Functional lesional neurosurgery for tremor: back to the future?

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Abstract

For nearly a century, functional neurosurgery has been applied in the treatment of tremor. While deep brain stimulation has been in the focus of academic interest in recent years, the establishment of incision-less technology, such as MRI-guided high-intensity focused ultrasound, has again stirred interest in lesional approaches.

In this article, we will discuss the historical development of surgical technique and targets, as well as the technological state-of-the-art of conventional and incision-less interventions for tremor due to Parkinson’s disease, essential and dystonic tremor, and tremor related to multiple sclerosis and midbrain lesions. We will also summarize technique-inherent advantages of each technology and compare their lesion characteristics. From this we identify gaps in the current literature and derive future directions for functional lesional neurosurgery, in particularly potential trial designs, alternative targets and the unsolved problem of bilateral lesional treatment. The results of a systematic review and meta-analysis of the consistency, efficacy and side-effect rate of lesional treatments for tremor are presented separately alongside this article.
Introduction

Tremor is defined as an involuntary, oscillating sinusoidal movement of a body part. Its semiology is defined by the limb posture, during which it becomes apparent, frequency and body distribution. While tremor phenomenology of the most frequent aetiologies namely Essential Tremor (ET) and Parkinson’s disease (PD) differ, they do share aspects of the underlying pathophysiology[1,2]. Dystonic tremor has been increasingly appreciated as a frequent entity[3], while ischaemic, traumatic or inflammatory lesions to midbrain or cerebellar structures are alternative frequent causes of tremor[4,5]. Although tremor represents the most frequent movement disorder, its treatment remains challenging and oral medication have proven to be only partially successful[6,7]. Until the advent of levodopa therapy in the mid 1960ies, lesional neurosurgery was the mainstay of symptomatic treatment for PD related tremor. It was the great success of levodopa and later of deep brain stimulation (DBS) that has led to a gradual decline in academic interest in lesional approaches over the following decades, while their efficacy remain appreciated[8]. However, recent technological advances in the development of incision-less technology and especially MRI-guided, high-intensity, focused ultrasound (MRIgFUS) has led to a revived interest in lesional procedures for tremor[9]. This article aims to summarize the historical development of lesional functional neurosurgery in the treatment of tremor disorders both with regards to targets and surgical technique. It also addresses and compares the surgical technique of radiofrequency (RF) ablation, Gamma Knife (GK) and MRIgFUS as well as the lesions characteristics created through them. Furthermore, we aim to address some of the emerging challenges to translate promising incision-less technology into treatment practice.

Nomenclature

Over time different thalamic nomenclature systems have been used and cited for the same structures[10]. Due to the limited applicability of retrograde tracer studies to human tissue it has been impossible to unanimously reconcile the anatomical, primate physiology and human neurosurgical nomenclature, which often creates confusion and particularly
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complicates the neurophysiological interpretation of surgical data. Hassler’s nomenclature is still the most frequently used terminology in functional neurosurgery and is based on thalamic cytoarchitecture (see Figure 1; camera lucida drawing adapted from[11]). Newer systems have tried to incorporate the findings in primates and to allow easier comparison between studies. In the following, Hassler’s ventral intermediate nucleus (V.im.) is used analogous to Walker’s VIM and the more recent concept of the ventral lateral posterior nucleus (VLp) by Jones. Hassler’s ventralis oralis anterior nucleus (V.o.a.) corresponds to Jones’ ventral lateral anterior nucleus (VLa), while the ventralis oralis posterior nucleus (V.o.p.) is considered a transition zone between VLa and VLp [10].

Subthalamic structures, i.e. the area directly caudal to the ventral thalamic nuclei, are referred to as the posterior subthalamic area (PSA). It is formed of the white matter tracts of the radiatio prelemniscalis (Ra.prl), which includes the cerebellothalamic tract (CTT) and the nucleus of the caudal zona incerta (cZI). The ansa lenticularis and the fasciculus lenticularis compose the pallidothalamic tract which is located in Forel’s field H2 and which enters the thalamus as the fasciculus thalamicus in H1 (see Figure 2; 3D-rendering from sagittal camera lucida drawings according to[12] using Free-D software[13]; see the corresponding 3D-version as an enhanced pdf in the supplement).

