWHM 6 mm and included one EV for faces and one EV for building stimuli, as well as polynomials of degrees 0:6 to model drift in the data. Stimulus EVs were 1 sec with ISIs between stimulus and feedback (green/red fixation point color change) ranging from 1.8 to 7.4 sec (jittered), with an intertrial interval of 1.8 sec. We included three contrasts Faces > Buildings, Buildings > Faces, and overall Visual Activation (Faces and Buildings). To define individual participant ROIs, we used minimum statistic conjunctions with visual activations. To localize the FFA, the conjunction was (Face > Building) & Visual. For the PPA, the conjunction was (Building > Face) & Visual. The rationale behind this conjunction is that functional ROIs should be not only simply selective but also visually responsive (all voxels that were deactivated by visual stimulation were not included). The conjunction was thresholded liberally at p < .01uncorrected. The peaks for each functional ROI were

detected visually in the SPM results viewer, and we extracted the top 100 contiguous voxels around that peak.

There were four participants for which we could not find clear peaks and clusters for the left FFA, five participants for the right FFA, seven participants for the left PPA, and six participants for the right PPA. Because we were unable to reliably localize these areas for all participants in both hemispheres, we used unilateral ROIs for participants with unilateral FFA/PPA ROIs and excluded participants for that ROI if they did not have either a left or right FFA or PPA ROI. The difficultly in localizing these areas for a subset of participants might have been because of our relatively short (two runs) event-related localizer design. In summary, when testing the FFA, we excluded two participants (no left or right FFA), and when testing the PPA, we excluded four participants (no left or right PPA).

We also performed a motion localizer, but likely because of the short localizer and the event-related design, it was not possible to reliably localize participant-specific motionsensitive regions.

To examine information during the category feedback, we performed an additional GLM modeling the same events as the main GLM (locked to motion stimuli and feedback stimuli), except that one EV was used to model each feedback trial (estimating trial-wise betas for subsequent MVPA) and one EV for each motion stimulus condition (12 EVs). This additional GLM was used to estimate the trial-wise feedback mainly for practical reasons. If modeling all cue and feedback trials, it becomes a substantially larger model for FMRIB Software Library. By modeling the cue period trials in a separate GLM to the feedback trials, we were able to reduce the number of EVs per model (96 rather than 168).

MVPA

To examine brain representations of category, stimulus, and motor response, we used MVPA across our selected ROIs. Specifically, we trained linear support vector machines (SVMs; cf. Kamitani & Tong, 2005) to assess which brain regions contained information about the category ("Face" or "Building"), stimulus (direction, orientation, and 12-way classifier), and motor response (left or right button press).

Decoding analyses were performed using linear support vector classifiers (C = 0.1) using Scikit-learn Python package (Pedregosa et al., 2011) with a leave-one-run-out cross-validation procedure.

To test for abstract category coding, we first trained a classifier to discriminate between motion directions belonging to the two categories for each participant's subjective category bound. To ensure that this was a pure category signal unrelated to stimulus differences (e.g., simply decoding opposite motion directions), we trained a classifier based on the participant's subjective category bound, rotated 90°. For a strict test of an abstract category signal, we subtracted the classification accuracy of the first

classifier from accuracy of the second classifier. The reasoning behind this is that, if a brain region contains information about the stimulus direction but no information about category, it is still possible to obtain significant classification accuracy for the category classifier (Category A vs. Category B). However, if the brain region primarily encoded stimulus information, there should be as much information for the orthogonal directions in the voxel activity patterns within an ROI (assuming sensory biases across voxels are equal). Therefore, if a brain region carries information about the category and sensory content, there would be greater classification accuracy when decoding across directions across the category boundary (with category and sensory information) than classification accuracy for the directions across the rotated boundary (sensory but no category information). The subtraction allows us to test whether the brain regions carry abstract category information over and above the sensory information. If there is only sensory information and no category information, the subtracted classification accuracies should be centered around zero. Negative values would suggest more information across directions across the boundary orthogonal to the category bound. This would most likely reflect unequal perceptual biases across voxels in that brain region, where that brain region contained more information about the motion directions across the rotated boundary compared to those across the category boundary (by chance, i.e., stimulus based, unrelated to the learned category). Different participants were randomly assigned to different objective category boundaries, which makes a systematic bias unlikely. Previous studies have tested whether a brain region contains information that can discriminate members of different categories. However, these studies could not rule out the contributions of the stimulus features to the category decoder. In our study, stimulus feature differences are matched when comparing stimuli across the category boundary versus stimuli across the orthogonal boundary. This subtraction method ensures that the sensory signal is not the main contributor to any category code found.

To ensure this category signal was not related to motor preparation or the response, we also subtracted the former category classifier accuracy from a motor response classifier accuracy (discriminating between left and right button presses).

For stimulus direction coding, we trained classifiers to discriminate between all six pairs of opposite motion directions (0° vs. 180°, 30° vs. 210°, etc.) and averaged across the classification accuracies.

To examine motor response coding, we trained classifiers to discriminate between left and right button presses on the GLM where we locked the EVs to the motor responses (RTs).

As a control analysis, we tested whether a classifier trained on the objective category structure (i.e., defined by the experimenter) produced similar results to the subjective category analysis. The procedure was the same as the abstract category classifier above, except that the directions in each category were determined by the experimenter. In another set of control analyses, we assessed if there was any information about stimulus. We tested for orientation coding by training a classifier on all 12 pairs of orthogonal orientations irrespective of the motion direction (0° vs. 90° and 0° vs. 270°, 30° vs. 120°, 30° vs. 300°) and averaged across the classification accuracies. Finally, for a more general measure of stimulus coding, we trained a 12-way classifier to assess stimulus coding for each motion direction.

