

1 **Title: Early phase trials of novel hearing therapeutics: avenues and opportunities**

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33 **Abstract**

34 Novel hearing therapeutics are rapidly progressing along the innovation pathway and into
35 the clinical trial domain. Because these trials are new to the hearing community, they come
36 with challenges in terms of trial design, regulation and delivery. In this paper, we address
37 the key scientific and operational issues and outline the opportunities for interdisciplinary
38 and international collaboration these trials offer. Vital to the future successful
39 implementation of these therapeutics is to evaluate their potential for adoption into
40 healthcare systems, including consideration of their health economic value. This requires
41 early engagement with all stakeholder groups along the hearing innovation pathway.

42

43 **Keywords:**

44 Hearing; aetiology; genetics; diagnosis; therapeutics; clinical trial

45

46 **1.0 Introduction**

47 Hearing loss represents the most common form of sensory dysfunction in humans and has
48 been recognised as an area of significant unmet clinical need (Looi et al., 2015; Müller and
49 Barr-Gillespie, 2015). 90% of hearing loss diagnoses relate to dysfunction of the inner ear
50 and central auditory pathways (Müller and Barr-Gillespie, 2015; Yamasoba et al., 2013). In
51 this type of hearing loss, scientific breakthroughs have enabled the identification of
52 potential therapeutic targets. Between 2011 and 2015 alone, 34 patents were granted for
53 new therapeutic and delivery approaches for inner ear disorders and a recent review
54 identified 43 companies working in the field (Nguyen et al., 2017; Schilder et al., 2019).
55 These novel approaches, which include a variety of drug, gene and cell therapies, are rapidly
56 progressing along the translational pathway to the stage of clinical testing for safety and
57 efficacy in humans (Schilder et al., 2018). Because these types of trials are new to the
58 hearing community, they come with challenges in terms of trial design, regulation and
59 delivery.

60

61 In this paper, we provide an overview of the key scientific issues, from understanding the
62 pathophysiology of hearing disorders, diagnosing and monitoring patients, to developing
63 and delivering therapeutics. We then discuss the challenges specific to clinical trials in this
64 field, outlining the opportunities for interdisciplinary collaboration¹, which extend to the

ABR: Auditory brainstem responses

AP: Action potential

ASSR: Auditory steady state response

COMET: Core Outcome Measures in Effectiveness Trials

CORE: Centre for Outcomes Research and Evaluation

COSMIN: Consensus-based Standards for the selection of health Measurement Instruments

CRO: Clinical research organisations

DOD: Department of Defence

BDNF: Brain derived neurotrophic factor

EEG: Electroencephalography

EPSRC: Engineering and physical sciences research council

HTA: health technology assessment

IHC: Inner hair cells

ISIET: International Society of Inner Ear Therapeutics

NIDCD: National Institute on Deafness and Other Communication Disorders

NIHR CRN: National Institute for Health Research Clinical Research Network

NGS: next generation sequencing

NT: neutrophin

NMDA: N-methyl-D-aspartate

65 adoption of novel hearing therapeutics into clinical practice. Based on a focused review of
66 the key scientific and grey literature and consultations with experts in this field, we present
67 the state of the science, identify gaps and propose solutions.

68

69 **2.0 Genotyping and Phenotyping hearing loss**

70 *2.1 Aetiologies of hearing loss*

71 Whilst most hearing disorders are sensorineural in nature, their underlying aetiologies are
72 diverse, meaning that there will be no future single cure for hearing loss (Nakagawa, 2014;
73 Okano, 2014; Yamasoba et al., 2013). **Pathological dysfunctions include those of the stria**
74 **vascularis (metabolic) or the basilar membrane (mechanical) with changes in the spiral**
75 **ligament, as well as loss of sensory hair cells (sensory) or spiral ganglion nerve cells (neural)**
76 **(Le et al., 2017; Yamasoba et al., 2013).** Genetic predisposition, environmental factors (noise
77 and ototoxic drug exposure), and combinations of the two determine the rate of
78 development and severity of sensorineural hearing loss (SNHL). Such combinations include
79 the increased risk of ototoxicity due to mitochondrial DNA mutations causing reduced
80 clearance and thus higher serum levels of aminoglycosides (Gao et al., 2017; Qian and Guan,
81 2009).

