

1 **The PTW microSilicon diode:**
2 **Performance in small 6 and 15 MV photon fields**
3 **and utility of density compensation**

4
5 Georgios Georgiou^{*1,2,3}, Sudhir Kumar⁴, Jan U. Würfel⁵,
6 Martyn Gilmore², Tracy S. A. Underwood⁶,
7 Carl G. Rowbottom^{2,3} and John D. Fenwick^{1,2}

8
9 1. Department of Molecular and Clinical Cancer Medicine,
10 Institute of Systems, Molecular and Integrative Biology, University of Liverpool,
11 The Sherrington Building, Ashton Street, Liverpool L69 3BX, UK

12 2. Department of Physics, Clatterbridge Cancer Centre,
13 Clatterbridge Road, Wirral CH63 4JY, UK

14 3. Department of Physics, University of Liverpool,
15 Oliver Lodge Laboratory, Oxford Street, Liverpool L69 7ZE, UK

16 4. Radiological Physics and Advisory Division, Bhabha Atomic Research Centre,
17 CT & CRS Building, Anushaktinagar, Mumbai-400094, India

18 5. PTW-Freiburg, Loerracher Str. 7, 79115, Freiburg, Germany

19 6. Division of Cancer Sciences, School of Medical Sciences,
20 Faculty of Biology, Medicine and Health, The University of Manchester,
21 Manchester M20 4BX, UK

22
23 **Running title** – Response of the PTW microSilicon diode in small fields

24
25 [†] Corresponding author, email: georgeorgh@gmail.com

26
27

^{*}Now at Radiotherapy Physics Department, North Wales Cancer Treatment Centre,
Glan Clwyd Hospital, Bodelwyddan LL18 5UJ, UK

28 **Abstract**

29 **Purpose:** We have experimentally and computationally characterized the PTW
30 *microSilicon* 60023-type diode's performance in 6 and 15 MV photon fields $\geq 5 \times 5$ mm²
31 projected to isocentre. We tested the detector on- and off-axis at 5 and 15 cm depths in
32 water, and investigated whether its response could be improved by including within it a
33 thin airgap.

34 **Methods:** Experimentally, detector readings were taken in fields generated by a Varian
35 TrueBeam linac and compared with doses-to-water measured using Gafchromic film and
36 ionization chambers. An unmodified 60023-type diode was tested along with detectors
37 modified to include 0.6, 0.8 and 1.0 mm thick airgaps. Computationally, doses absorbed
38 by water and detectors' sensitive volumes were calculated using the EGSnrc/BEAMnrc
39 Monte Carlo radiation transport code. Detector response was characterized using
40 $k_{Q_{clin,4\text{ cm}}}^{f_{clin,4\text{ cm}}}$, a factor that corrects for differences in the ratio of dose-to-water to detector
41 reading between small fields and the reference condition, in this study 5 cm deep on-axis
42 in a 4×4 cm² field.

43 **Results:** The greatest errors in measurements of small field doses made using
44 uncorrected readings from the unmodified 60023-type detector were over-responses of
45 $2.6\% \pm 0.5\%$ and $5.3\% \pm 2.0\%$ determined computationally and experimentally, relative
46 to the reading-per-dose in the reference field. Corresponding largest errors for the earlier
47 60017-type detector were $11.9\% \pm 0.6\%$ and $11.7\% \pm 1.4\%$ over-responses. Adding even
48 the thinnest, 0.6 mm, airgap to the 60023-type detector over-corrected it, leading to
49 under-responses of up to $4.8\% \pm 0.6\%$ and $5.0\% \pm 1.8\%$ determined computationally and
50 experimentally. Further Monte Carlo calculations indicate that a detector with a 0.3 mm
51 airgap would read correctly to within 1.3% on-axis. The ratio of doses at 15 and 5 cm

52 depths in water in a 6 MV 4×4 cm² field was measured more accurately using the
53 unmodified 60023-type detector than using the 60017-type detector, and was within 0.3%
54 of the ratio measured using an ion chamber. The 60023-type diode's sensitivity also
55 varied negligibly as dose-rate was reduced from 13 to 4 Gy min⁻¹ by decreasing the linac
56 pulse repetition frequency, whereas the sensitivity of the 60017-type detector fell by
57 1.5%.

58 **Conclusions:** The 60023-type detector performed well in small fields across a wide
59 range of beam energies, field sizes, depths and off-axis positions. Its response can
60 potentially be further improved by adding a thin, 0.3 mm, airgap.

61 **Key words:** microSilicon, diode, small field, density compensation, dose-rate

62

63 1. INTRODUCTION

64 Detectors used to measure radiation doses absorbed by water from small megavoltage
65 photon fields should ideally have sensitive volumes narrow enough to minimize volume-
66 averaging, and be built from materials with atomic numbers and densities sufficiently
67 close to water to minimize variations in photon spectral effects and electron fluence
68 perturbation with field-size.¹ Sensitive volumes of silicon diode detectors typically have
69 a 1 mm diameter, and silicon's atomic number is close enough to water to limit spectral
70 effects in small fields, especially when an intermediate field, for example 4×4 cm², is used
71 as a reference rather than the standard 10×10 cm² field. Nevertheless, diodes over-
72 respond in small fields relative to wider ones due largely to the non-water equivalent
73 densities of silicon (2.33 g cm⁻³) and other detector constituents in close proximity to the
74 sensitive volume.²⁻⁵

75 Several 'density compensation' studies have found that silicon diodes' responses
76 in small fields can be improved by building into them airgaps of judiciously chosen size.^{4,}
77 ⁶⁻⁹We previously tested an unmodified PTW 60017-type diode (Diode E) (PTW-Freiburg,
78 Germany) and diodes with airgaps of thickness 0.6-1.6 mm added.¹⁰ Density
79 compensation substantially improved diode performance on- and off-axis at depths of 5
80 and 15 cm in water in 6 and 15 MV photon fields of size $\geq 0.5 \times 0.5$ cm². The maximum
81 error in doses measured using uncorrected readings of the unmodified detector was
82 11.7% determined experimentally or 11.9% computationally, compared to 4.1% or 2.2%
83 for the best performing diode, which had a 1.6 mm airgap.

84 For some detectors there were notable differences between responses
85 determined experimentally and computationally in 0.5×0.5 cm² fields, a finding attributed
86 to detector-to-detector variations in the thickness of the dense epoxy resin housing of the

87 sensitive volume.¹⁰ This was supported by Monte Carlo calculations showing that the
88 response of the 60017-type detector in a 6 MV 0.5×0.5 cm² field relative to that in a 4×4
89 cm² field would be 4% higher if the epoxy housing was 0.3 mm thicker, a change within
90 manufacturing tolerance. It follows that detector response in small fields can only be
91 reproducibly fine-tuned using airgaps engineered to a tenth of a millimeter if comparable
92 tolerances are placed on the dimensions of dense detector components, or if these
93 components are replaced with less dense materials.

94 We also observed experimentally that the response of the 60017-type detector
95 relative to a PTW 31010-type *Semiflex* ionization chamber fell progressively, by up to
96 2%, at increasing depths in water.¹⁰ This is most likely due to the variation of silicon diode
97 sensitivity with dose-per-linac-pulse observed by Schönfeld et al.¹¹

98 Recently, PTW-Freiburg commercialized a new '*microSilicon*' diode detector, the
99 60023-type. Some materials used in this detector have densities closer to 1 g cm⁻³, and
100 the sensitive silicon lattice has been adjusted to minimize the diode's dose-rate
101 dependence. The 60023-type diode has been tested in 6 MV fields $\geq 0.5 \times 0.5$ cm² by
102 Schönfeld et al.¹¹ and Weber et al.¹², who characterized its response on-axis at 10 cm
103 depth in water and off-axis at 5 cm depth. Compared to the 60017-type diode, the new
104 detector required small field correction factors closer to unity. Akino et al.¹³ further tested
105 this detector at 10 cm depth in water, on-axis in 6 and 10 MV fields $\geq 0.5 \times 0.5$ cm² and off-
106 axis in a 6 MV 1×1 cm² field. These investigators also found that correction factors were
107 closer to unity for the 60023-type than for the 60017-type diode, and reported negligible
108 variation in the sensitivity of the new detector across a 0.07-10 Gy min⁻¹ range of dose-
109 rates, whereas the sensitivity of the 60017-type detector changed by over 5%. The
110 60023-type detector has also been tested in a 6 MV circular field of diameter 5 mm by
111 Francescon et al.¹⁴ who found that the on-axis dose measured at 1.5 cm depth required

112 a 2% correction compared to 5-6% for other stereotactic diodes. Wiedlich et al.¹⁵ tested
113 the detector in 3 MV circular fields down to a diameter of 4 mm and reported that the
114 penumbra width measured using this detector was greater than that measured using film
115 or a PTW 60018-type diode, but narrower than the width measured using a
116 *microDiamond* detector, reflecting the relative diameters of the detectors' sensitive
117 volumes.

118 Here, we describe our own experimental and computational testing of the 60023-
119 type diode in 6 and 15 MV photon beams, on- and off-axis at 5 and 15 cm depths in
120 water, and on-axis from the surface to depths up to 30 cm. To investigate the utility of
121 density-compensation we have additionally tested 60023-type diodes with airgaps
122 added.