We used one-sample t tests (one-tailed) against chancelevel performance of the classifier (using SciPy; Virtanen et al., 2020). Multiple comparisons across ROIs were corrected by controlling the expected false discovery rate (FDR) at 0.05 (Seabold & Perktold, 2010). For decoding category, we corrected across 12 ROIs (all apart from bilateral EVC and bilateral motor cortex), and for the direction and 12-way classifier, we corrected across 14 ROIs (excluding bilateral motor cortex). Bonferroni correction was used for tests with two ROIs (correcting for visual and motor hemispheres for orientation and motor decoding, respectively). For others, we report the uncorrected p values because none survived even without correction. MVPA and statistical analyses were performed in Python 3.7.

Brain-Behavior Correlations

To assess whether the brain's representation of the abstract category signal contributed to categorization performance, we performed robust regression (Seabold & Perktold, 2010) to assess the relationship between categorization performance (concordance to the estimated subjective category structure) with classifier accuracy for the category for the ROIs with greater-than-chance classification accuracy for category.

Matplotlib (Hunter, 2007) and Seaborn (Waskom, 2020) were used for plotting and creating figures in this article.

Data and Code Availability Statement

The code for the behavioral model and data analysis is available at github.com/robmok/memsampCode. The behavioral and fMRI data will be made publicly available at openneuro.org/.

RESULTS

To assess how learned concept structure is represented in the brain, 33 participants learned a probabilistic concept structure in an initial behavioral session and returned on a separate day to perform the probabilistic categorization task (the same task in the behavioral session) while they underwent an fMRI scan.

We used a model to estimate individual participants' subjective category bound (see Methods and Figure 3A and B). Briefly, the model assumes that participants form a mental decision boundary in the (circular) stimulus space to separate the categories, and there is some uncertainty of the placement of this bound. Formally, the model has three parameters: The first two determines bound placement $(b_1 \text{ and } b_2)$, and the third is a standard deviation parameter (σ) that models the (normally distributed) noise in this bound. σ provides an estimate of how certain (lower σ) participants are of their boundary placement. The model-estimated category bounds corresponded to participants' categorization behavior. To compute a measure of behavioral accuracy, we computed the proportion of categorization responses consistent with individual participants' estimated category bound. There was a strong correlation between the standard deviation parameter of the model σ and behavioral accuracy (r =-.90, p = 9.00e - 13), suggesting the standard deviation parameter characterizes an aspect of the categorization behavior well.

To evaluate the three main accounts of how the brain organizes information for categorization, we performed MVPA across visual, parietal, and prefrontal ROIs hypothesized to be involved in representing the learned concept structure (Figure 3). Specifically, we trained linear SVMs to assess which brain regions contained information about category (A or B), stimulus (directions), and response (left or right). For a strict test of an abstract category signal unrelated to stimulus features, we trained a classifier to discriminate between motion directions in Category A versus directions in Category B and subtracted this from a control classifier trained to discriminate between directions in Category A rotated 90° versus directions in Category B rotated 90°. This ensured that the classifier was not simply picking up information discriminating opposite stimulus directions (see Methods for details).

Our findings most strongly align with the hypothesis that the brain constructs an amodal symbol for representing category, independent of sensory–motor variables. Specifically, we found an abstract category signal over and above stimulus information in the middle portion of the left middle frontal gyrus (mMFG: p = .0025, q(FDR) = 0.029) and left motion-sensitive area MT (p = .0086, q(FDR) = 0.048; Figures 4A and 5A and B). This is particularly striking because the category is based on the stimulus direction, and there was no hint of a direction signal in these regions (ps > .41; Figures 4B and 5A and B).

Consistent with the idea that abstract category representations can aid performance, we found that the strength of category decoding was positively correlated with categorization accuracy (responses consistent with the modelestimated category bound) in the left MT (robust regression; $\beta = 0.74, p < .05$; Figure 5D) with a similar trend for the left mMFG ($\beta = 0.73, p = .067$; Figure 5C). We also confirmed that the category signal was stronger than the motor code in the left mMFG by subtracting the classifier

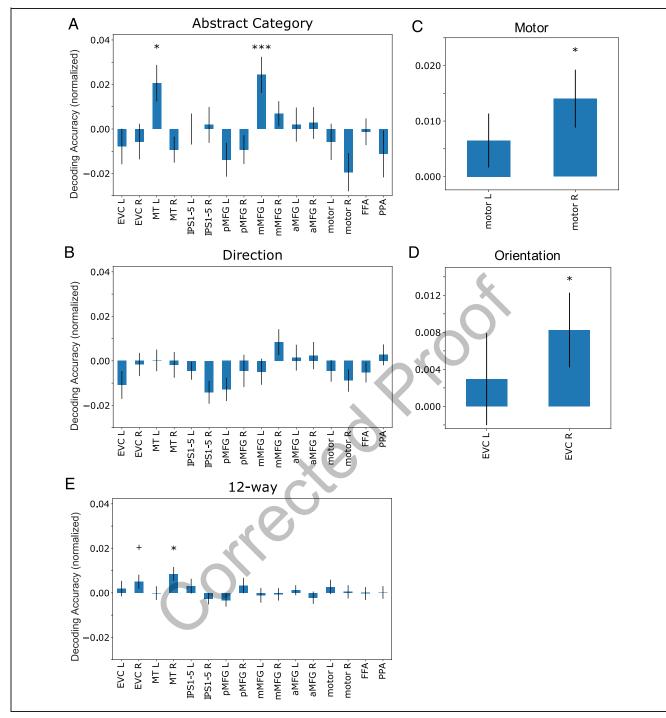


Figure 4. fMRI MVPA results. (A) Abstract category coding in the left mMFG cortex and left MT. Abstract category coding over and above sensory coding was computed by the category classifier accuracy minus the classifier accuracy trained on orthogonal (90° rotated) directions. (B) No strong effects showing stimulus motion direction information. (C) The right motor cortex showed significant information coding response. (D) The right EVC showed significant information coding orientation. (E) The right MT contained sensory information as shown by the 12-way stimulus classifier, with the right EVC showing a similar trend. Normalized decoding accuracy measures are normalized by subtracting chance values (direction = 1/2, 12-way = 1/12, motor = 1/2, orientation = 1/2), apart from abstract category that subtracts from a control classifier (chance = 0). ***p = .0025; *p < .05; +p < .06.

trained to discriminate motion directions across categories from the motor classifier (p = .015).

