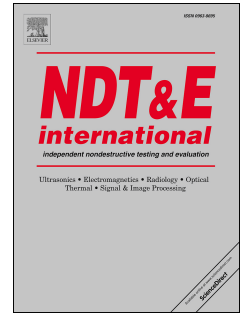


# Journal Pre-proof

Quantification of porosity in composite plates using planar X-ray phase contrast imaging

D. Shoukroun, L. Massimi, M. Endrizzi, A. Nesbitt, D. Bate, P. Fromme, A. Olivo



PII: S0963-8695(23)00150-0

DOI: <https://doi.org/10.1016/j.ndteint.2023.102935>

Reference: JNDT 102935

To appear in: *NDT and E International*

Received Date: 15 December 2021

Revised Date: 7 November 2022

Accepted Date: 6 August 2023

Please cite this article as: Shoukroun D, Massimi L, Endrizzi M, Nesbitt A, Bate D, Fromme P, Olivo A, Quantification of porosity in composite plates using planar X-ray phase contrast imaging, *NDT and E International* (2023), doi: <https://doi.org/10.1016/j.ndteint.2023.102935>.

This is a PDF file of an article that has undergone enhancements after acceptance, such as the addition of a cover page and metadata, and formatting for readability, but it is not yet the definitive version of record. This version will undergo additional copyediting, typesetting and review before it is published in its final form, but we are providing this version to give early visibility of the article. Please note that, during the production process, errors may be discovered which could affect the content, and all legal disclaimers that apply to the journal pertain.

© 2023 Published by Elsevier Ltd.

# 1 Quantification of Porosity in Composite Plates using Planar X-ray Phase Contrast Imaging

2  
3 D. Shoukroun<sup>1,2</sup>, L. Massimi<sup>1</sup>, M. Endrizzi<sup>1</sup>, A. Nesbitt<sup>3</sup>, D. Bate<sup>4</sup>, P. Fromme<sup>2</sup>, A. Olivo<sup>1</sup>

4 <sup>1</sup> Department of Medical Physics and Biomedical Engineering, University College London,  
5 WC1E 6BT, UK

6 <sup>2</sup> Department of Mechanical Engineering, University College London, WC1E 6BT, UK

7 <sup>3</sup> Department of Materials, University of Manchester, M13 9PL, UK

8 <sup>4</sup> Nikon, X-Tek Systems Ltd., Tring, Hertfordshire, HP23 4JX, UK

9 **Contact Author:** D. Shoukroun, [dana.shoukroun.17@ucl.ac.uk](mailto:dana.shoukroun.17@ucl.ac.uk)

## 10 11 Abstract

12 The application of planar Edge-Illumination X-ray Phase-Contrast imaging (EI-XPCi) for the  
13 non-destructive quantification of porosity in carbon fiber reinforced polymer (CFRP)  
14 specimens, a significant concern in aerospace applications, was investigated. The method  
15 enables fast, planar (2D) scans providing access to large samples. A set of woven CFRP plates  
16 with porosity content ranging from 0.7% to 10.7% was examined. In addition to standard X-  
17 ray attenuation, EI-XPCi provides differential phase and dark-field signals, sensitive to  
18 inhomogeneities and interfaces at scales above and below the system spatial resolution,  
19 respectively. The correlation with the porosity content from matrix digestion obtained from  
20 the dark-field signal was comparable to that from ultrasonic attenuation. The novel analysis  
21 of the standard deviation of differential phase (STDP), sensitive to inhomogeneities above  
22 the system resolution (approximately 12  $\mu\text{m}$ ), resulted in a very high correlation ( $R^2 = 0.995$ )  
23 with the matrix digestion porosity content, outperforming ultrasonic attenuation  
24 measurements.

25  
26 **Keywords:** Composites, CFRP, Porosity, Voids, Radiography, XPCi, Ultrasound

## 27 28 1. Introduction

29 Porosity and voids are a known problem for carbon fiber reinforced polymer (CFRP)  
30 structures that occurs during the manufacturing process [1]. Most non-destructive  
31 evaluation (NDE) techniques concentrate on the detection and quantification of porosities  
32 in the 1-5% range, with porosity levels above 2% typically considered not acceptable by the  
33 aerospace industry [2, 3]. CFRP porosity mainly affects mechanical properties, and studies  
34 have investigated void formation and distribution in composite samples, for different  
35 layups, processing parameters, and manufacturing techniques [4]. Accurate knowledge of  
36 void size, shape, and location is required for stress analysis to evaluate the influence on  
37 mechanical properties [5]. Matrix (acid) digestion is one of the commonly employed  
38 methods to evaluate porosity in composite plates [5], specified in relevant standards [6].  
39 However, it is destructive, and its accuracy depends on accurate knowledge of the  
40 properties of the composite constituents and the employed method [5]. The most common  
41 NDE methods include X-ray computed tomography (CT) [7-9] and ultrasonic testing [10-12].  
42 X-ray CT imaging offers high resolution and a reliable characterization of the pore size and  
43 shape distribution, but it is time consuming and has severe limitations on the sample size to  
44 achieve the required resolution. Ultrasonic attenuation measurement is a practical and cost-  
45 effective technique with approximately linear correlation to porosity content, but has lower  
46 resolution [2]. Ultrasonic C-scans allow the localization and sizing of larger voids, depending  
47 on the employed frequency and thus resolution [13]. Active infrared thermography has been  
48 shown to similarly allow for the nondestructive localization and sizing of voids above 0.2  
49 mm size in plate specimens [14]. The accuracy and repeatability of the different destructive

50 and nondestructive methods has been investigated and found to be approximately 0.5  
51 percentage points for both matrix digestion and ultrasound, with higher accuracy and  
52 repeatability achieved for X-ray CT measurements, depending on the resolution and  
53 thresholding technique [5, 7]. Matrix digestion is widely used as the destructive reference  
54 method and was shown to have very strong correlation against X-ray CT porosity data [7].

55

56 X-ray phase contrast imaging (XPCi) offers a solution for cases where conventional  
57 radiography yields low contrast and cannot detect the features of interest. While  
58 conventional radiography relies on features having sufficiently different levels of X-ray  
59 attenuation, XPCi uses the real part of the refractive index, which is larger than the  
60 imaginary part driving the attenuation effects, and is sensitive to phase effects induced by  
61 inhomogeneities, thus providing higher contrast [15, 16]. Various XPCi approaches exist,  
62 including Talbot-Lau interferometry [17] and free space propagation [18]. Edge Illumination  
63 XPCi (EI-XPCi) relies on the refraction of X-rays at the interfaces of inhomogeneities and  
64 translates these into a variation of detected intensity using a set of coded aperture masks.  
65 With the acquisition of at least three images for different relative mask positions, EI-XPCi  
66 allows for the retrieval of conventional attenuation, differential phase, and dark-field  
67 images [19]. The differential phase signal corresponds to the angle by which X-rays are  
68 refracted by the sample, most pronounced at interfaces. The dark-field signal corresponds  
69 to the ultra-small-angle scattering of X-rays due to sample inhomogeneities at the sub-pixel  
70 scale, allowing detection of the presence of micro-features smaller than the system  
71 resolution without additional adjustments to the experimental setup [20]. This relative  
72 simplicity of the setup makes EI-XPCi easily scalable to larger field of views, while enabling  
73 relatively fast scans. Using scan-based acquisition systems, samples up to 200 x 500 mm<sup>2</sup>  
74 have been imaged [21], which however is not the ultimate limit. EI-XPCi is robust against  
75 energy variations and environmental vibrations, and can be used using a polychromatic  
76 beam produced by a conventional X-ray source [16, 22].