**History and development of Targets**

The origin of functional neurosurgery for movement disorders dates back to the beginning of the 20th century, when lesions aiming at parts of the corticospinal system were used to alleviate motor symptoms. The procedures included initial attempts at spinal rhizotomies at the nerve root level, anterolateral cordotomies at the spinal level[14] and with time extended to pyramidotomies[15], pedunculodotomies[16], mesencephalic tractotomies[17] and even motor cortex excisions[18]. Although authors acknowledged the drastic expense of spastic paresis due to lesion of the first motor neuron, academics at the time followed eminent Paul Bucy’s dogmatic notion that the abolishment of tremor was “impossible without the interruption of the pyramidal system”[19]. It is now recognized that the establishment of the concept of the “extrapyramidal” motor system originates from Spatz’ article from 1927[20], which laid the foundation for the treatment of motor symptoms without causing pyramidal weakness.

Initial basal ganglia attempts
Meyers performed the first trans-ventricular caudate nucleus resection for post-encephalatic tremor in 1939 and ventured further including the anterior limb of the internal capsule, ansa lenticularis and the pallidum in the following years[21]. This for the first time allowed basal ganglia resections without damaging pyramidal structures, suppressing tremor without causing paresis. At 2 years follow-up, he reported 62% successful tremor suppression[22]. A more refined way of targeting the ansa lenticularis using electrocoagulation was deployed by Fenelon[23]. Although the first means to localize human brain structures had been published just before the turn of the century[24], the first stereotactic procedure on a patient with Huntington’s chorea was performed by Spiegel and Wycis only in 1947[25]. The first stereotactic pallidotomy followed shortly thereafter, introducing this technique to the treatment of movement disorders[26]. The first cases of electrocoagulation of the ansa lenticularis reported a 78% improvement of PD tremor[27]. In parallel, Cooper by accident observed the amelioration of tremor and rigidity in a post-encephalic PD patient by damaging and ligating the anterior choroidal artery during an attempted pedunculotomy[28]. Meanwhile Guiot and Brion already presented the results of the lesion of the pars interna of the Globus pallidum (GPi) in a series of 27 patients, resulting in an improvement in tremor and other motor symptoms in 42.5% of the cases[29]. In due course chemopallidotomy, consisting of the installation of alcohol directed at the GP through a transtemporal burr hole and catheter – at that time a free-hand procedure under pneumoencephalography control, was developed[30]. Similarly and independently, Narabayashi and colleagues performed the first pallidotomy procedures in Japan using a mixture of procaine and wax[31]. Cooper’s chemopallidectomies, although resulting in lesions of considerable variability in size and location on post-mortem analysis, were reported to improve tremor in 75% of cases[32]. In parallel to chemopallidotomy, various groups around the globe were developing and refining stereotactic apparatuses to improve the navigation of electrocoagulation devices[33]. Already at that time a functional sub-compartmentalization of the GP started to became apparent: in the conclusion of a series of 100 “pallido-ansotomies” placed in the region of the ansa lenticularis/medial GP, a target 3-6mm behind the anterior commissure appeared to be most effective in treating rigidity and tremor[34] or even 9mm behind the anterior commissure in cases of severe tremor[33]. Although overshadowed by the success of thalamotomy on tremor treatment and largely ignored at the time, the seminal work of Svennilson and Leksell showed that interventions in the posteroventral GPi resulted in a much more consistent benefit on tremor than anterior placed lesions[35]. Only in retrospect, data on Leksell’s success of his continued focus on the posteroventral pallidum (PVP) was recognized[36]. Some authors identified larger lesion size, a baseline of mental retardation, and advanced disease as risk factors for cognitive side effects of bilateral procedures, while Gillingham was the first to stress the importance of precise placement of the lesion over gross lesion size as a predictor
of safety and efficacy[37].

Ultimately, radiofrequency lesioning with temperature control became the method to replace all other technology.