As expected, we found information coding motor response in the motor cortex (right: p = .006; Bonferronicorrected for hemisphere, p = .011; left: p = .095;

Bonferroni-corrected p = .19; Figure 4C) but no information about category or direction (ps > .42).

Notably, abstract category coding was only present for the participant-specific subjective category structure ("objective" category bound classifiers across all ROIs:

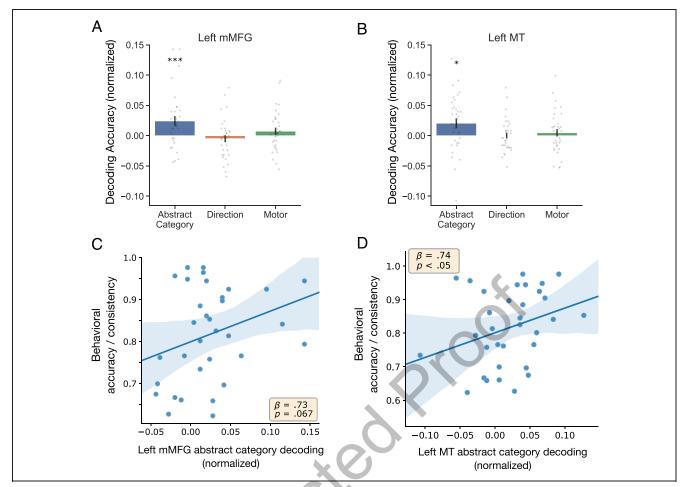


Figure 5. Abstract category coding and correlations with categorization behavior. (A–B) Univariate scatterplots showing significant abstract category coding in the left mMFG (A) and left MT (B), with no evidence of stimulus and motor coding. Gray dots are individual participants. (C–D) The strength of abstract category coding in MT (D) was correlated with categorization accuracy, that is, consistent responses with subjective category bound. There was a trend in the same direction in the left mMFG (C). In D and E, beta coefficients are from a robust regression analysis, and the shaded area represents 95% confidence intervals for the slope. ***p = .0025, *p < .05. Error bars represent *SEM*. Normalized decoding accuracy measures are normalized by subtracting chance values, apart from abstract category that subtracts from a control classifier (chance = 0).

ps > .06). Furthermore, we found no evidence of category coding in the FFA or in the PPA (ps > .31).

Although we did not find category and stimulus representations intertwined, this was not because stimulus representations were not decodable in our data. We trained a classifier on orientation in the EVC and found activity coding orientation (Figure 4D, p < .05, Bonferronicorrected for hemisphere). We also trained a 12-way classifier to assess if there was any information about the stimulus that would not be found simply by examining orientation or direction responses and found that the right MT encoded information on the stimulus (p = .005, q(FDR) = 0.03) and a trend for right EVC (p = .06, q(FDR) = 0.18; Figure 4E). Notably, there was no evidence for this in the left mMFG or left MT, which encoded abstract category (ps > .74).

DISCUSSION

We examined the neural representations underlying categorization and found that the brain constructs an abstract category signal with a different representational format to sensory and motor codes. Specifically, the left pFC and MT encoded category in the absence of stimulus information, despite category structure being based on those stimulus features. Furthermore, the strength of this representation was correlated with categorization performance based on participants' subjective category bound estimated by our model.

Although some representations may be grounded in bodily sensations, for tasks that require flexibility and representations to support abstract operations, an amodal symbol of a different representational format to that of sensorymotor representations may prove useful (Marcus, 2001; Pylyshyn, 1984; Newell, 1980; Fodor, 1975). Indeed, a category representation tied to a motor plan or stimulus feature would facilitate stimulus-motor representations effectively in specific circumstances but become unusable given slight changes in context. In this study, it was possible to solve the task in multiple ways, such as a combination of the sensory-motor variables, using a category-modulated sensory representation or additionally recruiting an amodal representation (Figure 1B–D). Despite this, we found the brain produces an additional abstract representation to support categorization (Figure 1D). Specifically, by applying a decoding approach to test for a category signal over and above a sensory code, we showed that the left mMFG and MT encoded a category signal abstracted from the sensory information. Furthermore, these areas did not carry any information about stimulus or response (evidenced by the motor, direction, orientation, and 12-way stimulus classifier), and the category code was significantly stronger than the motor code. In contrast, we did not find any regions that encoded both the category and stimulus, as predicted by the account where category information is grounded in category-modulated stimulus representations (Figure 1C). We also did not find any regions that encoded both the category and the motor response, as predicted by the account where category is grounded in stimulus-motor associations (Figure 1B). Therefore, our findings suggest that brain constructs an amodal symbol for representing category, independent of sensory-motor variables. It is worth noting that our results do not suggest that the brain does not use sensory information or that there are no grounded neural representations but, rather, that the brain constructs an additional category representation abstracted from the sensory-motor information for categorization.

In addition to the left pFC, we found that the left MT encoded a category signal in the absence of sensory information, whereas the right MT was only driven by sensory information. One possible explanation is that the category signal originated from the left pFC, which was sent back to modulate the left MT. This may have resulted in competition between the category and sensory signals, and the task-relevant category signal won out over the bottomup sensory signal. Because there was no category signal in the right pFC, the right MT was not affected by the task and coded the bottom-up stimulus signal. Alternatively, the left MT may simply be more affected by top-down modulation from pFC. For instance, task-relevant attentional modulation in the left PPA (when attending to scenes vs. faces) seems to be stronger and more reliable than the right PPA (Chadick, Zanto, & Gazzaley, 2014; Gazzaley, Cooney, McEvoy, Knight, & D'Esposito, 2005). Unfortunately, most fMRI studies of perceptual or category learning using motion-dot stimuli did not examine the left and right MT hemispheres separately and did not report differential effects of category and stimulus across hemispheres. Future studies or meta-analytic studies could examine whether or not the left or right MT is more strongly modulated by task demands or if the lateralized modulation of sensory cortices depends on the relative lateralized recruitment of control regions such as pFC.