82

83 Over the past decade our understanding of the genes, molecules and mechano-electrical
84 processes that determine hearing and hearing loss has improved dramatically, enabling the
85 detection of potential therapeutic targets. This includes the discovery of core components
86 of the transduction process, such as transmembrane channel-like proteins (TMC1, TMC2,
87 whirlin) (Ahmed et al., 2017), tip link filaments acting as gates for transduction channels
88 (CDHR23, CDHR15, USH1 family) (Araya-Secchi et al., 2016; Emptoz et al., 2017; Libé-
89 Philippot et al., 2017; Sakaguchi et al., 2009) and myosin motor proteins that play vital roles
90 in hair cell function (MYO1A, MYO6) (Petit and Richardson, 2009). Our insight into the

OHC: outer hair cells

PIHL: Pharmaceutical Interventions for Hearing Loss

PTA: Pure tone audiometry

RSV: Respiratory syncytial virus

SNHL: Sensorineural Hearing Loss

SP: Summating potentials

TEN: Threshold-equalising-noise

91 structures essential for cochlear cellular function such as tight junction proteins (TRIC and
92 TJP2) (Kamitani et al., 2015; Kazmierczak et al., 2015; Mariano et al., 2011), associated
93 proteins (including *Usp53*), synaptic transmission proteins (such as SLC17A8) (Ryu et al.,
94 2016) as well as transmembrane channels (OTOF) (Hams et al., 2017) has also developed.

95

96 The signalling and transcription factors belonging to the *Notch* and *Wnt* pathways are key to
97 regulating inner ear development and cell differentiation; mutations in the genes encoding
98 these pathways are increasingly recognised as a cause of hearing loss, opening avenues for
99 treatment (Li et al., 2015; Wu et al., 2016). Hearing is highly dependent on mitochondrial
100 energy supply (Böttger and Schacht, 2013). Whole mitochondrial genome screens have
101 allowed for the detection of specific mutations which are associated with ototoxic and non-
102 syndromic hearing loss (Yano et al., 2014).

103

104 *2.2 From Genotype to Phenotype*

105 These genetic and molecular insights are not yet matched by similar advances in
106 phenotyping hearing loss (Bitner-Glindzicz, 2002; Myint et al., 2016). This is in part due to
107 the breadth of the field (with over 1,000 genes linked to polygenic forms of genetic hearing
108 loss), as well as current gaps in phenotypic profiling ability. Many profiling efforts have
109 focused on monogenic hearing loss. Audiometric profiles of Usher syndrome type III and
110 DFNA10 patients followed over time have helped clinicians estimate and inform families
111 about hearing loss progression rates (Plantinga et al., 2005; van Beelen et al., 2016). The
112 AudioGene project captures hearing profiles of hundreds of patients with autosomal
113 dominant, non-syndromic forms of hearing loss caused by known mutations. It uses
114 machine learning to predict candidate genes based on these audiometric profiles, which
115 allows for prioritisation of genetic screening in affected families (Hildebrand et al., 2009,
116 2008).

117

118 Next-generation sequencing (NGS) technology that allows for whole-genome sequencing at
119 lower cost and greater efficiency has advanced the identification of hearing loss genes
120 (Vona et al., 2015). Parallel sequencing of linked loci has replaced single gene sequencing,
121 which is particularly important in the diagnosis of non-syndromic hearing loss which is most
122 common in genetic sensorineural hearing loss. With NGS now widely available, research

123 focus has shifted into gene-disease associations via auditory phenotyping (Abou Tayoun et
124 al., 2016).

125

126 **3.0 Diagnosing hearing loss**

127 *3.1 Auditory tests*

128 Precision medicine for hearing loss, which links underlying pathophysiology to targeted
129 treatment, requires precision diagnosis, which is not yet offered by our current hearing tests
130 (Rudman et al., 2018; Schilder et al., 2018).

131

132 Pure tone audiometry (PTA), the universal baseline hearing test, is a compound measure of
133 hearing reflecting dysfunction of outer hair cells (OHCs); the test is much less sensitive to
134 inner hair cell (IHC) loss and peripheral neuropathy (Lobarinas et al., 2013; Plack et al.,
135 2016). Similarly otoacoustic emissions, particularly distortion produced otoacoustic
136 emissions, are used to assess the integrity of OHCs that are critical to the sensitivity and
137 frequency selectivity of the cochlea and speech discrimination (Rüttiger et al., 2017). The
138 Threshold-Equalising-Noise (TEN) test, used in hearing aid fitting as an instrument for
139 detecting cochlear dead regions, still needs to prove its usability in precision hearing
140 medicine (Moore et al., 2004). Auditory brainstem responses (ABR) are commonplace in
141 both clinical and research settings; using comparative electrophysiological measurement,
142 they indicate firing of the auditory nerve (wave 1) and activation of brainstem pathways
143 (Rüttiger et al., 2017). The threshold of ABRs induced upon defined sound stimuli can be
144 used as a functional biomarker for loss of OHCs in defined cochlear regions; however, when
145 OHCs are functioning, ABRs are unable to detect diffuse neuronal loss (Rüttiger et al., 2017).

