

Title:

Calibration of bioelectrical impedance analysis against deuterium dilution for body composition assessment in stunted Ugandan children

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Running title: BIA calibration in stunted Ugandan children

Abbreviations:

^2H	Deuterium
BC	Body composition
BIA	Bioelectrical impedance analysis
BMI	Body mass index
CS	Cross-sectional area
FFM	Fat-free mass
FFMI	Fat-free mass index
FM	Fat mass
FMI	Fat mass index
HAZ	Height-for-age z-score
ND	Deuterium dilution space
PA	Phase angle
R	Resistance
RMSE	Root-mean square error
SAM	Severe acute malnutrition
TBW	Total body water
WHO	World Health Organization
WHZ	Weight-for-height z-score
Xc	Reactance
Z	Impedance
Z ₅₀	Impedance, measured at 50 kHz

1 *Abstract (250 words):*

2 **Background.** Bioelectrical impedance analysis (BIA) represents an important tool in body
3 composition (BC) assessment, especially in low-income settings where simple and affordable
4 options are preferred. There is a particular need to measure BC in stunted children, where
5 population-specific BIA estimating equations are lacking.

6 **Objective.** We calibrated an equation to estimate body composition from BIA using
7 deuterium dilution (^2H) as the criterion method in stunted children.

8 **Methods.** We measured BC with ^2H and performed BIA in stunted Ugandan children ($n =$
9 50). Multiple linear regression models were constructed to predict ^2H -derived fat-free mass
10 (FFM) from BIA-derived whole-body impedance (Z_{50}) and other relevant predictors. Model
11 performance was expressed as adjusted R^2 and root-mean square error (RMSE). Prediction
12 errors were also calculated.

13 **Results.** Participants were aged 16 to 59 months, 46% were girls and their median [IQR]
14 height-for-age z-score (HAZ) was -2.58 [-2.92, -2.37] according to WHO growth standards.
15 Impedance index (height^2/Z_{50}) alone explained 89.2% variation in FFM and had an RMSE of
16 583 g (precision error 6.5%). The final model contained age, sex, impedance index and HAZ
17 as predictors, and explained 94.5% variation in FFM with an RMSE of 402 g (precision error
18 4.5%).

19 **Conclusion.** We present a BIA calibration equation for a group of stunted children with
20 relatively low prediction error. This may help evaluate the efficacy of nutritional
21 supplementation in large-scale trials in the same population.

22 *Key words: stunting, body composition, deuterium dilution, bioelectrical impedance analysis*

23

24 *Introduction*

25 Current estimates suggest around 150 million children below 5 years globally suffer from
26 stunting, a form of undernutrition defined as a height-for-age z-score (HAZ) < -2 SD
27 according to the WHO growth standards (1). Childhood stunting increases mortality and
28 morbidity risk, and is associated with poor physical and cognitive development, lower
29 schooling attainment and unmet potential of human capacity (2).

30 Direct assessment of body composition (BC) is important for monitoring of healthy growth in
31 stunted children, with fat and fat-free tissues contributing to different domains of health
32 status, such as immune function (3) and homeostatic metabolic capacity (4), respectively. For
33 cruder measurements of body mass index (BMI), calculated as weight divided by the square
34 of height, the reduced height of stunted children could result in an inaccurate estimation of
35 childhood adiposity. There are several alternatives for accurately measuring BC in pediatric
36 populations (5,6), including air-displacement plethysmography (7), dual-energy X-ray
37 absorptiometry (8,9) and isotope dilution (10–13). However, the large-scale use of such
38 techniques is complicated by high costs, bulky equipment and/or extensive training
39 requirements.

40 Bioelectrical impedance analysis (BIA) provides a cheap, portable and relatively easy-to-use
41 alternative for BC estimation, making it well suited to research and monitoring in low-income
42 settings. It has been used extensively to evaluate variability in BC in association with
43 undernutrition and efforts to prevent or treat it (14–18). BIA uses principles of conductivity
44 to measure the electrical impedance of a body, which can then be used to estimate total body
45 water (TBW) and subsequently fat-free mass (FFM) using age- and sex-specific FFM
46 hydration factors (19). In both BIA and isotope dilution methods, the 2-compartment model
47 of BC can be used to derive FM as the difference between weight and FFM. To ensure

48 accurate conversion of electrical impedance to TBW, a population-specific calibration
49 equation is constructed using a reference method of BC assessment (20). Many examples
50 exist of these equations (11,21–23), which may further include predictive variables such as
51 sex, age and anthropometric measurements. Paradoxically, however, populations with the
52 highest prevalence of stunting, who may stand to gain the most from improved accuracy in
53 BIA assessment, remain the most under-represented in such equations.