123 **2. METHODS**

124 **2.A. PTW 60023-type microSilicon detectors**

125 An unmodified 60023-type diode was tested along with variants containing airgaps
126 of thickness 0.6, 0.8 and 1.0 mm. The outer casings of the detectors included RW3 plastic
127 caps.¹² Airgaps were built directly into these caps in modified diodes, keeping the
128 thickness of RW3 above the airgaps equal to that in the unmodified detector.

129 The sensitive volume of the 60023-type diode is a silicon disc of diameter 1.4 mm
130 and thickness 18 μm , whose short-axis is aligned with the long-axis of the detector. It is
131 located at the upper surface of a thicker silicon cuboid which is surrounded by an epoxy
132 housing located immediately below the RW3 cap or airgap. The manufacturer-specified
133 effective point of measurement (EPOM) of the unmodified PTW 60023-type diode lies
134 0.9 mm below the detector's top surface, slightly higher than in the 60017-type which has
135 denser epoxy.

136 **2.B. Characterizing detector response**

137 Response in small clinical fields f_{clin} of quality Q_{clin} was characterized relative to
138 the response at a reference point in a reference field, which in this study was a point on-
139 axis at 5 cm depth in a 4×4 cm² field. The difference in response between the two points
140 was accounted for via a standard correction factor, $k_{Q_{clin},4\text{ cm}}^{f_{clin},4\text{ cm}}$, given by the ratio of doses
141 absorbed by water at the measurement and reference points, divided by the ratio of
142 readings (M) of a detector with its EPOM located at those points^{1, 16}

$$143 \quad k_{Q_{clin},4\text{ cm}}^{f_{clin},4\text{ cm}} = \left[\frac{(D_{w\text{-point}})_{Q_{clin}}^{f_{clin}} / M_{Q_{clin}}^{f_{clin}}}{(D_{w\text{-point}})_{Q_{4\text{ cm}}}^{4\text{ cm}} / M_{Q_{4\text{ cm}}}^{4\text{ cm}}} \right] \quad (1)$$

144 **2.C. Monte Carlo calculations**

145 Radiation transport calculations were performed using the EGSnrc system
146 (version: v20017)¹⁷ run on a 64 core AMD 6378 Opteron-based computer. Phase-space
147 files were generated for linac jaw-defined fields of size 0.5×0.5, 0.7×0.7 and 4×4 cm²
148 projected to isocentre, using the BEAMnrc user-code¹⁸ and 6 and 15 MV beam models
149 previously built and validated for Varian Clinac iX and 2100 C treatment machines by
150 Underwood et al.¹⁹ and Scott et al.²⁰ For the phase-space calculations the electron and
151 photon cut-off parameters ECUT and PCUT were set to 700 and 10 keV respectively.
152 Electrons with total energies below 700 keV travel <0.5 mm in water²¹ while low energy
153 photons comprise a small part of the energy spectra of linac photon beams²²⁻²³ and those
154 with energies below 10 keV typically travel <0.5 cm through water before interacting.²⁴

155 **2.C.1. In-water doses**

156 The DOSXYZnrc code (version: v20017)²⁵ was used to calculate doses absorbed
157 from 6 and 15 MV fields by water voxels within a 50×50×50 cm³ water phantom located

158 at 100 cm source-to-surface distance (SSD). Radiation transport parameters were
159 selected as described previously, with ECUT and PCUT set to 521 and 1 keV¹⁰, electrons
160 and photons with lower energies typically travelling <10 μm through water before
161 stopping or interacting.^{21, 24}

162 On-axis doses were calculated at 5 and 15 cm depths in water for the three fields.
163 Off-axis dose-in-water profiles were calculated for the 0.5×0.5 cm² field at 5 and 15 cm
164 depths, and a percentage depth-dose (PDD) was calculated along the central axis down
165 to 30 cm depth. Water voxel dimensions were chosen to allow doses to be calculated
166 with good statistical precision and suitable spatial resolution in reasonable times, as
167 detailed in Table I. All doses in our Monte Carlo simulations were normalized by numbers
168 of electrons incident on the linac target.

169

170 **2.C.2. Detector readings**

171 Models of the unmodified 60023-type detector and the detector with a 0.6 mm
172 airgap added were built *in-silico* according to the manufacturer's blueprints, using the
173 EGS++ geometry package within the egs_chamber user-code (version: v20017).²⁶ Some
174 Monte Carlo calculations were also run for a 60023-type detector with a 0.3 mm thick
175 airgap, although a real detector with an airgap of this thickness has yet to be
176 manufactured. PEGS4 data-files containing detector material cross-section and
177 stopping-power data were created as described previously¹⁰, setting the AE and AP
178 thresholds for knock-on electrons and secondary bremsstrahlung photons to 512 and 1
179 keV respectively.

180 *In-silico*, detectors were aligned parallel to the beam and positioned within a
181 50×50×50 cm³ water phantom. Doses absorbed by detector sensitive volumes were
182 calculated using the egs_chamber user-code. Detector readings were considered to be

183 proportional to these doses, the proportionality constant cancelling in calculations of
184 relative readings. The global ECUT and PCUT thresholds were set to 521 and 1 keV,
185 electrons and photons with lower energies typically travelling <1.5 and $5\ \mu\text{m}$ respectively
186 through silicon before stopping or interacting.^{21, 24} Photon cross-section enhancement
187 was used to accelerate calculations.¹⁰

188 Doses absorbed by detector sensitive volumes located on-axis at 5 and 15 cm
189 depths in water in 6 and 15 MV fields of size 0.5×0.5 , 0.7×0.7 and $4\times 4\ \text{cm}^2$ were
190 computed to a precision of $\leq\pm 0.2\%$ (2 standard deviations, s.d.). To simulate field profiles
191 measured at these depths, sensitive volume doses were calculated for detectors
192 computationally shifted across the $0.5\times 0.5\ \text{cm}^2$ field in 0.25 mm steps, holding precision
193 to $\leq\pm 0.7\%$ up to 1 mm beyond the field-edge. Since the beam and detector models were
194 symmetric, only half-profiles were calculated.

195 PDD curves measured for the $0.5\times 0.5\ \text{cm}^2$ field were simulated by calculating
196 sensitive volume doses for detectors located on-axis at depths increasing from 0-2 cm in
197 0.5 mm steps, from 2-5 cm in 1 mm steps, 5-20 cm in 1 cm steps, and 20-30 cm in 5 cm
198 steps. Doses were calculated to a precision of $\leq\pm 0.7\%$ up to 15 cm deep, and $\leq\pm 1\%$
199 beyond this depth.

200 **2.D. Experimental measurements**

201 The 60023-type detectors were tested experimentally in a Blue Phantom 2 water
202 tank (IBA dosimetry, Schwarzenbruck, Germany) set up at an SSD of 100 cm. They were
203 placed one-by-one in the tank, aligned parallel to the beam-axis, connected to an
204 electrometer box and associated OmniPro-Accept 7.4 computer software with no bias
205 voltage¹⁰, and irradiated in 6 and 15 MV fields generated by a Varian TrueBeam linear

206 accelerator (linac) (Varian Medical systems, Palo Alta, California) oriented at 0° gantry
207 angle.

208 Measurements were made for filter-flattened 6 and 15 MV square-fields of nominal
209 side-length 0.5, 0.7, 1.0, 3.0, 4.0, 6.0 and 10.0 cm projected to isocentre, and for an
210 additional filter-flattened 6 MV square-field of side-length 1.5 cm. Fields were collimated
211 using the linac jaws with multileaves retracted. Once set for a particular field and beam
212 energy, jaw positions were maintained until measurements were complete for all
213 detectors. In-line and cross-line profiles were measured at depths of 5 and 15 cm for the
214 0.5×0.5 and 0.7×0.7 cm² fields. In these fields particular care was taken to ensure
215 detectors were centered, adjusting the zeroing of a detector's lateral coordinates if
216 measured profiles were offset by more than 0.3 mm from the origin, limiting possible
217 under-measurement of on-axis doses due to detector mis-positioning to the 1% level.¹⁹
218 On-axis readings were taken with the diodes positioned at 5 and 15 cm depths in water
219 and irradiated using fixed numbers of monitor units (MUs). Finally, PDD curves were
220 measured down the beam central-axis.

221 When making the on-axis measurements used to calculate $k_{Q_{clin,4\text{ cm}}}^{f_{clin,4\text{ cm}}}$ factors, the
222 top surfaces of diodes were positioned 0.9 mm above the intended measurement point,
223 on the assumption that EPOMs in the modified detectors lay 0.9 mm below the detector
224 tops, as for the unmodified 60023-type detector. Small changes in EPOM with airgap
225 thickness will have negligible effect on resulting $k_{Q_{clin,4\text{ cm}}}^{f_{clin,4\text{ cm}}}$ values, which depend only on
226 ratios of detector measurements.¹⁰ Doses-to-water also form part of the $k_{Q_{clin,4\text{ cm}}}^{f_{clin,4\text{ cm}}}$
227 calculation and were measured using EBT3 film for fields $\leq 1.5 \times 1.5$ cm² and an IBA CC13
228 ionization chamber for fields $\geq 3 \times 3$ cm².

229 To determine any dose-rate dependence, unmodified 60023- and 60017-type
230 diodes were placed on-axis at 5 cm depth in a water phantom set up with an SSD of 100
231 cm, and repeatedly irradiated to 300 MU in a 4×4 cm² 6 MV flattening-filter-free (FFF)
232 field. The linac's nominal dose-rate was varied right across the range deliverable for this
233 field, from 400 to 1300 MU min⁻¹ in increments of 200 MU min⁻¹ by changing the pulse
234 repetition frequency. Dose-per-MU was determined at the measurement point using an
235 NE2571A-type ionization chamber, allowing dose-rates to be calculated in Gy min⁻¹.
236 Detector sensitivities were measured as charge-per-Gy and normalized to the sensitivity
237 at 600 MU min⁻¹.