146

147 Auditory steady-state response (ASSR) is an auditory evoked potential measured in a similar
148 manner to ABRs, but in response to rapid stimuli. It represents phase locked discharging of
149 the auditory nerve and cortex activation, but is again insensitive to auditory neuropathy.
150 Importantly, both ABR and ASSR allow objective estimation of thresholds for those unable
151 to take part in traditional behavioural testing. Speech in noise testing probably best reflects
152 the hearing difficulties that prompt patients to present with hearing loss, but does not help
153 identify underlying pathology (Guest et al., 2018). An illustration of the limitations of these
154 hearing tests is in the diagnosis of 'hidden hearing loss', a term for hearing impairment in

155 people with normal PTA thresholds, and thought to be caused by dysfunction of the IHCs,
156 auditory neurons and their synaptic connections (cochlear synaptopathy) (Bakay et al.,
157 2018; Schaette and McAlpine, 2011). Speech in noise perception testing may help with its
158 identification, and ABR wave 1 analysis provides some insight but is highly variable in
159 humans, making interpretation challenging (Plack et al., 2016).

160

161 More precise diagnostic tests that are being used experimentally prior to their validation in
162 larger cohorts include electrocochleography, giving insights into cochlear function, and
163 compound action potentials and the cochlear microphonic detecting IHC dysfunction. The
164 difference between waveform peaks generated by hair cells (summing potentials) and
165 cochlear neurons (action potentials), known as the SP/AP ratio, indicates selective neural
166 loss (particularly those with low spontaneous rates), and may help in the diagnosis of
167 'hidden hearing loss' (Liberman et al., 2016). Other tests being used experimentally include
168 pupillometry as a measure of listening effort, and electroencephalography to reflect
169 listening effort and central auditory processing (Marsella et al., 2017; Miles et al., 2017;
170 Milner et al., 2018).

171

172 *3.2 Imaging*

173 Although the quality and resolution of current imaging techniques of the inner ear, including
174 CT scanning and MRI, are improving in line with technological advances, these techniques
175 do not yet have the resolution to identify the ultrastructural phenomena required for
176 precision hearing medicine. This can be achieved with micro-optical coherence tomography,
177 which has been used to show differentiation of cell types within the fixed guinea pig
178 cochlea, but is limited at present by the high radiation doses required (Iyer et al., 2016).

179

180 Preclinical tests of iodine based compounds and gold or silver nanoparticles as contrast
181 agents have been shown to improve image quality (Zou et al., 2015). For example,
182 intratympanic administration of iohexol greatly enhanced image resolution in a temporal
183 bone study (Abt et al., 2016).

184

185 As imaging resolution reaches the cellular level, the challenge will become its interpretation.
186 Bioinformatic and machine learning approaches, similar to those used in ophthalmology,

187 will be crucial to integrating these complex multidimensional data into clinical practice
188 (Burgansky-Eliash et al., 2005; Wong and Bressler, 2016).

189 *3.3 Biomarkers*

190 Many researchers are working on identifying molecular biomarkers for hearing disorders,
191 both circulating and in the inner ear fluids, with most projects still at the preclinical stage (Y.
192 H. Li et al., 2018; Rüttiger et al., 2017; Schmitt et al., 2018, 2017). Prestin, an OHC-specific
193 protein, has been identified as an otologic peripheral circulating biomarker for OHC damage
194 after acoustic trauma, chronic industrial noise exposure and cisplatin induced hearing loss
195 (Hana and Bawi., 2018; Liba et al., 2017; Naples et al., 2018; Parham and Dyhrfeld-Johnsen,
196 2016). In preclinical models of acoustic trauma, the severity of hearing loss and OHC death
197 correlates with patterns of change in blood levels of prestin (Parham et al., 2019, 2014). If
198 these findings could be validated clinically and be generally applicable as a surrogate marker
199 of OHC survival, this biomarker could also be of great value in the monitoring for ototoxicity
200 during drug treatments and hair cell regeneration in trials of regenerative therapeutics.

201

202 Other candidate biomarkers include circulating RNAs, which would offer high specificity, but
203 require validation in humans before entering clinical use (Lee et al., 2018; Pang et al., 2016).
204 Using preserved human temporal bones to investigate correlates of gene expression and
205 audiometric profiles is a further avenue which could substantially advance inner ear
206 biomarkers research (Bai et al., 1997; Fischel-Ghodsian et al., 1997; Markaryan et al., 2010).

207

208 Metabolomics and proteomics (measurement of complete cellular metabolic processes and
209 protein expression) offer vast potential for biomarker discovery, but require access to inner
210 ear cells and perilymph (Shew et al., 2018; Wong et al., 2018). This is a challenge that is
211 already being overcome by the use of sampling during operations such as vestibular
212 schwannoma resections and cochlear implantation (Edvardsson Rasmussen et al., 2018;
213 Lysaght et al., 2011).