54 From a theoretical perspective, BIA relies on the assumption that the body represents a
55 uniform cylinder, with impedance varying directly in proportion with its length (indexed by
56 height) and inversely with its cross-sectional area (CS) (24). In reality, the limbs (with
57 relatively greater length and smaller CS) contribute substantially more to whole-body
58 impedance than the trunk (25). In stunted children, a reduced limb-to-height ratio is observed
59 (26–28), which likely introduces error to the BIA assessment in these children if equations
60 have been calibrated for non-stunted children. Furthermore, reliable conversion of TBW to
61 FFM relies on accurate tissue hydration constants, which may be perturbed in children
62 suffering from undernutrition (5,29). For this reason, the reporting of TBW in addition to
63 FFM is valuable.

64 The primary aim of the present study was to calibrate BIA to estimate TBW and FFM in
65 stunted Ugandan children aged 12-59 months, using deuterium dilution as the reference
66 method. As a secondary aim, we compared the performance of two other equations calibrated
67 by deuterium dilution in paediatric populations, developed by Masuda and Komiya (30)
68 (hereon referred to as the “Masuda equation”) for children in Japan and Essa’a *et al.* (31)
69 (hereon referred to as the “Essa’a equation”) for children in Cameroon. We hypothesized that
70 stunting impacts BC-BIA associations owing to characteristic differences in limb to height
71 ratio, and that our new equation would be more appropriate for our study population.

72 *Materials and Methods*

73

74 This study was designed as an amendment to The Role of Milk Protein and Whey Permeate
75 in Lipid-based Nutrient Supplements (LNS) on the Growth and Development of Stunted
76 Children in Uganda (MAGNUS) intervention trial (ISRCTN13093195) (32). The primary
77 outcomes of the MAGNUS study were change in knee-heel and total length in stunted
78 Ugandan children aged 12-59 mo over a 12-week intervention with one of four LNS
79 formulations in a 2x2 factorial design ($n = 4 \times 150$) or non-supplemented control ($n = 150$).
80 Data collection for the MAGNUS study took place between February 2020 and December
81 2020 at two sites within the Jinja District of Eastern Uganda. Inclusion criteria for the
82 original MAGNUS study were children living within the study catchment area, aged 12-59
83 mo, a HAZ < -2 according to the WHO growth standards (1), and the primary caregiver
84 willing to return for follow-up visits. Children with severe acute malnutrition (SAM), defined
85 as a mid-upper arm circumference (MUAC) < 115 mm or a weight-for-height z-score (WHZ)
86 < -3 or bipedal pitting oedema were excluded from the study and referred to a local hospital
87 for treatment. Children with medical complications, disabilities effecting eating or
88 anthropometric measurement, or an allergy to peanuts or milk were further excluded. The
89 current study took place in October – November 2021 at one of the MAGNUS study sites,
90 Buwenge health center IV. Potential participants who were still aged < 59 mo were identified
91 from the original MAGNUS register. From this list, a sample of eligible participants were
92 selected to cover a wide range of size and nutritional status across ages and sex. This strategy
93 ensures a calibration equation relevant across the full range of the specific population (33).
94 Relevant caregivers were contacted by telephone and invited for screening. Due to aging of
95 original MAGNUS participants, some children from the local health center aged 12-24 mo
96 were identified and invited for screening. To be eligible for inclusion, participants had to be

97 aged 12-59 mo with supporting documentation, still stunted with a HAZ <-2 (1), with their
98 primary caregiver having provided written informed consent to participate. Participants were
99 excluded if they presented with clinical signs of sickness or if they were SAM according to
100 the above criteria.

101

102 Ethical approval and Informed consent:

103 The amended study was conducted in accordance with the ethical principles stated in the
104 current version of the Declaration of Helsinki and all applicable local regulatory
105 requirements. The study amendment was approved by the School of Medicine Research
106 Ethics Committee at Makerere University (Ref. 2019-013) and The Ugandan National
107 Council of Science and Technology (Ref. SS 4927). Study information was delivered to
108 caregivers in the local languages of Lusoga, Luganda or English, as appropriate. Written
109 informed consent was obtained from willing caregivers on behalf of their child according to
110 local regulations. Study staff were all involved in the original MAGNUS study and
111 completed a five-day training program before data collection. All participants were tested for
112 malaria infection, and additionally for HIV if they had not been tested in the MAGNUS
113 study.