77

78 EI-XPCi was previously used for damage detection in composites, and compared to  
79 immersion ultrasonic imaging [23, 24]. This demonstrated the complementarity of the  
80 differential phase and dark-field signals to the conventional attenuation signal. The signals  
81 have sensitivity to different types of defects, allowing better visualization of the extent of  
82 the damage by using the sub-pixel sensitivity of the dark-field signal [23]. XPCi was  
83 previously used both for the detection and quantification of porosity in aluminum welds  
84 using Talbot-Lau interferometry dark-field CT [25]. The same technique was used to perform  
85 CT scans on carbon and glass fiber reinforced composite plates, investigating all three XPCi  
86 signals [26]. Overall, these studies show that the phase-based X-ray signals allow for a better  
87 detection of inhomogeneities such as pores than can be obtained with conventional  
88 radiography. However, all the investigations reported above used XPCi CT imaging, and the  
89 option to detect and quantify porosity with planar (2D) XPCi was not explored, which is much  
90 faster than CT, removes limitations on sample size [21], and is compatible with online  
91 inspection.

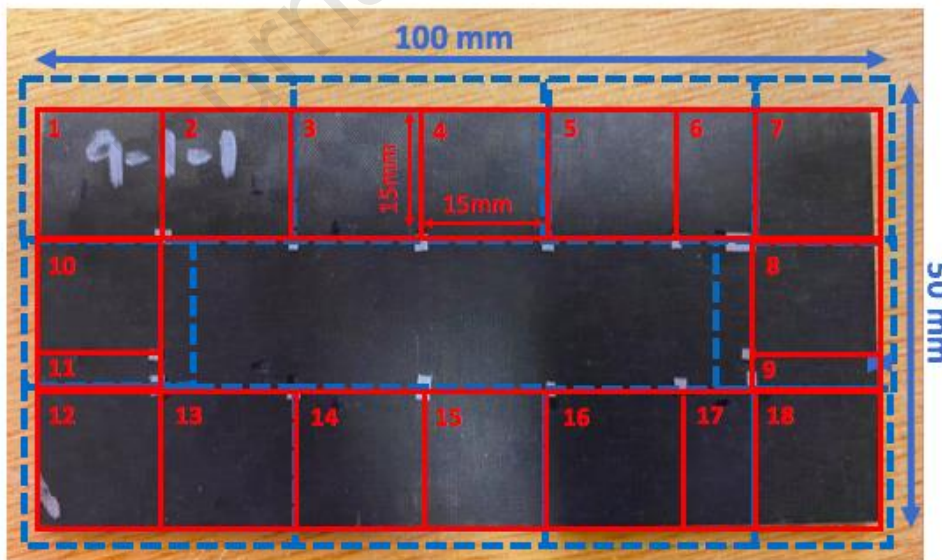
92

93 In this investigation, the differential phase and dark-field signals were used for the  
94 quantification of porosity content using planar EI-XPCi in cross-ply, woven fiber-reinforced  
95 composite plates with porosity content varying from 0.7% to 10.7%. The three EI-XPCi  
96 signals were compared to ultrasonic immersion through transmission absorption  
97 measurements and matrix digestion, the standard industry methods for non-destructive and  
98 destructive porosity content evaluation, respectively. This study introduces the use of the

standard deviation of the differential phase (STDP) as a means to measure and quantify the variation in the distribution of inhomogeneity in the sample on a scale equal to or above the system resolution and demonstrates this can produce a very high correlation with the porosity content determined by matrix digestion. This complements the results from the dark-field signal, which is sensitive to sub-resolution features.

## 2. Experimental Methods

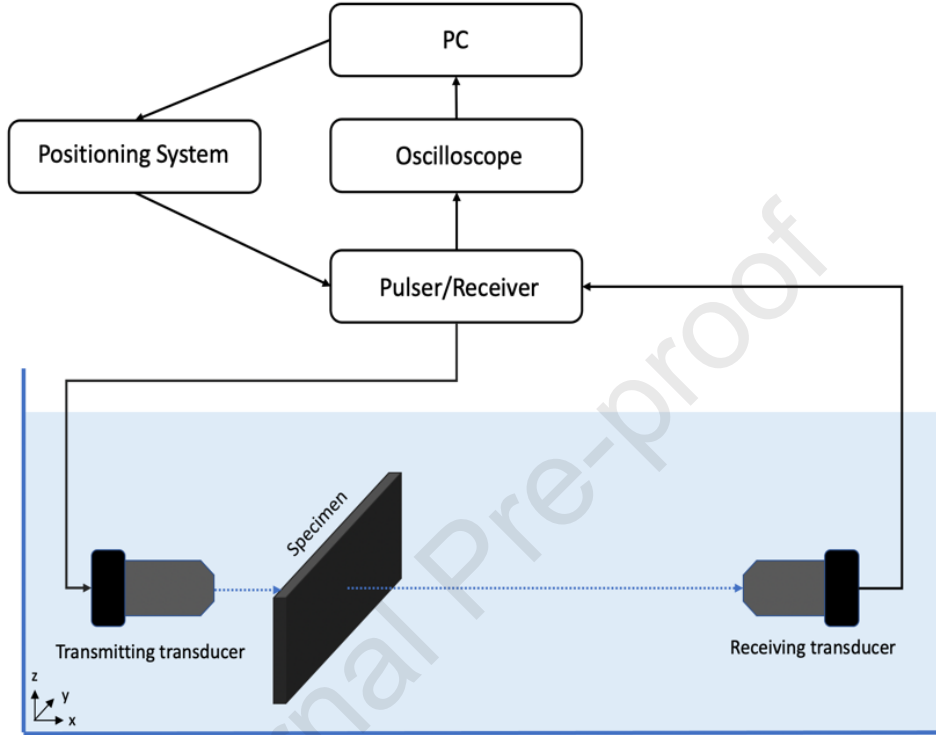
Nine CFRP specimens were manufactured with varying degrees of porosity, ranging from 0.7% to 10.7%, using ten 300 $\mu$ m thick plies of M21 epoxy-carbon woven fabric cross-ply pre-preg (Hexcel), with an average plate thickness of  $3.0\pm 0.2$ mm. The standard autoclave cure followed the recommendations for M21 pre-pregs [27] (pressurized at 7bar, heated at 2 $^{\circ}$ C/min, cure dwell at 180 $^{\circ}$ C for 120 min, cooled at 5 $^{\circ}$ C/min, depressurized when temperature is below 60 $^{\circ}$ C, under 100% vacuum for the total duration of the cure). Different parameters of the cure cycle were varied to obtain specimens with a range of porosities, including varying the debulk duration, edge breathing, autoclave pressure, heating rate, and intermediate dwell. Large panels (160mm by 240mm) were manufactured, and the investigated 100mm by 50mm specimens extracted. One of the specimens (1.5% porosity) was extracted from a smaller panel with dimensions 120 mm by 160 mm. Three smaller samples (20mm by 10mm) were extracted from each large panel adjacent to the extracted specimen (to ensure the main specimens remain available for additional measurements) and used for the determination of porosity content by matrix digestion (ASTM D3171 Procedure B, BS ISO 14127:2008) [28], using nominal densities of 1.78g/cm<sup>3</sup> for the fibers and 1.28g/cm<sup>3</sup> for the matrix. The calculated porosity values (0.7%, 0.9%, 0.9%, 1.3%, 1.5%, 3.9%, 5.9%, 6.6%, 10.7%) were used as comparison values in this investigation. Data on pore size distribution was not available, but changes of pore size and shape due to the different ways in which cure parameters were varied should be expected.



**Figure 1:** Photograph of one of the 100mm by 50mm porosity plate specimens with the 10 X-ray image acquisition areas and the corresponding 18 ROIs highlighted by dashed blue and solid red lines, respectively. Small reflective tape strips markers for ROI boundaries are visible.