214

215 In cardiovascular disease for example, advances in data science have allowed linkage of
216 extensive biological data (genomics, metabolomics, proteomics) on large numbers of people
217 with equally extensive information on lifestyle, environmental factors and health records
218 (Dale et al., 2017; Hemingway et al., 2017; Joshi et al., 2017; López-López et al., 2017). The

219 hearing loss field has yet to take advantage of these novel approaches and will benefit from
220 fostering collaborations with the data science field.

221

222 *3.4 Outcome Measures*

223 Linked to improved diagnostic testing and biomarkers in reflecting the underlying
224 pathophysiology of SNHL, as outlined above, is the choice of outcome measures for novel
225 hearing therapeutics; what are the early signals of efficacy and how are functional changes
226 in hearing best measured?

227

228 An example of the challenges faced in hearing outcomes is in age related hearing loss,
229 where current hearing tests rely on patients' ability to comprehend instructions given by an
230 audiologist, which can be challenging for older people with cognitive impairment and poses
231 the question of whether the test is capturing deficiency in hearing or in cognition. Given the
232 link between adult onset hearing loss and dementia, accurate testing to enable treatment
233 selection and measurement of its outcomes is vital. Such tests should capture listening
234 challenges (effort) and the effect of listening on cognitive resources, including
235 electroencephalography (EEG) and pupillometry, and outcome measures should capture
236 changes in these tests alongside changes in threshold testing (Piquado et al., 2010; Shen et
237 al., 2016).

238

239 At the same time the field needs to consider how these measures relate to patients'
240 experiences of changes in hearing. Current hearing tests performed in sound proof booths
241 may not reflect or detect the subtle changes in hearing that patients may experience in
242 challenging listening environments. A range of self-reported questionnaires are in use to
243 quantify patients' hearing experiences and measure changes in hearing and tinnitus over
244 time (Granberg et al., 2014; Hall et al., 2016).

245

246 There is also a need to achieve consensus and guidance on which outcome measures and
247 accompanying instruments to use in trials in this emerging field. Such consensus would form
248 the basis for a 'white paper' for industry, research institutions and regulatory agencies
249 regarding the minimum package of clinical assessments to deliver proof of concept studies
250 of novel hearing therapeutics. Initiatives like COMET (Core Outcome Measures in

251 Effectiveness Trials), COSMIN (Consensus-based Standards for the selection of health
252 Measurement Instruments) and CORE (Centre for Outcomes Research and Evaluation)
253 recommend approaches to developing agreed standardised sets of outcomes across (late
254 phase) clinical trials (COMET, 2019; CORE, 2019; COSMIN, 2019). Hall et al (2018) have
255 applied COMET's methodology to develop a core outcome set for tinnitus (Hall et al., 2018).

256

257 **4.0 Developing Novel Therapeutics**

258 *4.1.0 Tailored therapeutic approaches*

259 More than 75 therapeutic programs covering a range of therapeutic targets, approaches
260 and modalities and lead indications in hearing and balance are currently progressing along
261 the translational pathway (Crowson et al., 2017; Schilder et al., 2018). Clinical trials of
262 otoprotective, restorative and regenerative therapeutics are underway with several having
263 completed Phase III (Schilder et al., 2019). Some approaches have yet to fulfil their promise,
264 such as NMDA receptor antagonists and Kv3 ion channel modulators for the treatment of
265 tinnitus, while others have succeeded, such as sodium thiosulfate as an otoprotectant
266 against cisplatin induced hearing loss in children with hepatoblastoma (Auris Medical AG,
267 2015; Autifony, 2014; Brock et al., 2018, 2016). With age related hearing loss as the most
268 common cause of SNHL and given its association with dementia, treatments which could
269 regenerate hair cells, restore synapses and protect cochlear neurons would have the biggest
270 impact on health beyond hearing capabilities (Livingston et al., 2017).

271

272 The below highlights several of the therapeutic approaches that have recently translated to
273 trials.

274

275 *4.1.1 Notch Pathway*

276 Given their key roles in cell fate determination, Notch and Wnt pathways are prime targets
277 for hair cell regeneration (Atkinson et al., 2015; Mizutari et al., 2013). Trials of gene and
278 drug therapies aimed at regenerating hair cells have already begun, with modulation of the
279 Notch pathway as the focus of two ongoing clinical trials. One uses a small molecule drug
280 approach with transtympanic injections of a gamma secretase inhibitor to target Notch
281 signalling; the other utilises a gene therapy approach surgically delivering Atonal (Hath1), a
282 key determinant of cell fate in human inner ear hair cells, by a viral vector directly into the

283 inner ear (Novartis Pharmaceuticals, 2014; REGAIN, 2017). Trials of small molecule drugs
284 manipulating Wnt pathways are also progressing (Frequency Therapeutics, 2018). Screens
285 for potentially more efficacious modulators of this pathway are being developed (Zeng et
286 al., 2018).

