Cross-Sectional and Longitudinal Assessment of the Ellipsoid Zone in Childhood-Onset Stargardt Disease

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ABSTRACT

PURPOSE: To evaluate the reliability of ellipsoid zone (EZ) loss width and area measurements from spectral domain optical coherence tomography (SD-OCT) images and track disease progression in childhood-onset Stargardt disease (STGD1).

METHODS: Children with molecularly confirmed STGD1 (n=46, mean age 12.4 years) underwent SD-OCT for the measurement of the transverse (width) loss of the EZ and *en face* analysis to quantify the area of EZ loss. All scans were analysed twice by two graders to evaluate reliability. The annual rate of EZ width and area loss were calculated.

RESULTS: The intragrader and intergrader reliability of transverse EZ loss and area of EZ loss measurements at baseline for both graders was 0.99. The mean annual rate of transverse EZ loss ($\pm$ SD) was 279.5 $\pm$ 259.9 µm/year. The mean rate of area of EZ loss ($\pm$ SD) was 1.20 $\pm$ 1.29 mm^2/year. The percentage transverse EZ loss was 10.2 $\pm$ 9.9 %/year, which was significantly lower than the area of EZ loss at 19.4 $\pm$ 16.3 %/year. High degree of interocular symmetry was observed.

CONCLUSIONS: This is a prospective study on the quantification of EZ loss in children with STGD1 and highlights the reliability of SD-OCT in measuring EZ loss. High intragrader and intergrader reliability was observed, with good ability to detect changes over time.

TRANSLATIONAL RELEVANCE: Measuring the area of EZ loss was more sensitive compared to transverse EZ width loss measurements and will be valuable for natural history studies and clinical trials requiring sensitive and reliable structural endpoints.

INTRODUCTION

Stargardt disease (STGD1; OMIM 248200) is the most common inherited macular dystrophy with a prevalence of 1 in 8000–10 000.[1-7] Onset is most commonly in childhood where patients present with bilateral central visual loss and characteristic macular atrophy with yellow–white flecks at the level of the retinal pigment epithelium (RPE) at the posterior pole.[1, 2, 5, 8, 9] STGD1 has an autosomal recessive mode of inheritance associated with disease-causing sequence variants in the ATP-binding cassette, subfamily A, member 4 (*ABCA4*) gene (MIM; 601691).[1, 10-13] *ABCA4* encodes the retinal specific transmembrane protein, [14, 15] which is localized to the rim of rod and cone outer segment discs and involved in the active transport of retinoids from photoreceptors to RPE.[14-16] ABCA4 dysfunction results in lipofuscin accumulation in the RPE[14, 17, 18] and toxic levels of lipofuscin in the RPE are associated with photoreceptor degeneration and ultimately RPE loss.[19-21]

A robust measurement of photoreceptor integrity is therefore crucial for monitoring disease progression and for the design of any treatment strategy. The ellipsoid zone (EZ) is a hyperreflective layer in the outer retina and has been associated with photoreceptor integrity and function. Spectral-domain optical coherence tomography (SD-OCT) enables *in vivo* high-resolution cross-sectional retinal images, allowing for quantitative assessments of the EZ including manual identification of the transverse EZ loss and delineation of the area of EZ loss from an *en face* image. The EZ has been characterized in STGD1[22-24] yet only one study has tracked progression by the presence or absence of the EZ using *en face* OCT.[25]

Despite increasing evidence that early-onset STGD1 belongs to the severe end of the spectrum of *ABCA4*-associated retinal phenotypes,[26,4,7] no studies have assessed the EZ cross-sectionally or longitudinally in an exclusively paediatric population. Measuring photoreceptor layer integrity in children would be valuable in understanding the natural history of STGD1 in young patients and help determine whether children have better retinal potential for therapeutic intervention. Here, we evaluate the reliability of both the width of transverse loss of EZ and the area of EZ loss from *en face* SD-OCT analysis, as well as track disease progression to determine whether the EZ could serve as a robust anatomic outcome measure in children with molecularly confirmed STGD1.

METHODS

This prospective observational study adhered to the tenets of the Declaration of Helsinki and was approved by the Moorfields Eye Hospital Ethics Committee. Informed consent and assent were obtained from parents and children, respectively, prior to entering the study.