238 **2.E. Radiochromic film techniques**

239 In small fields, measurements of doses absorbed by water were made using 6×6
240 cm² squares of Gafchromic EBT3 film. The squares were handled with nitrile gloves
241 under minimum light, placed one-by-one in a metallic frame, submerged at the
242 measurement depth in water with an SSD of 100 cm and irradiated as previously
243 described.¹⁰

244 To generate calibration curves, films placed at 5 cm depth in a 4×4 cm² field were
245 irradiated to seven dose-levels ranging from 0 to 4.35 Gy. Five film-squares were
246 irradiated at each dose-level and separate curves were measured for the 6 and 15 MV
247 beams. Doses in small fields were then measured at 5 and 15 cm depths by irradiating
248 three film-squares at each field size and depth combination, scaling MUs so that roughly
249 2 Gy was delivered to each film.

250 At 48 hours after irradiation film-squares were scanned using an Epson V750 Pro
251 scanner (Epson UK, Hemel Hempstead). Using in-house software⁸ 6 and 15 MV

252 calibration curves were created and dose-maps extracted from scanned films as arrays
253 in which each point represents the average dose in a $0.51 \times 0.51 \text{ mm}^2$ area.¹⁰

254 **2.F. Uncertainty estimation**

255 Statistical uncertainties estimated history-by-history²⁷ in Monte Carlo calculated
256 doses were taken from output files, and uncertainties in doses measured using detectors
257 and film were calculated from repeat measurements. Uncertainties in quantities such as
258 detector correction factors and measurement inaccuracy were calculated from these
259 underlying uncertainties using standard error propagation techniques. All uncertainties
260 are shown at the ± 2 s.d. level.

261 **3. RESULTS**

262 **3.A. Monte Carlo simulated data**

263 **3.A.1. On-axis $k_{Q_{clin,4 \text{ cm}}}^{f_{clin,4 \text{ cm}}}$ factors**

264 Table II lists Monte Carlo-calculated on-axis $k_{Q_{clin,4 \text{ cm}}}^{f_{clin,4 \text{ cm}}}$ values for detectors
265 irradiated in 6 MV 0.5×0.5 and $0.7 \times 0.7 \text{ cm}^2$ fields at 5 cm depth in water.

266 For the unmodified 60023-type detector, $k_{Q_{0.5,4 \text{ cm}}}^{0.5,4 \text{ cm}}$ and $k_{Q_{0.7,4 \text{ cm}}}^{0.7,4 \text{ cm}}$ were 0.979 ± 0.006
267 and 0.977 ± 0.006 , indicating small over-responses. For the 60023-type variant with a
268 0.6 mm airgap corresponding values were 1.029 ± 0.006 and 1.002 ± 0.006 , and since
269 these values show that the detector was slightly over-corrected we did not carry out
270 calculations for detectors with 0.8 and 1.0 mm airgaps. For the hypothetical 60023-type
271 variant with a 0.3 mm airgap $k_{Q_{0.5,4 \text{ cm}}}^{0.5,4 \text{ cm}}$ and $k_{Q_{0.7,4 \text{ cm}}}^{0.7,4 \text{ cm}}$ were 1.007 ± 0.006 and 0.995 ± 0.006 ,
272 better than either the unmodified 60023 detector or its 0.6 mm airgap variant. For

273 comparison, corresponding values previously computed for the 60017-type diode were
274 0.910 ± 0.005 and 0.971 ± 0.007 .¹⁰

275 Table II also lists Monte Carlo $k_{Q_{clin,4\text{ cm}}}^{f_{clin,4\text{ cm}}}$ values calculated at 15 cm depth in water
276 for 6 MV 0.5×0.5 and 0.7×0.7 cm² fields. Results follow the pattern at 5 cm depth:
277 $k_{Q_{clin,4\text{ cm}}}^{f_{clin,4\text{ cm}}}$ factors were much closer to unity for the unmodified 60023-type than for the
278 60017-type diode; the 60023-type detector with the 0.6 mm airgap was over-corrected;
279 and factors calculated for the hypothetical 60023-type detector with the 0.3 mm airgap
280 were closest to unity. The table additionally includes $k_{Q_{clin,4\text{ cm}}}^{f_{clin,4\text{ cm}}}$ factors calculated for the
281 15 MV beam, which follow the same pattern.

282 **3.A.2. Off-axis detector response**

283 Monte Carlo simulations of errors in doses obtained from uncorrected off-axis
284 detector readings are plotted in Fig. 1 for the unmodified 60023-type detector and the 0.6
285 mm airgap variant. Readings were simulated for detectors located at 5 and 15 cm depths
286 in 6 and 15 MV 0.5×0.5 cm² fields, at cross-line positions along the direction of travel of
287 the X jaws. Errors are shown as fractions of on-axis dose.

288 Within fields the unmodified detector over-responded whereas the detector with
289 the 0.6 mm airgap under-responded. At 5 cm depth in the 6 MV 0.5×0.5 cm² field, the
290 maximum error for either detector was $\leq 3\%$ of the on-axis dose. At 15 cm depth the
291 unmodified detector over-responded by at most $2.1\% \pm 0.7\%$ normalized to the on-axis
292 dose, and the 0.6 mm airgap detector variant under-responded by at most $4.9\% \pm 0.7\%$.
293 In the 15 MV 0.5×0.5 cm² field the unmodified detector maximally over-responded by
294 2.2% and $1.6\% \pm 0.6\%$ at 5 and 15 cm depths, whereas the 0.6 mm airgap detector
295 maximally under-responded by $4.9\% \pm 0.5\%$ at both depths.

296 **3.A.3. PDD curves**

297 Monte Carlo PDD data calculated for the 6 MV 0.5×0.5 cm² field are shown in Fig.
298 2. Computed in-water depth-doses are graphed along with simulations of PDDs
299 measured using the unmodified 60023-type detector and the 0.6 mm airgap variant.
300 Figure 2(a) shows the build-up curves: a small lateral offset of 0.2 mm can be seen
301 between the curves calculated for the modified and unmodified diodes. Both curves were
302 plotted so that the ‘kick-points’ (at which the PDD gradients suddenly increase as the
303 tops of the detectors become submerged¹⁰) occur at 0.9 mm depth, and thus for the
304 unmodified detector the plotted measurement depths correspond to depths of the
305 manufacturer-specified EPOM.

306 Figure 2(b) shows whole PDD curves, with the modified detector’s PDD now
307 shifted by 0.2 mm. The PDDs simulated for the unmodified and modified diodes agree
308 well and concur with the calculated in-water PDD, both in the build-up region and at
309 greater depths. This is further demonstrated by the ratios of computed diode-measured
310 and in-water PDDs plotted in Fig. 2(c), which between 1 and 30 cm depths in water differ
311 from unity by less than 1%. These results indicate that the EPOM of the modified detector
312 lies 0.9 + 0.2 = 1.1 mm below its top. The same EPOM was obtained when Monte Carlo
313 15 MV data (not plotted) were analyzed.

314 **3.B. Experimentally measured data**

315 **3.B.1. On-axis $k_{Q_{0.5,4\text{ cm}}}^{f_{clin,4\text{ cm}}}$ factors**

316 On-axis $k_{Q_{0.5,4\text{ cm}}}^{0.5,4\text{ cm}}$ factors measured experimentally for the unmodified and modified
317 60023-type detectors at 5 cm depth in water in a 6 MV 0.5×0.5 cm² field are plotted in
318 Fig. 3. They increase with airgap thickness from 0.973 ± 0.010 (2 s.d.) for the unmodified

319 60023-type diode to 1.022, 1.035 and 1.050 ± 0.011 for detectors with airgaps of 0.6, 0.8
320 and 1.0 mm thickness respectively. Since the diodes with 0.8 mm and 1.0 mm airgaps
321 performed less well than the others, we did not test them further.

322 On-axis $k_{Q_{clin,4\text{ cm}}}^{f_{clin,4\text{ cm}}}$ values measured for the unmodified 60023-type detector and
323 the 0.6 mm airgap variant are plotted against field-size in Fig. 4. The factors were
324 measured at 5 and 15 cm depths in water for 6 and 15 MV fields of size 0.5×0.5 to 10×10
325 cm^2 . In the 6 MV small fields the unmodified and modified 60023-type detectors over-
326 and under-responded respectively. Both performed well, though, with $k_{Q_{clin,4\text{ cm}}}^{f_{clin,4\text{ cm}}}$ lying no
327 further from unity than $2.8\% \pm 1.0\%$ for the unmodified diode and $3.0\% \pm 1.2\%$ for the
328 0.6 mm airgap detector. On-axis $k_{Q_{clin,4\text{ cm}}}^{f_{clin,4\text{ cm}}}$ values obtained previously for an unmodified
329 60017-type diode¹⁰ are plotted for comparison and indicate over-responses of up to 8.6%
330 $\pm 1.1\%$.

331 In the 15 MV small fields, the unmodified and modified 60023-type detectors again
332 over- and under-responded by up to $3.6\% \pm 1.6\%$ and $4.7\% \pm 1.3\%$ respectively. The
333 60017-type detector over-responded by at most $10.6\% \pm 1.4\%$.