287

288 *4.1.2 Neurotrophins*

289 Cochlear synaptopathy as a target for therapeutics is being explored by various academic
290 and biotech groups, but difficulties with diagnosis pose a translational challenge in this area
291 (Hickox et al., 2017). There is increasing insight into the fate and function of cochlear
292 neurons with age and with progressing hearing loss; neuroprotection and
293 neuroregeneration therefore provide alternative therapeutic approaches. Neurotrophins
294 (NTs), such as brain derived neurotrophic factor (BDNF), have been shown to stimulate
295 neurite outgrowth of auditory nerve cells (Plontke et al., 2017; van Loon et al., 2013). A
296 phase I trial of a gene construct which stimulates the overexpression of BDNF using
297 electrophoresis in patients undergoing cochlear implantation is underway (Pinyon et al.,
298 2018, 2014). Viral delivery systems of BDNF and other NTs are being tested preclinically
299 (Budenz et al., 2015). The use of cochlear implants as a delivery device is very attractive; but
300 is limited to those eligible for implantation and its effectiveness relies on retaining neuronal
301 function.

302

303 *4.1.3 Stem cells*

304 Stem cells provide an attractive source of differentiable material and have multiple potential
305 applications (Lenarz, 2017; Lustig and Akil, 2012; Mittal et al., 2017). Their use as an inner
306 ear therapeutic has been stymied by limited understanding of specific signalling pathways
307 necessary to determine cell fate, as well as challenges in verifying viable function within the
308 resulting hair cell like structures (Takeda et al., 2018). Preclinical models have highlighted
309 the potential of mesenchymal stem cell therapeutics in parallel with cochlear implant
310 surgery via bio-hybrid electrodes (Roemer et al., 2016); nerve growth factors produced by
311 these stem cells can enhance implant success. Feasibility and safety of this approach has
312 recently been tested in a human trial (Roemer et al., 2016). Further work has highlighted the
313 opportunity to modulate inner ear cell behaviour following local delivery of mesenchymal
314 stromal cells (Schulze et al., 2018).

315

316 *4.1.4 Gene therapies*

317 Monogenic forms of hearing loss are potentially the most promising conditions for gene
318 therapies (Lustig and Akil, 2012; Yoshimura et al., 2018). Restoration of hearing for Tmc1
319 mutant mice has been achieved recently via local delivery of synthetic adeno-associated
320 viral vectors encoding Tmc1 (Nist-Lund et al., 2019). In murine models of Usher syndrome,
321 local adeno-associated viral delivery of wild-type whirlin cDNA resulted in improved hearing
322 and vestibular function (Isgrig et al., 2017). This offers promise for translation to human
323 trials, particularly given on-going trials of gene therapy via retinal injection in patients with
324 Usher syndrome type 1b related retinitis pigmentosa (Sanofi, 2012; UshTher, 2018).
325 Otoferlin mutations are an important cause of inherited auditory neuropathy and are being
326 explored for gene therapy in pre-clinical models; they are monogenic and leave the inner
327 ear structure relatively intact making them a promising target for interventions (Michalski et
328 al., 2017; Rodríguez-Ballesteros et al., 2008).

329

330 *4.1.5 Challenges in developing novel therapeutics*

331 Currently, potential therapeutics are tested in explant cultures and/or *in vivo* in small
332 mammals. This poses not only logistical and ethical constraints, but importantly it is
333 unknown how well positive results will translate to humans; some compounds proven
334 efficacious in animal models have failed to fulfil their promise in human trials (Le Prell et al.,
335 2016). Whilst difficulties in translating animal work are common across clinical research,
336 they are particularly significant for the emerging hearing therapeutic field (Denayer et al.,
337 2014; Frisina et al., 2018; Mak et al., 2014). These problems are compounded by difficulties
338 in identifying endpoints for drug testing (Bognar et al., 2017; Posey Norris et al., 2014;
339 Vasaikar et al., 2016).

