# Investigation of Electromagnetic Interaction Between RF Coil & Graphene-based Electrophysiology Probes at 7 Tesla Preclinical MRI

Suchit Kumar<sup>1</sup>, Samuel M. Flaherty<sup>2</sup>, Alejandro Labastida-Ramírez<sup>2</sup>, Anton Guimerà Brunet<sup>3</sup>, Ben Dickie<sup>4</sup>, Kostas Kostarelos<sup>2</sup>, Rob C. Wykes<sup>1,2</sup>, Louis Lemieux<sup>1\*</sup>

<sup>1</sup>University College London Queen Square Institute of Neurology, London, UK

<sup>2</sup>Centre for Nanotechnology in Medicine & Division Neuroscience, University of Manchester, UK

<sup>3</sup>Centro de Investigación Biomédica en Red en Bioingeniería, Biomateriales y Nanomedicina (CIBER-BBN), Madrid, Spain

<sup>4</sup>Division of Informatics, Imaging and Data Sciences, University of Manchester, Manchester, UK

# Introduction

#### **Introduction to Graphene-Based Recording Technology:**

- New advancements in electrophysiological recording technology, specifically Graphene Solution-Gated Field-Effect Transistors (gSGFET) [1].
- gSGFETs offer several advantages over traditional electrodes, particularly in MRI settings.

#### **Advantages of gSGFET:**

- Reduced Metal Interference: Significantly lowers the amount of metal that can interfere with MRI scans.
- High-Fidelity Brain Signal Recording: Enables DC-coupled brain signal recording with high fidelity,
   specifically demonstrated in rodent models [2].

#### Importance of MRI Compatibility:

- Interest in performing MRI acquisitions on animals implanted with gSGFET probes.
- Ensuring MR compatibility and safety of these graphene-based EEG probes is crucial for research continuity and accuracy.

#### **Study Objective:**

- Computational Simulations: Conducted to assess the electromagnetic (EM) interaction and safety of animals implanted with these probes within an MRI environment.
- Goal: Achieving the highest possible level of MR compatibility for these advanced probes.

# Methods

#### **EM Simulation Analysis:**

- Technique used: Finite-Difference Time-Domain (FDTD).
- Software: Sim4Life (V8.0, ZMT, Switzerland).
- Model: 3D rodent model comprising 68 tissues [3, 4].

#### RF Transmission Coil Setup and Specifications:

- Type: Quadrature highpass birdcage RF coil.
- Coil dimensions: Diameter: 72 mm, Length: 72 mm.
- Shield dimensions: Diameter: 90 mm, Length: 225 mm.
- Coil structure: 8 rungs, each 9.9 mm wide.
- Tuning capacitor: 14.2 pF placed on the end-rings, which are 11.5 mm wide. See figure 1.

#### 3D Modeling of EEG Probes:

• Generated from 2D drawings and exported to CAD format.

#### Simulation Setup:

- Excitation parameters: 300 MHz Gaussian excitation with a bandwidth of 650 MHz, excited in two-port, combined in circular-polarized mode.
- Sub-gridding feature: Utilized for localized mesh refinement, obtained from ZMT.

# SAR Calculation:

• Specific Absorption Rate (SAR): Mean and peak SAR averaged over 0.01g, 0.1g, and 1g tissue-mass were calculated following IEC guidelines [5].

# tissue-mass were calculated following IEC guidelines [5].

# Results

# B<sub>1</sub>+-Field and E-Field Distributions:

**Results & Conclusions** 

- Increase in Magnitude: Graphene-based probes increase B1+ and E-field magnitudes by approximately 15-20% near the probes.
- Cause: Induced current in the metal layers of the probes during transmission (see *figure 2*).

# • SAR Distributions:

- Elevated SAR due to probes:
  - Mean Mass-Averaged SAR (W/kg): Without probe: 0.63; With probe: 0.83
  - Peak Mass-Averaged SAR (W/kg): **Without probe**: 0.01g: 2.5, 0.1g: 1.3, 1g: 0.8

With probe: 0.01g: 5.9, 0.1g: 2.8, 1g: 1.6 (see *figure 3*).

• Localization: SAR peak localized in the skin.

# Computational Time:

- With probe: Approximately 160 h / port; Without probe: Approximately 1.5 h / port.
- Note: Computational power limitations on a single GPU require cluster GPU implementation.

# Conclusions

- **EM Interaction:** Successfully demonstrated the electromagnetic interaction of graphene-based EEG probes in an MRI environment.
- **RF Transmission and SAR:** Graphene-based probes can affect RF transmission and increase SAR deposition while staying within permissible limits, ensuring MR compatibility and safety.

