

**Case Studies in Neuroscience:
Evidence of motor thalamus reorganization following
bilateral forearm amputations**

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Running Head:

Motor thalamus reorganization following forearm amputations

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41 **Abstract**

42 Following injury, functional improvement can result from central nervous system
43 plasticity. Use-dependent plasticity of motor systems is evident, for example, in recovery of
44 function resulting from rehabilitative interventions. Here, we present a single patient who
45 underwent bilateral microelectrode-guided stereotactic implantation of deep brain stimulating
46 leads for the treatment of essential tremor 52 years following bilateral arm amputations. The
47 tremor affected his upper extremities, and had rendered him unable to perform fine motor tasks
48 with his prostheses, significantly reducing his independence. We found a large territory of
49 neurons in the ventral intermediate nucleus of his thalamus that responded to shoulder
50 protraction, the movement that he used to control fine motor movements of his terminal hook
51 prostheses. We propose that reorganization of this motor nucleus may have occurred
52 secondary to a use-dependent gain of function in neurons that were previously involved in hand
53 movement.

54

55 Keywords: Neuroplasticity, Tremor, Movement Disorder, Deep brain stimulation

56

57 **Introduction**

58 Neural circuits for movement are remarkably adaptable. Evidence for this can be seen in
59 people who have suffered acquired brain injuries, who with therapy and training recover
60 significant motor function (Dimyan and Cohen 2011). However, the corresponding sites of motor
61 circuit adaptive changes are not clear, and could include the cerebrum, diencephalon,
62 cerebellum, brain stem, and/or spinal cord.

63 Following limb amputation, there is evidence of neuroplastic changes in sensory nuclei
64 of the thalamus. Previous observations in the context of post-amputation phantom pain in
65 humans (eg. (Davis et al. 1998)), as well as from experimental animal studies (eg. (Rasmusson
66 1996)), have demonstrated that there is expansion of receptive fields (brain regions that
67 respond to somatic sensory stimulation) in the sensory thalamus arising from the amputation
68 stump. Projected fields (somatic regions where sensation is felt during brain stimulation)
69 involving the amputated limb may also be expanded and overlap with receptive fields of the
70 stump. But whether there are also changes in diencephalic motor regions is not known. The
71 absence of evidence for such reorganisation likely reflects the absence of recordings from motor
72 regions of the human thalamus in patients with amputation, as they seldom would have reason
73 to have these invasive recordings.

74 Here, we describe a case of a patient with remote bilateral arm amputations, who
75 subsequently developed essential tremor. He elected to proceed with a DBS procedure, which
76 was done with microelectrode guidance. We show that there is a large region of his thalamic
77 ventral intermediate (Vim) nucleus that comprises neurons that are active during shoulder
78 protraction, the movement he uses to open his prosthetic “hands.” We suggest that this reflects
79 reorganization of this motor region of his thalamus.

80

81 **Case Report**

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82 A 73-year-old, otherwise healthy male patient required bilateral forearm amputations in 1963
83 (age 19), after being electrocuted while working on a power line. His amputations were below
84 the elbow, and he was fit with transradial prostheses with hook terminal devices. The hooks
85 each included a pincer component held closed by an elastic band, and opened and manipulated
86 via protraction of the ipsilateral shoulder. Prior to 2004, the patient was functionally
87 independent, and could “pick up an ash from an ashtray” with his prostheses. Decades after his
88 initial injury, he was refit with more advanced prostheses, but soon insisted on switching back to
89 his hooks, so comfortable had he become with them.

90

91 In 2002, the patient developed a tremor in his lip. Within two years, he developed bilateral action
92 and postural tremor primarily affecting his upper extremities. This progressed such that he could
93 no longer use his prostheses to perform routine daily tasks. On the basis of his symptoms and
94 family history, he was diagnosed with familial essential tremor. Interestingly, the patient had
95 experienced phantom sensations for decades, but he had no somatosensory perception of his
96 new onset tremor, and indeed did not appreciate his tremor with his eyes closed.