Subjects

A total of 46 children (mean age at baseline, 12.4 years; range, 6-18) with molecularly confirmed STGD1, from 39 pedigrees, including 19 males and 27 females, were included in this study. **Table 1** summarizes the demographics and genetic findings for each subject.

SD-OCT Image Acquisition

All subjects underwent SD-OCT imaging using the Heidelberg Spectralis (Heidelberg Engineering, Heidelberg, Germany). A transfoveal horizontal line scan was acquired for the measurement of the extent of the transverse loss of the EZ. The protocol also included two horizontal volume scans centred at the fovea covering a 20°×20° area to enable an *en face* analysis for the measurement of the area of EZ loss. The first volume scan comprised of 49 horizontal B-scans with 124 microns interscan spacing, and the second comprised of 193 horizontal B-scans with 31 microns interscan spacing. The SD-OCT scans were automatically registered to a near-infrared reflectance (NIR-R) fundus image which was acquired simultaneously. All scans were obtained using the automatic retinal tracking (ART) mode and automatic registration was used for all follow-up scans.

SD-OCT Image Analysis

Images for each subject were analysed using the Heidelberg Eye Explorer software (Heidelberg Engineering, version 1.9.10.0) and were displayed in the 1:1 micron setting. The acquired transfoveal horizontal line scan was used to measure the extent of the transverse loss of the EZ. The nasal and temporal location of the EZ loss, identified as the point where the hyperreflective EZ was no longer discernible/continuous, was manually demarcated with the arrow tool. The caliper tool was then used to delineate the width of the transverse loss

of the EZ which was automatically calculated by the software. In all patients, with the exception of P2, no residual EZ structure was visible between the nasal and temporal borders. For consistency we decided to measure the EZW in the same way in P2 with 'foveal sparing', as undertaken in the rest of the cohort.

The acquired macula volume scans and associated NIR-R fundus image were used for *en face* analysis to measure the extent of the area of EZ loss. *En face* analysis was done manually by assessing each individual B-scan. All B-scans had a quality index greater than 25dB. The nasal and temporal location of the EZ loss for each consecutive B-scan was marked and the corresponding locations were annotated on the NIR-R fundus image. Once all the nasal and temporal borders were marked, the region finder tool was used to join the points delineating the area of EZ loss on the NIR-R fundus image and the area value was automatically calculated by the software. The denser scan when available was preferentially used for analysis. In a few patients the less dense scans were used because of better image quality (more reliable identification of EZ borders), since for the less dense scans it was easier to keep the ART at a higher value. In addition, having multiple scans at both baseline and follow-up made it easier to identify the exact same location for measuring EZW and track rate of progression over time, especially in cases where the single line scans were not over the same exact location at follow-up visit.

Baseline and follow-up line and volume scans from both eyes were analyzed twice in a masked fashion by two graders (PT and MG) to determine the reliability of both EZ measurements. Graders were masked to their previous measurements, as well as the measurement of the other grader. Measurements were repeated at least one week apart. Both graders have practised the method in ten scans (data not used for the study). The results were comparable between graders and so it was decided to apply the method to the study. In terms of expertise both graders are post-graduate students with 3 (PT) and 1.5 (MG) years of experience in clinical research in IRDs and retinal imaging.

All measurements, both at baseline and follow-up, given their transverse nature, were corrected using the ratio between the assumed axial length of the OCT system (24 mm) and

the actual axial length measurement for that eye (Zeiss IOL Master; Carl Zeiss Meditec, Dublin, CA).

Statistical Methods

The statistical analysis was carried out for transverse EZ loss measurements and area of EZ loss measurements using SPSS Statistics (Chicago, IL, USA). Significance for all statistical tests was set at $P < 0.05$. The Shapiro-Wilk test was used to test for normality for all variables.

A multilevel mixed-effects model was fitted with random grader and subject effects and intragrader and intergrader reliability were assessed by the intraclass correlation coefficient (ICC). The annual rate of transverse EZ loss and area of EZ loss was calculated for each eye.

The interocular symmetry was assessed with paired *t*-test for both, area and width measurements, at baseline and follow-up, as well as annual rates of EZ loss. Interocular correlation between eyes in the baseline measurements, follow-up measurements, and annual rate of transverse EZ loss and annual rate of area of EZ loss were assessed with Pearson's correlation coefficient.