114

115 Bioelectrical impedance analysis

116 Participants arrived on the morning of the one-day examination fasted since the night before.
117 Directly after enrollment, all participants underwent BIA assessment by a single study nurse.
118 Whole-body impedance was measured at 50 KHz using Bodystat 500 instrumentation
119 (Bodystat, Isle of Man, UK), calibrated daily according the manufacturers' instructions.
120 Measurements took place with the child in a supine position on an insulated matt wearing

121 only dry loose-fitting clothes. A position score was assigned by the nurse, ideally requiring
122 straight arms and legs resting on the ground without limbs touching. Disposable small-sized
123 gel-adhesive electrodes were placed in tetrapolar ipsilateral formation, on the right-hand side
124 of the body. Specifically, two electrodes of one cable were attached behind the knuckle of the
125 middle finger and beside the ulna head, and two electrodes of the other cable were attached
126 behind the second toe and between the medial and lateral malleoli. To avoid electrical
127 interference, a minimum distance of 3 cm between electrodes was maintained. For
128 particularly small infants, the proximal electrode could be moved up the arm or leg to
129 maintain this distance. Impedance (Z), resistance (R), reactance (X_c) and phase angle (PA)
130 were recorded; Z and R to the nearest whole ohm (Ω), X_c to the nearest 0.1 Ω and PA to the
131 nearest 0.1°. A duplicate measurement was taken approximately three minutes after the first.
132 Accepted ranges for individual measurements were; 300 – 1600 Ω for R , 20.0 – 90.0 Ω for
133 X_c and 2.0 – 7.0° for PA . Measures had to be within these accepted ranges, plus duplicate R
134 and X_c measures had to be within 20.0 Ω and 10.0 Ω of each other, respectively. A third
135 measure was taken if any range requirement was violated and a mean average of two
136 appropriate readings used in analysis. The within-subject coefficient of variation for Z was
137 0.05%.

138

139 Anthropometric measurements

140 Participant weight was measured to the nearest 100 g in light clothing using digital scales
141 (SECA 874, Hamburg, Germany) which were calibrated daily. Length (<24 mo) or height
142 (\geq 24 mo) was measured to the nearest 1 mm using a wooden measuring board
143 (Shorrboards®, Maryland, USA). MUAC was measured at the midpoint between the
144 acromion and olecranon processes using a non-stretchable coloured UNICEF tape to the

145 nearest 1 mm. All measurements were performed in triplicate and the median used for
146 analysis.

147

148 Deuterium dilution technique

149 Deuterium doses were prepared at the Department of Biochemistry & Sports Science,
150 Makerere University, Uganda. Two dose sizes were prepared, appropriate for smaller and
151 larger children, respectively. For small doses, 99.8% deuterium oxide (Cambridge Isotope
152 Laboratories Inc., MA, USA) was passed through a 0.2- μ m syringe filter into a borosilicate
153 stock bottle and diluted to a target concentration of 7.4% (w/w) with bottled water (Rwenzori,
154 Uganda). The solution was divided into individual 11-ml dose bottles to deliver ~0.74 g of
155 D₂O. For large doses, the same process was followed but to a target concentration of 5.0%
156 (w/w). The solution was divided into individual 21-ml dose bottles to deliver ~1 g of D₂O.
157 Both dose sizes contained a D₂O dose of between 0.05 and 0.10 g per kg body weight
158 according to previous recommendations (34). Dose bottles were sealed, frozen at -20°C, and
159 transferred to the field site freezer. These bottles stayed frozen until required for use each
160 morning, unused doses were returned to the freezer for a maximum of three days before being
161 discarded. The three stages of the deuterium dilution technique; pre-dose saliva sampling,
162 dosing, and post-dose saliva sampling took place at separate workstations to avoid
163 contamination. New dry gloves were worn at all times when processing saliva samples.

164 After a 20-minute nil-by-mouth period was observed, pre-dose saliva samples were collected
165 using a cotton stick with a closed mouth. The cotton was removed from the stick and saliva
166 expressed using a 10-ml syringe into a labeled cryotube. For small doses, 10 ml 7.4%
167 deuterium solution was drawn into a syringe which was wiped dry and weighed in a ziplock
168 bag along with five pieces of gauze to the nearest 0.01 g using calibrated laboratory scales.

169 The remaining 1 ml of solution was pipetted into a cryotube for later analysis. For large
 170 doses, 1 ml 5.0% deuterium solution was pipetted from the dose bottle into a cryotube for
 171 later analysis. The bottle and remaining 20 ml of solution was weighed in a ziplock bag along
 172 with a drinking straw and five pieces of gauze as above.