Due to the limited field of view of the X-ray system available for this experiment (20mm by 30mm) and the requirement to include a background area (i.e., keep the edge of the plate in the field of view) for image normalization, the plates were imaged in 10 separate

133 acquisitions, which covered 75% of the outer plate area marked in Fig. 1. The central part of  
 134 the samples could not be scanned with background area for normalization, and as a result  
 135 was left out. 18 Regions of Interest (ROIs) were located around the edges of the plates, and  
 136 identified using reflective tape markers, visible in both ultrasonic imaging and XPCi (13 ROIs  
 137 of 15 mm by 15 mm, 2 ROIs of 10 mm by 15 mm and 2 ROIs of 5 mm by 15 mm due to size  
 138 of sample).  
 139



140  
 141 **Figure 2:** Ultrasonic immersion single through transmission experimental set-up, using two  
 142 5MHz transducers for attenuation measurements of the porosity specimens.  
 143

144 The porosity specimens were first analyzed using ultrasonic through transmission C-scans  
 145 [29]. Two focussed transducers, both with 5 MHz center frequency, were placed on either  
 146 side on the specimen immersed in water, as shown in Fig. 2. The emitting transducer  
 147 (Olympus XL50-5-P3) had a nominal diameter of ½ inch (13mm) and a focal length of 19mm.  
 148 The focal spot diameter was calculated to be 650µm for a wavelength of 300µm. The  
 149 transducer was excited by the high voltage pulse created by the pulser/receiver  
 150 (Panametrics 5601T), with the ultrasonic wave propagating through the water and the  
 151 sample placed at the focal spot. The transmitted signal was captured by the receiving  
 152 transducer (Ultran U8420169), which had a nominal diameter of ½ inch (13mm), a focal  
 153 length of 76mm and focal spot of 2.6mm. The receiving transducer was connected to the  
 154 pulser/receiver, and the received signal was recorded using a digital storage oscilloscope  
 155 (LeCroy 9304). Each scan consisted of 221 by 121, 500µm steps, which required  
 156 approximately 8 hours to cover the full sample. The full A-scan signals transmitted through  
 157 the sample were saved for each scan point and the signal attenuation calculated by  
 158 comparing the maximum amplitude of the signal transmitted through the water ( $V_{water}$ )  
 159 and through the plate ( $V_{sample}$ ):

160

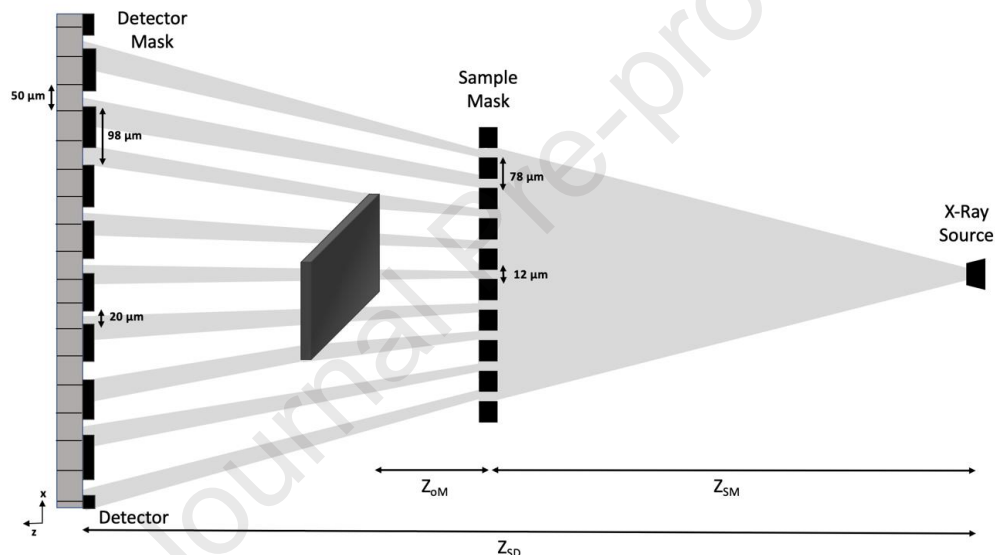
$$\Delta I(dB) = 20 \log \frac{V_{water}}{V_{sample}}$$



161 where  $\Delta I$  is the ultrasonic signal attenuation, measured in decibels (dB). C-scans of the signal  
 162 attenuation were generated for all plates, and the ultrasonic attenuation values averaged  
 163 for each specimen to allow comparison with the matrix digestion values.

164

165 Planar (2D) X-ray scans of all samples were performed using a laboratory EI-XPCi system  
 166 [30]. The setup included a Rigaku MicroMax 007 HF rotating anode molybdenum X-ray  
 167 source with a  $70\mu\text{m}$  focal spot, operated at 40kVp and 20mA. These parameters were  
 168 chosen as they gave the best trade-off between flux and sensitivity for this investigation  
 169 [30]. The detector used was a Hamamatsu C9732DK flat panel CMOS detector with a  $50\mu\text{m}$   
 170 by  $50\mu\text{m}$  pixel size. The source to detector distance,  $Z_{SD}$ , was 0.85m, and the sample stage  
 171 was positioned 0.7m away from the source. Two coded aperture masks are employed by an  
 172 EI system, with the first (“sample”) mask placed upstream of the sample, and the second  
 173 (“detector”) mask placed in front of the detector, as shown in Fig. 3. The optimal relative  
 174 positioning of source, masks, sample, and detector was determined previously based on  
 175 simulations and experimental validation [31].  
 176



177

178 **Figure 3:** Top-view schematic of the Edge Illumination XPCi experimental setup using a  
 179 skipped masks aperture system.

180

181 The sample and the sample mask were mounted on a series of motors, giving control over  
 182 the orientation and positioning of the setup components. The sample mask was mounted  
 183 on a Newport M-ILS150 motor that allows translation along the x-axis with a precision of  
 184  $0.1\mu\text{m}$ , a Newport MFA-CC for translation along the z-axis, and a Kohzu cradle SA04B-RM  
 185 for rotation about the x- and z-axes, with a precision of  $0.0014^\circ$ . This allowed the alignment  
 186 of the sample mask apertures with the detector pixel columns and detector mask apertures,  
 187 and to acquire images with different sample mask positions relative to the detector mask  
 188 [32]. The sample orientation was kept constant throughout the scanning of all 18 ROIs and  
 189 for all nine plates, to ensure the same fiber orientation for all scans. The masks were  
 190 fabricated by MicroWorks to the authors’ design by electroplating a layer of gold on a  
 191 patterned graphite substrate. Apertures consist of equally spaced, narrow slits extending  
 192 over the entire vertical (y with respect to Fig. 3) dimension of the masks, bar some  
 193 interruptions introduced at regular intervals to ensure a better adhesion between the gold  
 194 and substrate. The sample mask, with an aperture size of  $12\mu\text{m}$ , a period of  $78\mu\text{m}$  and  
 195 positioned  $0.65\text{m}$  away from the source ( $Z_{SM}$ ), splits the incoming divergent beam into an

196 array of small beamlets. The detector mask had an aperture of  $20\mu\text{m}$  and a period of  $98\mu\text{m}$   
197 to account for beam widening. Both masks were “skipped” masks [33], meaning that every  
198 other pixel column was covered by the detector mask (see Fig. 3); this reduces the effects  
199 of crosstalk between neighboring pixels in the detector and obtains an aperture limited  
200 spatial resolution when combined with dithering acquisition [34]. The overall system  
201 magnification was 1.25. The resulting system was only sensitive to phase effects in the x-  
202 direction. For radiation safety, the described system is located inside a shielded and  
203 interlocked room. Other system prototypes have been developed inside portable shielded  
204 cabinets. These typically feature larger sample masks allowing for extended fields of view  
205 (e.g.,  $90 \times 90 \text{ mm}^2$  [30]).