The difference between eyes in the baseline measurement, follow-up measurement, and the annual rate of progression was assessed using the paired samples *t*-test. The correlations between eyes were assessed with the Pearson's correlation coefficient. Subsequently, the strength of the correlations between the baseline measurement and annual rate of progression, baseline measurement and age at baseline, as well as the age at baseline and annual rate of progression were assessed with the Pearson's correlation coefficient. Strong, moderate, and weak correlation was set as r>0.7, 0.7>r>0.5, and r<0.5, respectively.

RESULTS

Thirty-eight subjects (P1-P38) underwent baseline testing on both eyes and contributed to the reliability analysis at baseline. The data from 7 subjects (P39-P45) could not be analyzed as the baseline images showed the loss to extend beyond the SD-OCT scan limits. In contrast,

subject P46 who was asymptomatic when recruited and was followed up for 15 months, showed a healthy EZ at baseline and follow-up bilaterally, and thereby excluded from the analysis. Twenty-two of these subjects (P1-P22) also underwent follow-up testing on both eyes and contributed to the reliability analysis at follow-up to assess reliability at a later cross-section in time. Nine subjects either did not have follow-up visits (n=7) or their EZ loss extended beyond the area imaged with OCT (n=2), and thereby were excluded from longitudinal analysis. In patients P32-P38 (**Table 2**), missing measurements are due to the EZ loss extending beyond the scan borders; with the exception of P37 which was due to poor compliance at baseline image acquisition. Some patients have only an EZW - since technically it was easier to center the lesion for a single line scan, and they thereby lack an EZ area because the whole area of the lesion was not imaged in the volume scans (e.g. P33 and P34). All measured variables were normally distributed. **Table 2** summarizes all measurements.

Intragrader and Intergrader Reliability

Data from the right eye of all subjects was used for this analysis, after proving disease symmetry and in order to avoid any clustering effect. At baseline, the mean absolute difference in the transverse EZ loss on repeat measurement for grader 1 (PT) and grader 2 (MG) was $223.2 \pm 178.5 \mu m$ and $176.4 \pm 196.6 \mu m$ respectively, and *between* graders after averaging their two sets of measurements was $161.3 \pm 137.6 \mu m$. The intragrader ICC at baseline for both graders and the intergrader ICC was 0.99. At follow-up, the mean absolute difference in the transverse EZ loss on repeat measurement for graders 1 and 2 was $279.5 \pm 362.1 \mu m$ and $255.3 \pm 331.6 \mu m$ respectively, and *between* graders, after averaging their two sets of measurements, was $89.6 \pm 79.1 \mu m$. The intragrader ICC at follow-up for both graders was 0.98, and intergrader ICC was 0.99.

At baseline, the mean absolute difference in the area of EZ loss on repeat measurement for graders 1 and 2 was 0.42 ± 0.38 mm^2 and 0.41 ± 0.39 mm^2 respectively, and *between* graders, after averaging their two sets of measurements, was 0.28 ± 0.33 mm^2. The intragrader ICC at baseline for both graders and the intergrader ICC was 0.99. At follow-up the mean absolute difference in the area of EZ loss on repeat measurement for graders 1 and 2 was 0.43 ± 0.38 mm^2 and 0.55 ± 0.76 mm^2 respectively, and *between* graders, after averaging their two sets

of measurements, was 0.23 ± 0.24 mm^2. The intragrader and the intergrader ICC at follow-up for both graders was 0.99.

Interocular Symmetry

Data from the 22 subjects (P1-P22) with baseline and follow-up testing on both eyes were analyzed further to assess interocular symmetry.

The mean absolute difference after averaging all four baseline measurements (2 from each observer) of the transverse EZ loss between eyes was 289.0 ± 291.3µm; and in the follow-up measurement was 176.4 ± 168.5µm. The mean difference in the annual rate of transverse EZ loss between eyes was 158.9 ± 194.6µm/year. There was no statistically significant difference between eyes in the baseline measurement (P = 0.092), follow-up measurement (P = 0.209), and annual rate of EZ loss width (P = 0.726). There was a strong positive correlation between eyes in the baseline measurement (r = 0.95), follow-up measurement (r = 0.98), and annual rate of transverse EZ loss (r = 0.75).