173 Small doses were administered into the corner of the mouth using the syringe and large doses
 174 were consumed through the straw provided. In both cases, any spillage was collected on the
 175 pre-weighed gauze and finally all items were returned to the same pre-weighed bag to
 176 calculate the exact dose received. Participants fasted for 15 minutes post-dose and were
 177 monitored in case of regurgitation. Participants then ate one banana to standardize food
 178 consumption during the equilibration period. They also had access to bottled water
 179 (Rwenzori, Uganda), but consumption was measured by study staff and limited to <200 ml.
 180 After a 3-hour equilibration period under observation, a post-dose saliva sample was
 181 collected using the same method as for the pre-dose sample. Pre-dose saliva, dose samples
 182 and post-dose saliva were collected into separate ziplock bags, and stored in separate freezer-
 183 boxes for up to 6 hours on site before being transferred to a freezer at -20°C. The complete
 184 sample set was transferred to Makerere biorepository for freezing at -80°C, before being sent
 185 to Iso-Analytical Ltd., United Kingdom, for analysis.

186

187 Deuterium analysis

188 Deuterium enrichment of saliva was analysed by isotope-ratio mass spectrometry. Deuterium
 189 dilution space (N_D) was calculated by the plateau method using the following equation (34):

$$190 \quad N_D (\text{kg}) = ((T * A)/a) * ((E_D - E_T)/(E_S - E_P))$$

191 where T is the mass of dose consumed by the child, a is the portion of dose diluted for
 192 analysis in grams, A is the mass of tapwater for the dilution, and E is isotopic enrichment in

193 delta per mille (‰) where D, T, S and P refer to the samples of the dose, tap water, post-dose
194 saliva and pre-dose saliva respectively. TBW was calculated as $N_D/1.044$ to account for non-
195 aqueous proton exchange (35). TBW was converted to FFM using previously published age-
196 and sex-specific lean tissue hydration factors best suited to the age range of our sample (19)
197 and as recommended by the International Atomic Energy Agency (36). FM was the
198 difference between weight and FFM.

199

200 Statistical analyses

201 All statistical analyses and plots were performed using R version 4.2.1 (37), including the
202 *anthro*, *lmtest* and *ggplot* packages. Fat-free mass index (FFMI) and fat mass index (FMI)
203 were generated using the formulae:

$$204 \text{ FFMI (kg/m}^2\text{)} = \text{FFM} / \text{height}^2$$

$$205 \text{ FMI (kg/m}^2\text{)} = \text{FM} / \text{height}^2$$

206 Impedance index was calculated as H^2/Z_{50} , where H was height or length in cm and Z_{50} was
207 whole-body impedance in Ω measured at 50 kHz.

208 Descriptive statistics are presented as mean (SD) for continuous variables except age, weight
209 and height, which are presented as mean (range). Stunting categories were defined using
210 cutoffs of below -2 and below -3 z-scores for HAZ according to the WHO growth standards
211 (1) for moderate and severe stunting, respectively. Sex differences at baseline were tested
212 using linear model ANOVA and Pearson's Chi-squared tests as appropriate.

213 The calibration equation was developed iteratively using multiple linear regression models
214 using the full ($n = 50$) sample. FFM measured by deuterium dilution, the dependent variable,
215 was modelled by independent variables added into the model in a stepwise fashion.

216 Independent variables of interest were identified *a priori*, as was the decision to omit
217 participant weight from model selection. Likelihood ratio tests for nested models were used
218 to compare model performance and assess benefit of added terms. The stepAIC function
219 within the *MASS* package confirmed the final model with a forward and backward stepwise
220 approach. The independent variables of the full model were used to prepare an additional
221 model predicting TBW and a simple calibration equation, containing only H^2/Z_{50} , was also
222 generated for FFM and TBW. Model assumptions of linearity, and normality and
223 homoscedasticity of residuals were confirmed using *autoplot*. Multicollinearity between
224 independent variables was further ruled out. Adjusted R^2 (%), root mean square error (RMSE)
225 (kg), and percentage of prediction error (RMSE / mean tissue weight by 2H (kg) x 100) were
226 calculated for FFM to assess prediction error of the calibration equation.

227 The Masuda and Essa'a equations were identified following a literature search for age-
228 appropriate BIA calibrations, further restricted to those in which deuterium dilution was used
229 as the reference technique. They were applied to our sample to generate FFM and FM. Bland-
230 Altman plots were constructed to compare their performance against body composition as
231 measured by 2H dilution. Simple linear regression models were constructed to assess
232 correlation between the average value and difference between methods. A *P*-value of <0.05
233 was considered significant.