Early Thalamic Experience

Guided by his research on the thalamus, Hassler came to the conclusion that targeting both the pallidothalamic and dentatothalamic system would be most useful in treating tremor[38], choosing the V.o.p. as an appropriate target. Subsequently, Mundinger and Riechert performed the first motor thalamotomy in 1952 in a 38-year old man with postencephalitic PD and severe tremor with great success[39], opening a decade of thalamotomies in the treatment for PD[40] and other hyperkinetic disorders[41]. It was only several years later, however, that the V.im. was identified as the optimal target for tremor, and that the pallidum was almost completely abandoned as a target. This has been corroborated in large series[42] and the GPi has not been targeted for sole tremor amelioration since.

Early Subthalamic literature

When reviewing subthalamic approaches one needs to differentiate between lesions to fibre tracts in the PSA, to the cZI and to the STN itself. Already in 1953 the first cases of electrocoagulation of the ansa lenticularis were published in an attempt to decrease the lesion size necessary to reduce tremor[43]. To avoid damage to the internal capsule and anterior choroidal artery the campotomy procedure was developed by placing the lesion at the junction of the ansa and fasciculus lenticularis in Forel’s field H with a significant reduction in tremor (88%) and rigidity (68%) in PD patients[44]. A series of 100 electrode insertions in 58 tremor-dominant PD patients showed the highest efficacy in tremor reduction for a lesion placed in the PSA[45]. Mundinger played an influential role to establish the cZI as a target and documented this in a large study, reporting a 68-75% rate of hand tremor suppression after cZI lesions in 456 patients[46]. This was further detailed by results from a mixed tremor cohort, in which the most effective target location
was shown to be the most posterior and inferior portion of the cZI, containing the Ra.prl[47]. From a similar series it was concluded that lesion placement in the PSA allowed for a smaller lesion size (40-60mm³) with greater efficacy on tremor and better safety than larger thalamic lesions[48]. However, with the advent of levodopa-based medical therapies from the late 1960s[49], interest in invasive surgical treatment dropped precipitously for decades.

Methodological shortcomings of the early literature

In this pre-CT/MRI era, pneumencephalography and later ventriculography were used for targeting, and post-mortem analysis was the only reliable tool to confirm targeting precision, which occasionally revealed significant misplacements[32]. When assessing clinical outcome in the first decades of functional neurosurgery for movement disorders, one always needs to bear in mind the systematic shortcomings of the early literature with regards to 1) clinical diagnosis, 2) target selection, 3) lack of physiological target identification, inhomogeneous 4) lesioning technique, 5) targeting precision and 6) lesioning size, as well as 7) non-standardized identification of 8) immediate and long-term benefits and 9) side-effects by non-impartial investigators [50]. We therefore agree we Guridi et al. that multiple limitations of the early lesional literature hamper a meaningful systematic interpretation of results[50].

1990ies revival of lesional approaches

There were only few lesional tremor studies aiming at the thalamus published during the 1980s[51,52], although thalamotomies were continued to be performed in specialized centres worldwide. It was not until the early 1990ies that lesional approaches re-emerged, primarily due to the recognition of levodopa-induced dyskinesia (LID) as sequelae of long-term oral levodopa treatment in PD and the rediscovery of alternative targets. At the same time, the increased insight into basal ganglia pathophysiology gained through the MPTP monkey model provided a much more detailed rationale for lesional interventions[53]. Postero-ventral pallidotomy (PVP) was reintroduced for treatment of PD after nearly 30 years of dormancy – and while this procedure drastically decreased LID, it also improved tremor[36]. With the advancing understanding of the basal ganglia circuitry by studies of the MPTP primate model in the late 1980ies[54], targeting the over-active subthalamic nucleus (STN) and in particular its dorsolateral sensorimotor region,
emerged as a novel target strategy which was particularly attractive for deep brain stimulation (DBS). It had been well known already at that time, that in healthy individuals a lesion to the STN invariably causes hemiballism. In PD, however, it was shown that the threshold for surgery-induced dyskinesia is increased due to altered striato-pallidal activity patterns following the hypo-dopaminergic state[55]. After promising primate lesional [56] and human DBS studies[57], a string of small studies also showed a beneficial effect with unilateral[58-62] and bilateral lesions of the dorsolateral portion of the STN on PD motor features including tremor[55,63]. Although staged bilateral procedures were described not to cause severe dyskinesia and ataxia[63], simultaneous bilateral lesions did[55]. Similarly, lesional procedures were tested again for tremor beyond PD as treatment success with oral medication remained limited. Increasingly MS and rubral tremor were studied once more both with DBS and lesioning. Since the late 1980ies, clinical data from well designed trials shifted the academic focus onto DBS[64] and with the progressive improvement of technology, stimulation replaced lesional protocols in the academic setting. Only very recently there has been again increasing interest in lesional approaches, as promising results from prospective trials with incision-less GK and MRIgFUS thalamotomy in ET were published[65-69].