334 **3.B.2. Off-axis detector response**

335 Responses of the unmodified 60023-type detector and the 0.6 mm airgap variant
336 off-axis at 5 and 15 cm depths in 6 and 15 MV $0.5 \times 0.5 \text{ cm}^2$ fields are plotted in Figs. 5
337 and 6. The plots show profiles of errors in doses obtained from uncorrected detector
338 readings, normalized to the on-axis dose. The errors were calculated from diode and
339 EBT3 film measurements taken cross-line along the direction of travel of the lower (X)
340 jaws.

341 At 5 cm depth in the 6 MV field, the maximum error for the unmodified 60023-type
342 detector was a 4.0% over-response within the field, normalized to on-axis dose. In
343 comparison the 60017-type detector over-responded by up to 9.7%.¹⁰ For the 0.6 mm
344 airgap detector, maximum errors were a 2.5% under-response within the field and a 3.0%
345 over-response just beyond the field-edge. At 15 cm depth the unmodified 60023-type
346 detector read correctly to within 2.8% of the on-axis dose across most of the measured
347 range, with a maximum 4.0% over-response in a narrow spike attributable to noise in the
348 film profiles. The 0.6 mm airgap detector had a maximum 4.0% under-response.

349 Similarly, in the 15 MV 0.5×0.5 cm² field, maximum errors at depths of 5 and 15
350 cm were over-responses of 5.3% and 2.9% respectively for the unmodified 60023-type
351 diode, and under-responses of 4.2% and 5.0% for the diode with the 0.6 mm airgap.

352 **3.B.3. PDD curves**

353 Depth-dose curves measured for the 6 MV 0.5×0.5 cm² field using the unmodified
354 60023-type detector and the 0.6 mm airgap variant are plotted in Fig. 7. Build-up curves
355 are shown in Fig. 7(a) with measurement depths plotted so that the kick-points for both
356 detectors occur at 0.9 mm depth. For the unmodified 60023-type diode, plotted
357 measurement depths thus correspond to depths of the EPOM. The longitudinal shift
358 visible between the two build-up curves, 0.2 mm at 80% of the maximum dose, suggests
359 the EPOM of the 0.6 mm airgap diode lies 1.1 mm below its top.

360 In Fig. 7(b) complete 0.5×0.5 cm² PDD curves are plotted for the two detectors,
361 with measurement depths adjusted for the modified diode so that the kick-point of its
362 PDD occurs at 1.1 mm depth. These curves agree well as demonstrated further in Fig.
363 7(c) in which their ratio is plotted, confirming that the modified detector's EPOM lies 1.1
364 mm below its top surface.

365 Table III lists the ratio of doses measured at 15 and 5 cm depths in the 6 MV 4×4
366 cm² field using the IBA CC13 ionization chamber, which is expected to accurately
367 represent the variation of dose in water with depth. The table also lists equivalent ratios
368 of readings for the 60017-type diode and the unmodified 60023-type detector and its 0.6
369 mm airgap variant. For the 60017-type detector the ratio was 1.1% ± 0.2% below that
370 measured using the ionization chamber, comparable to a 1% reduction in response of
371 the 60017-type detector relative to an ionization chamber previously observed between
372 5 and 15 cm depths in measured 4×4 cm² PDD curves.¹⁰ For the 60023-type detectors,
373 however, the ratio was only 0.3% ± 0.2% below the ionization chamber ratio.

374 **3.B.4. Dose-rate dependence**

375 Detector sensitivity is plotted against dose-rate in Fig. 8. Across the 4-13 Gy min⁻¹
376 range sensitivity varied by less than 0.1% for the unmodified 60023-type detector
377 compared to 1.5% for the 60017-type detector.

378 **4. DISCUSSION**

379 In 6 and 15 MV small fields ≥0.5×0.5 cm², radiation doses can be measured more
380 accurately on- and off-axis at 5 and 15 cm depths in water using uncorrected readings
381 from the new PTW 60023-type *microSilicon* diode than from a 60017-type diode. Monte
382 Carlo calculations show that the 60023-type detector over-responds in the small fields
383 compared to a reference 4×4 cm² field by up to 2.6% ± 0.5% and 2.2% ± 0.7%
384 (normalized to on-axis dose-levels) at 6 and 15 MV respectively, whereas earlier
385 calculations for the 60017-type detector indicated over-responses of up to 10.2% ± 0.7%
386 and 11.9% ± 0.6%.¹⁰ Similarly, experimental data show maximum over-responses in

387 small fields of $4.0\% \pm 1.0\%$ and $5.3\% \pm 2.0\%$ at 6 and 15 MV for the 60023-type detector,
388 compared to $9.7\% \pm 1.4\%$ and $11.7\% \pm 1.4\%$ for the 60017-type detector.

389 Other investigators have reported that doses in 6 and 10 MV small fields can be
390 measured more accurately at 5 and 10 cm depths in water using 60023-type rather than
391 60017-type diodes.¹¹⁻¹³ Our results extend these findings up to a beam energy of 15 MV,
392 and to a wider range of detector locations, on- and off-axis at both 5 and 15 cm depths.
393 Our on-axis 6 MV data are in good quantitative agreement with results reported by
394 Schönfeld et al.¹¹ and Weber et al.¹², who obtained correction factors of 0.960-0.988 for
395 60023-type detectors positioned at 10 cm depth in water with an SSD of 90 cm and
396 irradiated in 6 MV small fields of size 5.5×5.5 to 6.3×6.3 mm², compared to values of
397 0.973-0.988 reported here for a detector placed on-axis in a 5×5 mm² field at 5 and 15
398 cm depths with an SSD of 100 cm.

399 The maximum over-responses we measured experimentally for the 60023-type
400 diode were a little higher than those determined computationally. This may be because
401 readings were taken at many off-axis locations, leading to maximum recorded over-
402 responses being recorded at points where results lie at the upper end of uncertainty
403 ranges, which are wider for experimental than for computational results. Closer
404 agreement was seen when only the smaller quantity of on-axis data was considered.

405 Our off-axis computational and experimental results agreed quite well (Figs. 1, 5,
406 6). They show the unmodified 60023-type detector slightly over-responding within small
407 fields, and the detector with a 0.6 mm airgap under-responding within these fields but
408 slightly over-responding beyond their edges. The correction factors required vary with
409 detector location as well as field size, and consequently detectors with correction factors

410 that are small and potentially ignorable everywhere are preferable to those requiring a
411 multiplicity of correction factor values to be calculated and applied.

412 Anomalies in experimental data gathered for 60017-type diodes¹⁰ were not
413 present in data collected for 60023-type diodes. In particular, for 60023-type diodes
414 measured $k_{Q_{clin,4\text{ cm}}}^{f_{clin,4\text{ cm}}}$ factors rose monotonically with increasing airgap thickness (Fig. 3),
415 whereas for 60017-type diodes the analogous curve measured had notable inversions at
416 some points.¹⁰ This is likely a consequence of the epoxy housing being less dense in
417 60023- than in 60017-type detectors, which limits any detector-to-detector response
418 variability resulting from differences in epoxy thickness.

419 Furthermore, ratios of doses-to-water at 15 and 5 cm depths in a 6 MV 4×4 cm²
420 field measured using the unmodified 60023-type detector and its 0.6 mm variant lay
421 within 0.3% of the ratio measured using an IBA CC13 ionization chamber (Table III),
422 whereas the same ratio measured using the 60017-type detector was 1.1% below the
423 ionization chamber ratio. This improved depth-dose accuracy of the 60023-type detector
424 is likely a consequence of its response varying negligibly with the linac dose-per-pulse¹¹,
425 in turn a result of changes made to its silicon lattice. The 60023-type detector response
426 also varied little with linac pulse repetition frequency (Fig. 8), whereas the 60017-type
427 detector response rose with increasing frequency.

428 For the 60017-type diode, the best results were achieved by adding a 1.6 mm
429 airgap.¹⁰ For the 60023-type diode the best experimental results we obtained were for a
430 detector with a thin 0.6 mm airgap added, but even this over-corrected the detector.
431 Further Monte Carlo calculations suggest that close-to-optimal results can be obtained
432 using a 60023-type detector with an even thinner 0.3 mm airgap, for which computed
433 under-responses on-axis in 6 and 15 MV 0.5×0.5 cm² fields were just 1.0% ± 0.8% in the

434 6 MV beam and $1.3\% \pm 0.8\%$ in the 15 MV beam. We have not experimentally
435 characterized such a detector as PTW have yet to fabricate one. The gains achievable
436 in routine practice will depend on the accuracy and precision with which the airgap and
437 other components can be manufactured, and structural stability over time.