340

341 While vertebrates offer the opportunity to study the in-depth effects of drugs on both
342 cochlea structure and function, they are not suited to drug screening (Ou et al., 2010).
343 *Drosophila melanogaster*, a screening tool for many therapeutic classes has been
344 highlighted as a potential screening tool for hearing therapeutics and offers great potential
345 (Christie and Eberl, 2014; T. Li et al., 2018; Wang et al., 2016; Yadav et al., 2016). The
346 zebrafish has been identified as a valuable model for studying hair cell development and

347 function, and appears to be a useful screening tool for the identification of ototoxic drugs
348 (Chiu et al., 2008). Cell culture would offer the opportunity to screen a wide variety of novel
349 and existing compounds at a much lower time and economic cost, but inherent difficulties in
350 culturing the cells of the organ of Corti make developing an appropriate model enormously
351 challenging (Rivolta and Holley, 2002). Efforts to create such lines from stem cells have
352 shown promise in generating spiral ganglion neurones that can be used for drug screening
353 (Whitlon, 2017). This success has not yet been replicated with cochlea cells, although
354 significant advances have been made, with several groups progressing towards having
355 cultured hair cells or organoids (Jeong et al., 2018; Longworth-Mills et al., 2016; McLean et
356 al., 2017).

357

358 Developing human cell models is limited by access to human inner ear tissue. Recently,
359 vestibular tissue harvested during trans-labyrinthine acoustic neuroma surgery has been
360 regenerated with some success and is a good option for testing regenerative therapeutics
361 (Taylor et al., 2018, 2015).

362

363 *4.2 Delivery of therapeutics to the inner ear*

364 A key challenge in hearing loss trials is choice of delivery method. The decision will depend
365 on the pharmacokinetic profile of the individual agent, and the balance of risks associated
366 with delivery against the potential benefit of the treatment. Whilst some therapeutics
367 currently undergoing clinical trials can be delivered orally (EU Clinical Trials Register, 2018),
368 this mechanism of delivery is not always possible.

369

370 For small molecule delivery, systemic routes, or delivery via the middle ear have been in use
371 clinically for some time. The efficacy of systemic administration however depends on both
372 the pharmacokinetic properties of the molecule, and the underlying pathology. Molecules in
373 current clinical use, such as corticosteroids, require high blood concentrations to overcome
374 the tight junctions of the blood-perilymph barrier, increasing the chance of side effects
375 (Jahnke, 1980; Salt and Plontke, 2009). Middle ear approaches include transtympanic
376 injections of liquid or gel-form drugs, controlled release devices and surgical application of
377 drugs to the round window niche (Borenstein, 2009; Gurman et al., 2015; Hütten et al.,
378 2014; Liu et al., 2014; Plontke et al., 2014, 2006; Tandon et al., 2015). All rely on simple

379 diffusion through epithelial barriers, which is subject to inter-drug and inter-person
380 variation, and leads to formation of concentration gradients, with variable concentrations
381 reaching more apical regions of cochlea (W. Li et al., 2018; Liu et al., 2014; Salt et al., 2007;
382 Salt and Plontke, 2018). Work is on-going in animal models to develop ways to overcome
383 these problems, including magnetically targeted drug delivery and nanoparticles (Pyykkö et
384 al., 2016, 2011; Shapiro et al., 2014).

385

386 Intracochlear drug delivery offers the best control of delivery, but comes with the highest
387 risk to hearing, although the problem of base-apex gradient formation remains. Cochlear
388 implant associated drug delivery presents a unique opportunity to develop this route for a
389 subset of patients (Plontke et al., 2017). Options include coating implants with drugs or
390 cells, incorporating catheters into the implant to allow controlled release or injecting drugs
391 intracochlear at the time of surgery (Bas et al., 2016; Jolly et al., 2010; Roemer et al., 2016;
392 Ye et al., 2007).

393

394 For gene and cell therapy, intracochlear routes are necessary, and round window,
395 cochleostomy and canalostomy approaches have been developed in animals (Gehrke et al.,
396 2016; György et al., 2017; Plontke et al., 2016; Suzuki et al., 2017; Yoshimura et al., 2018).
397 The on-going phase I trial of intra-labyrinthine infusion of an adenoviral vector carrying
398 Atonal is the first to use intracochlear delivery in humans (Novartis Pharmaceuticals, 2014;
399 Peppi et al., 2018).

400

401 Translation of local delivery methods from animal models to human trials is challenging
402 primarily due to differences in the size of the cochlea altering diffusion and excretion of
403 agents. Computer modelling, currently used primarily to validate experimental data, may
404 offer the only opportunity to gain insight into the intracochlear behaviour of therapeutics in
405 humans and has potential to become a valuable translational tool (Plontke et al., 2007; Salt
406 and Hirose, 2018).

407

408 **5.0 Translating to clinical practice**

409 *5.1 Clinical trials capacity and capability*

410 With novel hearing therapeutics progressing along the innovation pathway, it is vital that
411 capacity and capability for delivering clinical trials is increased, by improving access to
412 patient populations and their hearing data through patient registries as well as by building
413 professional and clinical trials networks specialised in hearing research.