**Technology**

The following paragraphs summarize the currently available techniques for lesional treatments – Table 1 displays their inherent conceptual advantages and disadvantages.

**Radiofrequency ablation**

As described above, many of the conventional techniques for tissue lesioning, such as chemolysis, procain wax infusion or cutting using a stylette, were developed and then replaced by more advanced methods over time. RF ablation influenced lesional functional neurosurgery more than any other method and is still widely used around the globe today[70]. In principal, a radiofrequency electrode is introduced under stereotactic guidance via a burr hole to the target chosen to create a monopolar electrocoagulation lesion and among stereotactic neurosurgeons the original publication still serves as a guidance to the technical basis of the procedure[71]. Impedance measurements guide the surgeon as to whether the exposed tip of the electrode resides in grey or white matter. Microelectrode recording and macrostimulation
are frequently used to improve probe placement, although not deemed essential by some authors[72]. After target verification, temperature and time are set according to the target (thalamotomy 70°C applied for max. 60 sec.; pallidotomy 75-80°C applied for max. 60sec.) and energy is applied. To avoid potentially dangerous tissue bubble formation, the current is ramped up slowly during the latter[71]. The incidence of asymptomatic haemorrhage with RF ablation is reported as high as 29%[73].
Table 1: Conceptual and practical differences between state-of-the-art lesional functional neurosurgery technique

<table>
<thead>
<tr>
<th></th>
<th><strong>Radiofrequency Ablation</strong></th>
<th><strong>Gamma Knife radiosurgery</strong></th>
<th><strong>MRI-guided high intensity focused ultrasound</strong></th>
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</thead>
<tbody>
<tr>
<td></td>
<td>advantages</td>
<td>disadvantages</td>
<td>advantages</td>
</tr>
<tr>
<td><strong>Preparation</strong></td>
<td>shaving directly around burr hole only</td>
<td>stereotactic frame needed</td>
<td>no head shaving</td>
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<td></td>
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<td>no head shaving</td>
<td>stereotactic frame needed</td>
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<td>stereotypes frame needed</td>
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<td></td>
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<td></td>
<td>head shaving compulsory</td>
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<tr>
<td><strong>Target verification and adjustment</strong></td>
<td>possibility for electrophysiological target verification and adjustment (microrecording or macrostimulation)</td>
<td>bleeding risk increases with multiple recording trajectories</td>
<td>no electrophysiological target verification</td>
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<tr>
<td></td>
<td></td>
<td></td>
<td>no means for target adjustments due to delayed tissue response</td>
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<td></td>
<td>target adjustable during iterative sonications based on clinical or real-time imaging feedback</td>
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<td></td>
<td></td>
<td></td>
<td>no electro-physiological target verification</td>
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<tr>
<td><strong>Intervention</strong></td>
<td>approximate intervention duration</td>
<td>burr hole needed potential brain shift, infection and bleeding risk</td>
<td>incisionless real-time control of target voxel position and temperature via MR-imaging</td>
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<tr>
<td></td>
<td>60-120min</td>
<td>trajectories traversing healthy tissue</td>
<td>iterative confirmation of final sonication settings</td>
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<td></td>
<td>prolonged placement in supine position</td>
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<td>vertigo/nausea in some patients during sonication in supine position</td>
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<td></td>
<td></td>
<td></td>
<td>approximate intervention duration</td>
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<tr>
<td></td>
<td></td>
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<td>180-300 min (own data)</td>
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*a* intervention duration: from local anaesthesia to frame removal
INCISIONLESS TECHNIQUES