234

235

236

237 Results

238

239 A description of the study population is presented in **Table 1**. Of the 50 enrolled participants,
240 29 (58%) had taken part in the MAGNUS study and the remainder were newly recruited. The
241 MAGNUS study population in Buwenge was predominantly rural-dwelling, with few

242 mothers having received formal education and the local diet was low in animal-source foods.
243 The HAZ and WHZ of the current sample are comparable to the MAGNUS sample
244 (unpublished data, Grenov B & Friis H, University of Copenhagen, 2022). Most participants
245 were moderately stunted and one boy was moderately acutely malnourished.

246 The mean (sd) dose of deuterium was 1.22 (0.32) g/kg bodyweight. During the ^2H
247 equilibration period, participants consumed a median [IQR] of 65 [53, 118] ml of water. Boys
248 had 1.02 [95%CI: 0.31, 2.00] kg higher FFM and 0.87 [95%CI: 0.45, 1.28] kg/m² higher
249 FFMI than girls.

250 The equation containing impedance index only took the following form:

251

$$252 \text{ FFM (kg)} = 1.669 + 0.836 * (\text{H}^2 / \text{Z}_{50})$$

253

254 where height is measured in cm. This equation had an adjusted R² of 89.2% and an RMSE of
255 583 g, corresponding to a prediction error of 6.4% (**Table 2**). **Figure 1a** and **Figure 1b** show
256 the association between H²/Z₅₀ and FFM measured by ^2H . Following model selection, the
257 best performing model took the form:

258

$$259 \text{ FFM (kg)} = 3.796 + 0.214 * (\text{HAZ}) + 0.488 * (\text{Sex}) + 0.068 * (\text{Age}) + 0.400 * (\text{H}^2 / \text{Z}_{50})$$

260

261 where age was in months and sex was coded as female = 0 and male = 1. This full model
262 explained 94.5% variation in FFM, and had an RMSE of 402 g corresponding to a prediction
263 error of 4.6%. Each term in the model; LAZ, sex, age and impedance index, were
264 independent predictors of FFM and the addition of each term improved model performance
265 as tested by likelihood-ratio tests ($P < 0.001$). **Figure 1b** shows the association between FFM

266 measured by ^2H and estimated by the full BIA model. Accordingly, the same RMSE for FM
267 resulted in a prediction error of 16.7%. Equivalent model specifications for TBW are
268 presented in **Table 2**.

269 We tested for systematic differences between the methods with Bland-Altman plots. The
270 Masuda equation showed a small, non-significant underestimation of FFM by 119 g with
271 95% limits of agreement of -903; 665 g, compared to ^2H (**Figure 2a**). The reverse bias was
272 evident for FM (**Figure 2b**). Regression models did not detect an association between the
273 mean and difference of the Masuda equation- and ^2H -derived FFM ($P = 0.903$) or FM ($P =$
274 0.152). Bland-Altman plots for the Essa'a equation showed considerable underestimation of
275 FFM by 1708 g with 95% limits of agreement from -2969 to 447 g, compared to ^2H (**Figure**
276 **2c**). The reverse bias was evident for FM (**Figure 2d**). Regression models detected an inverse
277 association between the mean and difference of the two methods for FFM ($\beta = -256$ g, $P <$
278 0.001), and a borderline positive association for FM ($\beta = 249$ g, $P = 0.056$). Histograms of
279 residuals for impedance index-only and full models predicting FFM and TBW are presented
280 in **Supplementary figure 1**.

281

282

283 Discussion

284

285 In this study, we calibrated an equation to predict FFM from bioelectrical impedance
286 assessment in stunted Ugandan children using ^2H dilution as the criterion method. The simple
287 equation containing only impedance index as an independent variable performed well,
288 accounting for 89% of the variation in FFM. Similar equations calibrating BIA with ^2H in
289 children, relying on impedance index as a sole predictor, have R^2 ranging from 42% to 91%
290 (11,21,31,33,38–43), placing our equation well. The spread of data points from the
291 regression in **Figure 1a** and **Figure 1b** supports a strong performance across the full range of