# Future Work:

- Optimization: Further work needed to optimize computational efficiency using GPU clusters.
- Experimental Verification: Necessary using phantom studies.
- Concurrent Studies: EEG-fMRI studies in vivo in normal and chronically epileptic rodents.
- Scaling: Potential scaling of these probes for human application.

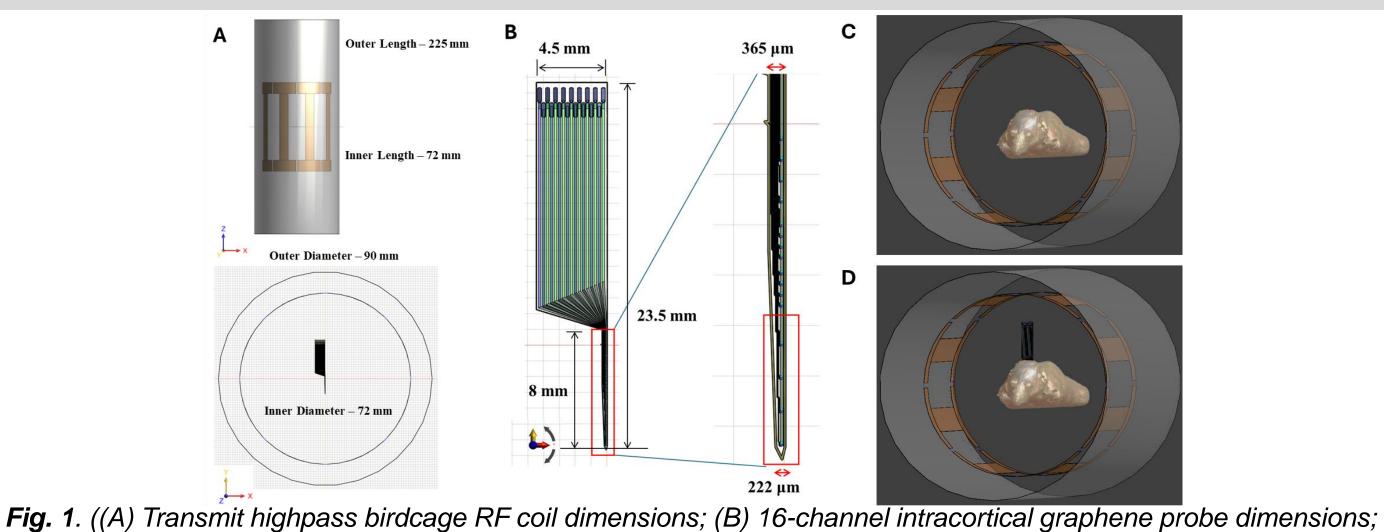
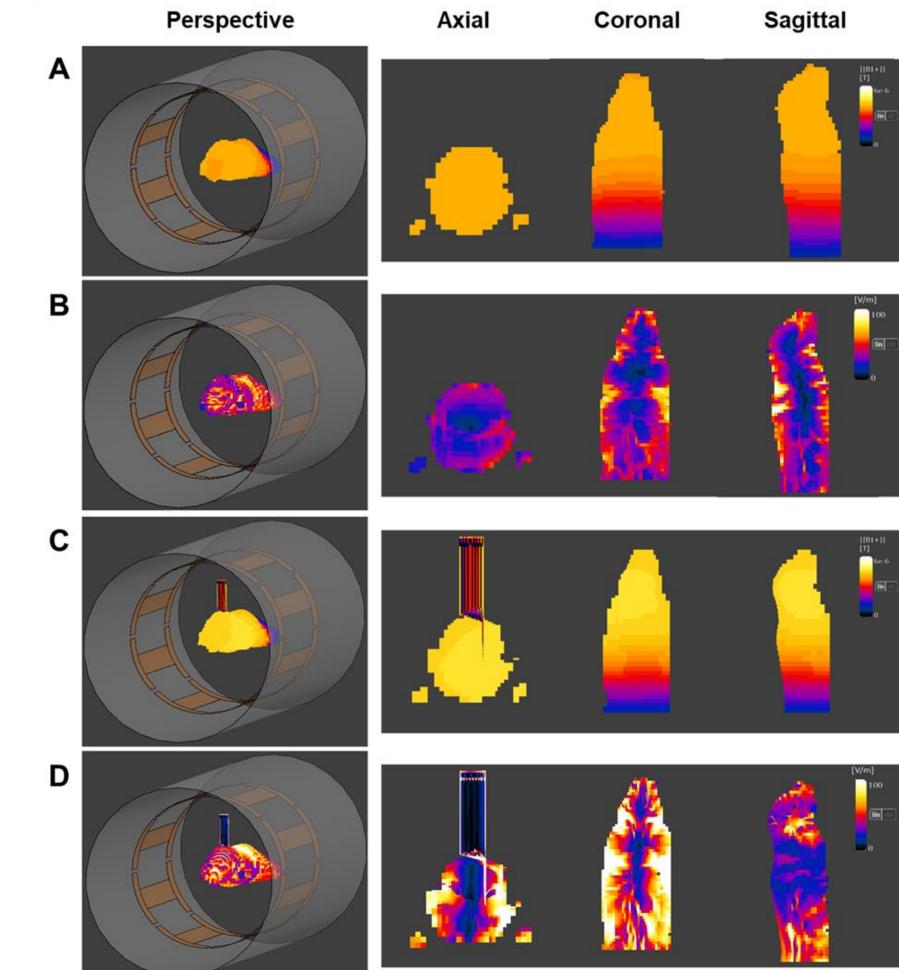
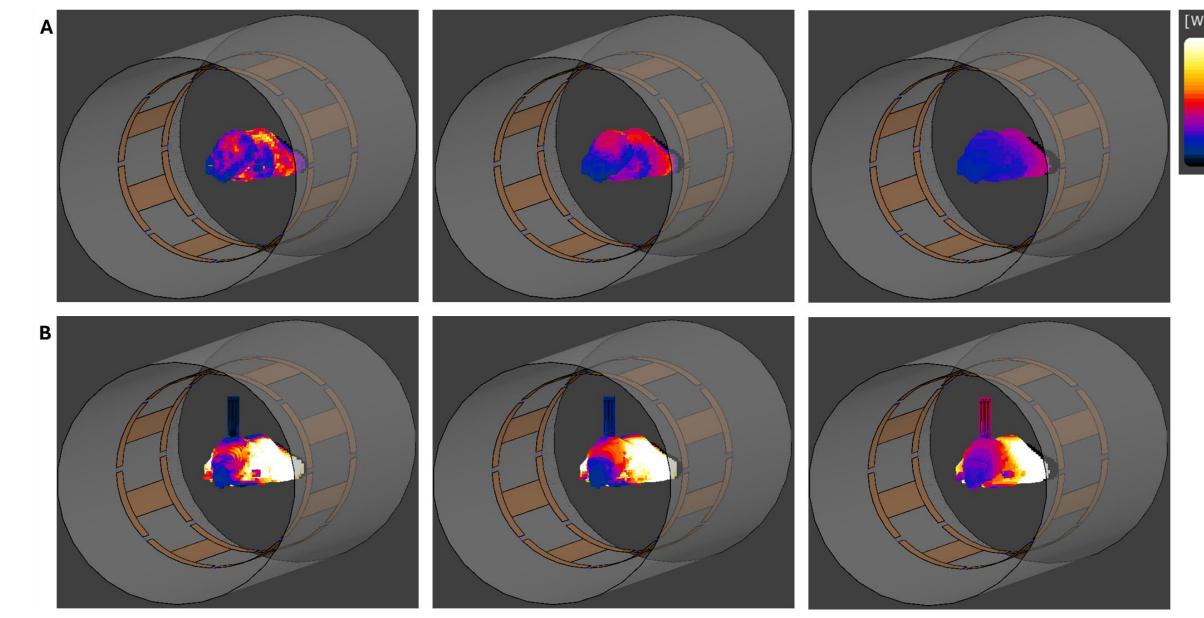