Conventional stereotactic procedures including DBS depend on the introduction of an instrument along a calculated trajectory and through surrounding tissue. The invariable opening of the skull via a burr hole introduces the risk to infection and brain shift with possible subsequent targeting inaccuracy. The surgical trajectory needs adequate planning to avoid damage to structures in its course. Non-invasive techniques aim at circumventing all of the above.

Gamma knife

During radiosurgery focused radiation energy is translated into tissue necrosis in the focus without damaging adjacent tissue. Since its first application in 1968[74], Gamma Knife (GK) has been continuously refined and amended to functional neurosurgery, while the bulk of its clinical application remains in the treatment of vascular malformation and tumours[75]. Over time, investigators reduced the radiation energy to create lesions from initially 180-200Gy to 130-140Gy, and it is now accepted that 120Gy is the minimum dose needed to evoke definite tissue changes. White matter fibre tracts however are far more susceptible to radiation energy and there is general agreement that doses to the internal capsule should not exceed 20-25Gy – therefore, PVP is not performed with GK due to the proximity of the target to the highly radiosensitive optic tract. The procedure does not allow for direct, i.e. electrophysiological, nor indirect, i.e. imaging-based target and lesion verification during the intervention. It is therefore key to limit the geometrical distortion on MRI-based pre-interventional planning during procedure planning[75]. The delayed onset of a clinical effect after treatment – to be expected 3 to 6 months after the intervention[76-78] – and the inability to monitor the target tissue during the intervention, are inherent conceptual disadvantages.

MRI-guided high-intensity focused ultrasound (MRIGFUS)

The first attempt to create lesions in the pallidal network using a single ultrasound source dates back to 1958. With the advance of technology, high-intensity focused ultrasound ablation was introduced again during the 1980ies and initially developed for gynaecological and urological interventions. The first study using the commercially available InSightec
Neuro platform reported the safe application of MRIgFUS to create thalamic lesions for neuropathic pain[79]. During the MRIgFUS intervention, the awake patient wearing the helmet-shaped ultrasound transducer is positioned in a 3T-MRI, which allows target verification and temperature control within the target voxel via MR thermometry sequences in real-time. The application of sonic energy (called “sonication”) for 10-20 seconds is followed by pauses for cooling and clinical assessment. Sonication energy is then increased in a step-wise manner until reaching temperature changes resulting in tissue effects[79]. Once this temperature threshold is reached (ca. 60°C for V.im.) there is immediate anatomical and clinical effect[67,68,79], which are the most important advantages of this technology over radiosurgery.

In 2013 two open-label, prospective interventional studies assessed the effect of non-invasive V.im. lesioning on tremor[67,68]. The promising results have since been replicated both for the V.im. as well as the CTT in the PSA[65,80]. A large skull volume and low skull density ratio are technology-related treatment limitations[81]. So far, only a single haemorrhage[79] has been reported after 130 published MRIgFUS tremor interventions.

**Lesion comparison**

Empirically, volumetric quantification of stereotactic lesions differentiates three concentric parts, representing the inner and middle zone (necrosis) and outer zone (oedema)[82]. The method and size of lesions reported in the literature is variable: for example, RF thalamic (V.im.)[83] and subthalamic lesions[48] have been reported between 40-60 mm³, lesions to the cZI have been reported at 18mm³ in size after 11 years of follow-up[84] and lesions to the GPi 65.5 mm³ at 4 months[85] and 40mm³ after 4-6 months follow-up[86]. Leucotome thalamic lesions have been reported around 400-500 mm³ size without reporting side-effects[87]. Given the inconsistencies in the neurosurgical literature with regards to the exact technique and time-point of volume quantification, the interpretation of these drastically different lesion sizes between studies is difficult if not impossible. Two studies that assessed the relationship between lesion size and clinical effect reported no correlation between the two for both pallidotomy and thalamotomy[88,89].