97

98 In 2015, the patient opted for bilateral deep brain stimulation (DBS) of the thalamic Vim nuclei.
99 Six weeks following initial implantation, allowing time for any microthalamotomy effects to
100 resolve, the patient underwent programming of his stimulator. This resulted in significant
101 improvement in fine motor control, writing, utensil use, and drinking using his hook prostheses
102 (Video 1). More than two years later, the patient continues to enjoy significant improvement in
103 his quality of life and functional independence.

104

105 **Methods**

106 Implantation of DBS leads was performed (by RMB) on May 4 (left side) & 26 (right
107 side), 2015, at the Halifax Infirmary (QEII Health Sciences Centre, Halifax, Canada). As part of

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108 our usual procedure, the patient's head was fixed in a stereotactic frame for an MRI-guided
109 stereotactic insertion of DBS leads (Medtronic 3387). An implantable pulse generator (Activa
110 PC, Medtronic) was inserted following insertion of the second lead.

111 Our routine for DBS procedure involves the use of microelectrode recording to localise
112 the targets for implantation. The Vim target was based on the AC-PC line and width of the third
113 ventricle (Papavassiliou et al. 2008)). Using a 40 μ m exposed tip microelectrode (FHC, Bowdoin,
114 ME), neurons were recorded, filtered (100Hz-5kHz), and digitized (20 kHz) using a GS3000
115 system (Molecular Devices, Sunnyvale, CA). Neuronal responses to a variety of voluntary
116 movements were recorded while advancing the microelectrode through the Vim nucleus of the
117 thalamus in a step-wise manner using an Alpha Omega microdrive (Nazareth, Israel),
118 approximately 11mm lateral to the wall of the third ventricle.

119 The extracellular microelectrode recordings were imported into Spike 2 (CED,
120 Cambridge, UK) for off-line analysis. Spikes were sorted using the software wave event
121 template function to discriminate spikes based on a principal component analysis of spike
122 properties including amplitude, shape, and duration (see Figure 2). For each recording, one to
123 three unique spike templates were detected, allowing <2% variability in parameters. At each
124 site, 6s periods were analysed (3s prior to and 3s following movement onset). For each
125 individual neuron, we measured the instantaneous firing frequency and quantified the number of
126 spikes in the pre-movement and movement conditions, and compared results using a paired
127 Student's t-test.

128

129 **Results**

130 While it is usual to find that most responsive neurons in the Vim would increase their
131 activity in response to digit, hand, and wrist movement, this was clearly not possible to test here
132 given the patient's amputations. Surprisingly, we also did not find neurons that were active
133 during volitional contralateral elbow movement. On the other hand, shoulder protraction, the

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134 movement used to open the hook terminal devices of his prostheses, was associated with an
135 increase in neuronal firing. Shoulder movements were not tested until late during the recording
136 protocol on the left (first) side, likely because in our practice, it is unusual to find any shoulder
137 movement-responsive neurons in Vim; we were initially focusing on elbow movements.
138 However, a more systematic investigation was subsequently conducted on the right side, where
139 we recorded shoulder movement-responsive neurons along a linear trajectory of over 5 mm
140 (Figure 1). To quantify these changes, we were able to definitively identify nine neurons across
141 this trajectory on the right side. Figure 1B illustrates 2 recordings at different locations, with the
142 recording in Figure 1Ba resolved into three neurons in Figure 2. Each of the 9 identified
143 neurons substantially increased their firing following movement initiation (Figure 3; $p=0.0001$).
144 Thus, there was a surprisingly large length of the Vim comprising neurons associated with fine
145 opening movements and manipulation of the prosthesis.

146 As we had not targeted the nucleus ventrocaudalis (Vc; equivalent to ventroposterior
147 lateral and medial nuclei in non-human primates; see Figure 1A), we did not ask whether
148 neurons in this region responded to tactile stimulation (receptive fields). However, as is our
149 routine in practice, we did study projected fields by microstimulation (300Hz, 0.3 – 0.5ms, 5 –
150 25 μ A stimuli) and found paresthesias involving the mouth region when stimulating the right
151 thalamus, and top of the head when stimulating the left thalamus.