292 FFM present in our sample. The addition of age, sex and LAZ into our model increased its
293 predictive performance to account for 94.5% variation in FFM, which remains strong
294 compared to existing fully-specified models (68% - 96%) (11,21,33,38–45). It should be
295 noted, however, that the majority of the previously calibrated equations are generated within
296 children over five years of age, often an easier age to achieve accurate BIA readings. This
297 improvement over our simple impedance index model is visualized by the residual reduction
298 in **Figure 1b** and **Supplementary figure 1**. The 402 g RMSE (4.6% prediction error) for
299 FFM in our full model is acceptable, but indicates some variation in BIA assessment at the
300 individual level. This is a well-established reality for BIA and supports its application in
301 group-level investigations and monitoring (46), moreover it should be noted that some of the
302 disagreement between techniques must relate to error in TBW assessment. Though the ideal
303 reference method from the perspective of BIA theory, as water is the primary conducting
304 substance in the body, deuterium dilution estimates TBW with an accuracy of 1-2% (47) for
305 reasons such as dosing inaccuracies and laboratory instrument error (48). Regardless of
306 methodology, such prediction error in TBW and hence FFM is propagated to FM estimation
307 with increased relative magnitude, owing to the fact that it is the minority component of body
308 weight. In the present case the prediction error for FM is 16.7% using the full equation,
309 although the magnitude of this prediction error could partly be explained by the relative
310 thinness of our stunted children.

311 Weight is often included in BIA calibration equations, offering a small improvement in R^2 .
312 However, our decision to omit weight from model selection was based on fundamental
313 principles of the technique. By including weight in the equation predicting FFM, the
314 calculation of FM from FFM and weight in the second step can result in an unwanted
315 autocorrelation across the two steps of FM prediction. The chosen approach allows more
316 independent assessment of the two components of body composition. The addition of HAZ

317 into our model increased adjusted R^2 by a further $\sim 1\%$ (**Table 2**), which we interpret as
318 suggesting the degree of stunting influences on the performance of BIA even within a wholly
319 stunted population, albeit to a small degree. The inclusion of a HAZ term into future
320 prediction equations would therefore be important in a population where the HAZ range
321 extended into non-stunted categories.

322 This is the first BIA calibration equation developed specifically for use in stunted children.
323 Being affordable and relatively simple to implement in low-income and field settings, BIA is
324 well-suited to populations with a greater stunting prevalence (46). The accuracy of BIA is
325 reliant on population-specific calibrations against a reference technique. With the presented
326 equation, we provide an opportunity for wider application of BIA in populations currently
327 under-represented by calibration equations and within whom body composition assessment is
328 increasingly recognized as valuable (5,27). As described by the nutrition transition (49), low-
329 income populations classically associated with nutritional deficits and higher rates of stunting
330 are increasingly exposed to energy-dense and nutrient-poor food. Accordingly, increasing
331 rates of overweight and obesity manifesting in the same individuals have particularly adverse
332 effects on the risk of non-communicable disease, termed a double-burden of malnutrition (3).
333 In these settings, body composition assessment appears to hold the key to understanding the
334 long-term consequences of catch-up growth (10,50). There has been a hesitancy in
335 recommending nutritional supplementation to combat stunting for fear of preferential accrual
336 of FM over FFM (51,52), and inadvertently contributing to the double burden³. Support for
337 this concern is mixed (53), and we anticipate this equation can be applied in further
338 investigations involving larger population samples to provide more concrete evidence of the
339 effects of nutritional supplementation in stunted children.

340 As a secondary aim, we compared the performance of two other calibration equations
341 generated in children using ^2H . The Masuda equation was developed in healthy Japanese

342 children aged 3 to 6 years and contained resistance index, weight, age and sex as independent
343 variables (30). The equation performed excellently in their own sample, accounting for 96%
344 of variation in TBW (our equation achieved 94% for TBW). The performance of the Masuda
345 equation for predicting FFM and FM in our children was excellent, as shown by Bland-
346 Altman comparison in **Figure 2a and Figure 2b**, respectively. The limits of agreement were
347 comparable to our own for FFM (-903; 665 g vs. -801; 792 g) and showed no bias across the
348 range of FFM. The Masuda children were overall older, taller and heavier (mean: ~5 years;
349 ~109 cm; ~20 kg) and based on a crude assessment of means were within expected growth
350 norms according to WHO standards. To interpret the performance, we believe it relevant to
351 consider the potential for similarities in body proportions between our stunted Ugandan
352 children and healthy Japanese children. A recent population-based study has shown Japanese
353 and Ugandan adolescents to have similar height deficits compared to the WHO reference
354 (54). This suggests that while the stunting prevalence of Japanese children may be low, other
355 sources of height variability may be sufficiently powerful to create similarities in limb
356 development compared to stunted children elsewhere. Supporting this notion, recently
357 published reference values have shown that Japanese children have relatively shorter legs
358 compared to British children from birth to 12 years, irrespective of height (55).