The only study directly comparing the *in vivo* effect of RF (72°C x 60 seconds), MRIgFUS (maximum temperature 55-60°C) and GK (130-160 Gy) on porcine thalamic tissue reported similar MR and histological tissue changes for RF and MRIgFUS with formation of peak lesion volumes within 72 hours after the intervention and subsequent formation of well-demarcated reactive gliosis[90]. These lesions then shrink over time most likely due to scarring and in humans reach a plateau around 6 months after the RF[91] and 3 months after the MRIgFUS interventions[65,92,93].
GK lesions differ in both the temporal as well as volumetric and histological evolution, as they are more diffuse, evolve over months[94,95] and induce diffuse macrophage infiltration to adjacent anatomical structures[90]. Volumetric quantification in humans indicates a peak lesion size at 6-9 months after GK lesioning[94,96]. Microelectrode-recordings from a limited number of patients suggest that the T2-hypointense core region represents the directly irradiated zone, while the surrounding irregular T2-hyperintense region is not functionally damaged[77]. Tissue reaction can vary and delayed effects months after the actual treatment have been repeatedly reported, resulting in drastically different lesion sizes between 188 – 871mm\(^3\)[97] with exceptional cases as large as 2030mm\(^3\) after 36months[98] or >6000mm\(^3\) after 18months[95] (see Figure 3). After GK V. thalamotomy cases without side effects showed smaller lesion sizes of 188 ± 224mm\(^3\) (n=157 procedures) than cases with side effects: 871±742mm\(^3\)[97]. Delayed adverse effects of GK lesioning due to unexpected large lesions has been reported in 7.7% [99], respectively 6.9% of cases[97]. Corticosteroids have no documented effect for these effects, which are mostly described as self-limiting over 12-18months[97]. Serious adverse events can develop after interventions with doses from 140Gy onwards[100]. It is argued that this is due to individual radio-sensitivity, which still cannot be predicted on an individual basis[66].

**Consistency, clinical efficacy and side-effect rate**

The clinical effect of different lesional interventions for tremor has never been formally and comprehensively assessed and compared between targets and indications. So far the literature has been summarized in a narrative way only, calling for an unbiased analysis of the existing literature.

To this end, we have undertaken a systematic review and meta-analysis according to a published, peer-reviewed protocol[101] in accordance to the recommendations from the Preferred Reporting Items for Systematic Review and Meta-Analysis Protocols (PRISMA-P) 2015 statement. This systematic review protocol has been registered in the International Prospective Register of Systematic reviews (PROSPERO) on September 20\(^{th}\) 2016 (CRD42016048049). The resulting meta-analysis covers published, peer-reviewed literature from 1990 to 2017 of lesional tremor treatments (reference to Schreglmann et al. systematic review and meta-analysis manuscript handled by same editor, currently under parallel revision with the journal). It systematically summarizes consistency, efficacy and side-effect rate of lesional interventions according to tremor aetiology, lesion target and lesion technique in detail, which therefore are not
discussed in this work.

**Future Directions**

The recent introduction of MRigFUS technology with its potential advantages has stirred considerable interest in the movement disorder field and it is conceivable that this might lead to a partial renaissance of lesional functional neurosurgery for tremor and possibly other disorders. The need for prospective, blinded, controlled trials has been acknowledged by leading figures in the field[9,102] and the first blind-assessed, prospective studies have been published[69,93]. This however can only be the beginning of the establishment of a solid evidence base to explore the potential of this very promising technology. With the number of operational MRigFUS centres (2017: 30 centers, 800 treatments; personal communication InSightec) increasing worldwide we are hopeful that very soon additional trial data is published, as it would be premature to judge the available data on safety, consistency and efficacy substantial enough to draw final conclusions. In addition to clinical safety and efficacy, intervention cost is another important factor for the wide-spread implementation of a novel neurosurgical technique. The fact that incisionless approaches do not rely on implantable hardware needing replacement at some point in the future, as well as a less intensive aftercare needed, could in the long run counterbalance the still high cost to acquire treatment devices. First data comparing DBS, GK and MRigFUS showed significantly lower projected costs for both incisionless techniques compared to DBS[103].