152

153 **Discussion**

154 We have had a rare opportunity to observe and report activity in a motor nucleus of the
155 thalamus (Vim) in the context of amputation and long-term motor adaptation following remote
156 bilateral upper extremity amputations. The territory of this patient's Vim that was activated
157 during shoulder protraction – the movement used to control fine opening movements of his
158 prosthetic 'hands' – was expanded in size compared to what we normally find in people with

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159 intact limbs, suggesting that in this patient, there has been some use-dependent reorganization
160 following amputation.

161

162 Vim is involved in motor coordination and is organised in a mediolateral somatotopic pattern
163 (Lenz et al. 1990). It is roughly equivalent to the ventroposterolateral, pars oralis nucleus
164 (VPLo) in non-human primates. This nucleus receives afferent kinesthetic input from
165 contralateral body parts, and responds to active and passive muscle stretch (Ohye et al. 1989).
166 Neurons in Vim receive direct excitatory input from deep cerebellar nuclei and cerebral cortex,
167 as well as inhibitory input from the thalamic reticular nucleus. Output from Vim is primarily to
168 cortical motor areas (Perlmutter and Mink 2006). Movement-related neurons in Vim increase
169 their firing rate at movement onset of their corresponding body parts, and are typically recorded
170 during microelectrode guided stereotactic Vim DBS surgery for tremor (Garonzik et al. 2002).

171

172 Plasticity of both Vim and the sensory ventrocaudalis (Vc; equivalent to ventroposterior lateral
173 and medial nuclei in non-human primates) nucleus has been demonstrated in patients with
174 tremor. In these patients, there is an expansion of the kinaesthetic representation of wrist and
175 elbow movements, possibly resulting from chronic increases in afferent input (Kiss et al. 2003).

176

177 Little is known about reorganization of nuclei of the motor thalamus following limb amputation
178 and adaptive recovery. Amputation-related plasticity has, however, been well documented in
179 human somatosensory cortex, sensory thalamus, and motor cortex. Early animal studies
180 demonstrated that peripheral median nerve transections in owl and squirrel monkeys leads to
181 expansion of neighbouring ulnar and radial innervated skin representation into deafferented
182 regions of somatosensory cortex (Kaas et al. 1983). Similar findings have been reported in
183 humans (eg. Chen et al. 2002). In patients with limb amputations undergoing DBS surgery for
184 pain, evidence for reorganization of sensory representations within Vc has been documented

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185 via single linear microelectrode trajectories (Schmid et al. 2016). Stump tactile receptive fields
186 within Vc are significantly enlarged after amputation, likely reflecting an expansion of stump
187 representation into deafferented regions of the sensory thalamus (Davis et al. 1998).

188

189 Motor regions are also plastic. Following focal, sub-total lesions of the dorsal forelimb (DFL)
190 area of rat primary motor cortex, the remaining DFL area can be either reduced or enlarged
191 after recovery depending on whether the animals receive rehabilitative training (Nudo 2013).

192 Limb amputation has been associated with reorganization of proximal muscle representations of
193 the primary motor cortex in humans (Cohen et al. 1991). It is plausible that there would be
194 corresponding plastic changes in the motor nuclei of the thalamus as well. Here we demonstrate
195 that in Vim, many shoulder movement-responsive cells can be seen over a length of at least
196 5mm, in contrast with recordings in our usual practice, in which shoulder-movement responsive
197 neurons are rarely recorded in this nucleus. We therefore conclude that the patient has had
198 reorganization of his Vim nucleus.