Previous studies have found strong stimulus coding and category-related modulation stimulus representations during concept or perceptual learning (Ester, Sprague, & Serences, 2020; Braunlich & Love, 2019; Kuai, Levi, & Kourtzi, 2013; Mack et al., 2013; Zhang & Kourtzi, 2010; Freedman & Assad, 2006; Kourtzi, Betts, Sarkheil, & Welchman, 2005). For example, concept learning studies that used object stimuli have shown strong modulation of sensory signals in the lateral occipital cortex after learning (Braunlich & Love, 2019; Kuai et al., 2013; Mack et al., 2013).

One major difference between prior work and the current study is the probabilistic relationship between stimulus and feedback. In the world outside the laboratory, the relationship between stimulus and feedback is not always deterministic and people must make decisions and learn in the presence of this uncertainty. For example, after viewing dark clouds and the weather forecast, a person with picnic plans is faced with the decision of whether to continue. After deciding, they update their knowledge based on whether it rained, which is a probabilistic function of what was known at the time of decision.

Another key difference between our study with many studies of concept learning is that the response mapping was switched after each block so that we could observe possible differences between category representations and stimulus-response mappings. Some researchers suggest that changing the response mapping should disrupt procedural learning processes involved in concept learning (Maddox & Ashby, 2004), which is one reason why response mappings are often held constant within a participant.

These two differences with previous studies made it possible for us to observe a strong category signal that was not strictly modulated by stimulus representations, nor motor response. This category signal was of a different format than information related to stimulus or response. We need not have observed this finding. It would have been possible for the brain to solve this task using a stimulus-modulated category representation (i.e., stimulus and category represented in related formats) in which the response mapping varied across blocks. Instead, it appears that an intermediate category signal was used by participants. Although our design did not necessitate our main finding, it is possible that the relatively loose coupling between stimulus, category, and response encouraged forming a category representation of a different format than either stimulus or response. Many real-world categories may place related demands on learners. For example, relational categories, such as thief, are not closely tied to sensory representations (Jones & Love, 2007).

It may be argued that, because participants had to flip the category-motor mapping across blocks, we encouraged participants to use the stimulus or the category information and discouraged a motor-based strategy. However, it was still possible to ground category information into motor representations by associating sensory representations to the motor plan within a block and reprogram the association across blocks. Because there were relatively few blocks, this would have been possible—and a viable strategy. If the brain primarily relies on the sensory-motor association for the category representation and behavior, we would find representation of motor plans without an abstract category code (i.e., not tied to motor plans), which is not in line with our results. Furthermore, we showed evidence for an amodal category signal using a decoding approach that tested for a category signal over and above stimulus coding and also showed that the category signal was stronger than the motor code. To test the hypothesis that our design might have discouraged participants to use motor-based representations, future studies could compare groups that had to switch the motor responses versus those that did not and whether the latter group would form a grounded, motor-based neural representation for categorization in the absence of abstract category representations.

Some of our analyses yielded negative classification accuracy values, including in the abstract category and the direction classifier accuracies (Figure 4A and B). As noted in the Methods, the purpose of subtracting the category classifier from the classifier trained on the orthogonal bound was to find category signal over and above any sensory information contained in the voxels. Negative values would simply reflect no category information, in addition to more information across directions across the boundary orthogonal to the category bound (i.e., sensory biases in the voxels unrelated to the task). For the direction classifier, there were some regions that showed negative classification accuracy values. In this analysis, the theoretically lowest possible value is zero, and values around zero would reflect the absence of any direction information. We were unable to find anything systematic that contributed to the negative values and suggest that these effects were most likely attributable to reasons unrelated to the task, such as some nonstationarity across blocks.

There are similarities between our probabilistic conceptual learning paradigm and tasks learning the transition probability structure of object-to-object sequences. In those tasks, the probability that an Object A is most likely followed by an Object B (e.g., with a probability of .75) but could also be followed by another Object C (probability of .25)-that is, participants learn the statistical dependencies between objects, like how our participants learn the probabilistic dependencies between stimuli and categories. Interestingly, one study by Schapiro, Rogers, Cordova, Turk-Browne, and Botvinick (2013) showed participants learnt and accurately represent object-object associations with a structured community structure in several brain regions including the left pFC. Specifically, pattern similarity analysis showed that the left pFC, anterior temporal lobe, and superior temporal gyrus encoded the statistical, relational structure across the objects. Other studies found that the regions in the medial temporal lobe including the hippocampus and entorhinal cortex are involved in the learning and retrieval of associations and prediction of object-object transitions (e.g., Garvert, Dolan, & Behrens, 2017; Schapiro, Turk-Browne, Norman, & Botvinick, 2016). Because our current study focused on category representations after learning, it

would be interesting for future studies to test whether medial temporal lobe structures are involved in learning probabilistic conceptual structures in a similar way.

There are several open questions to be explored in the future. Our study was not optimized to study to role of the hippocampus in category learning, as we examined category representations after learning. Future studies could examine the neural representations involved in probabilistic concept learning early in learning and compare them to representations during categorization after learning is complete, to explore whether how the neural representations change as concept information is consolidated into long-term memory.

Future work could also assess the causal involvement of these abstract category representations in mMFG and MT. One idea would be to use TMS to disrupt the left mMFG and left MT to assess whether these areas act causally to support categorization behavior. It would be interesting to test whether mMFG or MT plays a more important role, by observing the fMRI signal after disruption. It could be that the mMFG is the origin of the category signal, but it is its influence on MT that leads to effective categorization behavior (e.g., TMS to mMFG leads to disruption of the MT category representation but not vice versa, where stimulation at both sites disrupts behavior).