206 The acquisition procedure included collecting a series of flat field images at a range of  
207 positions on the “illumination curve” (IC). The IC is the bell-shaped curve obtained by shifting  
208 the sample mask along the x-direction while keeping the detector and detector mask fixed,  
209 and recording the beam intensity at every position [22]. 19 relative sample mask positions  
210 were acquired, with one point at the “top” of the IC where the two masks are perfectly  
211 aligned, and 9 additional points taken symmetrically on each side by translating the sample  
212 mask position in steps of  $4\mu\text{m}$ . All images were acquired with an exposure time of 6s,  
213 resulting in an overall total acquisition time of about 1 hour. Frames at the same 19 IC  
214 positions, with the same exposure time, are then acquired after the sample has been  
215 introduced. In order to increase the resolution, the samples were dithered, i.e., repositioned  
216 along the x-direction at 16 different sub-pixel locations for each sample mask position. This  
217 allows reaching a resolution determined by the size of the apertures in the sample mask  
218 [34], i.e.,  $12\mu\text{m}$ , in the x-direction, while resolution is driven by detector performance in the  
219 y-direction (approximately  $100\mu\text{m}$ , sampled at  $50\mu\text{m}$ ) [30]. Features equal to or above this  
220 resolution will be detected in the attenuation and differential phase signals, whereas sub-  
221 resolution features appear in the dark-field signal [19]. The retrieval of attenuation,  
222 differential phase, and dark-field images is based on fitting Gaussian distributions on a pixel-  
223 by-pixel basis to the 19 images acquired at the different IC points with and without the  
224 sample, and comparing the resulting curves. In this specific case, a retrieval algorithm based  
225 on the three Gaussians fitting technique [35] was used to improve precision and minimize  
226 residual cross-talk effects from neighboring beamlets. Attenuation corresponds to the  
227 change in the Gaussian’s amplitude, refraction (differential phase) to the shift of the  
228 Gaussian’s center position, and dark-field to the broadening of the curve. For features equal  
229 to or above the resolution of the system, the standard deviation of the differential phase  
230 (STDP) was calculated for each ROI. It is sensitive to variations in the distribution of  
231 inhomogeneities on a scale larger than  $12\mu\text{m}$  (since the system is only sensitive to phase  
232 effects in the x-direction, the resolution in y-direction is not relevant).

233

### 234 3. Results

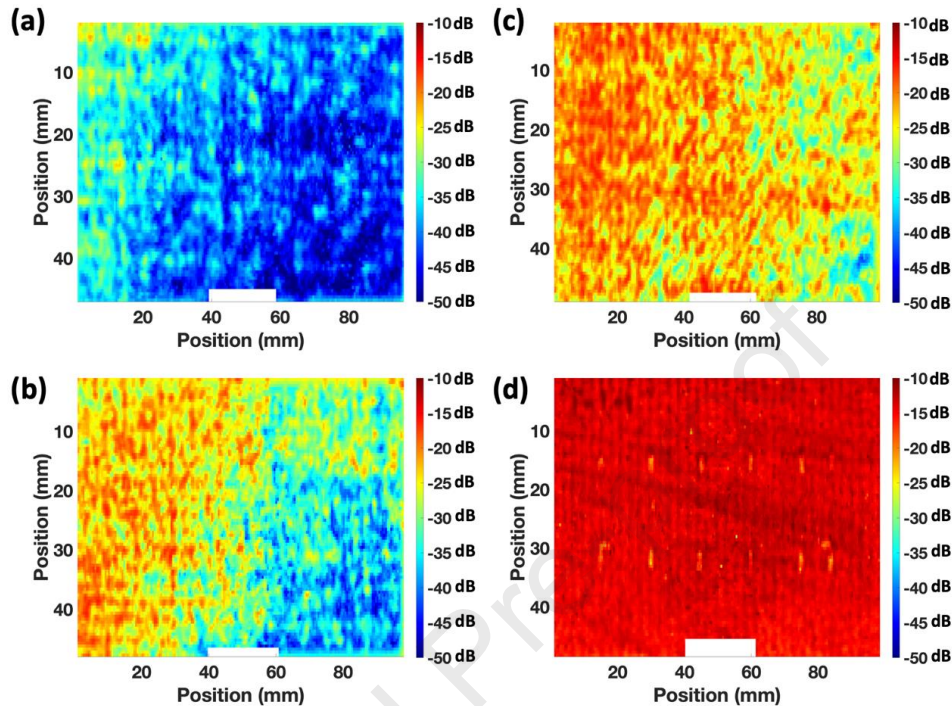
235 First, the results from ultrasonic through-transmission signal absorption at 5 MHz were  
236 compared with the porosity values from the matrix digestion. Secondly, the three XPCi  
237 signals (attenuation, differential phase, and dark-field) were compared with the porosity  
238 values for the nine specimens, initially on a qualitative basis, and then quantitatively. Finally,  
239 the STDP was introduced as a new method for measuring porosity in composite specimens  
240 and compared against the results of matrix digestion.

241

#### 242 3.1 Ultrasonic attenuation

243 Ultrasonic through-transmission C-scans of the nine plate specimens were performed as  
244 detailed in section 2 to quantify variations in signal attenuation due to porosity. Figure 4

245 shows the C-scans for 4 representative plates covering the range of porosities available  
 246 (10.7%, 6.6%, 3.9%, 0.7%). The bright yellow strips observed in the C-scan for the lowest  
 247 porosity specimen are caused by the tape used to delimit the different ROIs (at 15 mm and  
 248 30 mm in Fig. 4(d)).  
 249



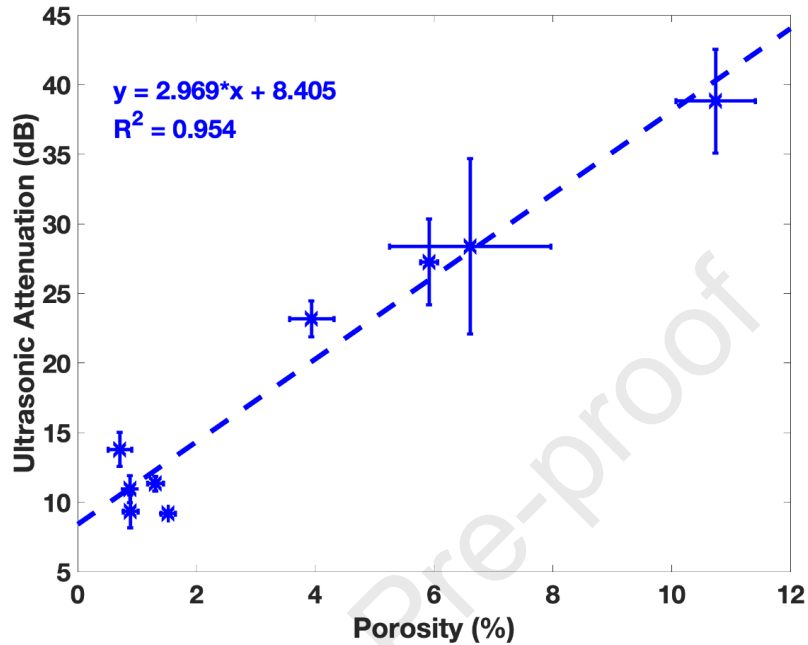
250  
 251 **Figure 4:** Ultrasonic signal attenuation (dB) C-scans of four plate specimens covering range  
 252 of porosity: (a) 10.7%; (b) 6.6%; (c) 3.9%; (d) 0.7% nominal porosity. Areas of high  
 253 attenuation (blue) correspond to increased porosity.