199

200 The mechanisms underlying plasticity in Vim are not clear, and are likely multifactorial. In
201 sensory thalamus, limb amputation leads to an increased number of bursting neurons in Vc
202 (Lenz et al. 1998). While the mechanism of these changes is not clear, it was suggested that
203 this pattern of spiking results from an activity-dependent increase in dendritic calcium spiking
204 (Lenz et al. 1998). While decreased kinesthetic input from the distal arms following amputation
205 could lead to similar changes in Vim, the fact that the activity was related to the movements that
206 the patient developed to finely control his prostheses suggests that there is also a degree of
207 use-dependent specificity to these changes.

208

209 It is possible that these types of changes following amputation lead to plasticity within Vim, with
210 two driving influences: i) decreased afferent input to thalamic regions previously associated with

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211 forearm, wrist, and hand movements, and ii) increased excitatory input from cerebellar and
212 cortical areas associated with shoulder movements, secondary to the learning effects of using
213 these movements for fine motor control. The combination of these mechanisms may have led to
214 shoulder representation in regions formerly dedicated to distal arm fine motor control.

215

216 These observations took place in the context of routine electrode placement for DBS. As such,
217 the patient did not have concurrent EMG recordings to correlate with Vim neuronal firing
218 frequencies, nor were multiple repeated trials completed at any given electrode position.

219 However, we have not previously encountered this extent of robust shoulder movement-
220 responsive neurons. It is likely that a strong indication for invasive recording in motor thalamic
221 nuclei of patients with remote amputations or other deafferenting injuries will remain a relatively
222 rare opportunity. We are therefore presenting these findings to perhaps offer insights into the
223 spectrum of neuroplastic changes that accompany amputation and adaptation.

224

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280

281 **FIGURE LEGENDS**

282 **Video 1:** Patient performing various motor tasks using his transradial prostheses, first with the
283 bilateral stimulators 'off', and then with the stimulators 'on'. The patient has provided signed
284 informed consent to be video-taped for publication.

285

286 **Figure 1:** Microelectrode recording in the right thalamus during stimulator lead placement.
287 Shoulder protraction led to an increase in Vim neuronal firing rates at each recording site over a
288 trajectory length of over 5mm.

289 **A:** Track of the recording microelectrode through the right thalamus. This atlas image was
290 stretched to match the patient's intercommissural distance, and the microelectrode track plotted
291 (yellow line) based on initial target and angle of approach, and corroborated by position of DBS
292 lead by overlaying with the post-operative MRI. The horizontal dashed line represents the AC-
293 PC line. The red shaded area represents the linear extent of the microelectrode track over
294 which neurons active during shoulder protraction were recorded. 'a' and 'b' denote recording
295 sites depicted in panel B. V.c.i: ventral caudal internal nucleus, V.c.pc: ventral caudal
296 parvocellular nucleus, V.im: ventral intermediate nucleus, V.o.p: ventral oral posterior nucleus,
297 V.o.a: ventral oral anterior nucleus, Rt: reticular nucleus. Adapted from Schaltenbrand &
298 Wahren (1977), Plate 44, 13mm right of midline.

299

300 **B:** Microelectrode recordings from sites indicated in panel A. Recording locations above target
301 are a: 6.59mm; b: 3.86mm. The lower traces are raw recordings. The upper traces have been
302 rectified and integrated. The vertical dashed line indicates the approximate time of onset of
303 shoulder protraction.

304

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305 **Figure 2:** Individual neurons increase their firing rate following movement onset.
306 Microelectrode recording at 6.59mm above target on the right side, showing the raw
307 extracellular microelectrode recording (bottom, black trace), and 3 discriminated neurons
308 (blue, green, and red). Spikes were identified (insets) and analysed for a period of 3s before and
309 3s after onset of shoulder protraction. The instantaneous spike frequency relative to the
310 previous spike is plotted above each sorted spike. The shaded area to the right of the figure
311 represents the period following onset of left shoulder protraction.

312

313 **Figure 3:** Neurons over a length > 5mm increased their firing rates following movement onset.
314 Total number of spikes before (3s) and after (3s) onset of shoulder protraction in 9 neurons at 5
315 microelectrode sites. The spike count was significantly greater after movement onset,
316 ($p=0.0001$).

317