438 Depth-dose data indicate that inclusion of the 0.6 mm thick airgap in the 60023-
439 type detector deepened its EPOM by 0.2 mm from its top surface, in line with a finding in
440 modified 60017-type detectors that EPOM depths were increased by around one-third of
441 airgap thicknesses.¹⁰

442 5. CONCLUSIONS

443 The 60023-type *microSilicon* diode measures radiation doses in small photon
444 fields substantially more accurately than does the 60017-type diode. At 5 and 15 cm
445 depths on- and off-axis in 6 and 15 MV fields $\geq 0.5 \times 0.5 \text{ cm}^2$, the greatest dosimetric errors
446 found for the 60023-type detector were over-responses of $2.6\% \pm 0.5\%$ determined
447 computationally and $5.3\% \pm 2.0\%$ determined experimentally, compared to $11.9\% \pm 0.6\%$
448 and $11.7\% \pm 0.8\%$ for a 60017-type detector. The ratio of doses at 15 and 5 cm depths
449 in a $4 \times 4 \text{ cm}^2$ field was also experimentally measured more accurately using the 60023-
450 type than the 60017-type diode; and whereas the sensitivity of the 60017-type detector
451 fell by 1.5% as dose-rates were reduced from 13 to 4 Gy min^{-1} by decreasing the linac
452 pulse repetition frequency, the sensitivity of the 60023-type detector changed little.

453 Building a 0.6 mm airgap into the 60023-type diode over-corrected the detector,
454 leading to maximum under-responses in small fields of around 5%. According to further
455 Monte Carlo calculations a 0.3 mm airgap would produce close-to-optimal detector
456 performance.

457

458 **ACKNOWLEDGEMENTS**

459 The authors thank PTW-Freiburg for manufacturing and providing the diode
460 detectors tested in this work.

461

462 **CONFLICTS OF INTEREST**

463 Dr Jan U Würfel is an employee of PTW-Freiburg.

464

465 **DATA AVAIABILITY STATEMENT**

466 The data supporting the findings of this study are presented in the figures and tables.

467

468

469 **References**

- 470 1. Alfonso R, Andreo P, Capote R, et al. Dosimetry of Small Static Fields Used in
471 External Beam Radiotherapy: An International Code of Practice for Reference and
472 Relative Dose Determination. Technical Report Series No. 483. Vienna:
473 International Atomic Energy Agency; 2017.
474
- 475 2. Scott AJD, Kumar S, Nahum AE, Fenwick JD. Characterizing the influence of
476 detector density on dosimeter response in non-equilibrium small photon fields.
477 *Phys Med Biol.* 2012; 57: 4461–4476.
478
- 479 3. Bassinet C, Huet C, Derreumaux S, et al. Small fields output factors
480 measurements and correction factors determination for several detectors for a
481 Cyberknife® and linear accelerators equipped with microMLC and circular cones.
482 *Med Phys.* 2013; 40: 071725.
483
- 484 4. Charles PH, Cranmer-Sargison G, Thwaites DI, Kairn T, Crowe SB, Pedrazzini G,
485 Aland T, Kenny J, Langton CM, Trapp JV. Design and experimental testing of air
486 slab caps which convert commercial electron diodes into dual purpose, correction-
487 free diodes for small field dosimetry. *Med Phys.* 2014; 41: 101701.
488
- 489 5. Fenwick JD, Georgiou G, Rowbottom CG, Underwood TSA, Kumar S, Nahum AE.
490 Origins of the changing detector response in small megavoltage photon radiation
491 fields. *Phys Med Biol.* 2018; 63: 125003.
492
- 493 6. Underwood TSA, Winter HC, Fenwick JD, Hill MA. OC-0512 Modifying detector
494 designs for small field dosimetry. *Radiother Oncol.* 2012; 103: S206.
495
- 496 7. Underwood TSA, Winter HC, Hill MA, Fenwick JD. Mass-density compensation
497 can improve the performance of a range of different detectors under non-
498 equilibrium conditions. *Phys Med Biol.* 2013; 58: 8295–8310.
499
- 500 8. Underwood TSA, Thompson J, Bird L, Scott AJD, Patmore P, Winter HC, Hill MA,
501 Fenwick JD. Validation of a prototype DiodeAir for small field dosimetry. *Phys Med*
502 *Biol.* 2015; 60: 2939–2953.
503

- 504 9. Charles PH, Crowe SB, Kairn T, Knight RT, Hill B, Kenny J, Langton CM, Trapp
505 JV. Monte Carlo-based diode design for correction-less small field dosimetry.
506 *Phys Med Biol.* 2013; 58: 4501–4512.
- 507
- 508 10. Georgiou G, Kumar S, Würfel JU, Underwood TSA, Thompson JM, Hill MA,
509 Rowbottom CG, Fenwick JD. Density compensated diodes for small field
510 dosimetry: comprehensive testing and implications for design. *Phys Med Biol.*
511 2020; 65: 155011.
- 512
- 513 11. Schönfeld AB, Poppinga D, Kranzer R, De Wilde RL, Willborn K, Poppe B, Looe
514 HK. Technical note: Characterization of the new microSilicon diode detector. *Med*
515 *Phys.* 2019; 46: 4257-4262.
- 516
- 517 12. Weber C, Kranzer R, Weidner J, Kröniger K, Poppe B, Looe H, Poppinga D.
518 Small field output correction factors of the microSilicon detector and a deeper
519 understanding of their origin by quantifying perturbation factors. *Med Phys.* 2020;
520 47: 3165-3173.
- 521
- 522 13. Akino Y, Fujiwara M, Okamura K, Shiomi H, Mizuno H, Isohashi F, Suzuki O, Seo
523 Y, Tamari K, Ogawa K. Characterization of a microSilicon diode detector for small-
524 field photon beam dosimetry. *J Radiat Res.* 2020; 61: 410-418.
- 525
- 526 14. Francescon P, Kilby W, Noll JM, Satariano N, Orlandi C. Small field dosimetry
527 correction factors for circular and MLC shaped fields with the CyberKnife M6
528 System: evaluation of the PTW 60023 microSilicon detector. *Phys Med Biol.* 2020;
529 65: 01NT01.
- 530
- 531 15. Weidlich GA, Chung W, Kolli S, Thirunarayan I, Loysel T. Characterization of the
532 ZAP-X peripheral dose fall-off. *Cureus.* 2021; 13: e13972.
- 533
- 534 16. Alfonso R, Andreo P, Capote R, Huq MS, Kilby W, Kjäll P, Mackie TR, Palmans
535 H, Rosser K, Seuntjens J, Ullrich W, Vatnitsky S. A new formalism for reference
536 dosimetry of small and nonstandard fields. *Med Phys.* 2008; 35: 5179–5186.
- 537
- 538 17. Kawrakow I, Mainegra-Hing E, Rogers DWO, Tessier F, Walters BRB. The
539 EGSnrc code system: Monte Carlo simulation of electron and photon transport.

540 Technical Report No. PIRS 701. Ottawa: National Research Council of Canada;
541 2017.

542

543 18. Rogers DWO, Walters B, Kawrakow I. BEAMnrc Users Manual. Technical Report
544 No. PIRS 509 (A) rev L. Ottawa: National Research Council of Canada; 2017.

545

546 19. Underwood TSA, Winter HC, Hill MA, Fenwick JD. Detector density and small field
547 dosimetry: integral versus point dose measurement schemes. *Med Phys.* 2013;
548 40: 082102.

549

550 20. Scott AJD, Nahum AE, Fenwick JD. Using a Monte Carlo model to predict
551 dosimetric properties of small radiotherapy photon fields. *Med Phys.* 2008; 35:
552 4671–4684.

553

554 21. National Institute of Science and Technology. Stopping Power and Range Tables
555 for Electrons (<https://physics.nist.gov/PhysRefData/Star/Text/ESTAR.html>);
556 2021. (Accessed: 5th July 2021)

557

558 22. Ali ESM, Rogers DWO. Functional forms for photon spectra of clinical linacs. *Phys*
559 *Med Biol.* 2012; 57: 31-50.

560

561 23. Khabaz R. Effect of each component of a LINAC therapy head on neutron and
562 photon spectra. *Appl Radiat Isot.* 2018; 139: 40-45.

563

564 24. Hubbell JH, Seltzer SM. Tables of X-Ray Mass Attenuation Coefficients and Mass
565 Energy-Absorption Coefficients (Version 1.4). Gaithersburg, MD: National
566 Institute of Standards and Technology; 2004

567

568 25. Rogers DWO, Kawrakow I, Seuntjens JP, Walters BRB, Mainegra-Hing E. NRC
569 User Codes for EGSnrc. Technical Report No. PIRS-702 rev C. Ottawa: National
570 Research Council of Canada; 2017.

571

572 26. Wulff J, Zink K, Kawrakow I. Efficiency improvements for ion chamber calculations
573 in high energy photon beams. *Med Phys.* 2008; 35: 1328-1336.

574

575 27. Walters BRB, Kawrakow I, Rogers DWO. History by history statistical estimators in
576 the BEAM code system. *Med Phys.* 2002; 29: 2745-2752.

577 **FIGURE LEGENDS:**

578

579

580 **FIG. 1.** Monte Carlo calculations of errors in doses obtained from uncorrected detector
581 readings off-axis at 5 and 15 cm depths in water for 6 and 15 MV 0.5×0.5 cm² fields,
582 normalized to on-axis doses. Results are plotted for the unmodified 60023-type detector
583 and the 0.6 mm airgap (a.g.) variant. ± 2 s.d. error bars are shown.

584

585

586 **FIG. 2.** Monte Carlo depth-dose data for a 6 MV 0.5×0.5cm² field, showing in-water doses
587 and simulations of PDDs measured using the unmodified 60023-type detector and the
588 0.6 mm airgap (a.g.) variant: (a) the build-up region; (b) complete PDD curves; (c) ratios
589 of diode-measured to in-water PDD curves, normalized to unity at 5 cm depth.
590 Measurement depths were defined as 0.9 mm below the top surface of both detectors in
591 panel (a), and 0.9 and 1.1 mm below the tops of the unmodified 60023-type diode and
592 the 0.6 mm airgap variant in (b) and (c). Statistical uncertainties on calculated doses
593 were ≤1% (2 s.d.) and are omitted to improve visual clarity.