What is the use of an abstract, symbol-like concept representation? In real-world scenarios, there are often no explicit rules and reliable feedback is rare. Building an abstract representation that can be mapped onto different contexts can be useful in real-world tasks, where the meaning of a situation can remain constant while the contextually appropriate stimulus or response changes. As we find here, the brain constructs an amodal, abstract representation with a different representational format separate from sensory–motor codes, well suited for flexible cognition in a complex world.

Acknowledgments

We thank Johan Carlin for his help on experimental design and data collection and Amna Ali for her help on data collection. We thank Kurt Braunlich for his advice on analysis tools. We thank the Love Lab for the helpful discussions on the project. We are grateful to the members of Cognitive Brain Mapping Lab at RIKEN BSI for sharing natural images used in this study.

Reprint requests should be sent to Robert M. Mok or Bradley C. Love, Department of Experimental Psychology, University College London, 26 Bedford Way, London, WC1H 0AP, UK, or via e-mails: robert.mok@ucl.ac.uk; b.love@ucl.ac.uk.

Funding Information

Royal Society (http://dx.doi.org/10.13039/501100000288), grant number: 18302. Wellcome Trust (http://dx.doi.org /10/13039/100004440), grant number: WT106931MA. National Institutes of Health (http://dx.doi.org/10.13039 /10000002), grant number: 1P01HD080679.

REFERENCES

Abraham, A., Pedregosa, F., Eickenberg, M., Gervais, P., Mueller, A., Kossaifi, J., et al. (2014). Machine learning for neuroimaging with scikit-learn. *Frontiers in Neuroinformatics*, *8*, 14. DOI: https://doi.org/10.3389/fninf.2014.00014, PMID: 24600388, PMCID: PMC3930868

Allison, T., Puce, A., Spencer, D. D., & McCarthy, G. (1999). Electrophysiological studies of human face perception. I: Potentials generated in occipitotemporal cortex by face and non-face stimuli. *Cerebral Cortex*, 9, 415–430. DOI: https:// doi.org/10.1093/cercor/9.5.415, PMID: 10450888

Avants, B. B., Epstein, C. L., Grossman, M., & Gee, J. C. (2008). Symmetric diffeomorphic image registration with crosscorrelation: Evaluating automated labeling of elderly and neurodegenerative brain. *Medical Image Analysis*, *12*, 26–41. **DOI:** https://doi.org/10.1016/j.media.2007.06.004, **PMID:** 17659998, **PMCID:** PMC2276735

Avants, B. B., Tustison, N., & Song, G. (2009). Advanced normalization tools (ANTS). *Insight Journal*, *2*, 1–35.

Barsalou, L. W. (1999). Perceptual symbol systems. *Behavioral and Brain Sciences*, 22, 577–609. DOI: https://doi.org/10 .1017/S0140525X99002149, PMID: 11301525

Barsalou, L. W. (2008). Grounded cognition. *Annual Review* of *Psychology*, 59, 617–645. **DOI:** https://doi.org/10.1146 /annurev.psych.59.103006.093639, **PMID:** 17705682

Behzadi, Y., Restom, K., Liau, J., & Liu, T. T. (2007). A component based noise correction method (CompCor) for BOLD and perfusion based fMRI. *Neuroimage*, *37*, 90–101.
DOI: https://doi.org/10.1016/j.neuroimage.2007.04.042,
PMID: 17560126, PMCID: PMC2214855

Bowman, C. R., & Zeithamova, D. (2018). Abstract memory representations in the ventromedial prefrontal cortex and hippocampus support concept generalization. *Journal of Neuroscience*, *38*, 2605–2614. DOI: https://doi.org/10.1523 /JNEUROSCI.2811-17.2018, PMID: 29437891, PMCID: PMC5858598

Braunlich, K., & Love, B. C. (2019). Occipitotemporal representations reflect individual differences in conceptual knowledge. *Journal of Experimental Psychology: General*, *148*, 1192–1203. DOI: https://doi.org/10.1037/xge0000501, PMID: 30382719, PMCID: PMC6586152

Chadick, J. Z., Zanto, T. P., & Gazzaley, A. (2014). Structural and functional differences in medial prefrontal cortex underlies distractibility and suppression deficits in aging. *Nature Communications*, 5, 4223. DOI: https://doi.org/10.1038 /ncomms5223, PMID: 24979364, PMCID: PMC4088291

Corbetta, M., Miezin, F. M., Shulman, G. L., & Petersen, S. E. (1993). A PET study of visuospatial attention. *Journal of Neuroscience*, *13*, 1202–1226. DOI: https://doi.org/10.1523
 /JNEUROSCI.13-03-01202.1993, PMID: 8441008, PMCID: PMC6576604

Cox, R. W., & Hyde, J. S. (1997). Software tools for analysis and visualization of fMRI data. *NMR in Biomedicine*, 10, 171–78.
DOI: https://doi.org/10.1002/(SICI)1099-1492(199706/08) 10:4/5<171::AID-NBM453>3.0.CO;2-L, PMID: 9430344

Cromer, J. A., Roy, J. E., & Miller, E. K. (2010). Representation of multiple, independent categories in the primate prefrontal cortex. *Neuron*, 66, 796–807. DOI: https://doi.org/10.1016/j .neuron.2010.05.005, PMID: 20547135, PMCID: PMC2909642

Davis, T., Love, B. C., & Preston, A. R. (2012a). Learning the exception to the rule: Model-based fMRI reveals specialized representations for surprising category members. *Cerebral Cortex*, 22, 260–273. DOI: https://doi.org/10.1093/cercor /bhr036, PMID: 21666132

Davis, T., Love, B. C., & Preston, A. R. (2012b). Striatal and hippocampal entropy and recognition signals in category learning: Simultaneous processes revealed by model-based fMRI. Journal of Experimental Psychology: Learning, Memory, and Cognition, 38, 821–839. DOI: https://doi.org /10.1037/a0027865, PMID: 22746951, PMCID: PMC3403290