We hope that the current excitement in the wake of the early FDA approval will boost its` continued scientific investigation and does not lead to indiscriminate use before credible evidence of substantial size has accumulated – ideally, therefore all patients undergoing MRigFUS treatment should be enrolled in trials and treatment registers.

**Trial Design**

The majority of published lesional functional neurosurgery studies for tremor carry methodological limitations with regards to prospective trial design, independent, validated symptom quantification, adequate follow-up and description of tremor recurrence and side-effects. It is imperative to deliver prospective trials with standardized, video-documented outcome evaluation by independent and blinded movement disorder neurologists using validated evaluation instruments. Similarly, side-effects should be documented in a standardized way.
The direct comparison of open neurosurgery with non-invasive MRIgFUS or GK poses methodological problems as a) double-blind assessments are difficult due to instrumentation, which cannot be concealed from the patient and b) as bilateral procedures are standard for DBS but still considered to carry a higher risk for lesional approaches. Several strategies could help circumventing such obstacles, including a) stringent single-blinded assessments aiming at compensating for the fact that a reasonable blinding of patients with regards to the method of intervention is simply impossible[104], b) delayed start of stimulation contralateral to the studied side after bilateral DBS implantation minimizing stimulation artefacts on the studied side without the need for a second operation (provided the micro-lesioning effect after electrode implantation is taken into account[105]), c) considering and addressing important and potentially confounding placebo, nocebo and lessebo effects by adequate trial design[106]. Finally, changes in quality of life and level of functioning should be reported as a standard and should be included as primary outcome variables in future tremor trials.

Bilateral treatment

Probably the biggest constraint with lesional surgery in the past and foreseeable future is bilateral treatment, since irrespective of the target, bilateral lesion surgery dramatically increases the risk to cause dysarthria and dysphagia[72,107-110]. The exact mechanism for this is still unclear. While it is assumed that lesion spread to corticobulbar fibres constitutes a major factor, a disturbance of the cortico-basal ganglia-thalamo-cortical loop is believed by some to play a role as well. Our meta-analysis (reference to Schreglmann et al. systematic review and meta-analysis manuscript handled by same editor, currently under parallel revision with the journal) for the first time allows to quantify the degree to which this risk increases according to target, tremor aetiology and lesional technique used. While experience from the past precludes investigators from further bilateral treatment attempts with RF ablation or GK radiosurgery, MRIgFUS would potentially allow for more precise targeting and/or titrating the final lesion by a multistep procedure to avoid interference with corticobulbar fibres. In this regard the possibility of staged bilateral interventions, as successfully pioneered by Young in 42 patients treated with RF at the V.im. without a single complication[97], is currently explored by various groups - a first uncontrolled, retrospective study reports this possibility for MRIgFUS in ET[80]. In addition to technique and aetiology, finding the optimal anatomical target is of additional importance. Irrespective of the prior, prospective studies of bilateral interventions should include speech and swallowing, as well as gait assessments to monitor the incidence and quantify the severity of these potential side effects.
Reappraisal of the Posterior Subthalamic Area

As one of the historically established tremor targets, the PSA was entertained by neurosurgeons who thought the higher density of fibres connecting the cerebellar output nuclei and the V.im. thalamic nucleus as well as its’ larger anatomical distance to vulnerable structures within the vicinity, i.e. sensory thalamic nuclei and internal capsule, to be of conceptual advantage – reviewed in[111]. It has recently been trialled again using MRIgFUS with a favourable effect and side effect profile[80,93]. In particular the very low rate of persistent side effects without paraesthesia could serve as first support to the conceptual advantages mentioned. In addition, collective evidence from DBS studies also indicates that the best stimulation effect on tremor is achieved in the white matter tracts of the PSA directly caudal to the Vim rather than the Vim itself[111-116]. Although this of course has to be confirmed in larger samples and compared with other targets, it serves as an example that state of the art technology can be used to reappraise established but out-of-fashion targets in order to optimize treatment options.