594

595

596 **FIG. 3.** On-axis $k_{Q_{0.5,4\text{ cm}}}^{0.5,4\text{ cm}}$ correction factors measured experimentally in a 6 MV beam for
597 unmodified and modified 60023-type detectors at 5 cm depth in water, plotted against
598 airgap thickness. ±2 s.d. error bars are shown.

599

600 **FIG. 4.** On-axis $k_{Q_{clin,4\text{ cm}}}^{f_{clin,4\text{ cm}}}$ values measured experimentally in 6 MV and 15 MV square
601 fields at 5 and 15 cm depths in water, for the unmodified 60023-type detector and the 0.6
602 mm airgap (a.g.) variant. Data for an unmodified 60017-type diode are shown for
603 comparison. The reference condition was on-axis in a 4×4 cm² field at 5 cm depth in
604 water. ±2 s.d. error bars are shown.

605

606

607

608

609

610 **FIG. 5.** Off-axis diode response measured experimentally in a 6 MV 0.5×0.5 cm² field for
611 the unmodified 60023-type detector and the 0.6 mm airgap (a.g.) variant. Plots show
612 errors in measured doses across the field at 5 and 15 cm depths in water, obtained from
613 uncorrected detector readings, relative to the on-axis dose. Data for the unmodified
614 60017-type diode at 5 cm depth are shown for comparison. ± 2 s.d. error bars are shown
615 on-axis, at the field-edge and 4.5 mm beyond the field-edge.

616
617
618

619 **FIG. 6.** Off-axis diode response measured experimentally in a 15 MV 0.5×0.5 cm² field
620 for the unmodified 60023-type detector and the 0.6 mm airgap (a.g.) variant. Data for the
621 unmodified 60017-type diode at 5 cm depth are shown for comparison. ± 2 s.d. error bars
622 are shown.

623

624 **FIG. 7.** 6 MV depth-dose data measured experimentally for a 0.5×0.5 cm² field using the
625 unmodified 60023-type diode and the 0.6 mm airgap (a.g.) variant, showing (a) the build-
626 up region, (b) complete PDD curves, (c) the ratio of PDD curves. In (a) measured depths
627 are plotted so that the kick-points occur at 0.9 mm for both detectors, whereas in (b) and
628 (c) depths have been shifted for the modified detector so that its kick-point occurs at 1.1
629 mm depth.

630

631 **FIG. 8.** Sensitivities of the unmodified 60017- and 60023-type detectors, measured
632 experimentally on-axis at 5 cm depth in water in a 6 MV 4×4 cm² field. Dose-rate was
633 varied by changing the linac pulse repetition frequency. Results are normalized to the
634 sensitivity at 600 MU min⁻¹.

635
636

637

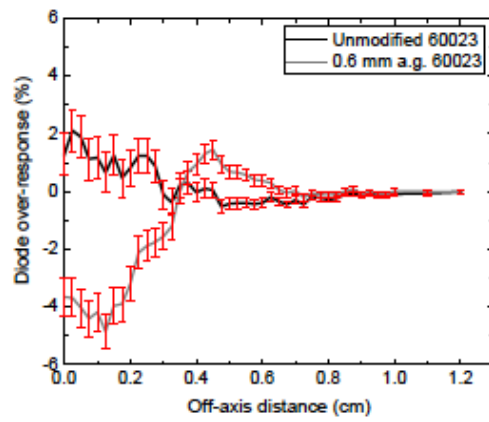
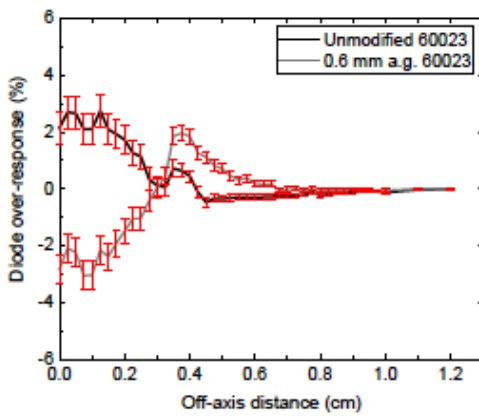
FIG. 1.

638

6 MV, 5 cm depth

6 MV, 15 cm depth

639



640

641

642

643

644

15 MV, 5 cm depth

15 MV, 15 cm depth

645

646

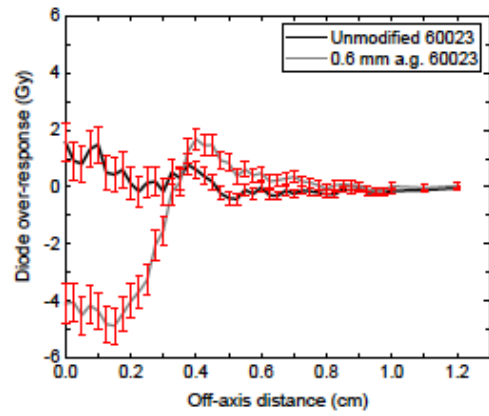
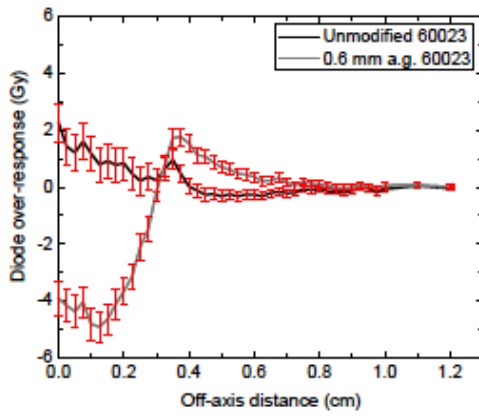
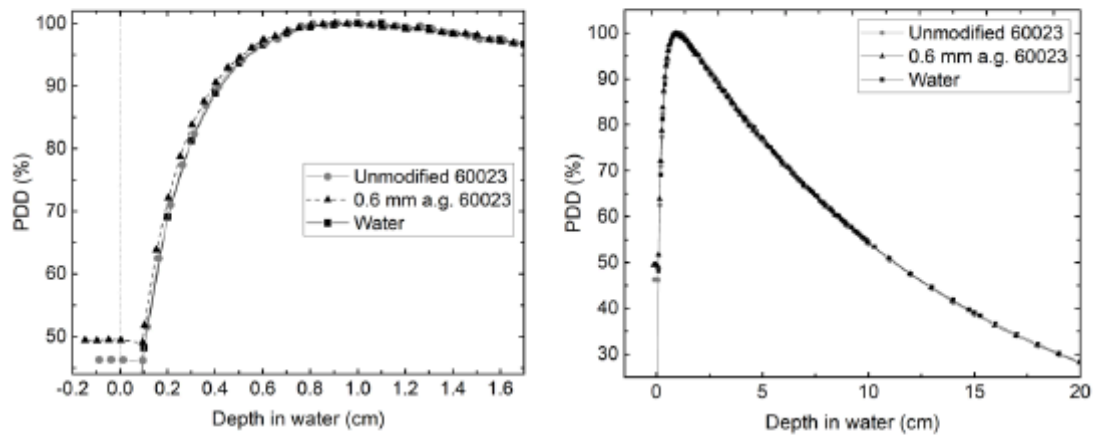
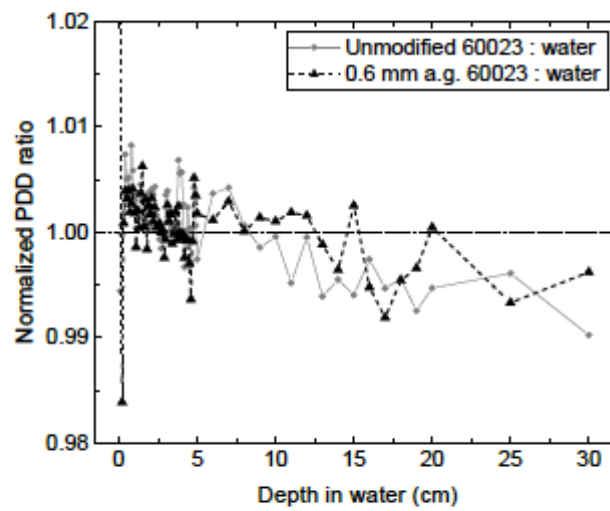


FIG. 2.



(a)

(b)



(c)

FIG. 3.

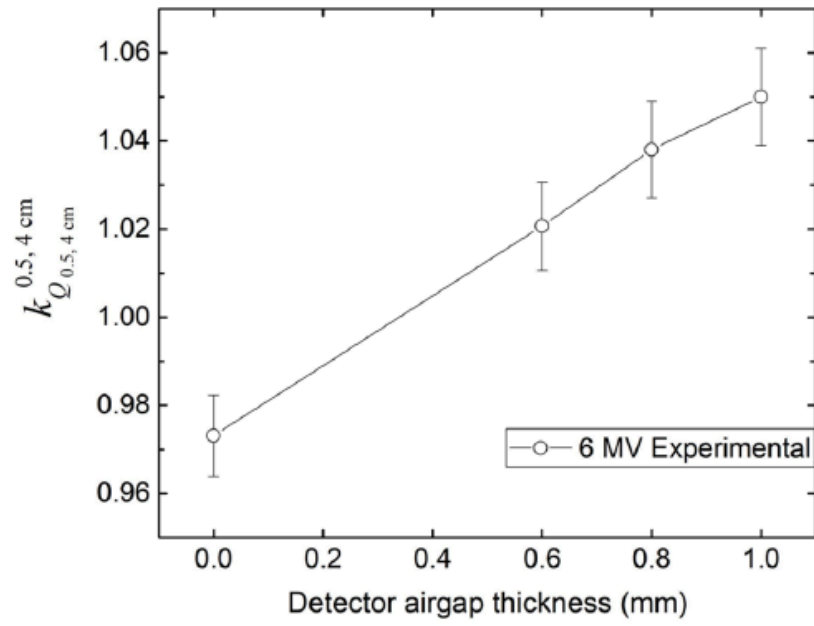


FIG. 4.