414

415 Development of successful patient registries and data repositories requires mapping-out
416 patient populations and establishing collaborations with other medical specialties and
417 professional organisations (Mandavia et al., 2017). This is particularly important considering
418 that many people with or at risk of hearing loss, and therefore potentially eligible for
419 hearing trials, are not 'on the radar of' existing hearing services. This includes people visiting
420 memory and dementia clinics; patients treated with ototoxic medication, military staff and
421 musicians exposed to occupational noise and individuals exposed to recreational noise
422 (Lanvers-Kaminsky and Ciarimboli, 2017; Le Prell and Brungart, 2016; Le Prell and Clavier,
423 2017; Livingston et al., 2017).

424

425 To screen and monitor these large populations for hearing loss systematically, there is a
426 need for alternatives to conventional sound-booth technologies with expensive audiometric
427 equipment and highly trained personnel. This has been recognised by a range of companies
428 developing and marketing novel strategies to bring hearing testing out of the booth and,
429 often directly into the hands of the patients (Barczik and Serpanos, 2018; Yousuf Hussein et
430 al., 2018). Early assessment of these technologies suggests that they may represent
431 accurate, cost-effective and efficient tools for screening and follow-up. The use of high-
432 quality sound attenuated insert earphones or circumaural earcups to compensate for the
433 less than ideal sound environment is critical. (Barczik and Serpanos, 2018; Mahomed-Asmail
434 et al., 2016). (Campbell et al., 2016; Rourke et al., 2016). Whilst these technologies are
435 rapidly progressing, they do not yet allow for precision diagnosis, limiting their current
436 applications in clinical and research settings.

437

438 Clinicians, scientists and industry have highlighted the importance of creating international
439 registries and data repositories of systematically collected clinical hearing data, combined
440 with biorepositories of blood samples and tissue specimens for future genomic, proteomic,
441 and metabolomic analysis. Provided patient consent-to-contact is in place, these registries

442 allow for efficient patient identification and recruitment to so called registry-based clinical
443 trials and provide an infrastructure for the collection of treatment and trial outcomes (Li et
444 al., 2016). Ethical, governance and quality standards would need to be established among
445 participating centres. These registries represent a long term investment for both patient and
446 professional stakeholders; expectations regarding short term patient benefit need to be
447 carefully managed.

448

449 *5.2 Clinical trials and research networks for delivery of hearing trials*

450 There is a need for clinical trials networks in the hearing field that will provide academic
451 teams, biotech, pharma and Clinical Research Organisations (CROs) access to expert trial
452 teams to deliver their hearing trials nationally and internationally. These expert teams with
453 a track record of successful trial delivery, will play a vital role in the delivery to time and
454 target of the rapidly increasing number of hearing trials and should share their expertise
455 with the wider community, whilst offering guidance to newer teams. Collaboration with
456 stakeholders including patients and advocacy groups will be essential for maximising trial
457 recruitment.

458

459 Examples of successful international trial networks are SIOPEL, the International Childhood
460 Liver Tumors Strategy Group, through which the trial of sodium thiosulfate in children
461 receiving cisplatin for hepatoblastoma was successfully delivered across 52 centres in 12
462 countries. A similar global network, called ReSViNET, has been established to facilitate trials
463 of new vaccines for Respiratory Syncytial Virus (RSV) infection as well as developing
464 validated outcome measures in this field (Justicia-Grande et al., 2016; Mazur et al., 2018).

465

466 In the UK, The National Institute for Health Research Clinical Research Network (NIHR CRN)
467 provides infrastructure and resources to support the rapid set-up and patient recruitment
468 into clinical studies by streamlined approval processes, funding local research support staff
469 and facilities, and linking NHS clinical research expertise across hospital sites. The NIHR CRN
470 has placed a focus on the life sciences industry to help patients gain earlier access to
471 breakthrough treatments: in the year 2016/17, the CRN brought 729 new commercial
472 clinical trials to the UK and recruited more than 34,000 participants to life sciences industry
473 research. A 2016 KPMG report on the impact and value of the NIHR CRN estimated that CRN

474 supported clinical research activity generated £2.4 billion of gross value added and almost
475 UK 40,000 jobs. Additional impacts included improved transparency in pricing and more
476 rapid uptake of treatments (KPMG, 2016). To build capacity for the growing NIHR CRN
477 portfolio of hearing, tinnitus and balance studies, Audiology Champions and Trainee
478 Speciality Leads have been appointed across the country; they signpost audiologists and ENT
479 trainees to opportunities to develop as hearing researchers.