Conclusion

Theoretical advantages and promising clinical data on safety and efficacy of incision-less procedures currently build up momentum to reappraise lesional interventions as treatment strategies for tremor disorders once more. Given the still small number of published cases, the evidence base for incision-less lesional treatment however has to be substantiated. The exciting technical possibilities especially of MRIgFUS should be geared not only to close various gaps in the existing literature highlighted in this review but also to further advance our knowledge base for treatment decisions. Together with our meta-analysis on lesional tremor treatments (reference to Schreglmann et al. systematic review and meta-analysis manuscript handled by same editor, currently under parallel revision with the journal), this work summarizes the current state of the art in lesional functional neurosurgery for tremor disorders. It also highlights the need for adequately designed prospective trials to support the existing data on safety and efficacy not only for established targets such as the V.im. nucleus, but also for rediscovered targets within the PSA. Ultimately, only carefully designed head-to-head comparison trials will be able to answer the question if incision-less lesional approaches without the need for open surgery and device implantation, such as with MRIgFUS, are comparable to established DBS surgery.
Figure captions:

Figure 1: Human thalamus in the axial/horizontal plane, depicting the four main ventral thalamic sub-nuclei according to Hassler (in brackets (according to Hirai and Jones in double brackets)) from anterior to posterior: lateropolaris / ventral anterior nucleus (L.po. (V A)), ventrooralis anterior and posterior / ventralis lateralis anterior (V.o.a. & V.o.p. (VLa)), ventrointermedius (V.im. (VIM)), and ventrocaudalis / ventralis posteriormedialis & ventralis posterolateralis (V.c (VPM & VPL). Adjacent structures include the nucleus centralis thalami (Ce (CM)), nucleus medialis dorsalis (M (MD)), nucleus intralamellaris (iLa (CL)), as well as the mamillo-thalamic tract (MTT), reticulatum thalami (Rt (R)) and internal capsule; camera lucida drawing adapted from[11].

Figure 2: Anatomy of sub-/thalamic basal ganglia and adjacent structures relevant in lesional functional stereotactic neurosurgery for tremor: Visualization of the posterior subthalamic area (PSA) containing the Zona incerta (ZI) and the prelemniscal radiation (Ra.prl), containing both cerebellothalamic (CTT) and pallidothalamic tract (PTT). The PSA is limited rostrally by the ventral thalamus and its ventro-intermedial nucleus (V.im.), medio-caudally by the Nucleus ruber (Ncl.r.), caudo-laterally by the Substantia nigra (SNr/c) and caudo-ventrally by the subthalamic nucleus (STN). 3D-rendering from sagittal camera lucida drawings according to[12] using Free-D software[13]. Scale-cube side-length: 2 mm. The enhanced PDF of this figure in the supplemental materials allows manipulation of the 3D-rendering for improved anatomical display (open PDF with Acrobat Reader).

Figure 3: Comparison of effects between state-of-the-art lesional functional neurosurgery techniques (radiofrequency, Gamma Knife radiosurgery and MRI-guided high intensity focused ultrasound ablations) on the evolution of lesion size, MR-imaging and histological characteristics over time. Dense line drawing depicting lesion volume over time with dotted line depicting variable development. Scale refers to percentage of intended lesion volume size.

Supplementary Figure 1: 3D-Version of Figure 2 allowing manipulation for improved anatomical display. File needs to be opened with Acrobat Reader for full functionality.

Contributors: SRS initiated the project, generated the figures and wrote the manuscript draft. JKK wrote several
manuscript chapters and critically reviewed the manuscript. JWC critically revised several manuscript chapters and reviewed the manuscript. SHL, BW and EM critically reviewed the manuscript. KPB provided input on manuscript structure and critically reviewed the manuscript. GK initiated and supervised the project and critically reviewed the manuscript. All authors agreed on the final manuscript draft.

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