- Dubner, R., & Zeki, S. M. (1971). Response properties and receptive fields of cells in an anatomically defined region of the superior temporal sulcus in the monkey. *Brain Research*, *35*, 528–532. **DOI:** https://doi.org/10.1016/0006-8993(71) 90494-X. **PMID:** 5002708
- Duncan, J. (2001). An adaptive coding model of neural function in prefrontal cortex. *Nature Reviews Neuroscience*, 2, 820–829. DOI: https://doi.org/10.1038/35097575, PMID: 11715058
- Duncan, J. (2010). The multiple-demand (MD) system of the primate brain: Mental programs for intelligent behaviour. *Trends in Cognitive Sciences*, 14, 172–179. DOI: https://doi .org/10.1016/j.tics.2010.01.004, PMID: 20171926
- Epstein, R., & Kanwisher, N. (1998). A cortical representation of the local visual environment. *Nature*, *392*, 598–601. **DOI:** https://doi.org/10.1038/33402, **PMID:** 9560155
- Erez, Y., & Duncan, J. (2015). Discrimination of visual categories based on behavioral relevance in widespread regions of frontoparietal cortex. *Journal of Neuroscience*, *35*, 12383–12393. **DOI:** https://doi.org/10.1523/JNEUROSCI .1134-15.2015, **PMID:** 26354907, **PMCID:** PMC4563032
- Esteban, O., Markiewicz, C. J., Blair, R. W., Moodie, C. A., Isik, A. I., Erramuzpe, A., et al. (2019). fMRIPrep: A robust preprocessing pipeline for functional MRI. *Nature Methods*, 16, 111–116.
 DOI: https://doi.org/10.1038/s41592-018-0235-4, PMID: 30532080, PMCID: PMC6319393
- Ester, E. F., Sprague, T. C., & Serences, J. T. (2020). Categorical biases in human occipitoparietal cortex. *Journal of Neuroscience*, 40, 917–931. DOI: https://doi.org/10.1523
 /JNEUROSCI.2700-19.2019, PMID: 31862856, PMCID: PMC6975303
- Fedorenko, E., Duncan, J., & Kanwisher, N. (2013). Broad domain generality in focal regions of frontal and parietal cortex. *Proceedings of the National Academy of Sciences*, U.S.A., 110, 16616–16621. DOI: https://doi.org/10.1073 /pnas.1315235110, PMID: 24062451, PMCID: PMC3799302
- Fodor, J. A. (1975). *The language of thought*. Cambridge, MA: Harvard University Press.
- Folstein, J. R., Palmeri, T. J., & Gauthier, I. (2013). Category learning increases discriminability of relevant object dimensions in visual cortex. *Cerebral Cortex*, 23, 814–823. DOI: https://doi .org/10.1093/cercor/bhs067, PMID: 22490547, PMCID: PMC3593573
- Fonov, V. S., Evans, A. C., McKinstry, R. C., Almli, C. R., & Collins, D. L. (2009). Unbiased nonlinear average age-appropriate brain templates from birth to adulthood. *Neuroimage*, 47(Suppl. 1), S102. DOI: https://doi.org/10.1016/s1053-8119 (09)70884-5
- Freedman, D. J., & Assad, J. A. (2006). Experience-dependent representation of visual categories in parietal cortex. *Nature*, 443, 85–88. DOI: https://doi.org/10.1038/nature05078, PMID: 16936716
- Freedman, D. J., & Assad, J. A. (2016). Neuronal mechanisms of visual categorization: An abstract view on decision making. *Annual Review of Neuroscience*, *39*, 129–147. **DOI:** https:// doi.org/10.1146/annurev-neuro-071714-033919, **PMID:** 27070552
- Garvert, M. M., Dolan, R. J., & Behrens, T. E. J. (2017). A map of abstract relational knowledge in the human hippocampal– entorhinal cortex. *eLife*, *6*, e17086. **DOI:** https://doi.org/10 .7554/eLife.17086, **PMID:** 28448253, **PMCID:** PMC5407855

Gazzaley, A., Cooney, J. W., McEvoy, K., Knight, R. T., & D'Esposito, M. (2005). Top–down enhancement and suppression of the magnitude and speed of neural activity. *Journal of Cognitive Neuroscience*, *17*, 507–517. **DOI:** https://doi.org/10.1162/0898929053279522, **PMID:** 15814009 Glasser, M. F., Sotiropoulos, S. N., Wilson, J. A., Coalson, T. S., Fischl, B., Andersson, J. L., et al. (2013). The minimal preprocessing pipelines for the Human Connectome Project. *Neuroimage*, *80*, 105–124. **DOI:** https://doi.org/10.1016 /j.neuroimage.2013.04.127, **PMID:** 23668970, **PMCID:** PMC3720813

 Goldman-Rakic, P. S. (1995). Cellular basis of working memory. *Neuron*, 14, 477–485. DOI: https://doi.org/10.1016/0896
 -6273(95)90304-6, PMID: 7695894

Gorgolewski, K., Burns, C. D., Madison, C., Clark, D., Halchenko, Y. O., Waskom, M. L., et al. (2011). Nipype: A flexible, lightweight and extensible neuroimaging data processing framework in Python. *Frontiers in Neuroinformatics*, *5*, 13. **DOI:** https://doi.org/10.3389/fninf.2011.00013, **PMID:** 21897815, **PMCID:** PMC3159964

Greve, D. N., & Fischl, B. (2009). Accurate and robust brain image alignment using boundary-based registration. *Neuroimage*, 48, 63–72. DOI: https://doi.org/10.1016 /j.neuroimage.2009.06.060, PMID: 19573611, PMCID: PMC2733527

Harnad, S. (1990). The symbol grounding problem. *Physica D: Nonlinear Phenomena*, 42, 335–346. **DOI:** https://doi.org /10.1016/0167-2789(90)90087-6

Hunter, J. D. (2007). Matplotlib: A 2D graphics environment. Computing in Science and Engineering, 9, 90–95. DOI: https://doi.org/10.1109/MCSE.2007.55