The mean absolute difference in the baseline measurements of the area of EZ loss between eyes was 0.39 ± 0.33 mm^2 and in the follow-up measurement was 0.48 ± 0.46 mm^2. The mean difference in the annual rate of area of EZ loss between eyes was 0.21 ± 0.22 mm^2/year. There was no statistically significant difference between eyes in the baseline measurement (P = 0.75), follow-up measurement (P = 0.923), and annual rate of area of EZ loss (P = 0.424). There was a strong positive correlation between eyes in the baseline measurement (r = 0.99), follow-up measurement (r = 0.99), and annual rate of area of EZ loss (r = 0.94). **(Figure 1)**

Rate of Progression

A total of 29 subjects (P1-P22, P32-P38) (mean age at baseline, 12.7 years; range, 6-17) with both baseline and follow-up testing on at least one eye were included to determine the annual rate of progression. In subjects with testing on both eyes, one eye was chosen at random, given the symmetry between eyes, for the examined parameters. The mean follow-up period for this subgroup was 27 months (range, 12-52 months). **Figure 2** shows representative examples of the variability in progression.

The mean annual rate of transverse EZ loss was 279.5 ± 259.9µm/year. The mean baseline measurement of the transverse EZ loss was 2939.9 ± 1294.0µm. There was a weak positive correlation (r = 0.15) between the baseline measurement and the annual rate of transverse EZ loss, and a weak negative correlation (r =-0.21) between the baseline measurement and age at baseline. There was no correlation between the age at baseline and annual rate of transverse EZ loss (r = -0.01).

The mean annual rate of area of EZ loss was 1.20 ± 1.29 mm^2/year. The mean baseline measurement of area of EZ loss was 6.43 ± 4.67 mm^2. There was a strong moderate positive correlation (r = 0.55) between the baseline measurement and the annual rate of area of EZ loss, and a weak negative correlation (r = -0.22) between the baseline measurement and age at baseline. There was no correlation between the age at baseline and annual rate of area of EZ loss (r = -0.03) **(Figure 2)**.

The mean annual rates of transverse EZ loss and area of EZ loss were 10.2 ± 9.9%/year and 19.4 ± 16.3 %/year respectively, which were significantly different (P = 0.004). **Figure 3** illustrates the variability in the percentage annual rate of loss.

DISCUSSION

This is the first prospective study on the characterization of the EZ in a large cohort of molecularly confirmed children with STGD1. The high intragrader and intergrader ICCs of both the transverse EZ loss and area of EZ loss measurements, as well as the ability to detect change over time, suggests the EZ could serve as a robust anatomic outcome measure in children.

There are no studies in children with STGD1 on the quantification of EZ loss both cross-sectionally, and longitudinally to determine rates of progression. One study which characterized the baseline transverse EZ loss in STGD1 subjects (mean age 34.4 years) showed the mean measurement was 3911 ± 1423µm.[27] In our study, although the mean age of the

cohort was notably younger (mean age 12.4 years), the mean baseline measurement of the transverse EZ loss was comparable (2939.9 $\pm$ 1294.0μm). However, no studies have previously assessed rate of progression of the transverse EZ loss over time in STGD1.

Only one study has assessed the area of EZ loss longitudinally in STGD1 subjects (mean age 33.0 years) and demonstrated a gradual expansion in the area of EZ loss of 0.31 mm^2/year, with the mean ($\pm$SD) initial area of EZ loss being 4.18 $\pm$1.91 mm^2.[25] In contrast, our study identified a higher mean baseline measurement (6.43 $\pm$ 4.67 mm^2), and notably the mean annual rate of area of EZ loss was more than 3 times faster (1.20 $\pm$ 1.29 mm^2/year). This is likely to be due to our cohort having earlier-onset disease associated with more rapid progression than adult cohorts.[4] This is also supported by the relatively high proportion (52%) of subjects harbouring severe disease-causing variants in our cohort that would be expected to affect splicing, or to introduce a premature truncating codon in the protein if translated.

All measurements were higher than the inherent variability in measurements taken from Spectralis images (lateral optical resolution=14μm). However, the data from 7 subjects (P39-P45) were excluded as the baseline images showed the loss to extend beyond the limits of the SD-OCT scan. Six of these subjects were aged 12 or younger at baseline. This indicates that the phenotype can be variable, with highly progressive disease from early childhood, highlighting the importance of analyzing children and adults independently, and that there is a group of children who have very rapidly progressive disease who would be ideal for clinical trials both in terms of rapid readouts and also potentially deriving the most benefit.