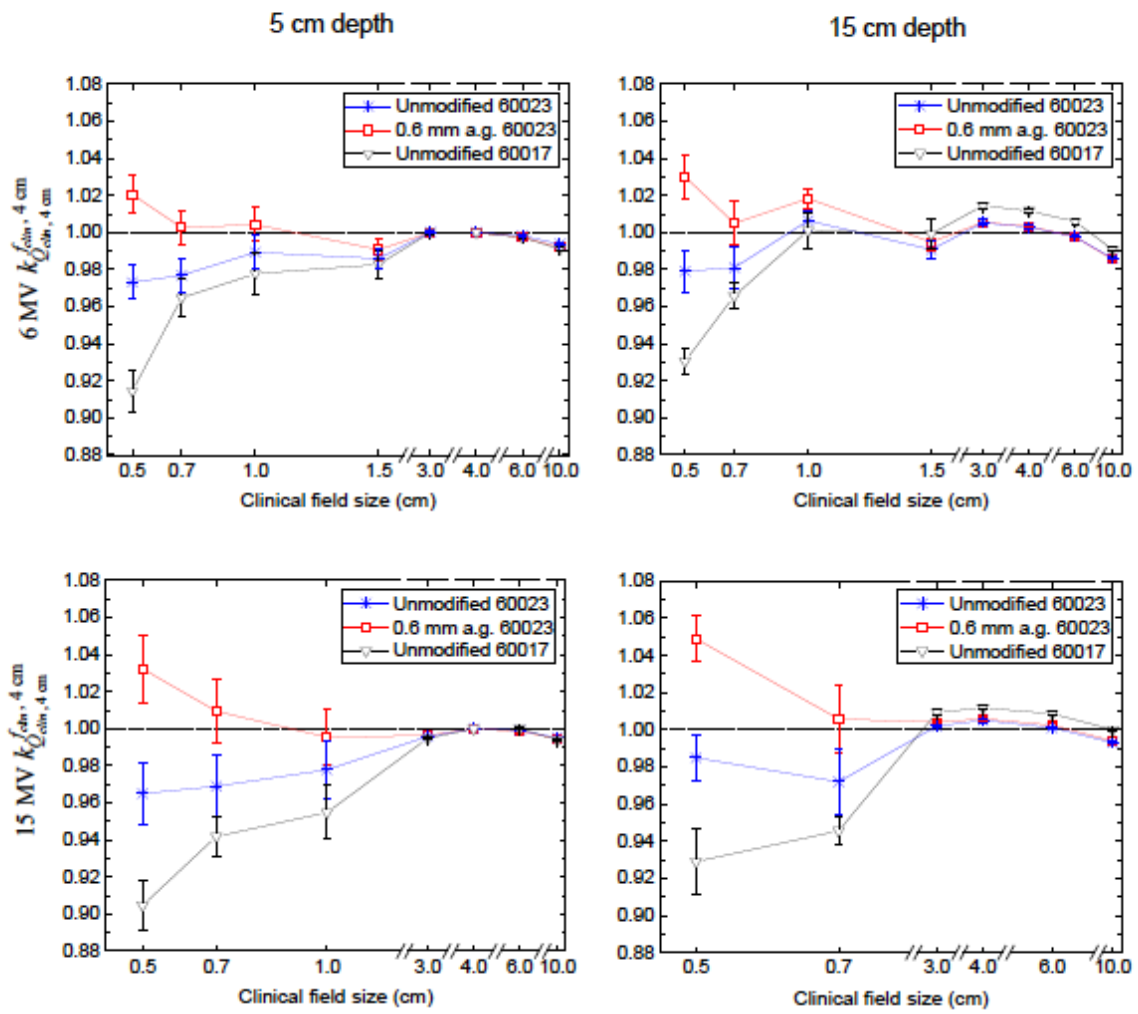


FIG. 5.

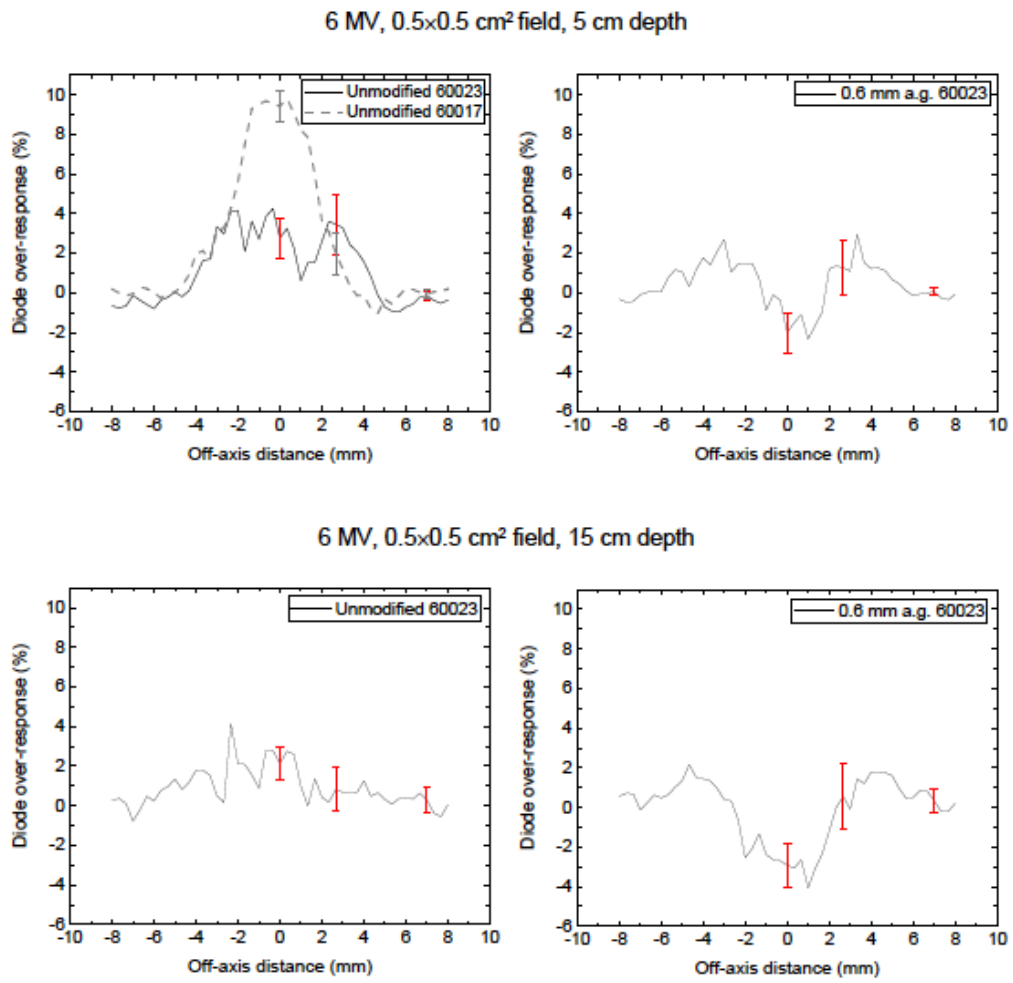


FIG. 6.