Jackson, J., Rich, A. N., Williams, M. A., & Woolgar, A. (2017). Feature-selective attention in frontoparietal cortex: Multivoxel codes adjust to prioritize task-relevant information. *Journal* of Cognitive Neuroscience, 29, 310–321. DOI: https://doi.org /10.1162/jocn a 01039, PMID: 27626230

Jenkinson, M., Bannister, P., Brady, M., & Smith, S. (2002). Improved optimisation for the robust and accurate linear registration and motion correction of brain images. *Neuroimage*, *17*, 825–841. DOI: https://doi.org/10.1016 /S1053-8119(02)91132-8. PMID: 12377157

Jenkinson, M., & Smith, S. (2001). A global optimisation method for robust affine registration of brain images. *Medical Image Analysis*, 5, 143–156. DOI: https://doi.org/10.1016/S1361-8415 (01)00036-6, PMID: 11516708

Jones, M., & Love, B. C. (2007). Beyond common features: The role of roles in determining similarity. *Cognitive Psychology*, 55, 196–231. DOI: https://doi.org/10.1016/j.cogpsych.2006 .09.004, PMID: 17094958, PMCID: PMC2096740

Kamitani, Y., & Tong, F. (2005). Decoding the visual and subjective contents of the human brain. *Nature Neuroscience*, 8, 679–685. DOI: https://doi.org/10.1038/nn1444, PMID: 15852014, PMCID: PMC1808230

Kanwisher, N., McDermott, J., & Chun, M. M. (1997). The fusiform face area: A module in human extrastriate cortex specialized for face perception. *Journal of Neuroscience*, *17*, 4302–4311. DOI: https://doi.org/10.1523/JNEUROSCI.17-11 -04302.1997, PMID: 9151747, PMCID: PMC6573547

Kastner, S., & Ungerleider, L. G. (2000). Mechanisms of visual attention in the human cortex. *Annual Review of Neuroscience*, 23, 315–341. DOI: https://doi.org/10.1146/annurev.neuro.23 .1.315, PMID: 10845067

Kourtzi, Z., Betts, L. R., Sarkheil, P., & Welchman, A. E. (2005). Distributed neural plasticity for shape learning in the human visual cortex. *PLoS Biology*, *3*, e204. **DOI:** https://doi.org /10.1371/journal.pbio.0030204, **PMID:** 15934786, **PMCID:** PMC1150289

Kruschke, J. K. (1992). ALCOVE: An exemplar-based connectionist model of category learning. *Psychological Review*, 99, 22–44. **DOI:** https://doi.org/10.1037/0033-295X.99.1.22, **PMID:** 1546117

Kuai, S.-G., Levi, D., & Kourtzi, Z. (2013). Learning optimizes decision templates in the human visual cortex. *Current*

Biology, *23*, 1799–1804. **DOI:** https://doi.org/10.1016/j.cub .2013.07.052, **PMID:** 24012311, **PMCID:** PMC5533590

Lanczos, C. (1964). Evaluation of noisy data. Journal of the Society for Industrial and Applied Mathematics, Series B: Numerical Analysis, 1, 76–85. DOI: https://doi.org/10.1137 /0701007

Love, B. C., Medin, D. L., & Gureckis, T. M. (2004). SUSTAIN: A network model of category learning. *Psychological Review*, *111*, 309–332. **DOI**: https://doi.org/10.1037/0033-295X.111.2.309, **PMID**: 15065912

Mack, M. L., Love, B. C., & Preston, A. R. (2016). Dynamic updating of hippocampal object representations reflects new conceptual knowledge. *Proceedings of the National Academy of Sciences*, U.S.A., 113, 13203–13208. DOI: https:// doi.org/10.1073/pnas.1614048113, PMID: 27803320, PMCID: PMC5135299

Mack, M. L., Preston, A. R., & Love, B. C. (2013). Decoding the brain's algorithm for categorization from its neural implementation. *Current Biology*, 23, 2023–2027. DOI: https://doi.org/10.1016/j.cub.2013.08.035, PMID: 24094852, PMCID: PMC3874407

Maddox, W. T., & Ashby, F. G. (2004). Dissociating explicit and procedural-learning based systems of perceptual category learning. *Behavioural Processes*, 66, 309–332. **DOI:** https:// doi.org/10.1016/j.beproc.2004.03.011, **PMID:** 15157979

Marcus, G. F. (2001). The algebraic mind: Integrating connectionism and cognitive science. Cambridge, MA: MIT Press. DOI: https://doi.org/10.7551/mitpress/1187.001.0001

Markman, A. B., & Dietrich, E. (2000). Extending the classical view of representation. *Trends in Cognitive Sciences*, 4, 470–475. DOI: https://doi.org/10.1016/S1364-6613(00)01559-X, PMID: 11115761

Mesulam, M. M. (1981). A cortical network for directed attention and unilateral neglect. *Annals of Neurology*, *10*, 309–325. **DOI:** https://doi.org/10.1002/ana.410100402, **PMID:** 7032417

Meyers, E. M., Freedman, D. J., Kreiman, G., Miller, E. K., & Poggio, T. (2008). Dynamic population coding of category information in inferior temporal and prefrontal cortex. *Journal of Neurophysiology*, *100*, 1407–1419. **DOI:** https:// doi.org/10.1152/jn.90248.2008, **PMID:** 18562555, **PMCID:** PMC2544466

Miller, E. K., & Cohen, J. D. (2001). An integrative theory of prefrontal cortex function. *Annual Review of Neuroscience*, 24, 167–202. DOI: https://doi.org/10.1146/annurev.neuro.24 .1.167, PMID: 11283309

Newell, A. (1980). Physical symbol systems. *Cognitive Science*, 4, 135–183. **DOI:** https://doi.org/10.1016/S0364-0213(80) 80015-2

Nosofsky, R. M. (1986). Attention, similarity, and the identification– categorization relationship. *Journal of Experimental Psychology: General*, *115*, 39–61. DOI: https://doi.org/10 .1037/0096-3445.115.1.39, PMID: 2937873

Pedregosa, F., Varoquaux, G., Gramfort, A., Michel, V., Thirion, B., Grisel, O., et al. (2011). Scikit-learn: Machine learning in Python. *Journal of Machine Learning Research*, 12, 2825–2830.