359 The Essa'a equation was developed in Cameroonian children aged 2 to 5 years, with a mean
360 (sd) weight of 16.7 (2.0) kg and height of 107.0 (6.3) cm, i.e. heavier and taller than our
361 population, and contained resistance index, weight, age and height as independent variables
362 predicting TBW (31). Although one might expect this demographic to compare more
363 similarly to our own, the equation performed poorly in our sample, substantially
364 underestimating FFM with a bias towards underestimating further at greater levels of FFM
365 (**Figure 2c, Figure 2d**) making it unsuitable for use. The equation also did not perform well
366 in the sample from which it was generated, accounting for 68% of variation in TBW, which

367 could begin to explain its performance in ours. The mean (sd) HAZ of the Essa'a sample was
368 0.66 (1.35) z-scores above the WHO median and therefore much greater than our children.
369 We originally hypothesized that altered limb to trunk proportions in stunted children could be
370 an important consideration in a calibration equation, which is perhaps evidenced here and is
371 further supported by the significant HAZ term in our own equation.

372 A strength of our study was the use of ^2H dilution as the criterion method, with proven
373 agreement with the gold-standard four-component model (56). The quality of our BIA
374 measurements was also high, with all position scores achieving an "ideal" rating, inter-
375 observer variability removed due to a single trained nurse performing all assessments, and
376 intra-observer variation minimal. This is an important consideration for future studies
377 utilizing the equation, in which the accuracy and standardization of BIA measurements
378 should be a priority. Factors critical to BIA methodology in children have been discussed in a
379 recent review and include electrode placement, voiding, skin preparation and body position
380 (57). However, with adequate standardization and training with these factors in mind, inter-
381 measurer CVs of 2.6% and 0.2% for R have been achieved in neonates and children,
382 respectively (58,59). The careful sample selection ensured that we had good coverage across
383 wide ranges of age, weight and height in each sex.

384 Regarding limitations of the study, many BIA calibration studies perform a form of cross-
385 validation to assess the performance of the final equation on a different sub-sample of the
386 population. We took the decision to avoid such a validation technique due to our sample size,
387 instead opting to allocate all data points ($n = 50$) to equation generation. We also carefully
388 selected the sample across a wide range of nutritional status, in order to ensure high accuracy
389 of the equation in thinner and heavier children. Although this could be seen as a weakness of
390 the study, the equation would likely have been similar, but due to the smaller sample size the
391 RMSE would have been greater, and confidence in each coefficient would have been lower.

392 Nevertheless, one may consider the lack of cross-validation as a preclusion to comparing this
393 equation's performance with others as we have done. The predictive error between BIA
394 devices has been discussed in various reviews (57,60), and should be considered when
395 comparing BC studies. However, the devices used in our study and the compared studies
396 have important commonalities, namely a single (50 kHz)-frequency whole-body assessment
397 with hand-hand and foot-foot electrode placement, which provides a good foundation for
398 comparison. We intended to generate an equation relevant for ages one to five years but were
399 unable to recruit children below 16 months. The performance of the equation along the full
400 range of FFM without bias, though, encourages us to believe it remains relevant for
401 application in children from 12 months. Although this study was designed to maximize the
402 predictive ability of the generated equation among the stunted population of the MAGNUS
403 intervention trial, the inclusion of non-stunted children from the same population would have
404 strengthened our investigation and may have provided further evidence that stunted linear
405 growth influences BIA-BC assessment. It may be further argued that the applicability of our
406 equation may falter longitudinally as children recover from stunting. Further investigations to
407 test our hypothesis are therefore encouraged.

408 In conclusion, we have developed a prediction equation for estimating body composition
409 from bioelectrical impedance, which may perform well in stunted Ugandan children. The
410 study supports the use of BIA as a reliable technique in a low-income setting where children
411 may have higher rates of stunting and that stunting may affect the prediction of TBW from BIA
412 assessment.

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419

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421 the study; JIL and JW analyzed the data; JIL, HF, JW and BG interpreted the data; JIL
422 drafted the manuscript, which has been critically reviewed and approved by all authors.

423 Data described in the manuscript, code book, and analytic code will be made available upon
424 request pending application and approval.