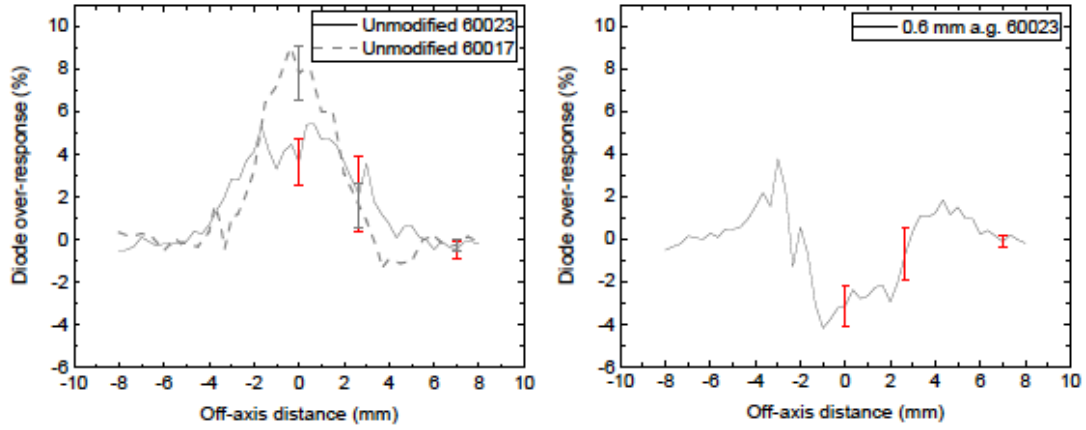
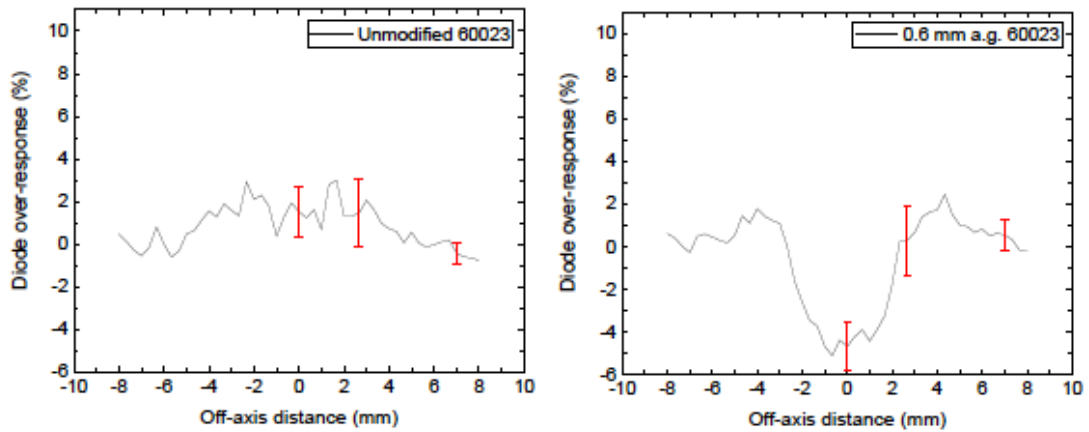
15 MV, 0.5x0.5 cm² field, 5 cm depth15 MV, 0.5x0.5 cm² field, 15 cm depth

FIG. 7.

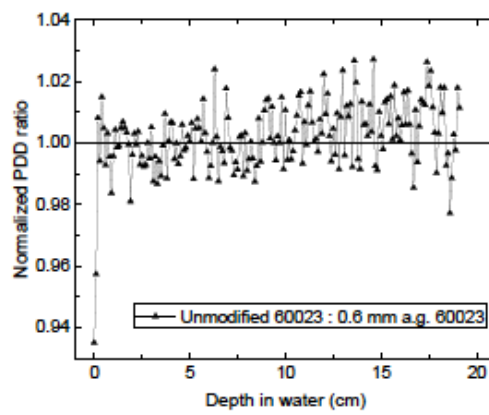
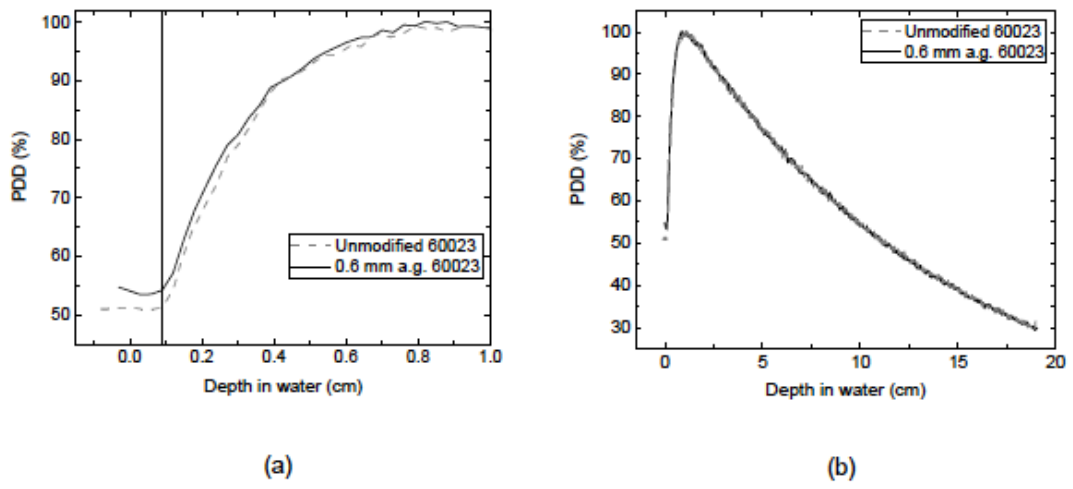
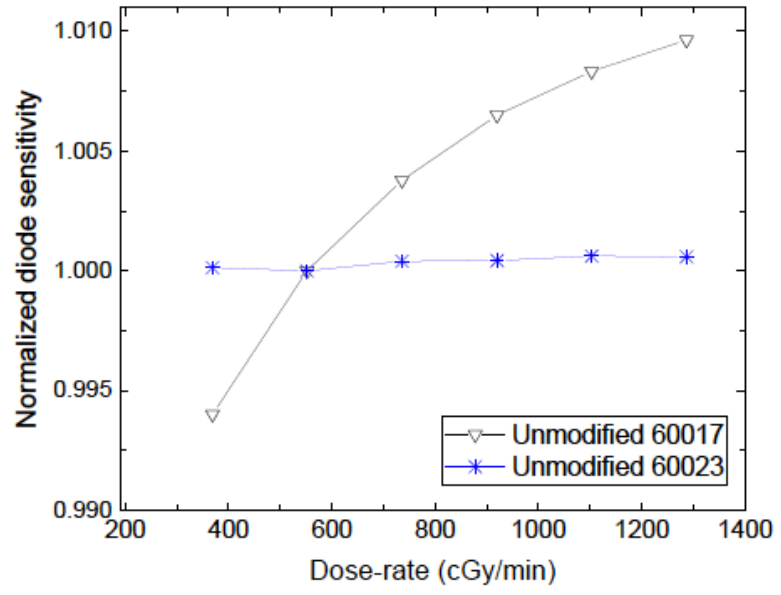


FIG. 8.



654 **TABLE I.** Voxel dimensions used in Monte Carlo calculations of doses absorbed by
 655 water. The first two voxel dimensions listed are perpendicular to the beam axis, the third
 656 along it. Levels of precision achieved in dose calculations are also shown as ± 2 standard
 657 deviation (s.d.) uncertainties.

658

Field size (mm ²)	5×5	7×7	40×40	
Voxel location	Voxel dimensions (mm³)			Dosimetric precision (%)
On-axis 5 & 15 cm depth	0.25×0.25×0.5	0.25×0.25×0.5	2×2×0.5	± 0.5
Off-axis	0.25×0.25×0.5	–	–	± 1.1
PDD up to 10 cm depth	0.25×0.25×1.0	–	–	± 0.4
PDD 10-30 cm depth	0.25×0.25×10.0	–	–	± 0.4

659

660

661

662

663

664

665

666

667

668

669

670

671

672 **TABLE II.** Monte Carlo $k_{Q_{clin,4\text{ cm}}}^{f_{clin,4\text{ cm}}}$ factors calculated on-axis in 6 and 15 MV beams for
 673 unmodified 60017- and 60023-type detectors, and for 60023-type detectors modified to
 674 include 0.6 mm and hypothetical 0.3 mm airgaps. ± 2 s.d. confidence intervals are shown.

675
 676

Detector model	Airgap thickness (mm)	6 MV $k_{Q_{0.5,4\text{ cm}}}^{0.5,4\text{ cm}}$	6 MV $k_{Q_{0.5,4\text{ cm}}}^{0.7,4\text{ cm}}$	15 MV $k_{Q_{0.5,4\text{ cm}}}^{0.5,4\text{ cm}}$	15 MV $k_{Q_{0.5,4\text{ cm}}}^{0.7,4\text{ cm}}$
5 cm depth in water					
60017	0	0.910 ± 0.005	0.971 ± 0.007	0.896 ± 0.005	0.959 ± 0.009
60023	0	0.979 ± 0.006	0.977 ± 0.006	0.978 ± 0.007	0.984 ± 0.007
60023	0.3	1.007 ± 0.006	0.995 ± 0.006	1.009 ± 0.007	1.003 ± 0.007
60023	0.6	1.029 ± 0.006	1.002 ± 0.006	1.041 ± 0.007	1.020 ± 0.007
15 cm depth in water					
60017	0	0.913 ± 0.005	0.967 ± 0.009	0.900 ± 0.005	0.958 ± 0.009
60023	0	0.987 ± 0.008	0.988 ± 0.007	0.985 ± 0.008	0.984 ± 0.008
60023	0.3	1.010 ± 0.008	1.007 ± 0.008	1.013 ± 0.008	1.002 ± 0.008
60023	0.6	1.038 ± 0.008	1.012 ± 0.008	1.043 ± 0.008	1.017 ± 0.008

677
 678
 679
 680
 681

682 **TABLE III.** Ratios of readings at 15 and 5 cm depths in water on-axis in a 6 MV 4×4 cm²
 683 field. ± 2 s.d. confidence intervals are shown. Ratios are shown for different detectors in
 684 the centre column, while the right-hand column shows how these ratios compare to that
 685 measured using the ionization chamber.

Detector	Ratio of readings at 15 and 5 cm depths	Detector ratio / ionization chamber ratio
IBA CC13 ionization chamber	0.540 ± 0.001	-
PTW 60017-type diode	0.534 ± 0.001	0.989 ± 0.002
PTW 60023-type diode (no airgap)	0.538 ± 0.001	0.997 ± 0.002
PTW 60023-type diode (0.6 mm airgap)	0.538 ± 0.001	0.997 ± 0.002

686

687