254  
 255 For the three higher porosity specimens, high and non-uniform ultrasonic attenuation was  
 256 observed. For the specimen with the highest porosity (10.7%, Fig. 4(a)), a wide attenuation  
 257 range of 35dB was measured across the plate, with the largest attenuation observed at the  
 258 bottom right corner (blue color, corresponding to high porosity), and an average attenuation  
 259 of  $-39 \pm 4$  dB (uncertainty corresponding to standard deviation, calculated over the scanned  
 260 area). Even higher relative variation was observed for the 6.6% porosity plate (Fig. 4(b)),  
 261 with  $-28 \pm 6$  dB attenuation. A lower average attenuation and variability of  $-23 \pm 1$  dB were  
 262 measured for the 3.9% porosity plate (Fig. 4(c)). The areas of highest attenuation seem to  
 263 be localized in the bottom right corner (blue color), which corresponds to the center of the  
 264 large, manufactured panels, with lower attenuation observed on the left-hand side of the  
 265 specimen. For the lowest porosity plate (0.7%, Fig. 4(d)), low and uniform ultrasonic signal  
 266 attenuation with an average value of  $-14 \pm 1$  dB was observed.

267  
 268 The average ultrasonic attenuation and standard deviation for the nine plates is plotted  
 269 against the porosity values obtained from matrix digestion in Fig. 5. The error bars for the  
 270 porosity values from the destructive matrix digestion correspond to the standard error from  
 271 the three small panels used, and not the accuracy stated in literature as approximately 0.5  
 272 percentage points [5, 7]. A strong correlation can be observed between the ultrasonic  
 273 attenuation measurements and the porosity values obtained from matrix digestion, with an  
 274  $R^2$  of 0.95. Ultrasonic attenuation increases approximately linearly with increasing porosity,  
 275 as expected. However, for porosities below 2%, the ultrasonic measurements do not



276 correlate well to the matrix digestion values, e.g., higher ultrasonic attenuation (-14±1dB)  
 277 was measured for the lowest porosity plate (0.7%) than for the specimen with 1.5% porosity,  
 278 which has the lowest ultrasonic attenuation signal (-9.2±0.2dB). Partially, the limited  
 279 correlation could be due to the accuracy of matrix digestion making it difficult to resolve  
 280 small differences between specimens with low porosity.



281  
 282 **Figure 5:** Average and standard deviation of ultrasonic attenuation for 9 plate specimens  
 283 plotted against the porosity values obtained from matrix digestion.

## 285 3.2 XPCi measurements

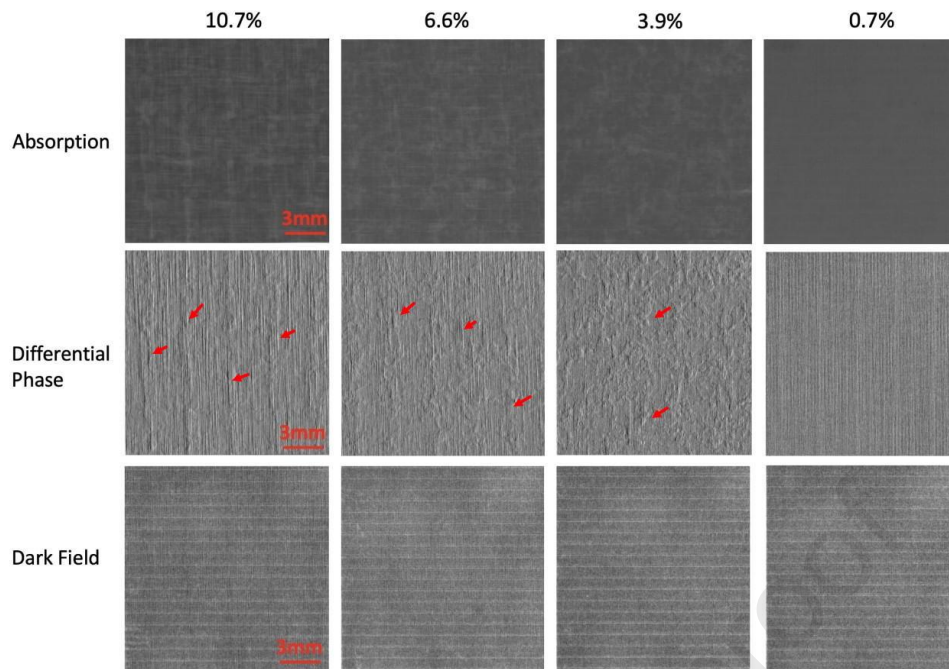
### 286 3.2.1 Qualitative comparison of retrieved signals

287 The XPCi system can resolve inhomogeneities with a resolution of 12µm in the (one-  
 288 directional) differential phase signal, and is sensitive to smaller (sub-micron) features  
 289 through the dark-field signal [34]. The attenuation, differential phase, and dark-field signals  
 290 were retrieved for the nine plates. Fig. 6 shows the three signals for a ROI extracted from  
 291 the same plates with varying degrees of porosity shown in Fig. 4.

292

293 The one-dimensional phase sensitivity of the system makes the differential phase images  
 294 directional, i.e., only features in the vertical direction in Fig. 6 are detected. The differential  
 295 phase signal shows the edges of the inhomogeneities present in the samples, as these cause  
 296 X-ray refraction at their interfaces. The attenuation and differential phase images show that  
 297 the shape and structure of the inhomogeneities change between specimens with different  
 298 levels of porosities. For the highest porosity plate (10.7%), and partly for the second highest  
 299 (6.6%), the observed features seem to follow the woven pattern, with strong vertical  
 300 features visible across the ROIs. Features become more irregular in the latter plate,  
 301 suggesting a reduced clustering of the porosity around the fiber yarns. This is even more  
 302 pronounced in the 3.9% porosity plate. Almost no irregular features are observed in the  
 303 lowest (0.7%) porosity plate, with the aligned vertical features observed in the (direction of  
 304 sensitivity of the) differential phase image thought to be due to the woven fiber yarn  
 305 structures in the cross-ply plate.

306



307  
308

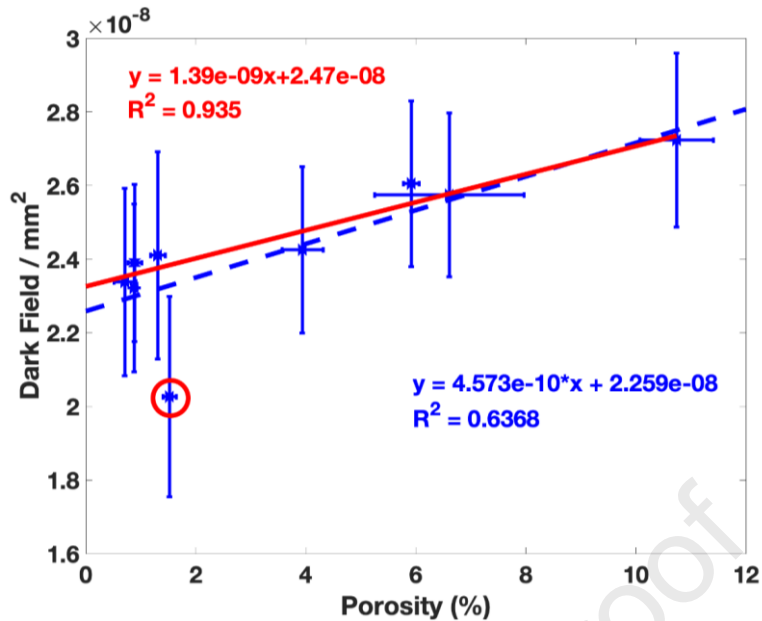
309 **Figure 6:** Attenuation (top), differential phase (middle), and dark-field (bottom) images of  
310 ROIs extracted from four plate specimens covering the considered range of porosities (left  
311 to right: 10.7%, 6.6%, 3.9%, and 0.7%). Arrows in the differential phase images indicate areas  
312 of high porosity.  
313