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Tables and figures

Table 1. Characteristics of 50 stunted Ugandan children aged 16-59 months¹

	Male (<i>n</i> = 27)	Female (<i>n</i> = 23)	<i>P</i> -value
Age (months)	37 (17 - 59)	37 (16 - 56)	0.940
Anthropometrics			
Weight (kg)	11.8 (7.3 - 15.0)	10.9 (6.7 - 13.8)	0.243
Height (cm)	86.0 (72.0 - 98.2)	84.3 (66.7 - 96.5)	0.508
Mid-upper arm circumference (cm)	14.9 (1.0)	14.5 (1.2)	0.248
Body mass index (kg/m ²)	15.9 (1.0)	15.3 (0.9)	0.062
Height for age	-2.71 (0.55)	-2.81 (0.89)	0.853
Weight for height	-0.24 (0.82)	-0.39 (0.69)	0.500
Body mass index for age	0.15 (0.80)	-0.09 (0.68)	0.262
Height-for-age Z category			
Moderate stunting	22 (82%)	18 (78%)	0.777
Severe	5 (19%)	5 (22%)	
Weight-for-height Z category			
≥0	11 (41%)	8 (35%)	0.560
-2 to <0	15 (56%)	15 (65%)	
-3 to <-2	1 (4%)	0 (0%)	
Body composition (² H)			
Fat-free mass (kg)	9.5 (1.9)	8.5 (1.6)	0.046
Fat mass (kg)	2.3 (0.7)	2.5 (0.7)	0.298
Fat-free mass index (kg/m ²)	12.7 (0.7)	11.9 (0.7)	<0.001
Fat mass index (kg/m ²)	3.2 (0.8)	3.5 (0.8)	0.143
Body fat (%)	19.7 (4.5)	22.6 (4.4)	0.023
Bioelectrical impedance			
Impedance, Z ₅₀ (Ω)	803 (70)	895 (93)	0.001
Impedance index (H ² /Z ₅₀)	9.4 (2.0)	8.1 (2.0)	0.033

¹Presented as mean (range), mean (sd) or n (%), as appropriate; Age, Weight and Height presented as mean (range)

Table 2. Multiple regression analyses of sex, age (months), impedance index (H^2/Z_{50}) and height-for-age as predictors of total body water and fat-free mass (kg) as measured by 2H -dilution in 50 stunted Ugandan children aged 16-59 months

<i>Equation</i>	Adjusted R ²	RMSE (g)	Prediction error (%)
Predicting FFM			
1.669 + 0.836*(H^2/Z_{50})	0.892	583	6.5
5.065 + 0.984*(sex) + 0.119*(age)	0.868	638	7.1
2.756 + 0.406*(sex) + 0.059*(age) + 0.485*(H^2/Z_{50})	0.941	421	4.7
3.796 + 0.488*(sex) + 0.068*(age) + 0.400*(H^2/Z_{50}) + 0.214*(HAZ)	0.950	402	4.5
Predicting TBW			
1.486 + 0.628*(H^2/Z_{50})	0.893	435	6.2
4.042 + 0.720*(sex) + 0.089*(age)	0.858	496	7.1
2.239 + 0.269*(sex) + 0.042*(age) + 0.379*(H^2/Z_{50})	0.937	326	4.7
3.050 + 0.333*(sex) + 0.049*(age) + 0.312*(H^2/Z_{50}) + 0.167*(HAZ)	0.942	311	4.4

Sex coded as male = 1, female = 0.

FFM Fat-free mass, H^2 height squared, HAZ height-for-age z-score, RMSE root mean square error, TBW total body water, Z_{50} impedance at 50 KHz

Figure 1

A) Fat-free mass measured by ^2H dilution plotted against impedance index (H^2/Z_{50}) among 50 stunted Ugandan children aged 16-59 months. Grey shading represents 95% confidence error of estimate. **B)** Fat-free mass estimated by newly generated bioelectrical impedance equation plotted against fat-free mass measured by ^2H dilution among 50 stunted Ugandan children aged 16-59 months. Grey shading represents 95% confidence error of estimate. BIA bioelectrical impedance analysis.

Figure 2

Bland-Altman plots of 50 stunted Ugandan children aged 16-59 months comparing **A)** fat-free mass estimated by the Masuda bioelectrical impedance equation and measured by ^2H dilution, **B)** fat mass estimated by the Masuda bioelectrical impedance equation and measured by ^2H dilution, **C)** fat-free mass estimated by the Essa'a bioelectrical impedance equation and measured by ^2H dilution, **D)** fat mass estimated by the Essa'a bioelectrical impedance equation and measured by ^2H dilution. Dotted lines represent ± 1.96 SD limits of agreement. Regression line presented with 95% confidence error of estimate.