The intergrader and intragrader reliability of EZ area and transverse EZ measurements in this study were consistently excellent. The annual rate of transverse EZ loss was 10.2 $\pm$ 9.9%/year and the annual rate of area of EZ loss was significantly higher at 19.4 $\pm$ 16.3 %/year. Although both measurements are assessing the EZ, measuring transverse EZ loss is considerably quicker as only a single image is analysed. In contrast, EZ area measurements require several B-scans to be analyzed and therefore the resulting value is based on more than a single measurement. Assessing the area of EZ loss is more time consuming yet evidently may be twice as sensitive in measuring progression in children compared to measuring transverse EZ loss. Furthermore,

the area of EZ loss may provide greater statistical power to detect significant differences in a given sample and may also be a more robust outcome measure in observational studies or therapeutic trials. There are other potential endpoints derived from SD-OCT measurements under investigation in STGD1, including total macular volume.[28]

The annual rate of area of EZ loss showed a stronger correlation with the baseline measurement compared with the annual rate of transverse EZ loss; suggesting the area of EZ may be more valuable in assessing prognosis – with baseline EZ area better predictive of progression than baseline EZ width. However, both baseline measurements showed a weak negative correlation with age at baseline. These findings are in keeping with younger children presenting with larger width and area of EZ loss at baseline, leading to a higher annual rate of EZ loss. In other words, subjects with earlier onset present with a severe and rapidly progressive phenotype at the photoreceptor microstructural level, in keeping with other clinical parameters.[4] Given this greater rate of progression in children, they represent good candidates for therapeutic intervention, thereby highlighting the need to initiate structural assessments in cohorts of young children.

Interocular symmetry in terms of baseline measurements, follow-up measurements, and annual rate of loss was observed. Although both EZ measurements showed a strong correlation and no significant difference between eyes in the baseline measurement, follow-up measurement, and annual rate of loss, the EZ area measurements consistently showed a higher correlation between eyes. This is valuable for future treatment strategies both for stratification, since both eyes appear to have comparable potential, as well as for the use of the non-treated eye as 'control'.

Image quality affected subsequent analysis for both transverse and area EZ measurements. Poor image quality makes EZ borders on line scans less distinct. In addition, since scans for 15% of the subjects were excluded from analysis as the initial loss extended beyond the scan area, it is important to be aware of this potential limitation of the testing device for children with a severe phenotype/high rate of progression and those at advanced stages of disease. Widefield SD-OCT and swept-source OCT imaging may help address this limitation.

In conclusion, this is the first prospective study on the quantification of EZ loss in children with molecularly confirmed STGD1 and highlights the utility of SD-OCT in measuring EZ loss in young subjects. In this cohort, measuring the area of EZ loss was more sensitive compared with transverse EZ loss measurements, and will be valuable both for monitoring disease progression and clinical trials requiring a robust structural outcome measure.

[FIGURE LEGENDS]

Figure 1. Representation of interocular symmetry of EZ loss measurements of a 20 years old female (P6) with STGD1 at the 4 years follow-up visit. The areas of EZ loss are delineated with blue lines on the NIR-R images and the area imaged in the OCT B-scan below is represented with blue arrows. The blue arrows on the OCT images mark the boundaries of the EZ loss. The disease shows high interocular symmetry in this individual. All images on the first two rows are at the same scale. The delineated areas with the white rectangle are magnified (×3) in the third row.

Figure 2. Disease progression in two STGD1 patients. The areas of EZ loss are delineated with blue lines on the NIR-R images and the section imaged in the OCT B-scan below is represented with green lines. The blue arrows on the OCT images mark the boundaries of the EZ loss. Patient **(A)** is a 16 years old female (P11) with 24 months of follow-up. The disease was relatively stable for that patient with an annual rate of EZ area loss of $0.02mm^2$ and of EZ width expansion of 33µm/yr. Patient **(B)** is a 14 years old female (P5) with rapid disease progression over 38 months, with an annual rate of EZ area loss of $0.73mm^2$ and of EZ width loss of 128µm. The delineated areas with the white rectangles are magnified (×3) in the third row of panel (A) and (B).

Figure 3. Stacked scatterplot showing the variability of the percentage annual rate of change in transverse EZ loss and area of EZ loss. Values represent mean ± standard deviation.

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