480

481 UK ENT trainees have recently united in INTEGRATE, a National ENT Trainee Research
482 Collaborative conducting multicentre research within clinical training and NHS services
483 (Smith et al., 2018). Our author group is working with INTEGRATE on a trainee led national
484 prospective cohort study of adult patients presenting to the NHS with sudden onset SNHL.
485 With trainees being the frontline staff managing these patients, this study will engage them
486 in a better understanding of the condition and the patient pathways; as such paving the way
487 for the successful delivery of upcoming trials of novel therapeutics for sudden onset SNHL.

488

489 *5.3 Funding opportunities*

490 Funding opportunities for hearing research have never been better. Support from: EU
491 Research and Innovation Programmes, national public funders such as the National Institute
492 on Deafness and Other Communication Disorders (NIDCD), the US Department of Defence
493 (DoD) Hearing Center of Excellence, the NIHR, The UK Engineering and Physical Sciences
494 Research Council (EPSRC), and charities like the Wellcome, Hearing Health Foundation,
495 Action on Hearing Loss and Fondation Pour l'Audition have enabled major advances in the
496 understanding of hearing loss and the development of innovative treatments.

497

498 At the same time biotech start-ups have benefitted from a sharp increase in funding; from
499 2007-12 to 2013-17, private funding rose from \$86.4 million to \$299.3 million, and public
500 funding from \$57 million to \$469.7 million (Li, 2017). Recently large capital raised from
501 private investors, pharmaceuticals and biotechnology companies as well as venture
502 capitalists have recognised the growing investment opportunities in this field and are
503 funding a pipeline of research into novel hearing therapeutics. The Cochlear Centre for
504 Hearing and Public Health at the John Hopkins University is an excellent example of joint
505 funding, including public, private and philanthropic support (Johns Hopkins Bloomberg

506 School of Public Health, 2018). Moving forward, to continue this funding trend, positive trial
507 results will be needed to justify such investments in the longer term.

508

509 *5.4 Adoption into clinical practice*

510 If proven effective, novel hearing therapeutics are set to have a major impact on hearing
511 services. It is therefore essential that the field starts thinking now about implementation
512 and how these treatments can be of most value to patients. Lessons should be learned from
513 other health fields, particularly Ophthalmology where anti-VEGF injections befell clinical
514 services, and insufficient preparation by funders and providers led to inequalities in patient
515 access, economic inefficiency and sub-optimal outcomes (Hollingworth et al., 2017; Shalaby
516 et al., 2016). Crucial to implementation of these novel therapeutics, is to assess and
517 evaluate their potential for adoption into healthcare systems (The Academy of Medical
518 Sciences, 2018). This is determined by multiple interacting factors, each with their own
519 intentions, including: “market makers” (discovery scientists, industry, investors) driving the
520 uptake of novel therapeutics; “bodies of strategic constraint” (regulators, funders, guideline
521 and policy makers) trying to impose order and cost-control; and “users” (patients and
522 clinicians) extracting opportunities for treatment and ‘coping’ with potential service
523 redistribution from secondary to primary care (May and Finch, 2009). Predicted cost-
524 effectiveness represents another key factor within this arena, *influencing and influenced by*
525 the decisions and perspectives of these agents (Ijzerman et al., 2017; Ijzerman and Steuten,
526 2011). Figure 1 introduces the core research components that must come together for the
527 successful implementation of hearing innovations.

528

529 Figure 1

530

531 Our author team has constructed an early health economic model comparing novel
532 regenerative hearing therapeutics with the current standard of care for people with age
533 related hearing loss. Input data were derived from systematic literature searches and
534 stakeholder expert opinion. We adopted a healthcare perspective of the UK National Health
535 Service (NHS) and applied: headroom analysis to explore the maximum potential value;
536 threshold analysis to search for the minimum effectiveness needed for the innovation to be
537 cost-effective; and sensitivity and scenario analyses to evaluate relevant uncertainty. Figure

538 2 illustrates the key steps in our economic model development. Though this work focuses
539 on regenerative hearing therapies for age related hearing loss, this model has the potential
540 to serve as a framework for other hearing therapeutics and patient populations.

541

542 Figure 2

543

544 *5.5 Moving forward, 'collaboration is the new competition'*

545 Interdisciplinary discussion and cooperation involving stakeholders from each section of the
546 innovation pathway are necessary in order to enable the latest developments in inner ear
547 therapies to progress along the clinical pathway. The recently established International
548 Society of Inner Ear Therapies (ISIET) will provide a forum for potential collaborators to
549 share information and experiences as well as set standards.

550

551 Coordinated activities with The Pharmaceutical Interventions for Hearing Loss (PIHL) group
552 also enables hearing stakeholders to discuss the latest advances in discovery science and
553 clinical trials, as well as develop evidence-based standards for clinical research. The PIHL
554 group, which is organised by the DOD's Hearing Centre of Excellence, is dedicated to
555 disseminating the results of these discussions to the wider community.

556

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