314 No obvious features are discernible in the absorption and dark-field images, as the  
315 absorption signal has an inherent lack of sensitivity to small pores. As highlighted previously  
316 [23, 24], features in the dark-field images would arise from local variations in the distribution  
317 of inhomogeneities on the sub-resolution (i.e.,  $<12\ \mu\text{m}$ ) scale. The lack of contrast variation  
318 in these images, alongside the clear visualization of structural inhomogeneities in the  
319 differential phase images (features  $>12\ \mu\text{m}$  resolved), suggests a lack of inhomogeneously  
320 distributed features on a scale below  $12\ \mu\text{m}$ . This does not imply an absence of such  
321 microscopic features, and indeed a degree of correlation between dark-field signal and  
322 overall porosity level has been observed and is discussed below; only that they do not seem  
323 to cluster at specific locations. The horizontal lines visible in the dark-field images, as well  
324 as the brighter areas visible in the four corners of all images, are artefacts caused by  
325 interruptions in the mask apertures (see section 2).  
326

327

### 3.2.2 Quantitative Comparison of EI-XPCi signals

328 Despite some features that can be attributed to porosity being visible in the attenuation  
329 images for the higher porosity plates (Fig. 6), very limited correlation was found between  
330 the average attenuation signal and the porosity values from the matrix digestion. As  
331 expected, no correlation was observed between the differential phase signals averaged over  
332 the scanned plate areas and the porosity values from the matrix digestion, since differential  
333 phase images highlight the edges of inhomogeneities with dark and bright fringes, which  
334 cancel out when averaged.

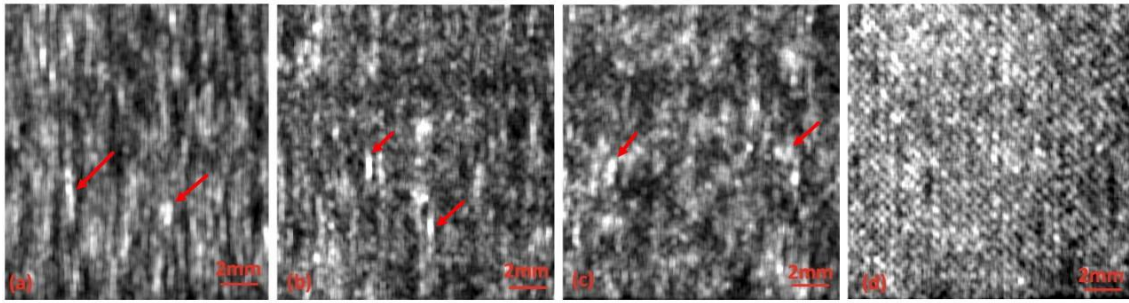


335  
 336 **Figure 7:** Average dark-field signal compared with the porosity values from matrix digestion  
 337 for 9 specimens; linear fit for all specimens (blue, dashed), and improved fit obtained by  
 338 eliminating the outlier in the red circle (red, solid).

339  
 340 Figure 7 shows the average dark-field signal plotted against the matrix digestion porosity  
 341 values. Although no clear variation in inhomogeneity was observed in individual dark-field  
 342 images (Fig. 6), correlation is observed between the averaged dark-field signals and porosity.  
 343 Such correlation was previously observed for the presence of micro-cracks in CFRP, where  
 344 the presence of features in the dark-field increased with increasing overall damage in the  
 345 samples [17]. This supports the hypothesis that the dark-field signal is sensitive to sub-  
 346 resolution features, and that their prevalence increases with increasing porosity levels.  
 347 However, these appear to be uniformly distributed across the plates, leading to a variation  
 348 in the overall value but not to observable local changes. The linear fit applied to all nine  
 349 values has an  $R^2$  value of 0.64 due to an outlier (circled in red). This outlier corresponds to  
 350 the plate that was manufactured differently (section 2). The  $R^2$  value increases to 0.94 when  
 351 this plate is not considered, which is comparable to the results obtained with ultrasonic  
 352 attenuation (0.95, see Fig. 5). However, it can be observed that, for plates below 4%  
 353 porosity, the correlation is weak. This could indicate either that the number of sub-  
 354 resolution features for the low porosity plates is similar, or that the sensitivity limits of the  
 355 technique have been reached. Most importantly, the differential phase images in Fig. 6  
 356 clearly show the presence of inhomogeneities well above the resolution level, to which the  
 357 dark-field signal is not sensitive.

### 358 359 3.2.3 Standard deviation of the differential phase

360 To take the above point into account, the analysis was extended by considering an additional  
 361 approach, the standard deviation of the differential phase (STDP). This is sensitive to how  
 362 many “edges” of features (on a scale above the resolution limit, i.e.,  $>12\mu\text{m}$ ) are detected  
 363 per unit area, similar to the signal dark-field for inhomogeneities below the resolution limit.  
 364 The STDP was calculated for each ROI, to ensure that a large enough area was covered.  
 365 Images of the standard deviation of the differential phase for the same ROIs as in Fig. 6 are  
 366 shown in Fig. 8. The images were produced by calculating the STDP over an area of  $300\mu\text{m}$   
 367 by  $300\mu\text{m}$ , thus extracting the signal over an area comparable to the ultrasonic resolution.



368  
369

370 **Figure 8:** Comparison of the standard deviation of the differential phase (STDP) calculated  
371 over areas comparable to the resolution of the ultrasonic images (300 $\mu$ m by 300 $\mu$ m) for  
372 four plate specimens covering range of porosities: (a) 10.7%; (b) 6.6%; (c) 3.9%; (d) 0.7%.  
373 Arrows in panels (a-c) indicate areas of high porosity.

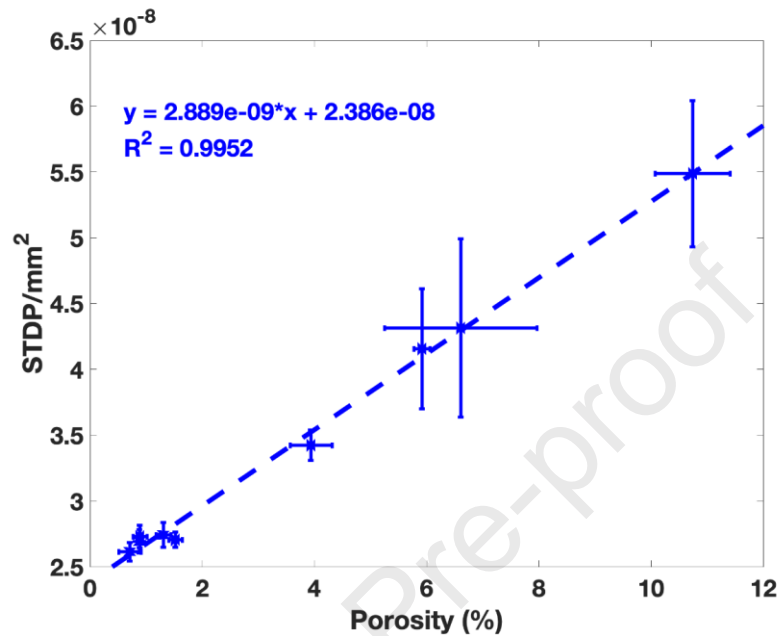
374

375 Areas with relatively high STDP correspond to large variations in the sample inhomogeneity  
376 on a scale equal to or larger than 12 $\mu$ m and are show as bright areas in Fig. 8. The contrast  
377 was adjusted independently for each image. In the highest porosity plate (10.7%), as  
378 expected, a feature distribution similar to the differential phase images is observed along  
379 the woven fiber yarns (see arrows in panel (a)), with bright vertical lines visible across the  
380 sample (due to the 1D sensitivity of the system). While the differential phase images  
381 highlight the edges of the porous regions, the STDP corresponds to their local distribution,  
382 with a high value effectively indicating “more features”. In the 6.6% porosity plate, the  
383 vertical porosity features are also visible but with lower intensity (see arrows in panel (b)),  
384 with additional high porosity areas distributed across the plate. For the 3.9% plate, the  
385 porosity is not aligned along the woven structure, and randomly distributed high intensity  
386 areas are visible across the ROI (examples indicated by arrows in panel (c)). A possible  
387 explanation might be that the reduction in porosity corresponds to a significantly decreased  
388 incidence of pores and defects aligned along the woven fiber yarns, but this would need  
389 further verification. In the image of the lowest porosity plate, the contrast has been  
390 stretched to an extent where some degree of the sample structure becomes visible;  
391 however, a gradient is also visible, indicating that more pores are present in the top/left  
392 area of the ROI compared to the bottom/right part.