Fig. 1. ((A) Transmit highpass birdcage RF coil dimensions; (B) 16-channel intracortical graphene probe dimensions; (C) Configuration of rodent model placed in RF coil without, and (D) with graphene-based probe model as a brain implant.



**Fig. 2.** Simulated  $B_1^+$ -field distribution in rodent model (A) without, (C) with probe model; E-field distribution in rodent model (B) without, (D) with probe model.



**Fig. 3**. Simulated mass-avg SAR distribution in rodent model (A) without, (B) with EEG probe model for 0.01g (left), 0.1g (middle) and 1g (right) tissue mass.

**References:** [1] Bonaccini Calia, Andrea, et al. Nature Nanotechnology 17.3 (2022): 301-309. [2] Wykes, Rob C., et al. Clinical and Translational Medicine 12.7 (2022): 1-4. [3] Sim4Life, ZMT, <a href="http://www.zurichmedtech.com">http://www.zurichmedtech.com</a>. [4] Kainz, Wolfgang, et al. Physics in Medicine & Biology 51.20 (2006): 5211. [5] International Electrotechnical Commission (IEC) (2022): IEC 60601-2-33.

**Acknowledgements**: This project is funded by the EPSRC under grant no. EP/X013669/1. The authors are grateful for the support from Sim4life, ZMT for providing the science license.