Peirce, J., Gray, J. R., Simpson, S., MacAskill, M., Höchenberger, R., Sogo, H., et al. (2019). PsychoPy2: Experiments in behavior made easy. *Behavior Research Methods*, *51*, 195–203. DOI: https://doi.org/10.3758/s13428-018-01193-y, PMID: 30734206, PMCID: PMC6420413

Power, J. D., Barnes, K. A., Snyder, A. Z., Schlaggar, B. L., & Petersen, S. E. (2012). Spurious but systematic correlations in functional connectivity MRI networks arise from subject motion. *Neuroimage*, *59*, 2142–2154. **DOI**: https://doi.org /10.1016/j.neuroimage.2011.10.018, **PMID**: 22019881, **PMCID**: PMC3254728

Pylyshyn, Z. W. (1984). Computation and cognition: Toward a foundation for cognitive science. Cambridge, MA: MIT Press.

- Rizzolatti, G., Riggio, L., Dascola, I., & Umiltá, C. (1987). Reorienting attention across the horizontal and vertical meridians: Evidence in favor of a premotor theory of attention. *Neuropsychologia*, 25, 31–40. DOI: https://doi. org/10.1016/0028-3932(87)90041-8, PMID: 3574648
- Roy, J. E., Riesenhuber, M., Poggio, T., & Miller, E. K. (2010). Prefrontal cortex activity during flexible categorization. *Journal of Neuroscience*, *30*, 8519–8528. DOI: https://doi .org/10.1523/JNEUROSCI.4837-09.2010, PMID: 20573899, PMCID: PMC3709835
- Schapiro, A. C., Rogers, T. T., Cordova, N. I., Turk-Browne, N. B., & Botvinick, M. M. (2013). Neural representations of events arise from temporal community structure. *Nature Neuroscience*, *16*, 486–492. **DOI**: https://doi.org/10.1038 /nn.3331, **PMID**: 23416451, **PMCID**: PMC3749823
- Schapiro, A. C., Turk-Browne, N. B., Norman, K. A., & Botvinick, M. M. (2016). Statistical learning of temporal community structure in the hippocampus. *Hippocampus*, *26*, 3–8. DOI: https://doi.org/10.1002/hipo.22523, PMID: 26332666, PMCID: PMC4715493
- Seabold, S., & Perktold, J. (2010). Statsmodels: Econometric and statistical modeling with Python. In *Proceedings of the* 9th Python in Science Conference (pp. 92–96). DOI: https:// doi.org/10.25080/Majora-92bf1922-011
- Seger, C. A., & Miller, E. K. (2010). Category learning in the brain. Annual Review of Neuroscience, 33, 203–219. DOI: https://doi.org/10.1146/annurev.neuro.051508.135546, PMID: 20572771, PMCID: PMC3709834
- Sigala, N., & Logothetis, N. K. (2002). Visual categorization shapes feature selectivity in the primate temporal cortex. *Nature*, 415, 318–320. DOI: https://doi.org/10.1038/415318a, PMID: 11797008
- Virtanen, P., Gommers, R., Oliphant, T. E., Haberland, M., Reddy, T., Cournapeau, D., et al. (2020). SciPy 1.0: Fundamental algorithms for scientific computing in Python. *Nature Methods*,

-,orret

17, 261–272. **DOI:** https://doi.org/10.1038/s41592-019-0686-2, **PMID:** 32015543, **PMCID:** PMC7056644

- Wang, J. X., Rogers, L. M., Gross, E. Z., Ryals, A. J., Dokucu, M. E., Brandstatt, K. L., et al. (2014). Targeted enhancement of cortical–hippocampal brain networks and associative memory. *Science*, *345*, 1054–1057. DOI: https://doi.org/10.1126/science .1252900, PMID: 25170153, PMCID: PMC4307924
- Waskom, M. (2020). An introduction to Seaborn—Seaborn 0.10.1 documentation. Statistical Data Visualization.
- Wolpert, D. M., & Ghahramani, Z. (2000). Computational principles of movement neuroscience. *Nature Neuroscience*, *3*, 1212–1217. DOI: https://doi.org/10.1038/81497, PMID: 11127840
- Wolpert, D. M., & Witkowski, J. (2014). A conversation with Daniel Wolpert. *Cold Spring Harbor Symposia on Quantitative Biology*, 79, 297–298. DOI: https://doi.org/10.1101/sqb.2014 .79.19, PMID: 26092903
- Woolrich, M. W., Ripley, B. D., Brady, M., & Smith, S. M. (2001). Temporal autocorrelation in univariate linear modeling of fMRI data. *Neuroimage*, 14, 1370–1386. DOI: https://doi.org /10.1006/nimg.2001.0931, PMID: 11707093
- Zeithamova, D., Mack, M. L., Braunlich, K., Davis, T., Seger, C. A., van Kesteren, M. T. R., et al. (2019). Brain mechanisms of concept learning. *Journal of Neuroscience*, *39*, 8259–8266.
 DOI: https://doi.org/10.1523/JNEUROSCI.1166-19.2019, PMID: 31619495, PMCID: PMC6794919
- Zhang, Y., Brady, M., & Smith, S. (2001). Segmentation of brain MR images through a hidden Markov random field model and the expectation–maximization algorithm. *IEEE Transactions* on Medical Imaging, 20, 45–57. DOI: https://doi.org/10 .1109/42.906424, PMID: 11293691
- Zhang, J., & Kourtzi, Z. (2010). Learning-dependent plasticity with and without training in the human brain. *Proceedings of the National Academy of Sciences, U.S.A.*, *107*, 13503–13508.
 DOI: https://doi.org/10.1073/pnas.1002506107, PMID: 20628009, PMCID: PMC2922179