393

394 The average STDP was calculated over the whole area of each ROI and integrated over the  
395 entire plate. This was plotted against the porosity obtained from the matrix digestion, as  
396 shown in Fig. 9. A strong correlation can be observed between STDP and the matrix digestion  
397 porosity values, demonstrating that STDP is capable of quantifying the degree of porosity in  
398 the plates. The  $R^2$  value of 0.99 for the correlation between the standard deviation of the  
399 differential phase with the matrix digestion porosity values is the highest observed across  
400 all techniques, indicating even better correspondence than ultrasonic signal attenuation.  
401 Similarly, Kastner et al [7] found better correlation of porosity values obtained using  
402 nondestructive X-ray CT with matrix (acid) digestion than compared to ultrasonic testing,  
403 even though they state the same accuracy for matrix digestion and ultrasonic testing. For  
404 the low porosity plates (below 2%), the STDP increases with increasing matrix digestion  
405 porosity, showing better correlation than both the ultrasonic attenuation and the dark-field  
406 signal. STDP was capable of quantifying porosity content in the investigated woven  
407 composite plates down to low porosity values (<1%), whereas our ultrasonic attenuation  
408 measurements could not differentiate well between porosity values below 2%. These results  
409 correspond to a single sample orientation, resulting in sensitivity in a single direction.

410 However, STDP provides an estimate of the number of interfaces, expected to be  
 411 approximately the same regardless of orientation, due to the continuous nature of the  
 412 voids. It should be noted that the STDP signal intensity does not provide specific information  
 413 on pore shape or size required for detailed stress analysis but enables rapid determination  
 414 of the overall amount of porosity.  
 415



416  
 417 **Figure 9:** Comparison of average STDP with matrix digestion porosity values for all nine  
 418 specimens.  
 419

#### 420 4. Conclusions

421 Planar EI-XPCi was used for the quantification of porosity in fiber reinforced woven  
 422 composite specimens, by comparing the retrieved signals to porosity content based on  
 423 matrix digestion and ultrasonic attenuation measurements. Correlation was found between  
 424 the porosity content calculated using matrix digestion and the dark-field signal, which is  
 425 sensitive to inhomogeneities in the sub-resolution scale of the XPCi system (<12 μm). It was  
 426 found that, for the set of specimens used in this investigation, the dark-field signal did not  
 427 lead to a better correlation with matrix digestion porosity values than ultrasonic  
 428 attenuation, possibly because of the relatively large pore size. The STDP (standard deviation  
 429 of the differential phase) was therefore introduced, as a means to measure the variation in  
 430 the distribution of inhomogeneity for features on a scale equal to or above the system  
 431 resolution. The STDP was shown to have a better correlation than ultrasonic attenuation  
 432 when compared with porosity values from matrix digestion, including for low porosity  
 433 specimens (<2%), where ultrasonic attenuation and dark-field signals showed the least  
 434 correlation. With the caveat that only the amount of porosity and not pore shape and size  
 435 can be determined, and that some degree of calibration may be required, these results  
 436 indicate significant potential for this new approach in the non-destructive evaluation of  
 437 porosity content for fiber-reinforced composite specimens. In particular, STDP values can  
 438 be extracted from relatively fast scans of large plate specimens [21] using planar (2D)  
 439 imaging, which is faster and less restrictive on specimen size than X-ray micro-CT. However,  
 440 it should also be noted that X-ray micro-CT can provide information on the spatial  
 441 distribution in 3D, size, and shape of pores [7], which the proposed method cannot offer.  
 442 Future work should include the investigation of the relation between STDP and dark-field



443 signals. Scans with varying levels of system resolution (using masks with different aperture  
444 size) may allow effective means to combine the two signals, and offer the possibility to  
445 characterize pore and void size distribution on multiple scales through a single scan.

446

447 **Declaration of interest:**

448 DB is a Nikon employee. ME and AO are named inventors on UCL-owned patents protecting  
449 the EI-XPCI technology used to obtain the results presented in this paper. All other authors  
450 have no conflicts of interest to disclose.

451

452 **Data Availability Statement**

453 The raw/processed data required to reproduce these findings will be made available by  
454 the corresponding author upon request.

455

456 **Funding:** This work was supported by the UK Engineering and Physical Sciences Research  
457 Council (EPSRC) [grant numbers EP/N509577/1 and EP/T005408/1]. M. Endrizzi was  
458 supported by the Royal Academy of Engineering under their Eng. Research Fellowship  
459 scheme. A. Olivo was supported by the Royal Academy of Engineering under their Chairs in  
460 Emerging Technologies scheme.

461 **References**

- 462 1. Donadon M V., Iannucci L, Falzon BG, Hodgkinson JM, de Almeida SFM. A progressive  
 463 failure model for composite laminates subjected to low velocity impact damage.  
 464 *Comput Struct.* 2008;86:1232–52.
- 465 2. Birt EA, Smith RA. A review of NDE methods for porosity measurement in fibre-  
 466 reinforced polymer composites. *Insight.* 2004;46(11):681–6.
- 467 3. Fernlund G, Wells J, Fahrang L, Kay J, Poursartip A. Causes and remedies for porosity  
 468 in composite manufacturing. *IOP Conf Ser Mater Sci Eng.* 2016;139(1).
- 469 4. Mehdikhani M, Gorbatikh L, Verpoest I, Lomov S V. Voids in fiber-reinforced polymer  
 470 composites: A review on their formation, characteristics, and effects on mechanical  
 471 performance. *J Compos Mater.* 2019;53(12):1579–669.
- 472 5. Elkolali M, Nogueira LP, Rønning PO, Alcocer A. Void Content Determination of Carbon  
 473 Fiber Reinforced Polymers: A Comparison between Destructive and Non-Destructive  
 474 Methods. *Polymers* 2022, 14:1212.
- 475 6. EN 2564:2018. Aerospace series - Carbon fibre laminates - Determination of the fibre,  
 476 resin and void contents (2018).
- 477 7. Kastner J, Plank B, Salaberger D, Sekelja J. Defect and porosity determination of fibre  
 478 reinforced polymers by X-ray computed tomography. *NDT in Aerospace 2010*
- 479 8. Yang P, Elhajjar R. Porosity Content Evaluation in Carbon-Fiber/Epoxy Composites  
 480 Using X-ray Computed Tomography. *Polym - Plast Technol Eng.* 2014;53(3):217–22.
- 481 9. Wildenschild D, Sheppard AP. X-ray imaging and analysis techniques for quantifying  
 482 pore-scale structure and processes in subsurface porous medium systems. *Adv Water*  
 483 *Resour.* 2013;51:217–46.
- 484 10. Guo N, Cawley P. The non-destructive assessment of porosity in composite repairs.  
 485 *Composites.* 1994;25(9):842–50.
- 486 11. Daniel IM, Wooh SC, Komsky I. Quantitative porosity characterization of composite  
 487 materials by means of ultrasonic attenuation measurements. *J Nondestruct Eval.*  
 488 1992;11(1):1–8.
- 489 12. Smith RA, Nelson LJ, Mienczakowski MJ, Wilcox PD. Ultrasonic Analytic-Signal  
 490 Responses from Polymer-Matrix Composite Laminates. *IEEE Trans Ultrason*  
 491 *Ferroelectr Freq Control.* 2018;65(2):231–43.
- 492 13. van Dreumel WHM. Ultrasonic scanning for quality control of advanced fibre  
 493 composites, *NDT Int.* 1978;11(5):233-5.
- 494 14. Manta A, Gresil, M, Soutis, C. Infrared thermography for void mapping of a  
 495 graphene/epoxy composite and its full-field thermal simulation, *Fatigue Fract Eng*  
 496 *Mater Struct.* 2019;42:1441–1453.
- 497 15. Fitzgerald R. Phase-Sensitive X-Ray Imaging. *Phys Today.* 2000;53:23–6.
- 498 16. Olivo A, Castelli E. X-Ray Phase Contrast Imaging: From Synchrotrons to Conventional  
 499 Sources. *Riv del Nuovo Cim.* 2014;37(9):467–508.
- 500 17. Senck S, Scheerer M, Revol V, Plank B, Hanneschläger C, Gusenbauer C, et al.  
 501 Microcrack characterization in loaded CFRP laminates using quantitative two- and  
 502 three-dimensional X-ray dark-field imaging. *Compos Part A Appl Sci Manuf.* 2018  
 503 Dec;115:206–14.
- 504 18. Coindreau O, Vignoles G, Goyheneche J-M. Multiscale X-Ray CMT of C/C Composite  
 505 Preforms: A Tool for Properties Assessment. In: *Ceramic Transactions, Advances in*  
 506 *Ceramic Matrix Composites.* Hoboken, NJ, USA: John Wiley & Sons, Inc.; 2006. p. 77–  
 507 84.

- 508 19. Endrizzi M, Diemoz PC, Millard TP, Louise Jones J, Speller RD, Robinson IK, et al. Hard  
509 X-Ray Dark-Field Imaging with Incoherent Sample Illumination. *Appl Phys Lett*.  
510 2014;104(2):3–6.
- 511 20. Endrizzi M, Diemoz PC, Hagen CK, Millard TP, Vittoria FA, Wagner UH, et al.  
512 Laboratory-based Edge-illumination Phase-contrast Imaging : Dark-field Retrieval and  
513 High-resolution Implementations. In: 2014 IEEE Nuclear Science Symposium and  
514 Medical Imaging Conference (NSS/MIC). 2012. p. 1–3.
- 515 21. Astolfo A, Endrizzi M, Vittoria FA, Diemoz PC, Price B, Haig I, et al. Large field of view,  
516 fast and low dose multimodal phase-contrast imaging at high x-ray energy. *Sci Rep*.  
517 2017;7(1):1–8.
- 518 22. Diemoz PC, Hagen CK, Endrizzi M, Olivo A. Sensitivity of laboratory based  
519 implementations of edge illumination X-ray phase-contrast imaging. *Appl Phys Lett*.  
520 2013;103(24).
- 521 23. Shoukroun D, Massimi L, Iacoviello F, Endrizzi M, Bate D, Olivo A, et al. Enhanced  
522 composite plate impact damage detection and characterisation using X-Ray refraction  
523 and scattering contrast combined with ultrasonic imaging. *Compos Part B*.  
524 2020;181(107579):1–10.
- 525 24. Endrizzi M, Murat BIS, Fromme P, Olivo A. Edge-illumination X-Ray Dark-Field Imaging  
526 for Visualising Defects in Composite Structures. *Compos Struct*. 2015;134(1):895–9.
- 527 25. Revol V, Jerjen I, Kottler C, Schtz P, Kaufmann R, Lthi T, et al. Sub-pixel porosity  
528 revealed by x-ray scatter dark field imaging. *J Appl Phys*. 2011;110(4):1–6.
- 529 26. Gusenbauer C, Reiter M, Plank B, Salaberger D, Senck S, Kastner J. Porosity  
530 Determination of Carbon and Glass Fibre Reinforced Polymers Using Phase-Contrast  
531 Imaging. *J Nondestruct Eval*. 2019;38(1):1–10.
- 532 27. HexPly® M21 180C Curing Epoxy Matrix Report. 2020.
- 533 28. ASTM D3171-15. In: *Standard Test Methods for Constituent Content of Composite*  
534 *Materials*. West Conshohocken, PA: ASTM International; 2015.
- 535 29. Stone DEW, Clarke B. Ultrasonic attenuation as a measure of void content in carbon-  
536 fibre reinforced plastics. *Non-Destructive Test*. 1975;8(3):137–45.
- 537 30. Massimi L, Suaris T, Hagen CK, Endrizzi M, Munro PRT, Havariyoun G, et al. Detection  
538 of involved margins in breast specimens with X-ray phase-contrast computed  
539 tomography. *Sci Rep*. 2021;11(3663):1–9.
- 540 31. Olivo A, Ignatyev K, Munro PRT, Speller RD. Design and realization of a coded-aperture  
541 based x-ray phase contrast imaging for homeland security applications. *Nucl. Instrum.*  
542 *Meth. Phys. Res. A* 2009;610:604-14
- 543 32. Millard TP, Endrizzi M, Ignatyev K, Hagen CK, Munro PRT, Speller RD, et al. Method for  
544 automatization of the alignment of a laboratory based x-ray phase contrast edge  
545 illumination system. *Rev Sci Instrum*. 2013;84(8).
- 546 33. Ignatyev K, Munro PRT, Speller RD, Olivo A. Effects of signal diffusion on x-ray phase  
547 contrast images. *Rev Sci Instrum*. 2011;82(073702):1–9.
- 548 34. Diemoz PC, Vittoria FA, Olivo A. Spatial resolution of edge illumination X-ray phase-  
549 contrast imaging. *Opt Express*. 2014;22(13):15514.
- 550 35. Maughan Jones CJ, Vittoria FA, Olivo A, Endrizzi M, Munro PRT. Retrieval of weak x-  
551 ray scattering using edge illumination. *Opt Lett*. 2018;43(16):3874.
- 552

15th December 2021

**Re: Author Contributions**

The Contributor Roles Taxonomy for the manuscript “Quantification of Porosity in Composite Plates using Planar X-ray Phase Contrast Imaging” are:

**Dana Shoukroun:** Methodology, Formal Analysis, Validation, Investigation, Data Curation, Writing – Original Draft, Visualization; **Lorenzo Massimi:** Methodology, Writing – Review & Editing; **Marco Endrizzi:** Methodology, Writing – Review & Editing; **Alan Nesbitt:** Resources, Data Curation, Writing – Review & Editing; **David Bate:** Resources, Writing – Review & Editing, Funding Acquisition; **Paul Fromme:** Conceptualization, Validation, Resources, Writing – Review & Editing, Supervision; **Alessandro Olivo:** Conceptualization, Methodology, Validation, Resources, Writing – Review & Editing, Supervision, Funding Acquisition.

Yours sincerely,  
Dana Shoukroun

**Declaration of interests**

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

The authors declare the following financial interests/personal relationships which may be considered as potential competing interests:

DB is a Nikon employee. ME and AO are named inventors on UCL-owned patents protecting the EI-XPCI technology used to obtain the results presented in this paper. All other authors have no conflicts of interest to disclose.